# MRI Systems I: B0 and Bulk Magnetization

#### M219 - Principles and Applications of MRI Kyung Sung, Ph.D. 1/11/2022

# **Course Overview**

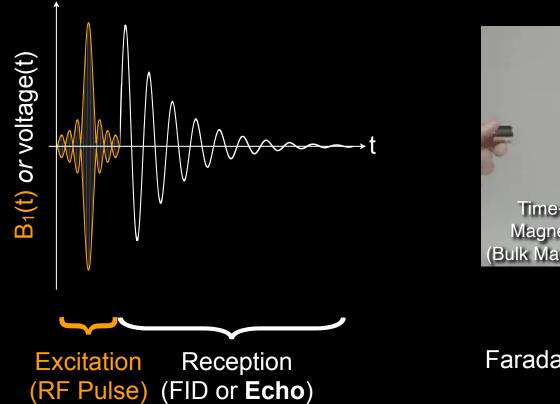
- Course website
  - https://mrrl.ucla.edu/pages/m219
- 2023 course schedule
  - https://mrrl.ucla.edu/pages/m219\_2023
- Assignments
  - Homework #1 will be out on 1/16 (due on 1/30)
- Office hours, Fridays 10-12pm
  - In-person (Ueberroth, 1417B)
  - Zoom is also available

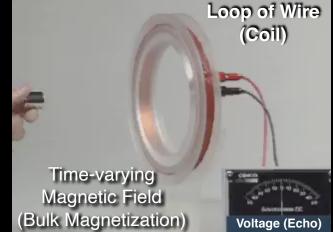
### What is MRI?

- Magnetic
  - We need a big magnet
- Resonance
  - Excitation energy has to be on-resonance
- Imaging
  - We can make pretty pictures

#### What is MRI?

MRI follows a classic excitation-reception paradigm.





Faraday's Law of Induction

MRI encodes spatial information and image contrast in the echo.

#### **Requirements for MRI**

- NMR Active Nuclei
  - e.g. <sup>1</sup>H in H<sub>2</sub>0
- Magnetic Field (B<sub>0</sub>): Polarizer
- RF System (B<sub>1</sub>): Exciter
- Coil: Receiver
- Gradients (G<sub>X</sub>, G<sub>Y</sub>, G<sub>Z</sub>): Spatial Encoding

#### **MRI Hardware**

Cryostat Z-grad

Body Tx/Rx Coil (B<sub>1</sub>)

Y-grad

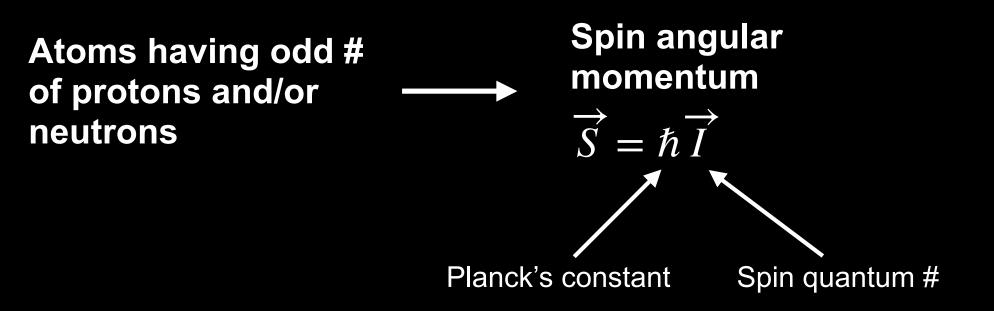
X-grad

Main Coil  $(B_0)$ 

Image Adapted From: http://www.ee.duke.edu/~jshorey

Nuclear Spin

## **Classical View**



- Nuclei with an odd mass number have *half-integral spin* 
  - Spin-1/2 <sup>1</sup>H, <sup>13</sup>C, <sup>15</sup>N, <sup>19</sup>F, <sup>31</sup>P
  - Spin-3/2 <sup>23</sup>Na
- Nuclei with an even mass number and an even charge number have zero spin
  - <sup>12</sup>C and <sup>16</sup>O





# **Spin Angular Momentum**

Spin + Mass  $\rightarrow$  Spin Angular Momentum  $\rightarrow$   $\vec{S}$  [kg·m<sup>2</sup>s<sup>-1</sup>]

ec v

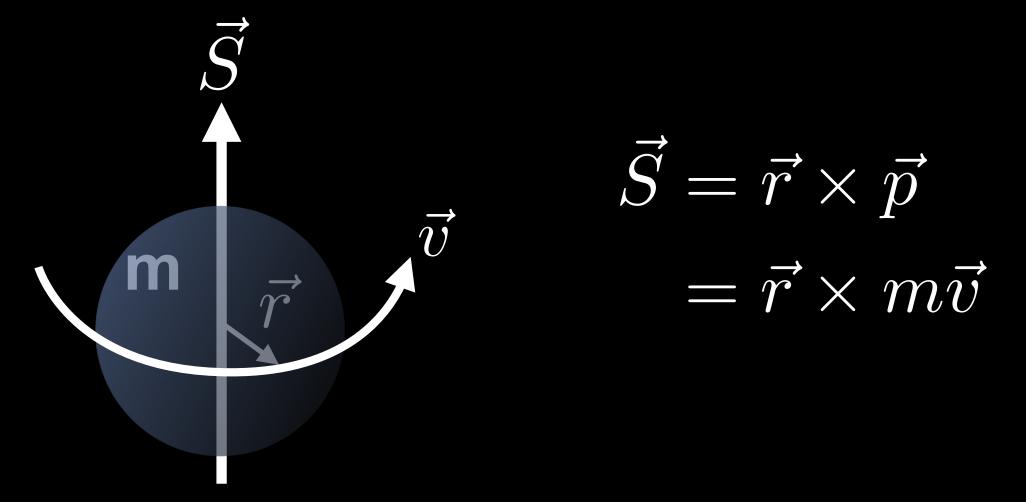






## **Spin Angular Momentum**

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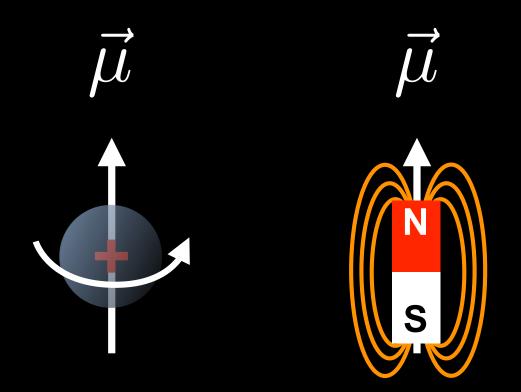




## **Magnetic Dipole Moments**

Spin + Charge  $\rightarrow$  Magnetic Moment  $\rightarrow$   $\vec{\mu}$  [J•T<sup>-1</sup> or kg•m<sup>2</sup>/s<sup>2</sup>/T]

"a measure of the strength of the system's net magnetic source" --http://en.wikipedia.org/wiki/Magnetic\_moment



Hydrogen nuclei have magnetic dipole moments.





# **Gyromagnetic Ratio**

- Gyromagnetic Ratio
  - Physical constant
  - Unique for each NMR active nuclei
  - Ratio of the magnetic moment to the angular momentum

$$\overrightarrow{\mu} = \gamma \overrightarrow{S} = \gamma \hbar \overrightarrow{I}$$

- Governs the frequency of *precession*
- Gamma vs. Gamma-bar

$$\gamma = \gamma/2\pi$$





# **NMR Active Nuclei**

lsotope	Spin [I]	Natural Abundance	Gyromagnetic Ratio [MHz/T]	Relative Sensitivity	Absolute Sensitivity
1 <b>H</b>	1/2	0.9980	42.57	1	9.98E-01
<sup>2</sup> H	1	0.0160	6.54	0.015	2.40E-04
12 <b>C</b>	0	0.9890			
13 <b>C</b>	1/2	0.0110	10.71	0.016	1.76E-04
<sup>14</sup> N	1	0.9960	3.08	0.001	9.96E-04
15 <b>N</b>	1/2	0.0040	-4.32	0.001	4.00E-06
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<sup>17</sup> O	5/2	0.0004	-5.77	0.029	1.16E-05
<sup>19</sup> F	1/2	1.0000	40.05	0.83	8.30E-01
<sup>23</sup> Na	3/2	1.0000	11.26	0.093	9.30E-02
<sup>31</sup> P	1/2	1.0000	17.24	0.066	6.60E-02

The *relative* sensitivity is at constant magnetic field and equal number of nuclei.

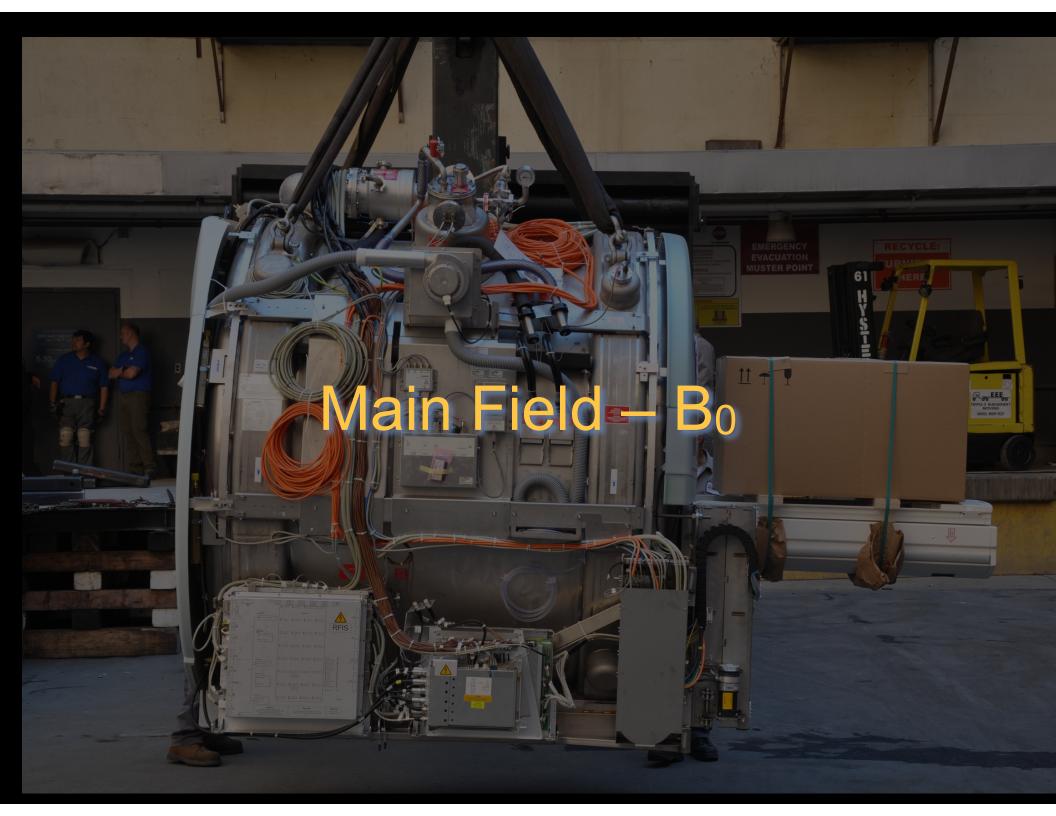
- Using a factor of  $\gamma^{\frac{11}{4}}I(\overline{I+1})$ ; <sup>1</sup>H is the reference standard.

The *absolute* sensitivity is the relative sensitivity multiplied by natural abundance.

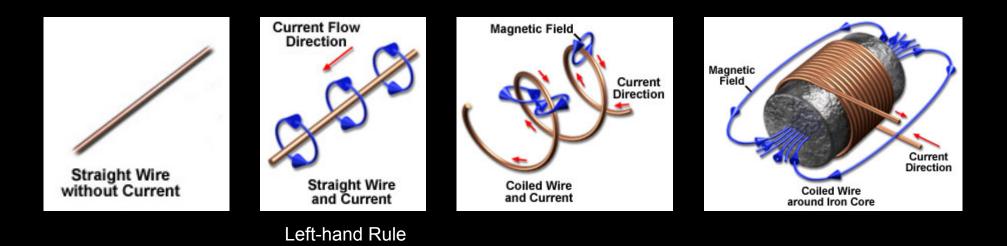


P. Callaghan & http://www.cryst.bbk.ac.uk/PPS2/projects/schirra/html/nuclei.htm





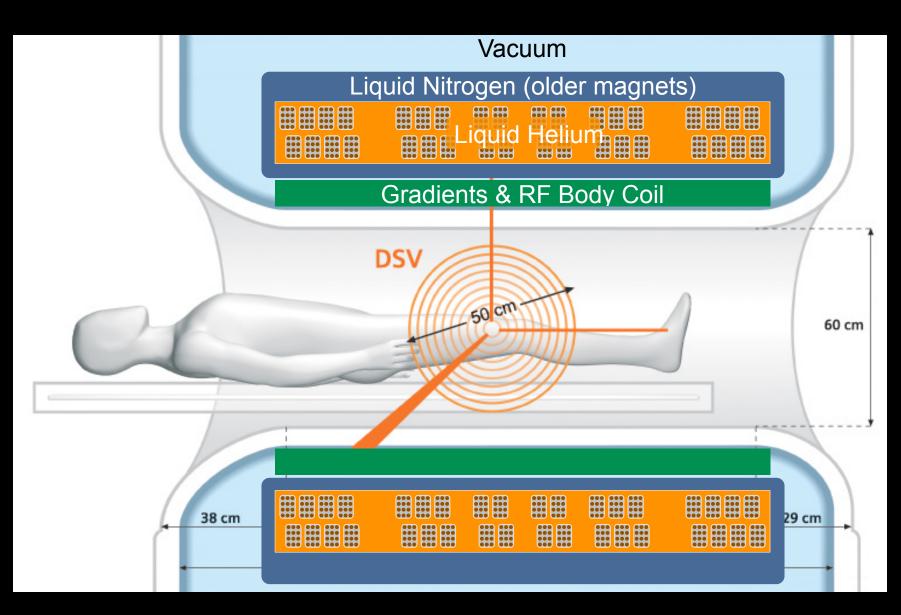
### **Currents & Magnetic Fields**



#### Electromagnet – A current in a wire generates a magnetic field.

http://www.magnet.fsu.edu/education/tutorials/magnetacademy/

## Superconducting Electromagnet



#### MRI scanners are superconducting electromagnets.

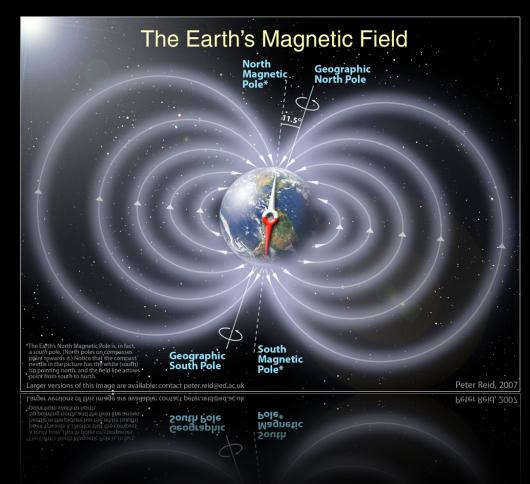
#### B<sub>0</sub> Field

- B<sub>0</sub> field is:
  - Spatially uniform (over a volume of interest)
    - ~50cm @ isocenter
  - Temporally stable
    - $B_0(t)=B_0(t=0)e^{-(R/L)/t}$
    - Decays <1ppm/hour</li>
  - Oriented along the z-axis (  $\vec{k}$  )
    - Long axis of the scanner.

$$\vec{B}_0 = B_0 \vec{k}$$

## Main Field (B<sub>0</sub>) – Strength

- Earth's magnetic field
   0.5 Gauss
- Refrigerator magnet
   10-100 Gauss
- B<sub>0</sub> Field
  - 0.5T = 5000 Gauss
  - 1.5T = 15000 Gauss
  - 3.0T = 30000 Gauss



## B<sub>0</sub> Strength - Advantages

- $\uparrow B_0 \implies \uparrow Polarization (|\vec{M}|) = \uparrow SNR$ 
  - **t**Polarization, therefore more  $\vec{M}$  for imaging.
  - SNR  $\propto B_0^{7/4}$  (Polarization + Larmor Frequency)
    - Spatial resolution
    - Temporal resolution
    - Scan time

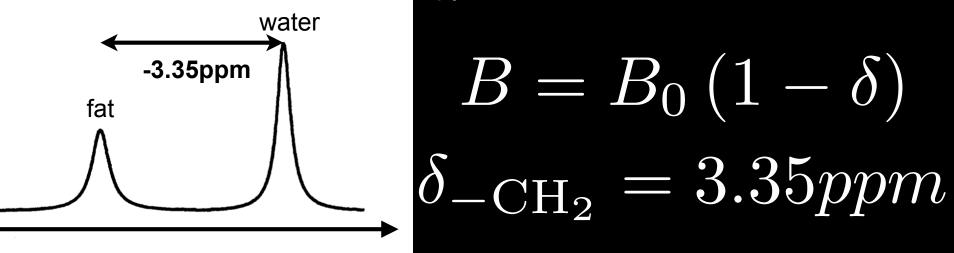
## B<sub>0</sub> Strength - Disadvantages

- $\clubsuit B_0 \implies \clubsuit$  Specific Absorption Ratio (SAR)
  - Energy absorbed by body [W/kg]
  - SAR $\propto$ B<sub>0</sub><sup>2</sup>
- $\clubsuit B_0 \Longrightarrow \clubsuit Cost$ 
  - ~\$1,000,000 per Tesla
  - More shielding

Higher B<sub>0</sub> leads to higher SAR for patients and higher costs.

## B<sub>0</sub> Strength - Disadvantages

- $\clubsuit B_0 \Longrightarrow \clubsuit$  Chemical shift ( $\Delta f$ )
  - $\uparrow$   $\Delta f$  between fat and water
    - Fat and water have different Larmor frequencies
      - ~220Hz different at 1.5T
      - ~440Hz different at 3.0T
    - Fat is more spatially mis-registered @ 3T
  - Good for spectroscopy...



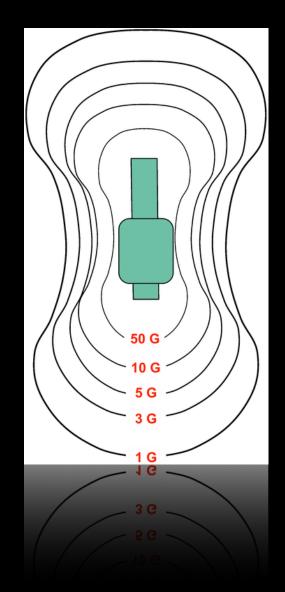
Chemical Shift – Fat (–CH<sub>2</sub>) is ~220Hz lower at 1.5T

## Main Field (B<sub>0</sub>) – Shielding

- Problem: The B<sub>0</sub> field extends well beyond the scanner.
- Shielding reduces B<sub>0</sub> foot print
  - Reduces install cost
  - Reduces interference

#### Passive Shielding

- Iron room shielding
- Heavy, not cheap
- Active Shielding
  - Super-conducting coils that oppose (shield) B<sub>0</sub> fringe field
- "Five Gauss Line"
  - Threshold beyond which ferromagnetic objects are strictly prohibited
  - 5G=0.5mT



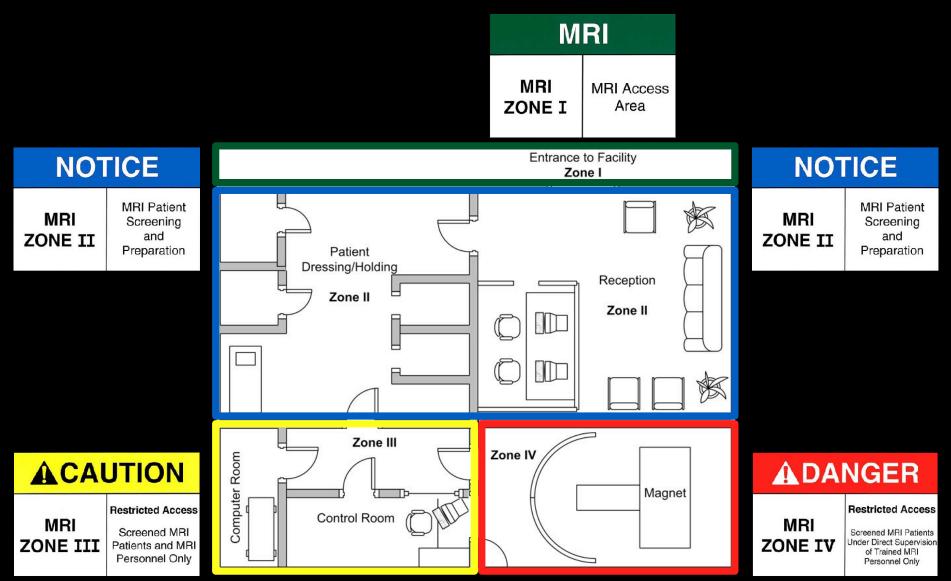
ACR Guidance Document on MR Safe Practices: 2013; JMRI 37:501–530 (2013)

## **RF** Shielding

- RF fields are close to FM radio
  - <sup>1</sup>H @ 1.5T  $\Rightarrow$  63.85 MHz
  - <sup>1</sup>H @ 3.0T  $\Rightarrow$  127.71 MHz
  - KROQ  $\Rightarrow$  106.7 MHz
- Need to shield local sources from interfering
- Copper room shielding required



#### **MRI** Zones

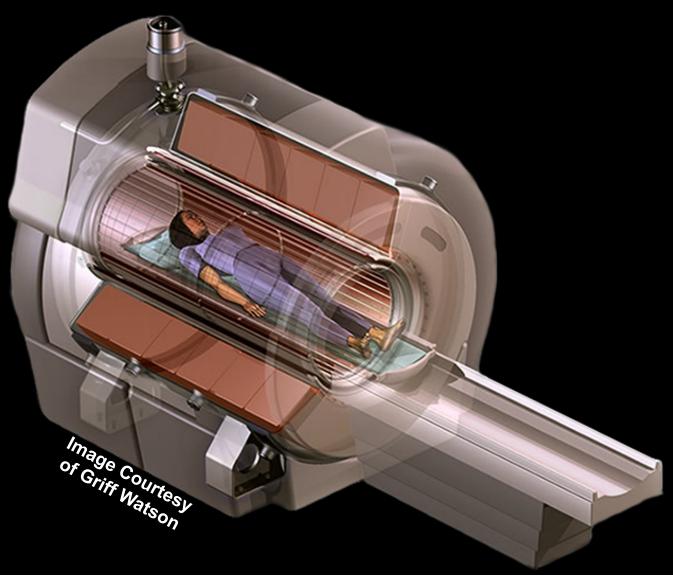


ACR Guidance Document on MR Safe Practices: 2013; JMRI 37:501–530 (2013)

# **Bo Hardware Anatomy**

# Superconducting Electromagnets

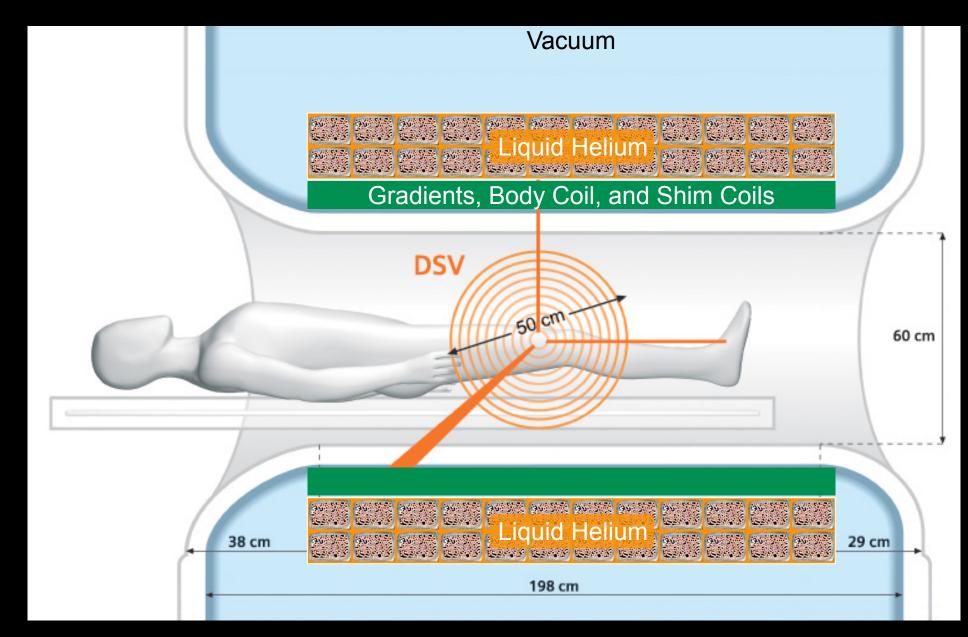
- MRI scanners are superconducting electromagnets
  - B-field is generated by flowing electricity
  - Permanent magnet MRI are uncommon







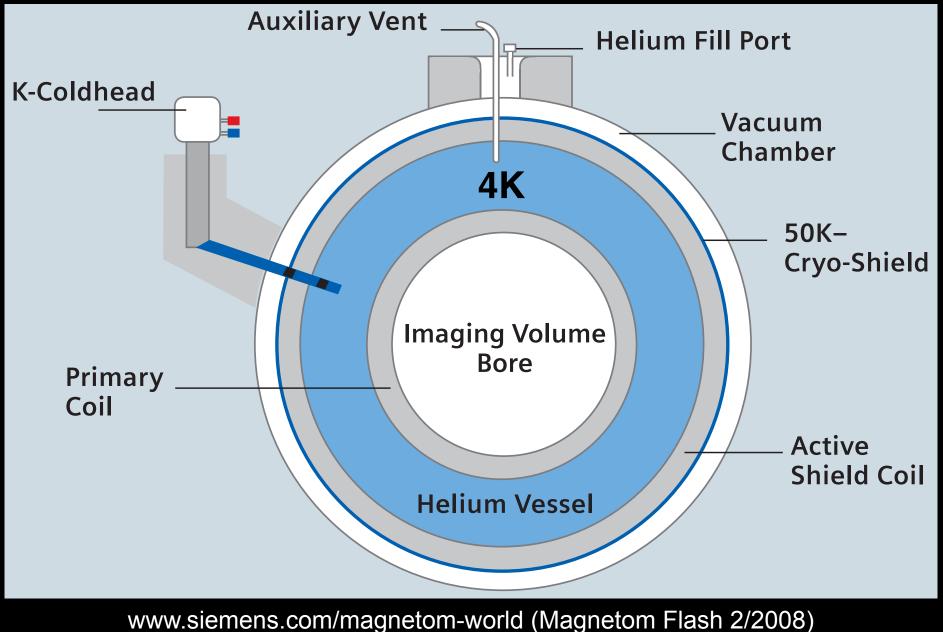
## **Superconducting Magnet**







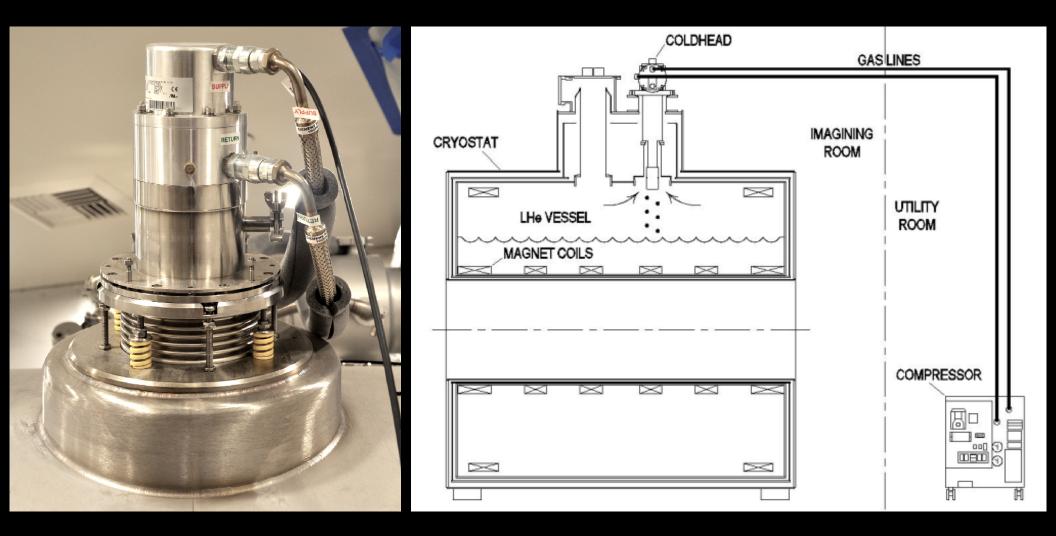
# Superconducting Electromagnets







## Coldhead (Cryocooler)



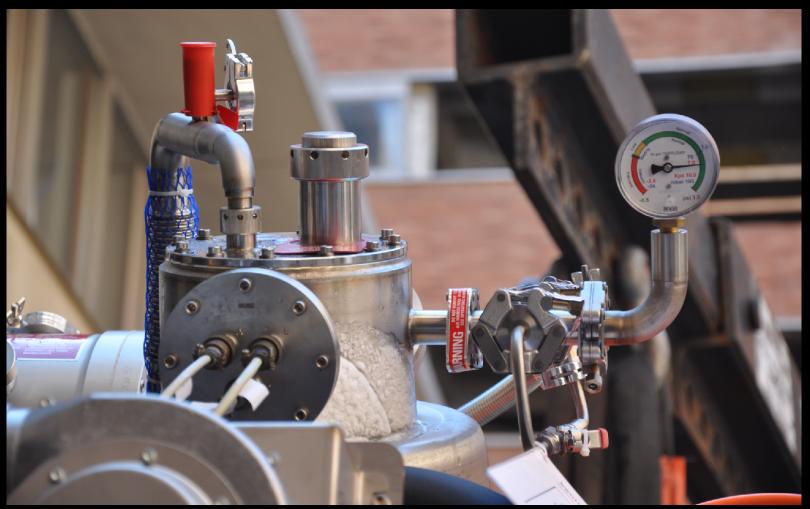
#### Re-condenses helium vapor and returns liquid helium to vessel.



Advances in Whole-Body MRI Magnets by Thomas C. Cosmus and Michael Parizh



## **Helium Fill Port**



Helium boils off at 0 to 0.03 L/hour. \$10-\$25 per liter of liquid Helium.

Zero Boil-off and Low Volume (~20L vs 2000L) systems are emerging.

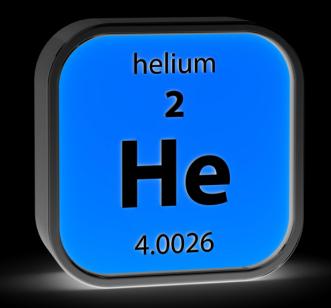


Advances in Whole-Body MRI Magnets by Thomas C. Cosmus and Michael Parizh



# Liquid Helium

- Where does helium come from?
  - Extracted from natural gas
  - Strategic helium reserve
  - Helium that escapes to atmosphere is lost *forever*.
- Zero boil-off design
  - Captures and re-compresses cryogen
  - Saves 700-1300L per year







# Main Field (B<sub>0</sub>) - Principles

B<sub>0</sub> is a strong magnetic field

 $\dot{B_0} = B_0 \dot{k}$ 

- ->1.5T
- Z-oriented
- B₀ generates bulk magnetization (M)
   – More B₀, more

Ntotal  $n \equiv$ 

- B<sub>0</sub> forces  $\vec{M}$  to precess
  - Larmor Equation

$$\omega = \gamma B$$





# Main Field (B<sub>0</sub>) - Principles

 $B_0 = B_0 k$ 

 $\omega = \gamma B$ 

- B<sub>0</sub> is a strong magnetic field
  - ->1.5T
  - Z-oriented
- B<sub>0</sub> generates bulk magnetization (*M*)
   – More B<sub>0</sub>, more
- $ec{M} = \sum_{n=1}^{N_{total}} ec{\mu_n}$  Eqn. 3.26

- B<sub>0</sub> forces  $\vec{M}$  to precess
  - Larmor Equation





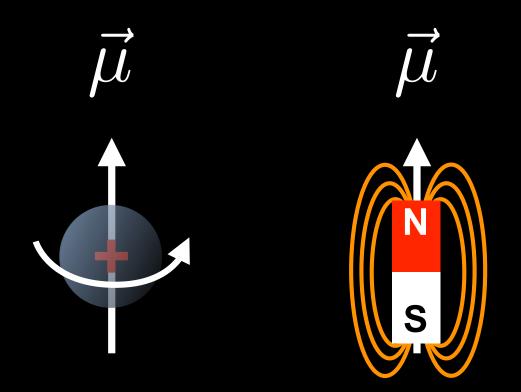
Eqn. 3.5

Eqn. 3.18

## **Magnetic Dipole Moments**

Spin + Charge  $\rightarrow$  Magnetic Moment  $\rightarrow$   $\vec{\mu}$  [J•T<sup>-1</sup> or kg•m<sup>2</sup>/s<sup>2</sup>/T]

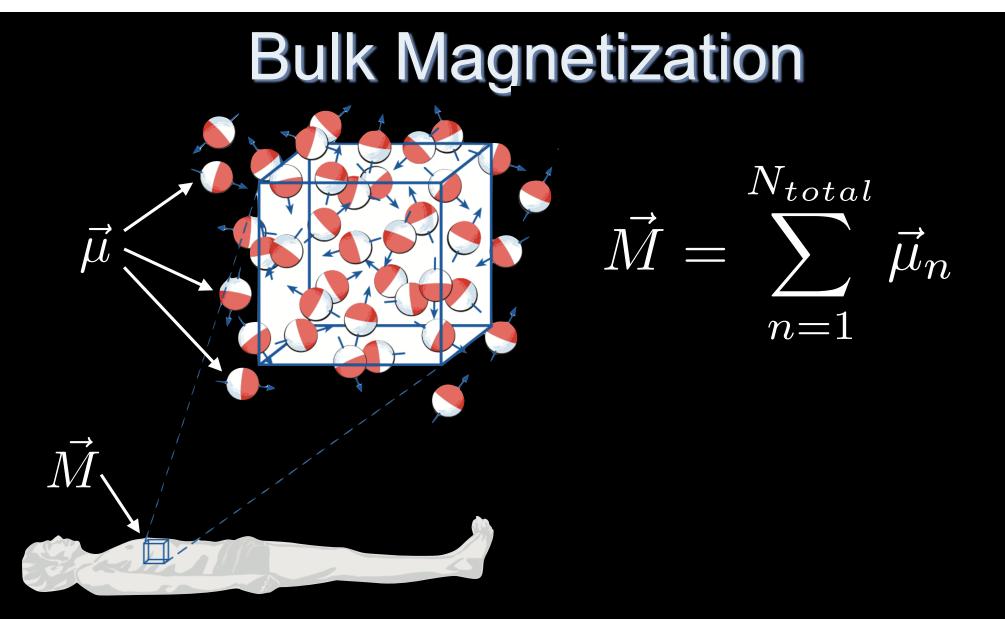
"a measure of the strength of the system's net magnetic source" --http://en.wikipedia.org/wiki/Magnetic\_moment



Hydrogen nuclei have magnetic dipole moments.



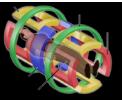




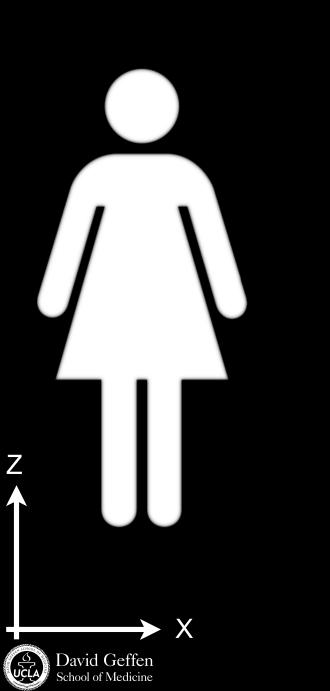
#### N<sub>total</sub>=0.24x10<sup>23</sup> spins in a 2x2x10mm voxel But not all spins contribute to our measured signal...

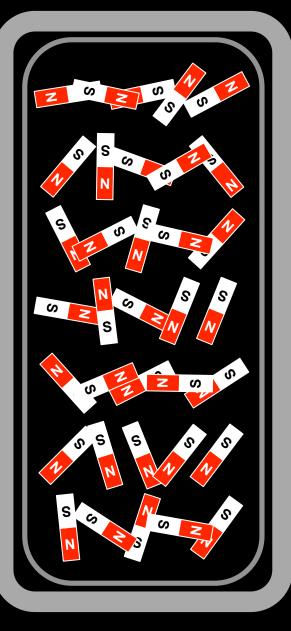






## **B**<sub>0</sub> Field OFF

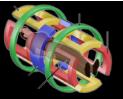




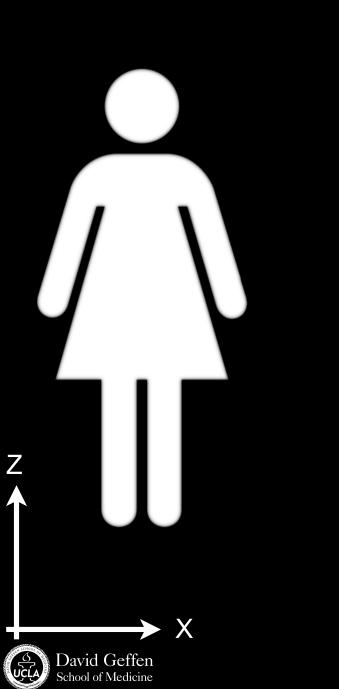
$$\vec{M} = \sum_{n=1}^{N_{total}} \vec{\mu}_n = 0$$

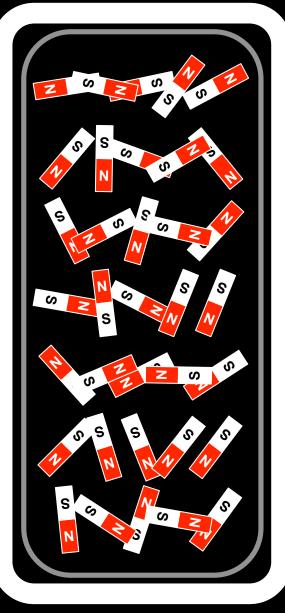
Spins point in all directions.





# **B**<sub>0</sub> Field ON

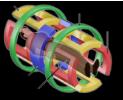




B<sub>0</sub> polarizes the spins and generates bulk magnetization.

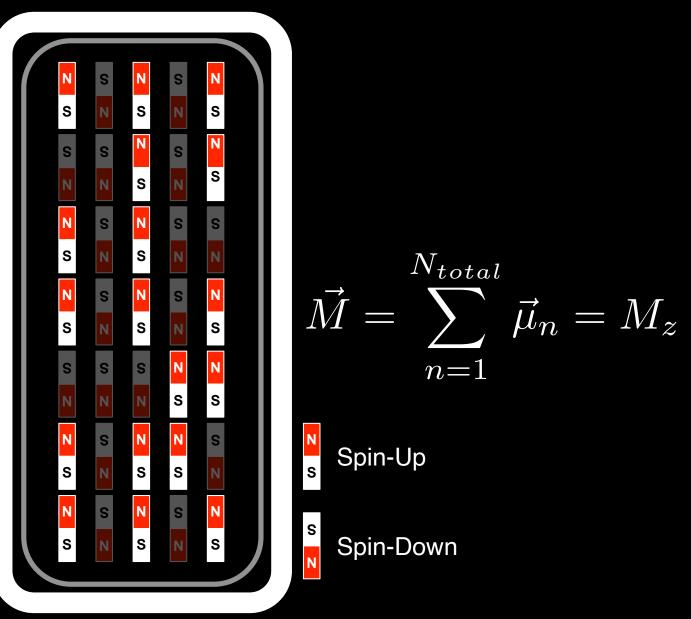
$$\vec{M} = \sum_{n=1}^{N_{total}} \vec{\mu}_n = M_z$$







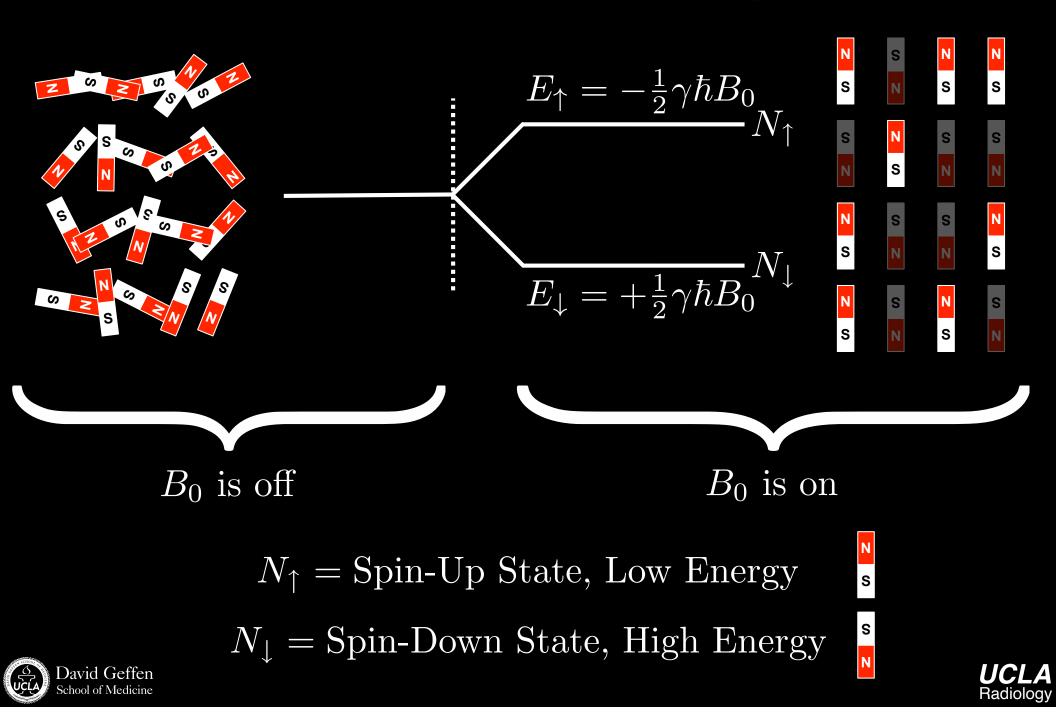
# **B**<sub>0</sub> Field ON



Only a very small number are spin-up relative to spin-down.



## Zeeman Splitting



# **Zeeman Splitting**

 The spin population difference in the two spin states is related to their energy difference. According to the well-known Boltzmann distribution:

$$\frac{N_{\uparrow}}{N_{\downarrow}} = e^{-\Delta E/\kappa T}$$

$$\Delta E = \gamma \hbar B_0$$

- $\kappa =$ Bolzmann constant
- T = Absolute temperature of the spin system

• At 1.5T, 
$$\frac{N_{\uparrow}}{N_{\downarrow}}$$
 = 0.999993

- All imaging is based on weak polarization (enough for clinical)





# Main Field (B<sub>0</sub>) - Principles

- B<sub>0</sub> is a strong magnetic field
  - ->1.5T
  - Z-oriented
- B<sub>0</sub> generates bulk magnetization (*M*)
   – More B<sub>0</sub>, more

 $\vec{B_0} = B_0 \vec{k}$  Eqn. 3.5

$$\vec{M} = \sum_{n=1}^{N_{total}} \vec{\mu}_n$$
 Eqn. 3.26

- B<sub>0</sub> forces  $\vec{M}$  to precess
  - Larmor Equation







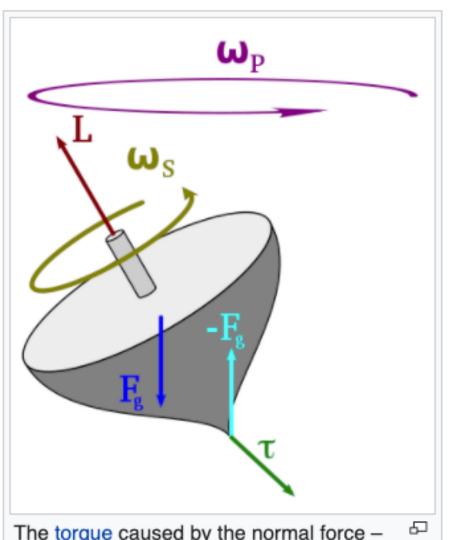
# Spin vs. Precession

- Spin
  - Intrinsic form of angular momentum
  - Quantum mechanical phenomena
  - No classical physics counterpart
    - Except by hand-waving analogy...
- Precession
  - Spin+Mass+Charge give rise to precession





### Precession



The torque caused by the normal force –  $\Box$   $\mathbf{F}_{g}$  and the weight of the top causes a change in the angular momentum  $\mathbf{L}$  in the direction of that torque. This causes the top to precess.

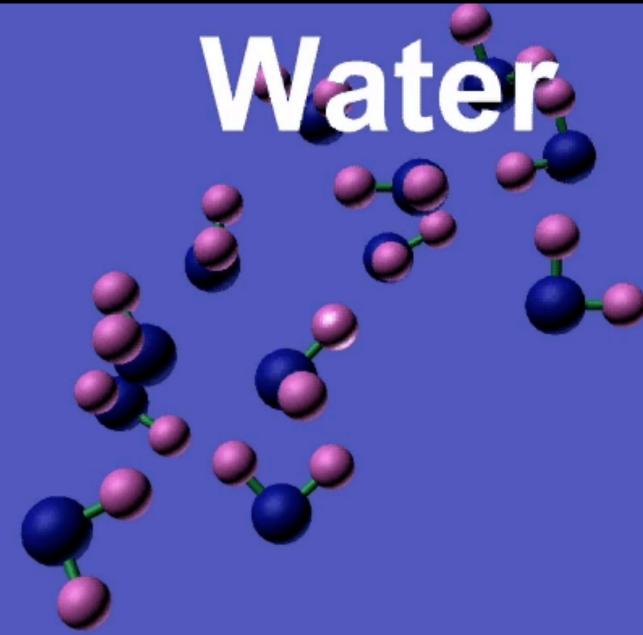
David Geffen School of Medicine

https://en.wikipedia.org/wiki/Precession

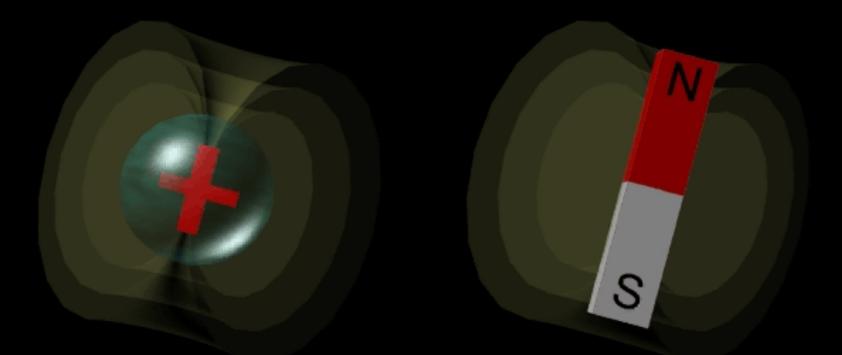


Nuclear Magnetic Resonance

#### NMR Phenomena



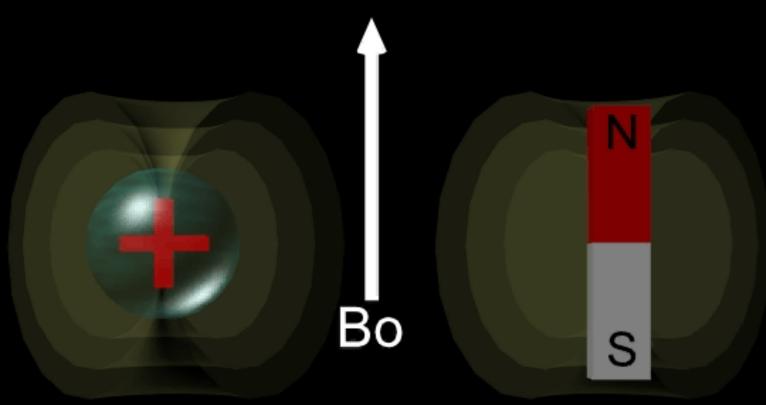
#### Magnetic Moment



# Charge Magnetic Spin Moment

Protons behave like small magnets because of spin and charge.

#### Magnetic Moment



# Charge } Magnetic Spin

Protons (small magnets) align with an external magnetic field (B<sub>0</sub>).

#### Angular Momentum





Protons have angular momentum because of spin and mass.

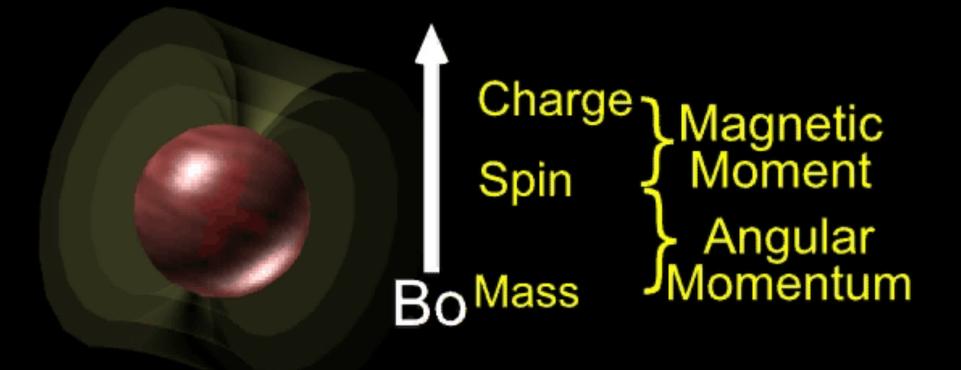
#### Precession (Top Analogy)

#### Gravity

# Precession Spin Mass Momentum

A spinning tops precesses in a gravitational field. A spinning proton precesses in a magnetic (B<sub>0</sub>) field.

#### Larmor Frequency



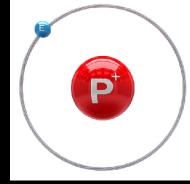
# Larmor Frequency $=\omega = \gamma Bo$

The frequency of precession is the Larmor frequency.

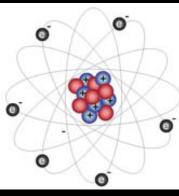
### **NMR Active Nuclei**

- Spin + Charge + Mass  $\implies$  NMR Active igodot
  - Spin? *Intrinsic* form of angular momentum.
- Nuclei have spin angular momentum if: ullet
  - Odd atomic mass (# protons+neutrons) And/Or
  - Odd atomic number (# of protons)
- Spin angular momentum
  - Leads to precession
  - Spin  $\neq$  precession (a top spins *and* precesses)
- Frequency of precession (Larmor Frequency)
  - Gyromagnetic Ratio ( $\gamma$ )
    - Physical constant
    - Unique for each NMR active nuclei





Hydrogen



Carbon-13

#### What is so special about <sup>1</sup>H? Spin, charge, and mass!

#### Larmor Equation

- Spin≠Precession
  - Protons *intrinsically* have spin
  - Protons *precess* in the presence of a B-field
- Larmor frequency increases with:
  - Larger  $B_0$
  - Higher gyromagnetic ratio
  - Higher frequencies produce stronger signals...

# $\omega = \gamma B_0$

#### **NMR Active Nuclei**

lsotope	Spin [I]	Gyromagnetic Ratio [MHz/T]	Relative Sensitivity	Natural Abundance	Absolute Sensitivity
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The *relative sensitivity* is at constant magnetic field and equal number of nuclei The *absolute sensitivity* is the relative sensitivity multiplied by natural abundance

#### Quiz: NMR - True or False?

- 1. Electron spin is the key to NMR
- 2. MRI is *nothing* without spin, charge, and mass
- 3. All atomic nuclei are NMR active.
- 4. Spin and precession are the same.
- 5. Higher fields lead to faster precession

#### Quiz: Main Field - True or False?

- 1.  $B_0$  is rare earth permanent magnet.
- 2. 1 Tesla=1000 Gauss.
- Higher fields increase polarization, which contributes to better image quality
- 4. Exams at higher fields have lower SAR.
- 5. <sup>1</sup>H always precesses at the same Larmor frequency.



- Related reading materials
  - Nishimura Chap 3 and 4

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