

MRI Systems III: Gradients

M219 - Principles and Applications of MRI

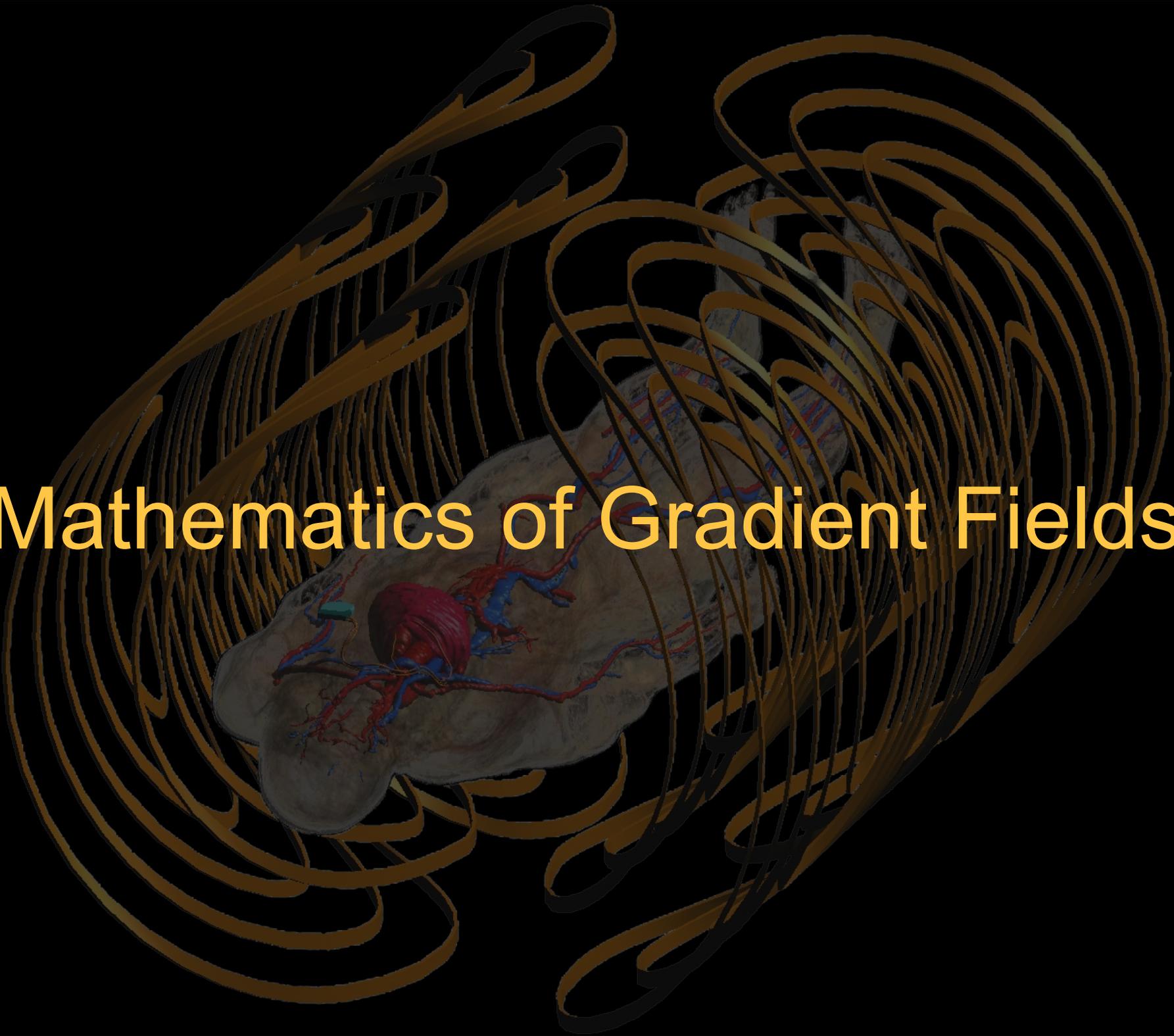
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1/30/2023

Course Overview

- Course website
 - <https://mrrl.ucla.edu/pages/m219>
- 2023 course schedule
 - https://mrrl.ucla.edu/pages/m219_2023
- Assignments
 - Homework #1 is due today
 - Homework #2 is out
- Office hours, Fridays 10-12pm
 - In-person (Ueberroth, 1417B)
 - Zoom is also available

Mathematics of Gradient Fields



Gradients

Gradients are a special kind of inhomogeneous field whose z-component varies linearly along a specific direction called the gradient direction.

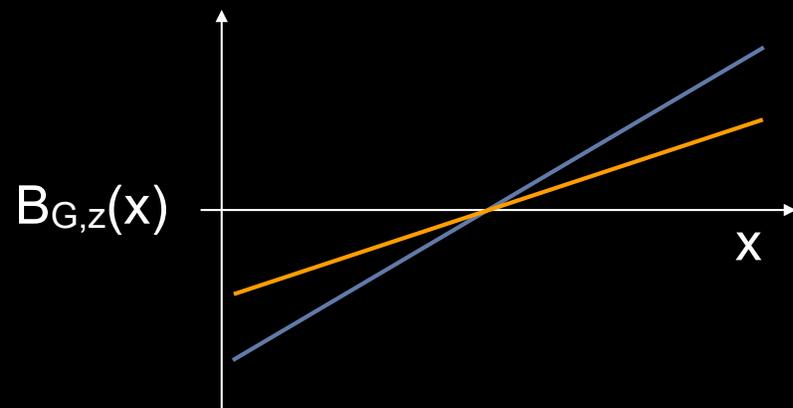
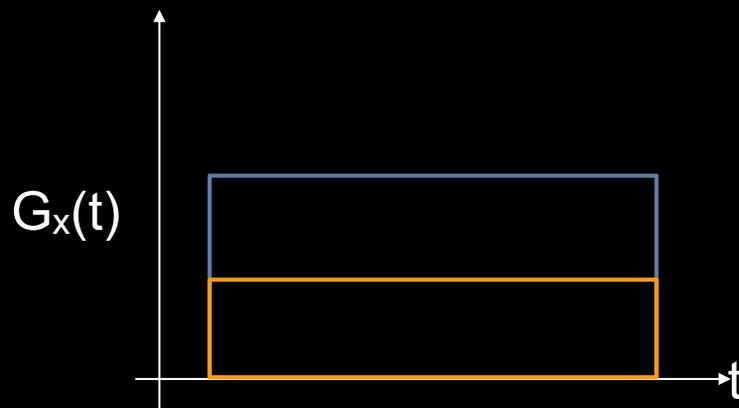
$$\underbrace{B_G}_{\text{B-field from a gradient}}, \underbrace{z}_{\text{Points along the z-direction}} \underbrace{(x)}_{\text{Varies with the x-direction}} = \underbrace{G_x}_{\text{x-gradient amplitude}} \underbrace{x}_{\text{x-distance from isocenter}}$$

Gradient Induced B-Fields

$$B_{G,z}(x) = G_x x \quad \text{x-gradient}$$

$$B_{G,z}(y) = G_y y \quad \text{y-gradient}$$

$$B_{G,z}(z) = G_z z \quad \text{z-gradient}$$



Gradient Induced B-Fields

- Each gradient coil can be activated independently and simultaneously

$$\begin{aligned} B_{G,z} \vec{k} &= (G_x x + G_y y + G_z z) \vec{k} \\ &= (\vec{G} \cdot \vec{r}) \vec{k} \end{aligned}$$

The magnetic field at a position depends on the magnitude of the applied gradient.

Combined B_0 and Gradient Fields

- Gradients contribute to the net B-field, but only along the z-direction

$$\begin{aligned}\vec{B}(\vec{r}, t) &= (B_0 + B_{G,z}) \vec{k} \\ &= \left(B_0 + \vec{G}(t) \cdot \vec{r} \right) \vec{k}\end{aligned}$$

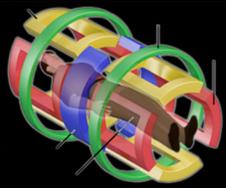
B-Field Assumptions in MRI

- **B_0 -field is:**
 - Perfectly uniform over space.
 - “ B_0 homogeneity”
 - Perfectly stable with time.
- **B_1 -field is:**
 - Perfectly uniform over space.
 - “ B_1 homogeneity”
 - Temporally modulated exactly as specified.
- **Gradient Fields are:**
 - Perfectly linear over space.
 - “Gradient linearity”
 - Temporally modulated exactly as specified

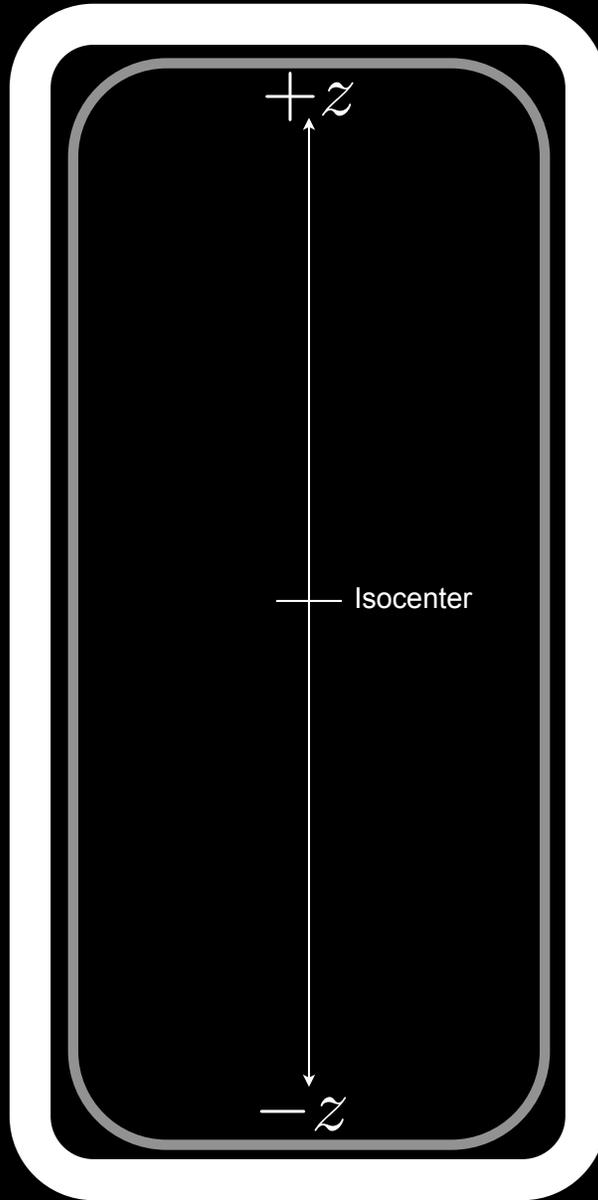
Imperfections of Gradient Fields

- Gradient coils aren't perfect
 - Non-linearity
 - Eddy Currents
 - Maxwell terms
(Concomitant fields)
 - But they are small
 - Much smaller than B_0

Gradient Fields & Spins



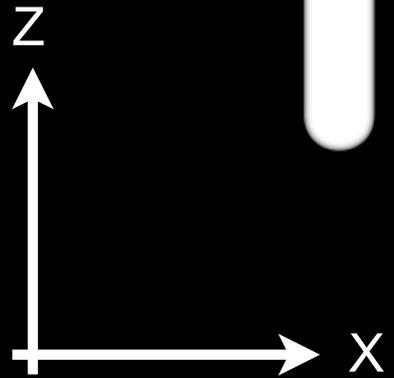
No Gradients Turned On



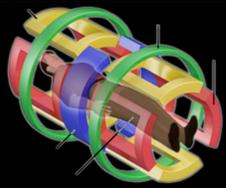
B_0

B_0

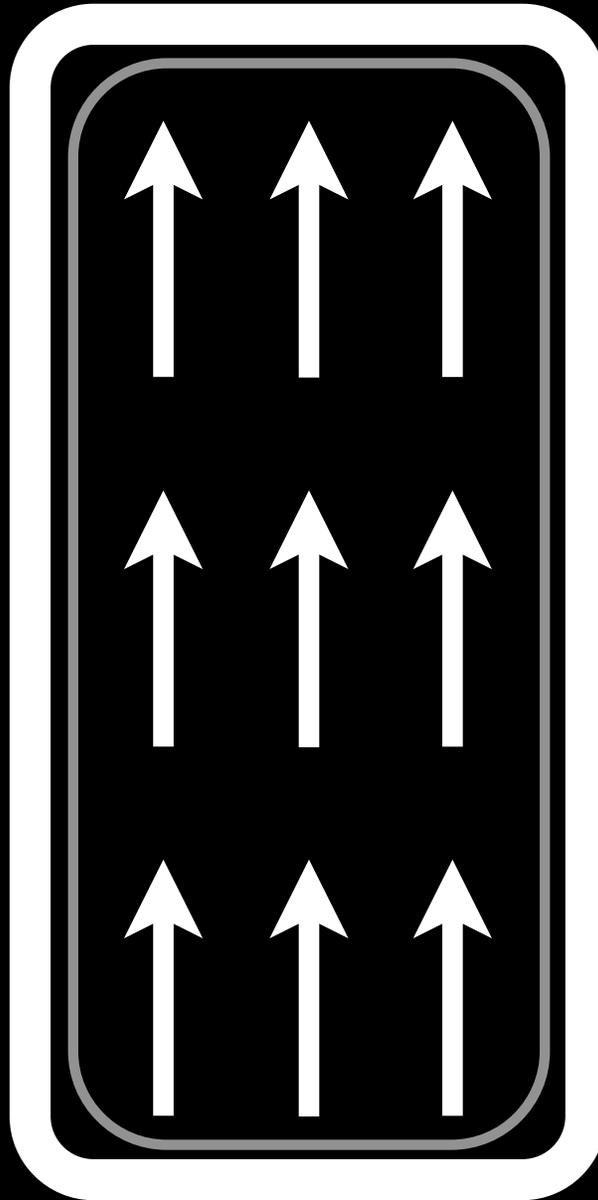
B_0



$$\omega = \gamma B_0$$



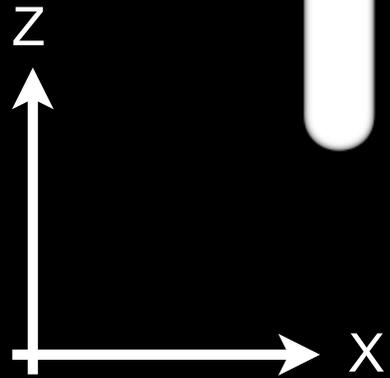
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B_0

B_0

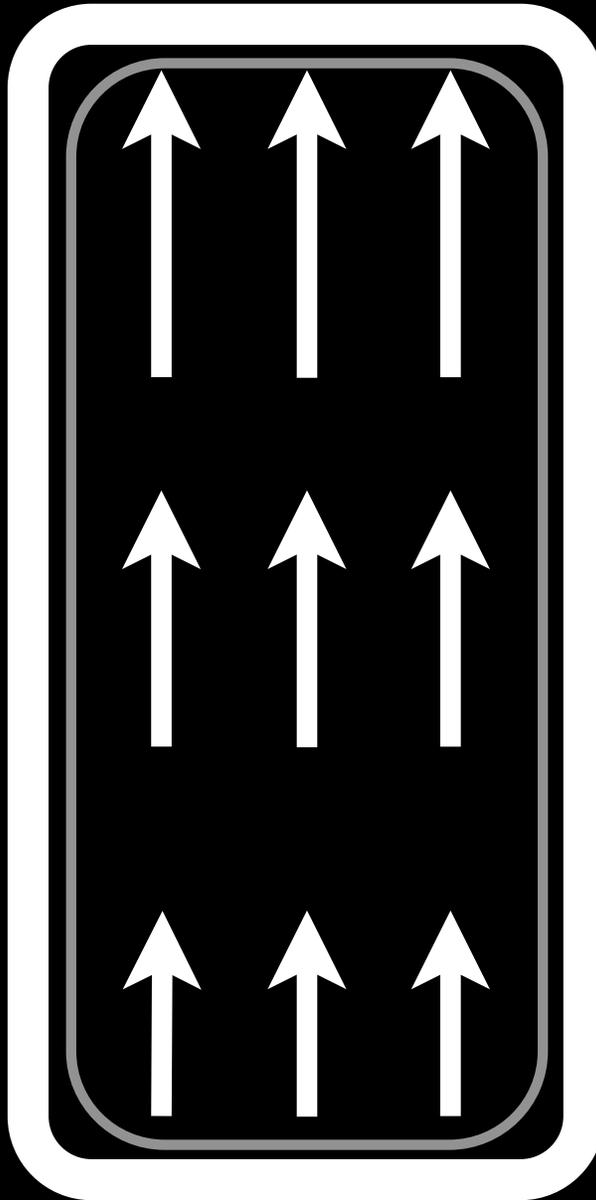
B_0



$$\omega = \gamma B_0$$

Length of arrow indicates strength of local field.

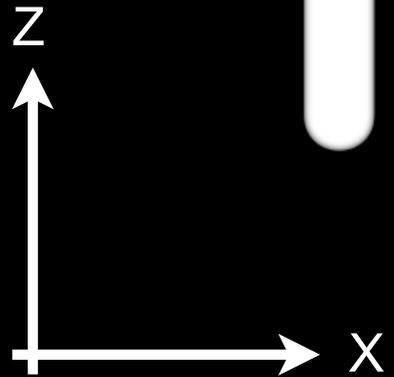
Z-Gradients



$$B_0 + \delta B_0$$

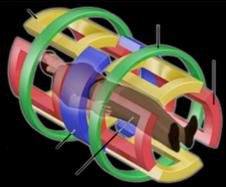
$$B_0$$

$$B_0 - \delta B_0$$

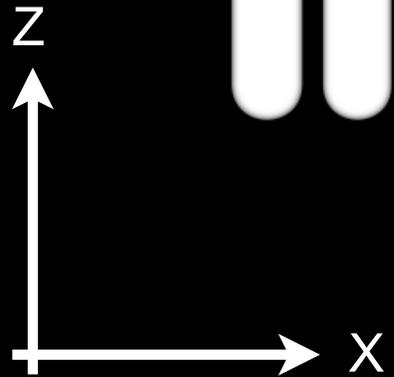
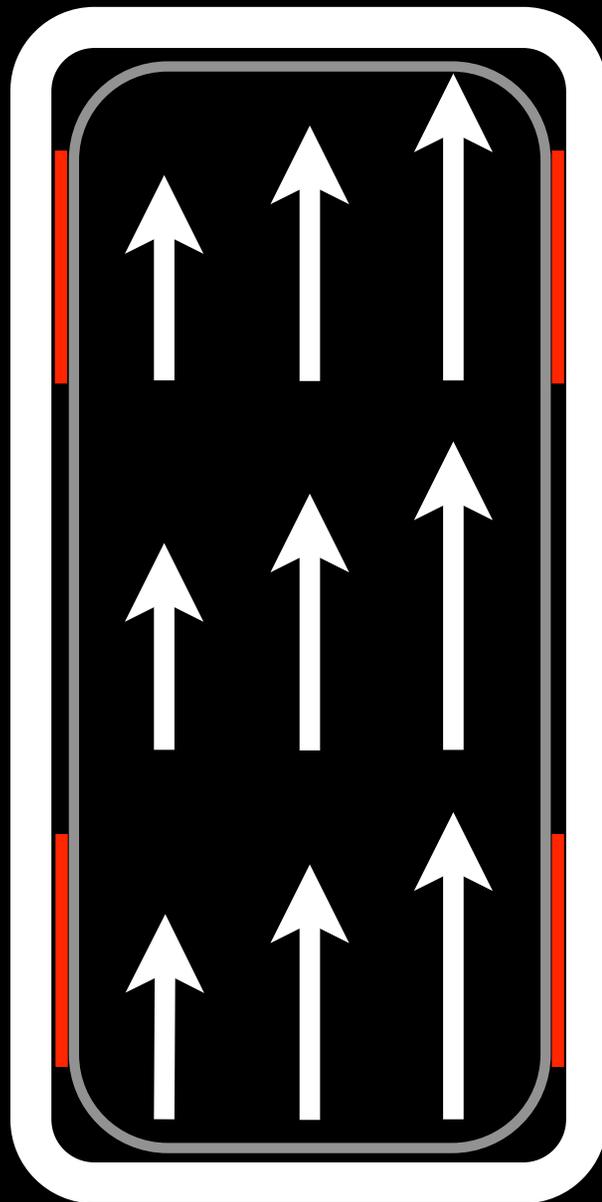


$$\omega(z) = B_0 + G_z \cdot z$$

What coordinate frame are we in?

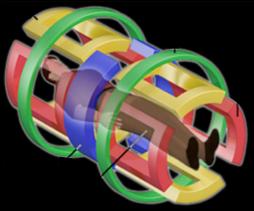


X-Gradients

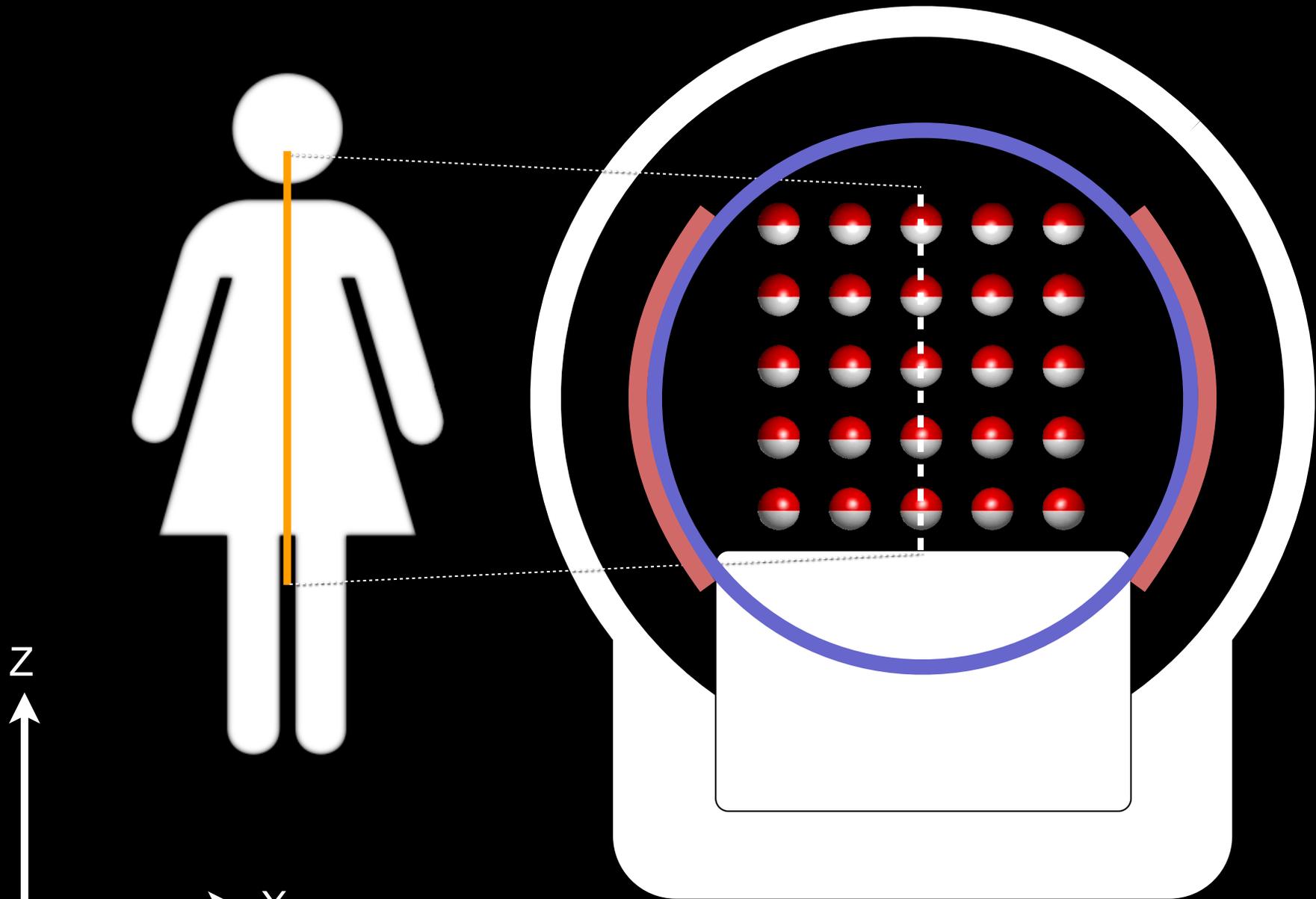


$$\omega(x, z) = B_0 + G_x \cdot x + G_z \cdot z$$

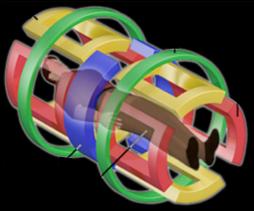
$B_0 - \delta B_0 \quad B_0 \quad B_0 + \delta B_0$



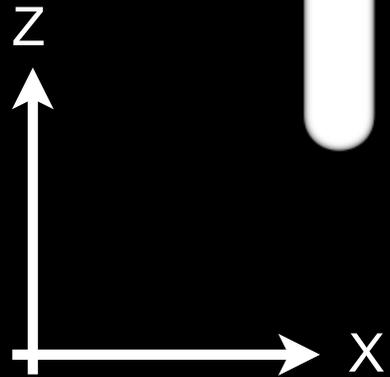
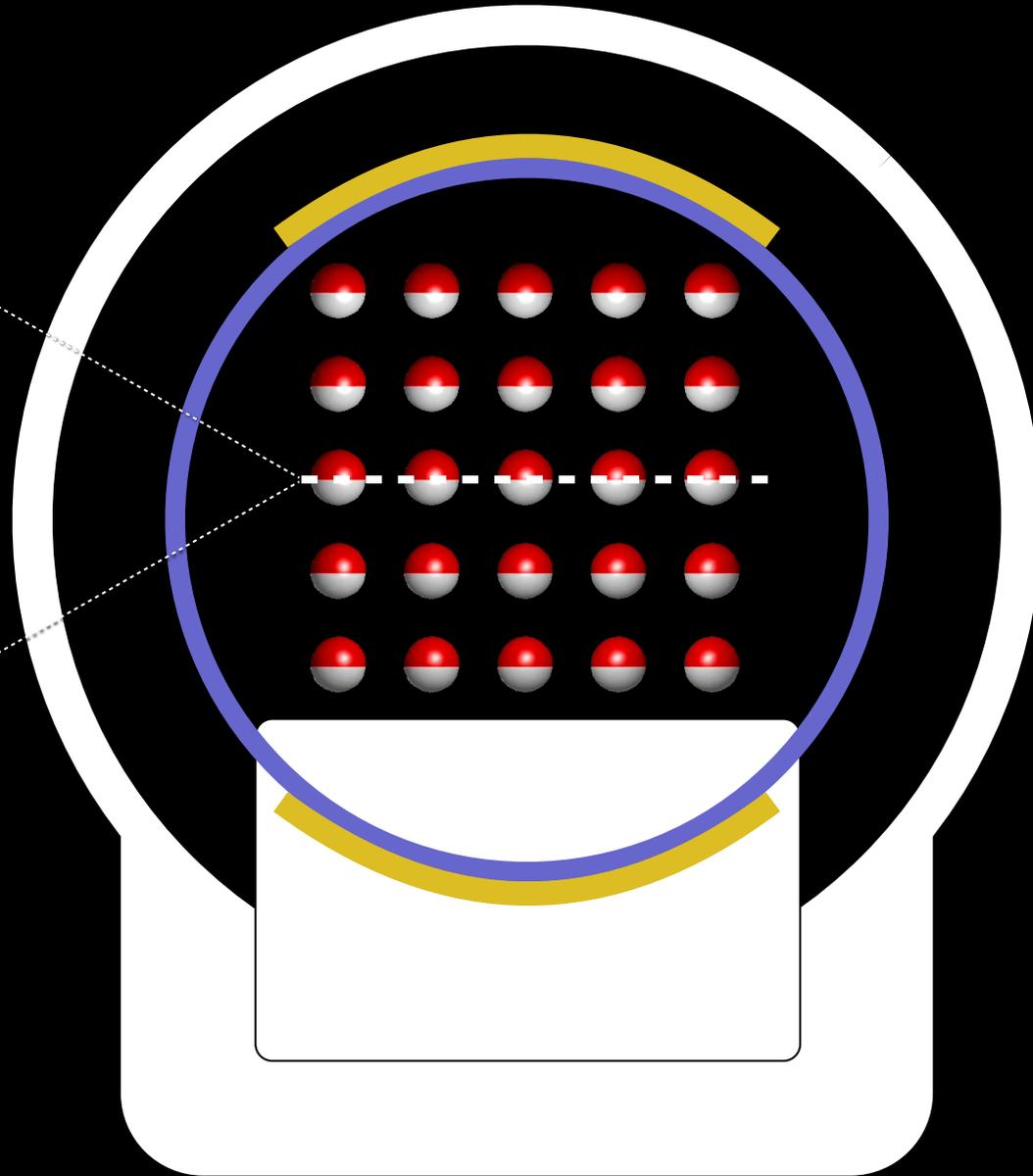
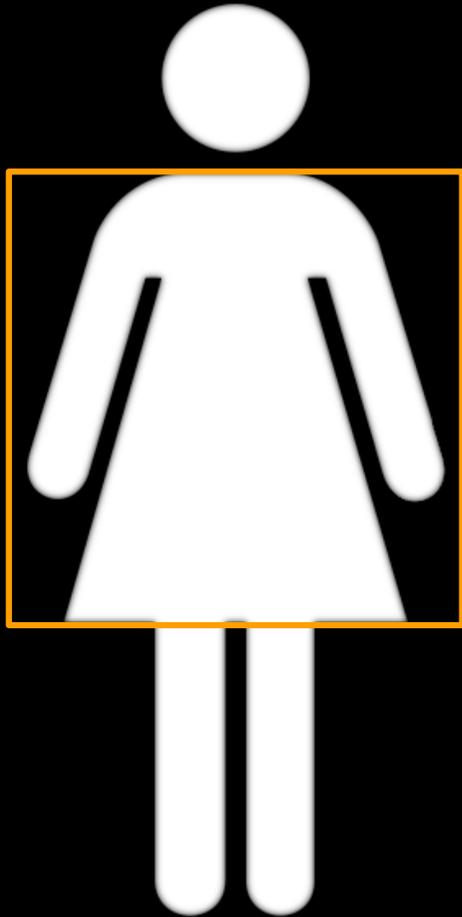
Spins and X-Gradients



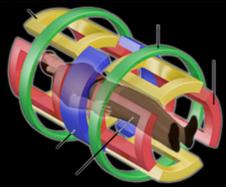
Gradients give rise to isochromats (planes of common frequency).



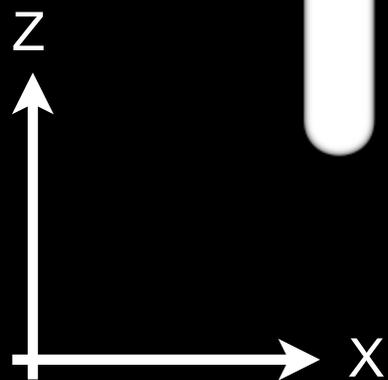
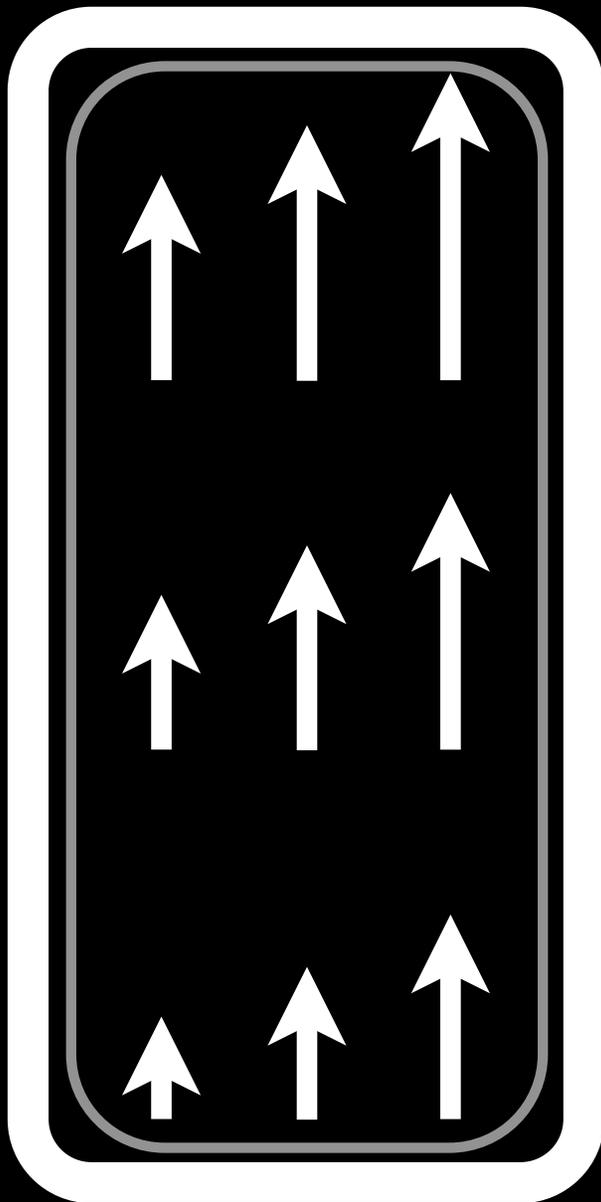
Spins and Y-Gradients

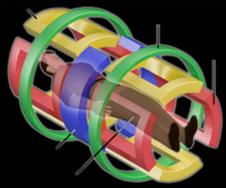


Gradients add/subtract to B_0 along a specific direction.



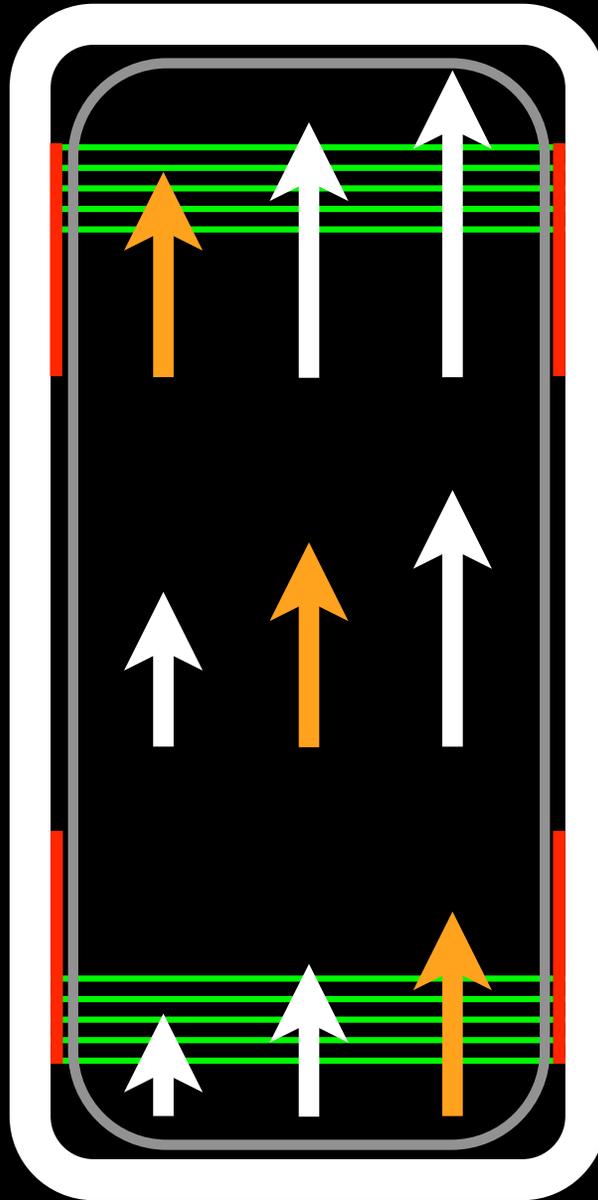
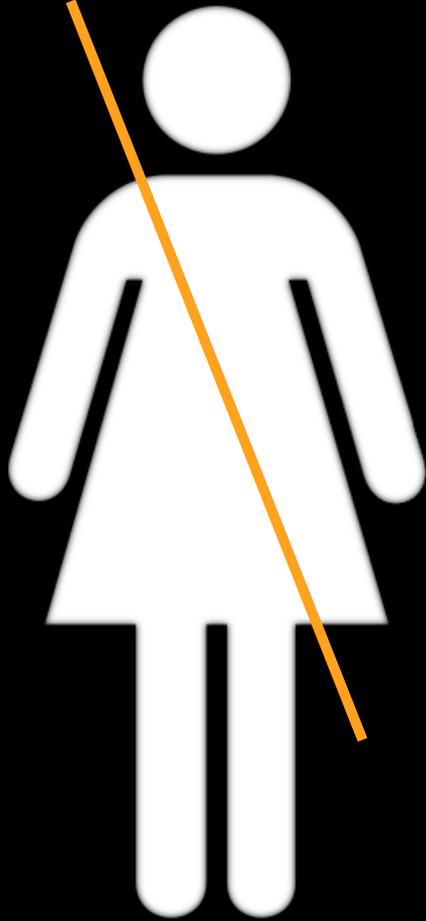
How do we do this?



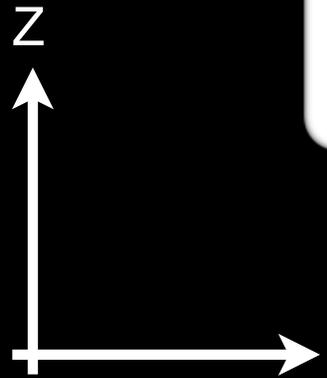


X+Z-Gradients

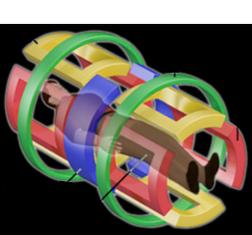
Possible Slice



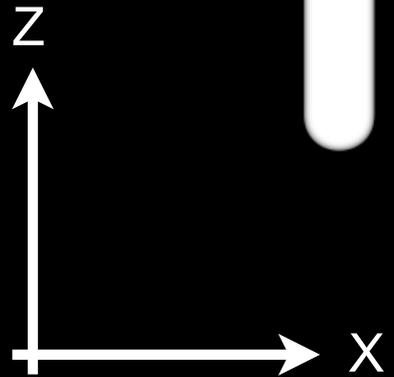
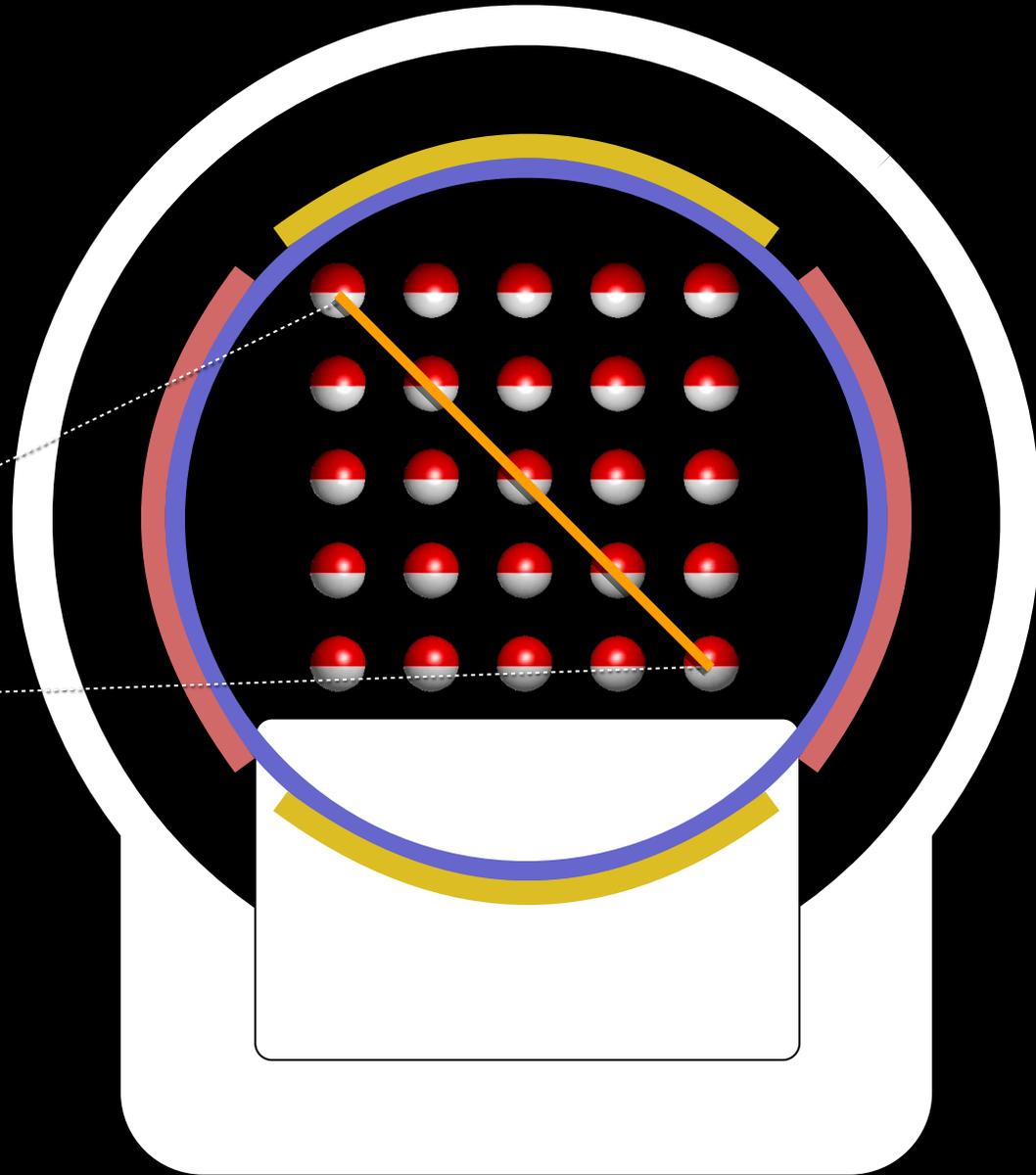
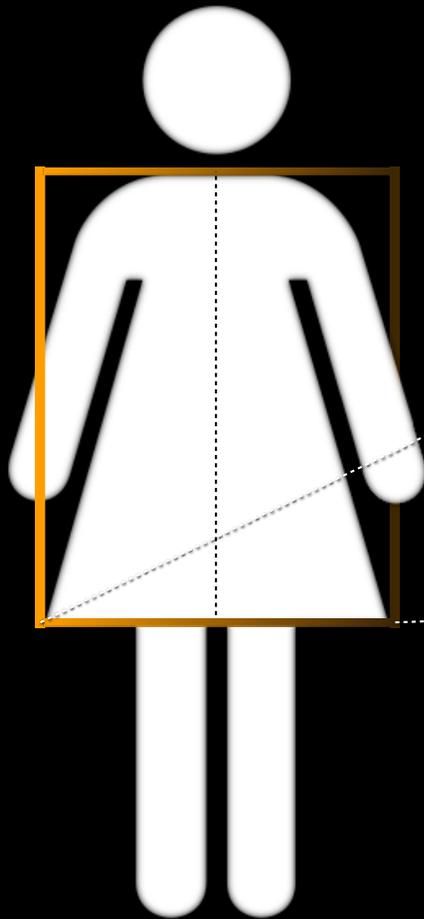
Spin
Isochromat



$$\omega(x, z) = B_0 + G_x \cdot x + G_z \cdot z$$



Spins and X- & Y-Gradients



Simultaneous gradients create an arbitrary isochromat plane.

To the Board

Gradient Hardware

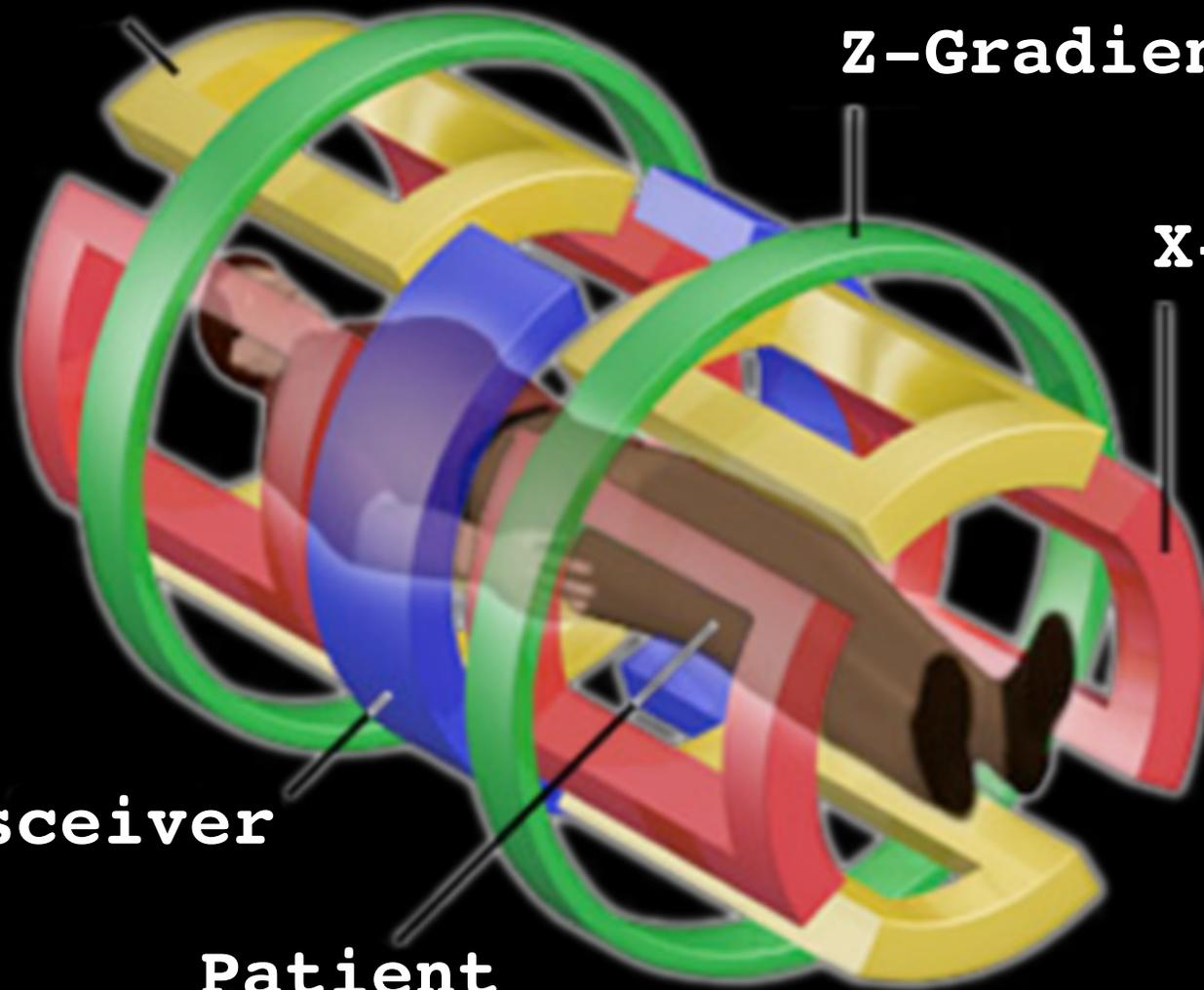
Y-Gradient

Z-Gradient

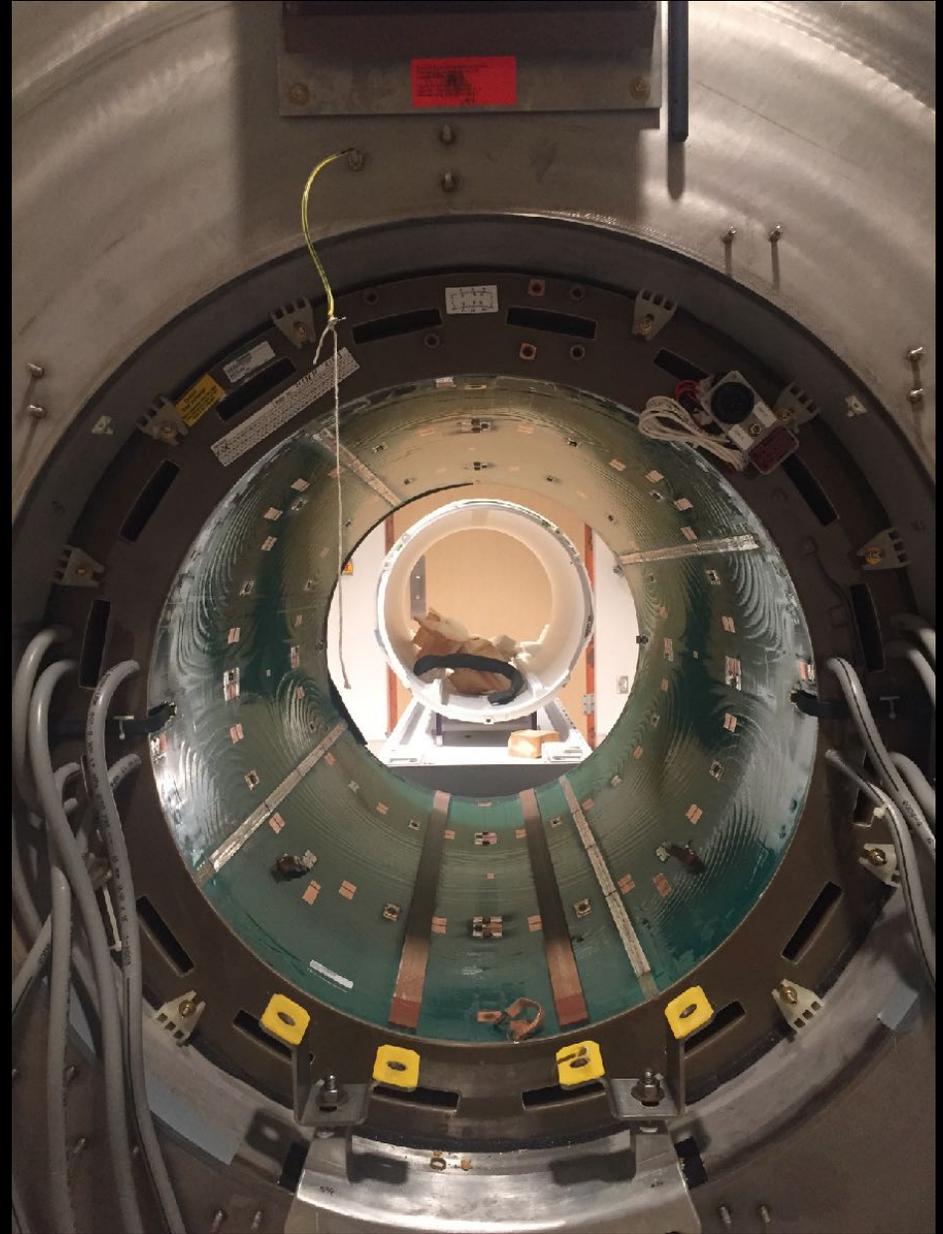
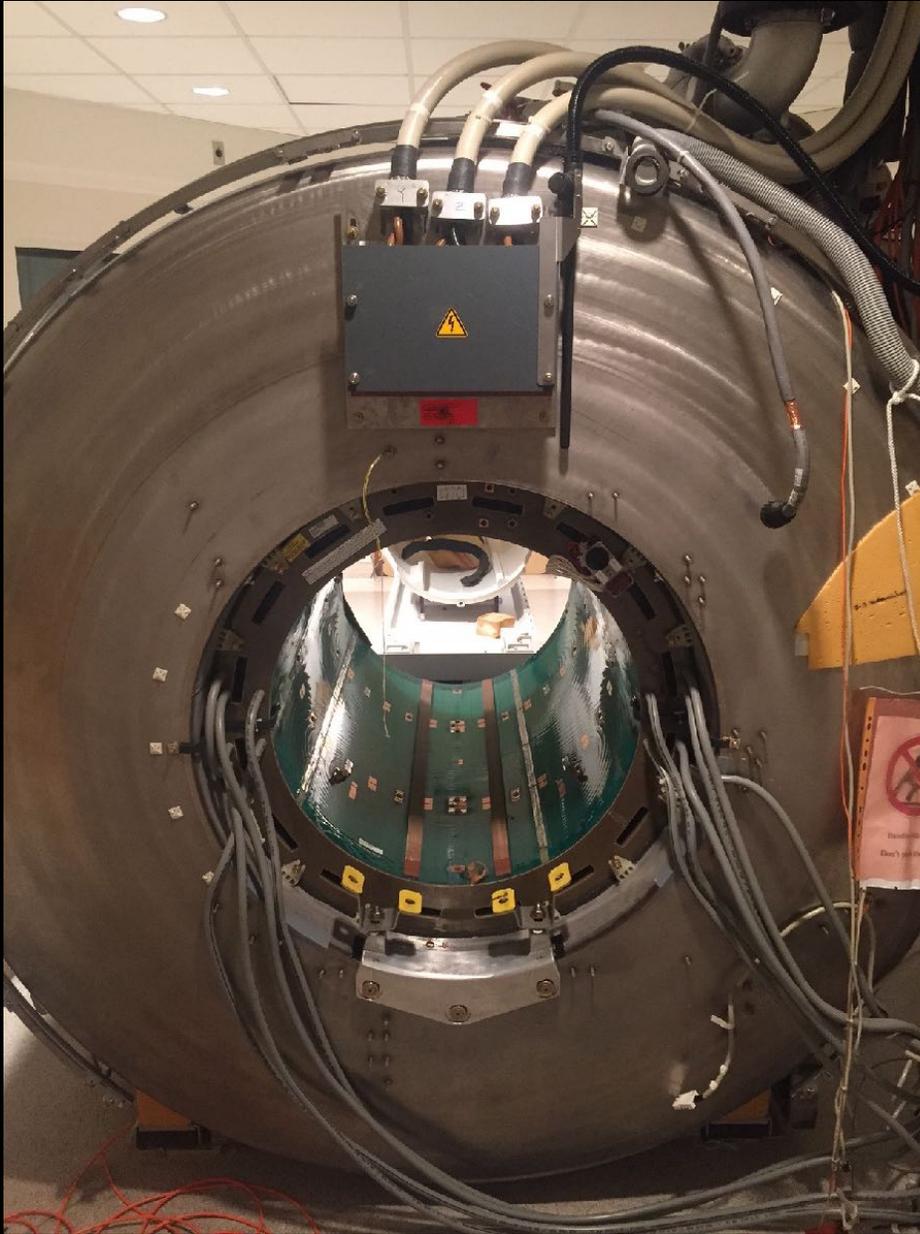
X-Gradient

Transceiver

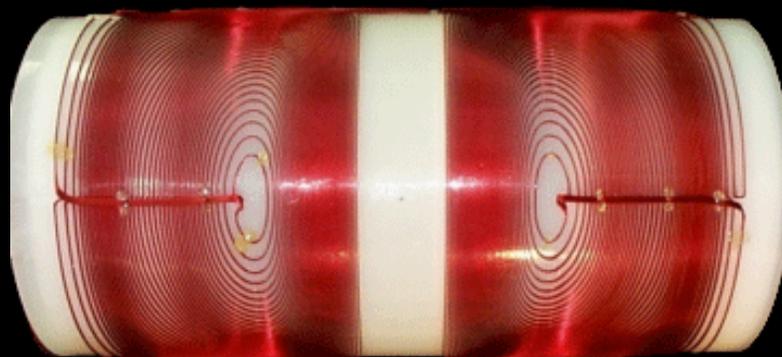
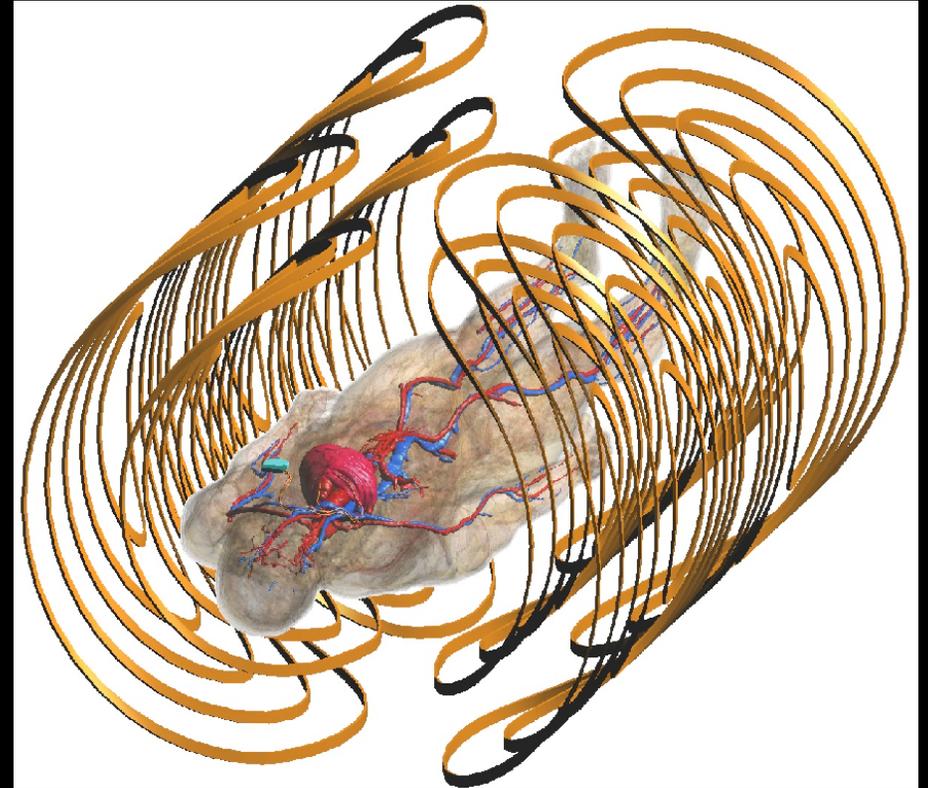
Patient



Gradient Hardware

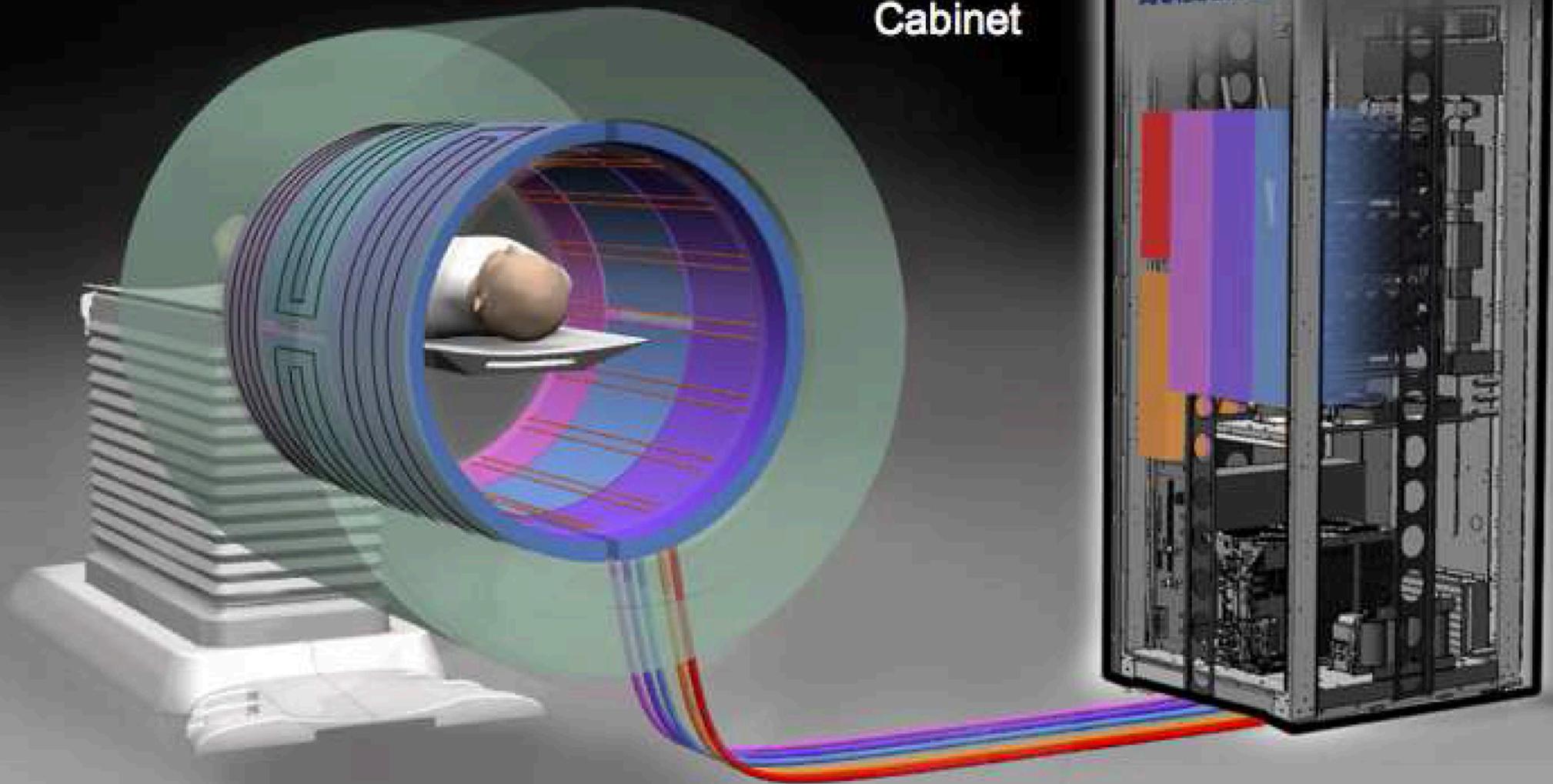


Gradient Hardware



Gradient Hardware

Integrated
MR Power
Cabinet



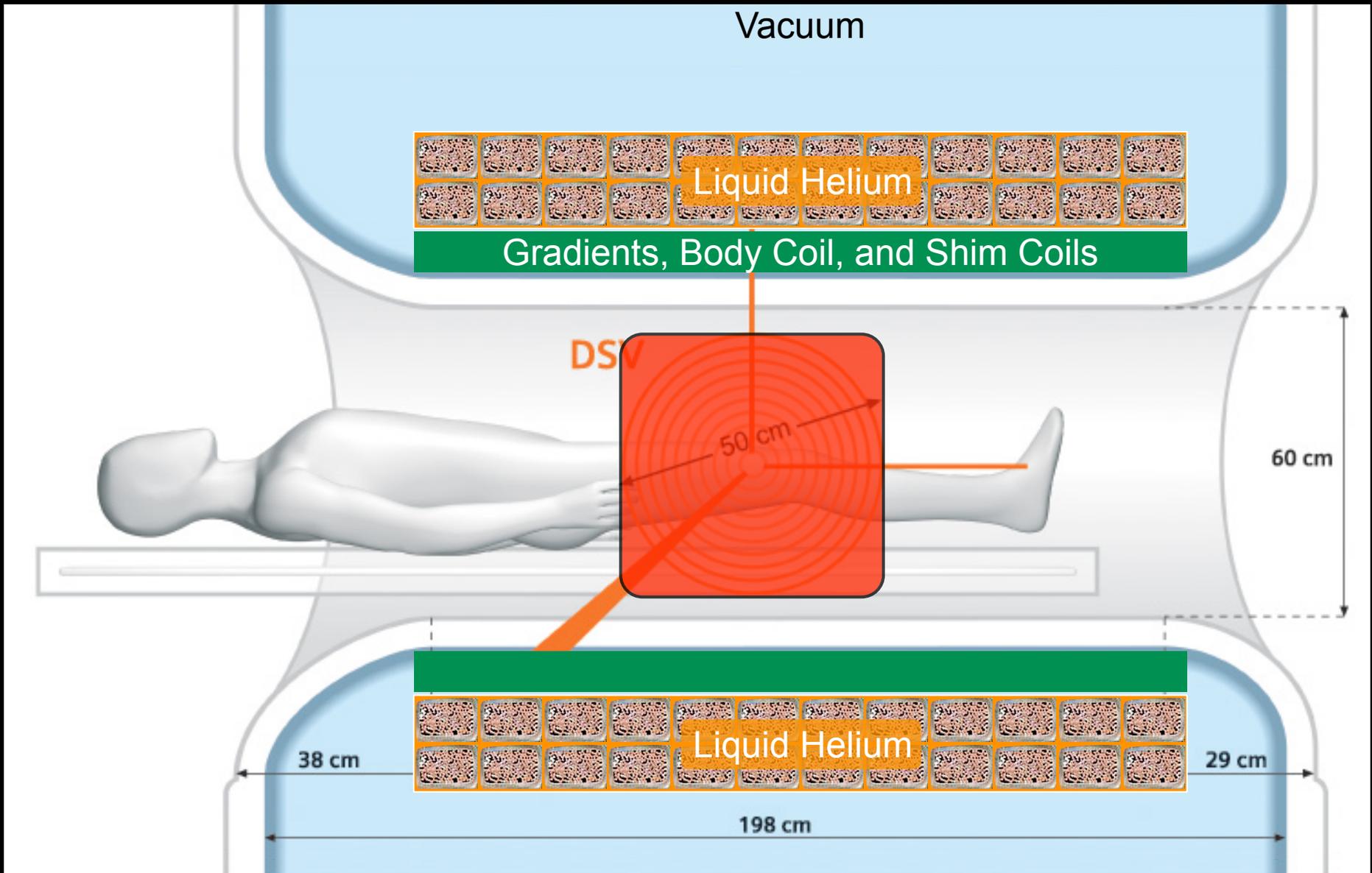
Gradients

- Primary function
 - Encode spatial information
 - Slice selection
 - Phase encoding
 - Frequency encoding
- Secondary functions
 - Sensitize/de-sensitize images to motion
 - Minimize artifacts (crushers & spoilers)
 - Magnetization **re**-phasing in slice selection
 - Magnetization **de**-phasing during readout

Gradients

- Gradients are a:
 - Small
 - $<5\text{G/cm}$ ($<0.0075\text{T}$ @ edge of 30cm FOV)
 - Spatially varying
 - Linear gradients
 - Adds to B_0 only in Z-direction
 - Time varying
 - Slewrate Max. $\sim 150\text{-}200\text{mT/m/ms}$
 - Magnetic field
 - Adds/Subtracts to the B_0 field
 - Parallel to B_0
- Gradients are NOT:
 - Fields perpendicular to B_0

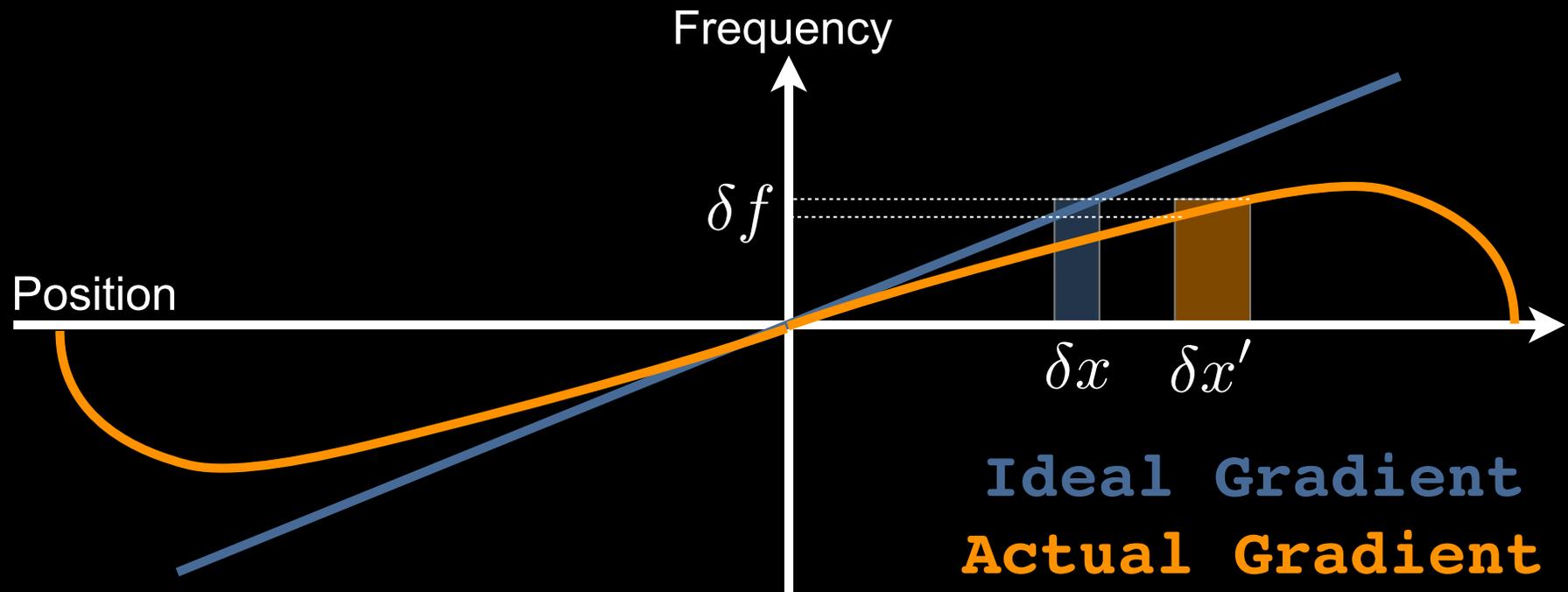
Gradients



Gradients are “linear” over ~40-50cm on each axis.

Gradient Non-linearity

Gradient Non-linearity

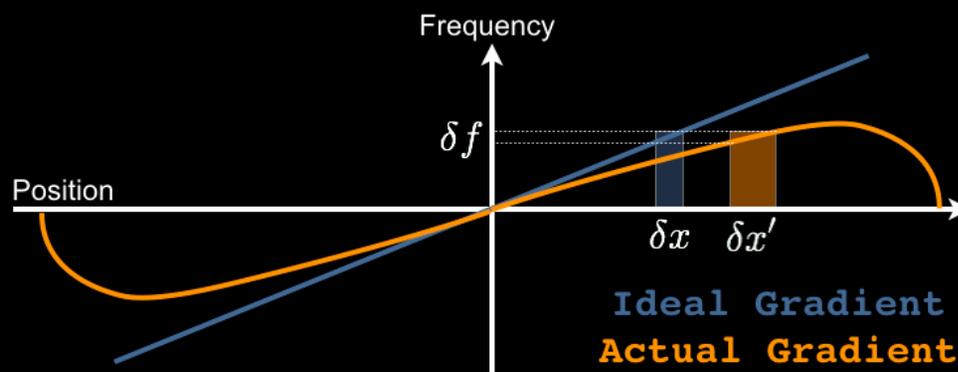


Ideally spatial position is linearly related to frequency.

Gradient Non-linearity

- Basic assumption in MRI is that the z-component of the B-field created by the gradient coils varies linearly with x, y, or z over the FOV.
- Higher gradient amplitudes and slew rates can be achieved by compromising on spatial linearity.
- Gradient non-linearity causes geometric and intensity distortions.

Gradient Non-linearity



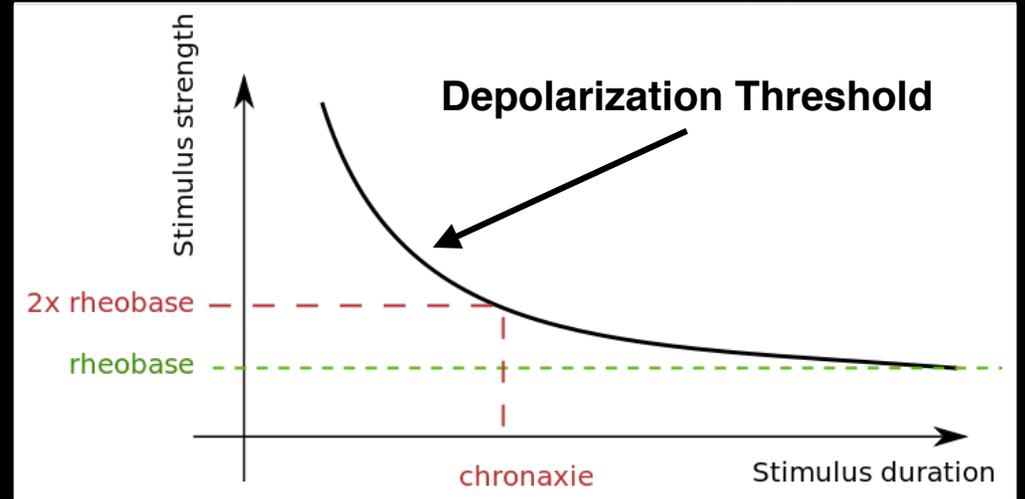
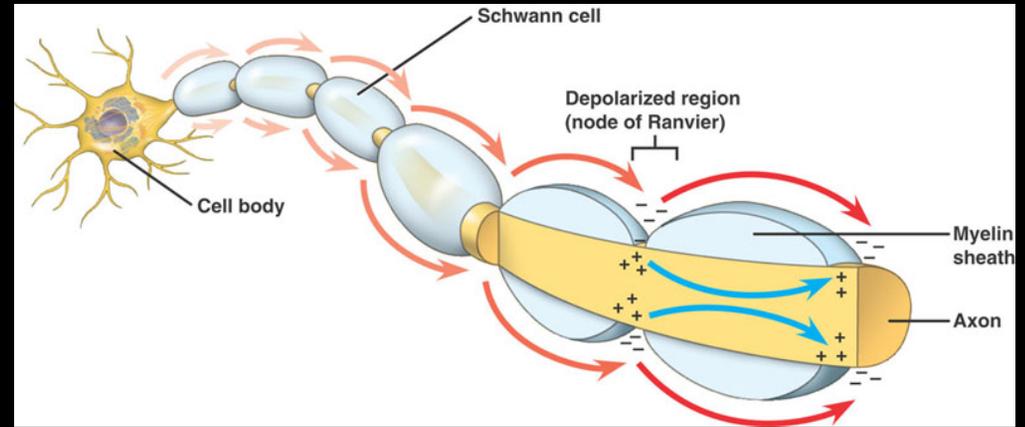
Solution

- **Improve hardware and linearity!**
- **Pay attention to FOV!**
- **Image warping parameters that are system specific and applied to all images.**
 - **Works well qualitatively.**
 - **Can be problematic quantitatively.**

Gradient Safety

Gradient Safety

- Noise
- Peripheral nerve stimulation (PNS)



Solution: De-rate gradient slew rates, but this increases scan time.



Solution: Ear plugs



Head phones

Time-varying gradients induce mechanical vibrations and PNS.

MRI Gradient Noise



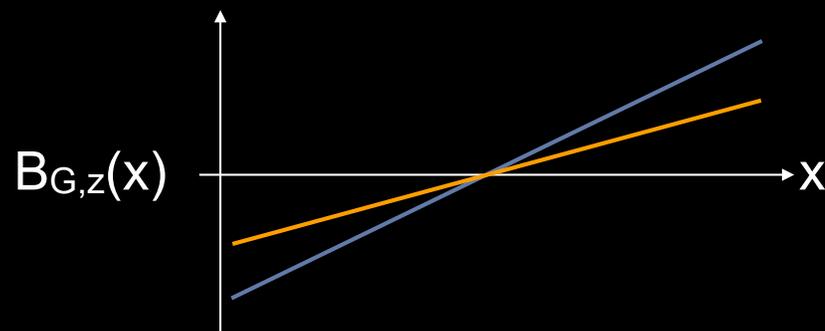
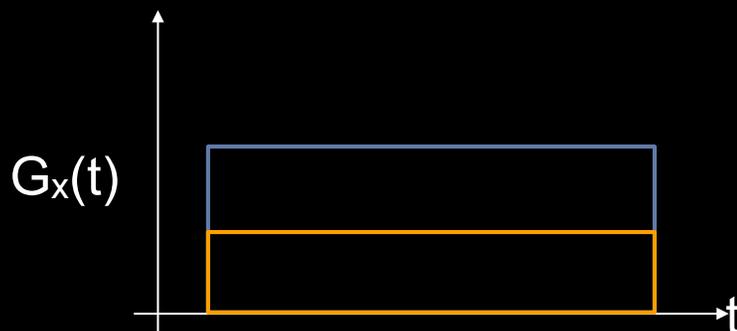
Gradient Noise

- Jet take-off @ 25m ~150 dB (eardrum rupture)
- Car horn @ 1m ~110 dB (borderline painful)
- Live rock band ~100 dB
- **MRI gradients full load** ≤99 dB
- Garbage disposal ~80 dB
- **MRI gradients basic load** ≤75 dB
- Radio or TV Audio ~70dB



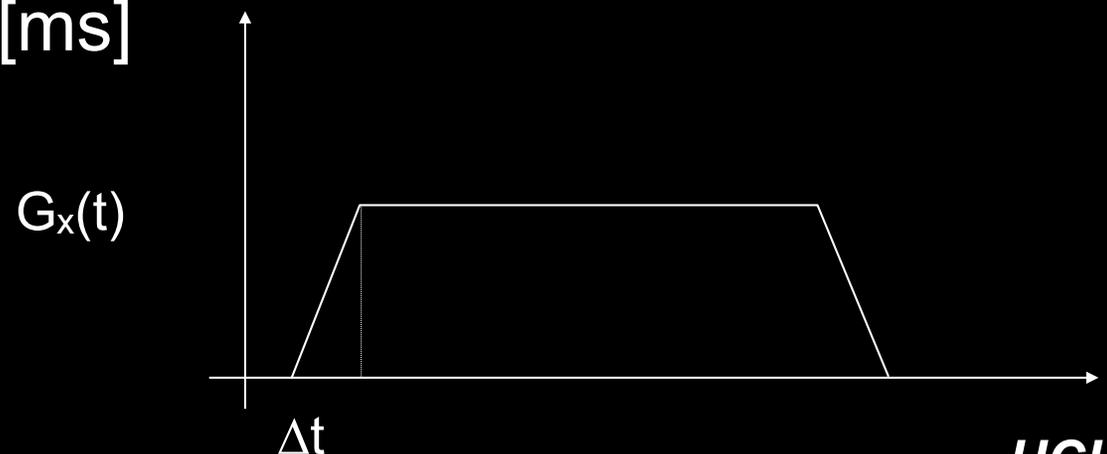
Gradient Safety – G_{Max}

- G_{max} limitations:
 - Concern: None known.
 - B_0 is already pretty big.
 - Conventional Gradients
 - $G_{Max} = 4$ to $5G/cm$ ($=50mT/m$)
 - Cutting Edge Gradients
 - $G_{Max} = 8G/cm$ ($=80mT/m$)
 - Connectome Gradients
 - $G_{Max} = 30G/cm$ ($=300mT/m$)
 - Consider the ΔB contributed by a gradient...



Gradient Slewrate

- **Gradient slew rate**
 - T/m/s (or G/cm/s)
 - dG/dt – Rate of change of gradient amplitude
- **Slew rate limited by dB/dt:**
 - Concern: Peripheral Nerve Stimulation
 - Regulated by FDA
 - Normal Mode: $dB/dt = 16 \text{ T/s} \cdot (1 + 0.36/\beta)$
 - First Level Mode: $dB/dt = 20 \text{ T/s} \cdot (1 + 0.36/\beta)$
 - $\beta = \text{stimulus duration [ms]}$



Questions?

- Related reading materials
 - Nishimura - Chap 5

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