# MRI Systems I: B0 and Bulk Magnetization

#### M219 - Principles and Applications of MRI Kyung Sung, Ph.D. 1/11/2022

## Course Overview

- Course website
	- https://mrrl.ucla.edu/pages/m219
- 2023 course schedule
	- https://mrrl.ucla.edu/pages/m219 2023
- Assignments
	- Homework #1 will be out on 1/16 (due on 1/30)
- Office hours, Fridays 10-12pm
	- In-person (Ueberroth, 1417B)
	- Zoom is also available

## What is MRI?

- Magnetic
	- We need a big magnet
- Resonance
	- Excitation energy has to be on-resonance
- Imaging
	- We can make pretty pictures

#### What is MRI?

MRI follows a classic excitation-reception paradigm.





Faraday's Law of Induction

MRI encodes spatial information and image contrast in the echo.

#### Requirements for MRI

- NMR Active Nuclei
	- $-$  e.g. <sup>1</sup>H in H<sub>2</sub>0
- Magnetic Field (B<sub>0</sub>): Polarizer
- RF System (B<sub>1</sub>): Exciter
- Coil: Receiver
- Gradients  $(G_X, G_Y, G_Z)$ : Spatial Encoding

#### MRI Hardware

**Cryostat**

**Z-grad**

**X-grad**

**Y-grad**

**Body Tx/Rx Coil (B1)**

Main Coil (B<sub>0</sub>)

Image Adapted From: http://www.ee.duke.edu/~jshorey

Nuclear Spin

## Classical View



- Nuclei with an odd mass number have *half-integral spin*
	- Spin-1/2 1H, 13C, 15N, 19F, 31P
	- $-$  Spin-3/2  $-$  <sup>23</sup>Na
- Nuclei with an even mass number and an even charge number have *zero spin*
	- $-$  12C and 16O





## Spin Angular Momentum

Spin + Mass  $\spmb{\mathfrak{m}}$  Spin Angular Momentum  $\spmb{\mathfrak{m}}$   $\vec{S}$  [kg·m<sup>2</sup>s<sup>-1</sup>]

⇥ *r* **m** *S* ⇥ ⇥ *v*







## Spin Angular Momentum

Spin + Mass  $\spmb{\mathfrak{m}}$  Spin Angular Momentum  $\spmb{\mathfrak{m}}$   $\vec{S}$  [kg·m<sup>2</sup>s<sup>-1</sup>]







David Geffen



## Magnetic Dipole Moments

Spin + Charge ➠ Magnetic Moment ➠  $\vec{\mu}$  [J•T<sup>-1</sup> *or* kg•m<sup>2</sup>/s<sup>2</sup>/T]

"a measure of the strength of the system's net magnetic source" --http://en.wikipedia.org/wiki/Magnetic\_moment



Hydrogen nuclei have magnetic dipole moments.





## Gyromagnetic Ratio

- Gyromagnetic Ratio
	- Physical constant
	- Unique for each NMR active nuclei
	- Ratio of the magnetic moment to the angular momentum

$$
\overrightarrow{\mu} = \gamma \overrightarrow{S} = \gamma \hbar \overrightarrow{I}
$$

- Governs the frequency of *precession*
- Gamma vs. Gamma-bar

$$
\gamma = \gamma/2\pi
$$





## NMR Active Nuclei



The *relative* sensitivity is at constant magnetic field and equal number of nuclei.

– Using a factor of  $\,\,\gamma^{\,\overline{4}}\,I\,(I+1)\,$  ; 1H is the reference standard. 11  $\overline{4}$   $I$   $(I+1)$ 

The *absolute* sensitivity is the relative sensitivity multiplied by natural abundance.



P. Callaghan & http://www.cryst.bbk.ac.uk/PPS2/projects/schirra/html/nuclei.htm





### Currents & Magnetic Fields



#### **Electromagnet – A current in a wire generates a magnetic field.**

http://www.magnet.fsu.edu/education/tutorials/magnetacademy/

## Superconducting Electromagnet



#### **MRI scanners are superconducting electromagnets.**

#### **B<sub>0</sub>** Field

- $\cdot$  B<sub>0</sub> field is:
	- Spatially uniform (over a volume of interest)
		- ~50cm @ isocenter
	- Temporally stable
		- $B_0(t)=B_0(t=0)e^{-(R/L)/t}$
		- Decays <1ppm/hour
	- $-$  Oriented along the z-axis (  $\vec{k}$ )
		- Long axis of the scanner.

$$
\vec{B}_0 = B_0 \vec{k}
$$

## Main Field (B<sub>0</sub>) – Strength

- Earth's magnetic field – 0.5 Gauss
- Refrigerator magnet – 10-100 Gauss
- $\cdot$  B<sub>0</sub> Field
	- $-0.5T = 5000$  Gauss
	- $-1.5T = 15000$  Gauss
	- 3.0T = 30000 Gauss



## B0 Strength - Advantages

- **↑**  $B_0 \Longrightarrow$  **↑** Polarization ( $|\vec{M}|$ ) = **↑** SNR
	- $-$  **1** Polarization, therefore more  $\vec{M}$  for imaging.
	- SNR  $\propto$  B<sub>0</sub><sup>7/4</sup> (**↑**Polarization + **↑Larmor Frequency**)
		- **1** Spatial resolution
		- **1** Temporal resolution
		- $\blacklozenge$  Scan time

## B0 Strength - Disadvantages

- $\bullet$  B<sub>0</sub>  $\Rightarrow$   $\bullet$  Specific Absorption Ratio (SAR)
	- Energy absorbed by body [W/kg]
	- $-$  SAR∝B<sub>0</sub><sup>2</sup>
- $\bullet$  B<sub>0</sub>  $\Longrightarrow$   $\bullet$  Cost
	- ~\$1,000,000 per Tesla
	- More shielding

Higher B<sub>0</sub> leads to higher SAR for patients and higher costs.

## B0 Strength - Disadvantages

- **↑ B**<sub>0</sub>  $\Rightarrow$  **↑** Chemical shift ( $\Delta f$ )
	- 䢖 ∆f between fat and water
		- Fat and water have different Larmor frequencies
			- $\sim$ 220Hz different at 1.5T
			- ~440Hz different at 3.0T
		- Fat is *more* spatially mis-registered @ 3T
	- Good for spectroscopy...



Chemical Shift – Fat (–CH2) is ~220Hz *lower* at 1.5T

## Main Field (B<sub>0</sub>) – Shielding

- **Problem**: The B<sub>0</sub> field extends well beyond the scanner.
- **Shielding** reduces B<sub>0</sub> foot print
	- Reduces install cost
	- Reduces interference

#### **• Passive Shielding**

- Iron room shielding
- Heavy, not cheap
- **• Active Shielding** 
	- Super-conducting coils that oppose (shield)  $B_0$  fringe field
- "**Five Gauss Line**"
	- Threshold beyond which ferromagnetic objects are strictly prohibited
	- 5G=0.5mT



ACR Guidance Document on MR Safe Practices: 2013; *JMRI* 37:501–530 (2013)

## RF Shielding

- RF fields are close to FM radio
	- $-$  1H @ 1.5T  $\Rightarrow$  63.85 MHz
	- $1H$  @ 3.0T ⇒ 127.71 MHz
	- KROQ  $\Rightarrow$  106.7 MHz
- Need to shield local sources from interfering
- Copper room shielding required



#### MRI Zones



ACR Guidance Document on MR Safe Practices: 2013; *JMRI* 37:501–530 (2013)

# B0 Hardware Anatomy

## Superconducting Electromagnets

- MRI scanners are superconducting electromagnets
	- B-field is generated by flowing electricity
	- Permanent magnet MRI are uncommon



![](_page_25_Picture_5.jpeg)

![](_page_25_Picture_6.jpeg)

## Superconducting Magnet

![](_page_26_Figure_1.jpeg)

![](_page_26_Picture_2.jpeg)

![](_page_26_Picture_3.jpeg)

## Superconducting Electromagnets

of when both the line voltage and children both the line voltage and children  $\alpha$ 

magnet no longer boils of or consumer boils of or consumer boils of or consumer boils of or consumer boils of

![](_page_27_Figure_1.jpeg)

![](_page_27_Picture_2.jpeg)

![](_page_27_Picture_3.jpeg)

## Coldhead (Cryocooler)

![](_page_28_Figure_1.jpeg)

#### Re-condenses helium vapor and returns liquid helium to vessel.

![](_page_28_Picture_3.jpeg)

Advances in Whole-Body MRI Magnets by Thomas C. Cosmus and Michael Parizh

![](_page_28_Picture_5.jpeg)

## Helium Fill Port

![](_page_29_Picture_1.jpeg)

Helium boils off at 0 to 0.03 L/hour. \$10-\$25 per liter of liquid Helium.

Zero Boil-off and Low Volume (~20L vs 2000L) systems are emerging.

![](_page_29_Picture_4.jpeg)

Advances in Whole-Body MRI Magnets by Thomas C. Cosmus and Michael Parizh

![](_page_29_Picture_6.jpeg)

## Liquid Helium

- **• Where does helium come from?** 
	- **– Extracted from natural gas**
	- **– Strategic helium reserve**
	- **– Helium that escapes to atmosphere is lost** *forever***.**
- **• Zero boil-off design** 
	- **– Captures and re-compresses cryogen**
	- **– Saves 700-1300L per year**

![](_page_30_Picture_8.jpeg)

![](_page_30_Picture_9.jpeg)

![](_page_30_Picture_10.jpeg)

## Main Field (B0) - Principles

 $\cdot$  B<sub>0</sub> is a strong magnetic field

*B*  $\bar{\bar B}$  $_0 = B_0$  $\overline{k}$ *k*

- $> 1.5T$
- Z-oriented
- magnetization  $(\vec{M})^T$  $\cdot$  B<sub>0</sub> generates bulk  $-$  More  $B_0$ , more

*M*  $\overline{\text{V}}$ *N total*  $\sqrt{}$  $n =$  $\vec{\mu}$  $\vec{\mu}_n$ 

- B<sub>0</sub> forces  $\vec{M}$  to precess
	- Larmor Equation

$$
\omega=\gamma B
$$

![](_page_31_Picture_10.jpeg)

![](_page_31_Picture_11.jpeg)

## Main Field (B0) - Principles

- $\cdot$  B<sub>0</sub> is a strong magnetic field
	- $> 1.5T$
	- Z-oriented
- magnetization  $(\vec{M})^T$ • B<sub>0</sub> generates bulk
	- $-$  More  $B_0$ , more

*B* B  $_0 = B_0$  $\overline{k}$ *k* Eqn. 3.5

$$
\vec{M} = \sum_{n=1}^{N_{total}} \vec{\mu}_n
$$
 Eqn. 3.26

 $\omega = \gamma B$  Eqn. 3.18

- *M* precess
	- Larmor Equation

![](_page_32_Picture_10.jpeg)

![](_page_32_Picture_11.jpeg)

## Magnetic Dipole Moments

Spin + Charge ➠ Magnetic Moment ➠  $\vec{\mu}$  [J•T<sup>-1</sup> *or* kg•m<sup>2</sup>/s<sup>2</sup>/T]

"a measure of the strength of the system's net magnetic source" --http://en.wikipedia.org/wiki/Magnetic\_moment

![](_page_33_Figure_3.jpeg)

Hydrogen nuclei have magnetic dipole moments.

![](_page_33_Picture_5.jpeg)

![](_page_33_Picture_6.jpeg)

![](_page_34_Figure_0.jpeg)

#### Ntotal=0.24x1023 spins in a 2x2x10mm voxel **But not all spins contribute to our measured signal...**

![](_page_34_Picture_2.jpeg)

![](_page_34_Picture_3.jpeg)

![](_page_35_Picture_0.jpeg)

## B0 Field OFF

![](_page_35_Picture_2.jpeg)

![](_page_35_Picture_3.jpeg)

$$
\vec{M} = \sum_{n=1}^{N_{total}} \vec{\mu}_n = 0
$$

Spins point in all directions.

![](_page_35_Picture_6.jpeg)

![](_page_36_Picture_0.jpeg)

## B<sub>0</sub> Field ON

![](_page_36_Picture_2.jpeg)

![](_page_36_Picture_3.jpeg)

B0 polarizes the spins and generates bulk magnetization.

$$
\vec{M} = \sum_{n=1}^{N_{total}} \vec{\mu}_n = M_z
$$

![](_page_36_Picture_6.jpeg)

![](_page_37_Picture_0.jpeg)

![](_page_37_Picture_1.jpeg)

## B0 Field ON

![](_page_37_Figure_3.jpeg)

Only a very small number are spin-up relative to spin-down.

![](_page_37_Picture_5.jpeg)

## Zeeman Splitting

![](_page_38_Figure_1.jpeg)

## Zeeman Splitting

**• The spin population difference in the two spin states is related to their energy difference. According to the well-known Boltzmann distribution:** 

$$
\frac{N_{\uparrow}}{N_{\downarrow}} = e^{-\Delta E/\kappa T}
$$

$$
\Delta E = \gamma \hbar B_0
$$

- *κ* = **Bolzmann constant**
- *T* = **Absolute temperature of the spin system**

At 1.5T, 
$$
\frac{N_1}{N_1} = 0.999993
$$

**– All imaging is based on weak polarization (enough for clinical)**

![](_page_39_Picture_8.jpeg)

![](_page_39_Picture_9.jpeg)

## Main Field (B0) - Principles

- $\cdot$  B<sub>0</sub> is a strong magnetic field
	- $> 1.5T$
	- Z-oriented
- magnetization  $(\vec{M})^T$  $\cdot$  B<sub>0</sub> generates bulk  $-$  More  $B_0$ , more

*B* B  $_0 = B_0$  $\overline{k}$ *k* Eqn. 3.5

$$
\vec{M} = \sum_{n=1}^{N_{total}} \vec{\mu}_n
$$
 Eqn. 3.26

- $\vec{M}$ precess
	- Larmor Equation

![](_page_40_Picture_9.jpeg)

![](_page_40_Picture_10.jpeg)

![](_page_40_Picture_11.jpeg)

## Spin vs. Precession

- **• Spin** 
	- Intrinsic form of angular momentum
	- Quantum mechanical phenomena
	- No classical physics counterpart
		- Except by hand-waving analogy…
- **• Precession** 
	- Spin+Mass+Charge give rise to precession

![](_page_41_Picture_8.jpeg)

![](_page_41_Picture_9.jpeg)

## Precession

![](_page_42_Figure_1.jpeg)

 $\mathbf{F}_{\text{g}}$  and the weight of the top causes a change in the angular momentum  $L$  in the direction of that torque. This causes the top to precess.

![](_page_42_Picture_3.jpeg)

https://en.wikipedia.org/wiki/Precession

![](_page_42_Picture_5.jpeg)

Nuclear Magnetic Resonance

#### NMR Phenomena

![](_page_44_Picture_1.jpeg)

#### Magnetic Moment

![](_page_45_Picture_1.jpeg)

# Charge Magnetic<br>Spin Moment

**Protons behave like small magnets because of spin and charge.**

#### Magnetic Moment

![](_page_46_Picture_1.jpeg)

# Charge Magnetic<br>Spin Moment

Protons (small magnets) align with an external magnetic field (B<sub>0</sub>).

#### Angular Momentum

![](_page_47_Picture_1.jpeg)

![](_page_47_Picture_2.jpeg)

**Protons have angular momentum because of spin and mass.**

#### Precession (Top Analogy)

#### Gravity

#### **Precession** Spin │ Angular<br>∫Momentum **Mass**

**A spinning tops precesses in a gravitational field.** A spinning proton precesses in a magnetic (B<sub>0</sub>) field.

#### Larmor Frequency

![](_page_49_Figure_1.jpeg)

## Larmor Frequency  $=\omega = \gamma$ Bo

**The frequency of precession is the Larmor frequency.**

## NMR Active Nuclei

- Spin + Charge + Mass  $\Longrightarrow$  NMR Active
	- Spin? *Intrinsic* form of angular momentum.
- Nuclei have spin angular momentum if:
	- Odd atomic mass (# protons+neutrons) **And/Or**
	- Odd atomic number (# of protons)
- Spin angular momentum
	- Leads to precession
	- Spin ≠ precession (a top spins *and* precesses)
- Frequency of precession (Larmor Frequency)
	- Gyromagnetic Ratio (γ)
		- Physical constant
		- Unique for each NMR active nuclei

![](_page_50_Picture_13.jpeg)

![](_page_50_Picture_14.jpeg)

Hydrogen

![](_page_50_Figure_16.jpeg)

Carbon-13

#### **What is so special about 1H? Spin, charge, and mass!**

### Larmor Equation

- Spin≠Precession
	- Protons *intrinsically* have spin
	- Protons *precess* in the presence of a B-field
- Larmor frequency increases with:
	- $-$  Larger B<sub>0</sub>
	- Higher gyromagnetic ratio
	- Higher frequencies produce stronger signals...

# $\omega = \gamma B_0$

### NMR Active Nuclei

![](_page_52_Picture_192.jpeg)

The *relative sensitivity* is at constant magnetic field and equal number of nuclei The *absolute sensitivity* is the relative sensitivity multiplied by natural abundance

#### Quiz: NMR - True or False?

- 1. Electron spin is the key to NMR
- 2. MRI is *nothing* without spin, charge, and mass
- 3. All atomic nuclei are NMR active.
- 4. Spin and precession are the same.
- 5. Higher fields lead to faster precession

#### Quiz: Main Field - True or False?

- 1. B<sub>0</sub> is rare earth permanent magnet.
- 2. 1 Tesla=1000 Gauss.
- 3. Higher fields increase polarization, which contributes to better image quality
- 4. Exams at higher fields have lower SAR.
- 5. 1H always precesses at the same Larmor frequency.

![](_page_55_Picture_0.jpeg)

- Related reading materials
	- Nishimura Chap 3 and 4

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