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# Fast Imaging, Advanced Image Reconstruction

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M219 Principles and Applications of MRI

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# Review: Basic Recon

# The Fourier Transform

$$S(\vec{k}) = \int_{-\infty}^{+\infty} I(\vec{r}) e^{-i2\pi\vec{k}\cdot\vec{r}} d\vec{r}$$

MRI Signal Equation

$$S(\vec{k}) \xleftrightarrow{\mathcal{F}} I(\vec{r})$$

$$S(k_x) = \int_{-\infty}^{+\infty} I(x) e^{-i2\pi(k_x x)} dx$$

1D

$$S(k_x, k_y) = \int_{-\infty}^{+\infty} \int_{-\infty}^{+\infty} I(x, y) e^{-i2\pi(k_x x + k_y y)} dx dy$$

2D

$$S(k_x, k_y, k_z) = \int_{-\infty}^{+\infty} \int_{-\infty}^{+\infty} \int_{-\infty}^{+\infty} I(x, y, z) e^{-i2\pi(k_x x + k_y y + k_z z)} dx dy dz$$

3D

# Finite Sampling

$S(k)$  is measured at  $k \in \mathcal{D}$

$$\mathcal{D} = \{n\Delta k, -N/2 \leq n \leq +N/2\}$$



Fourier  
Step-size

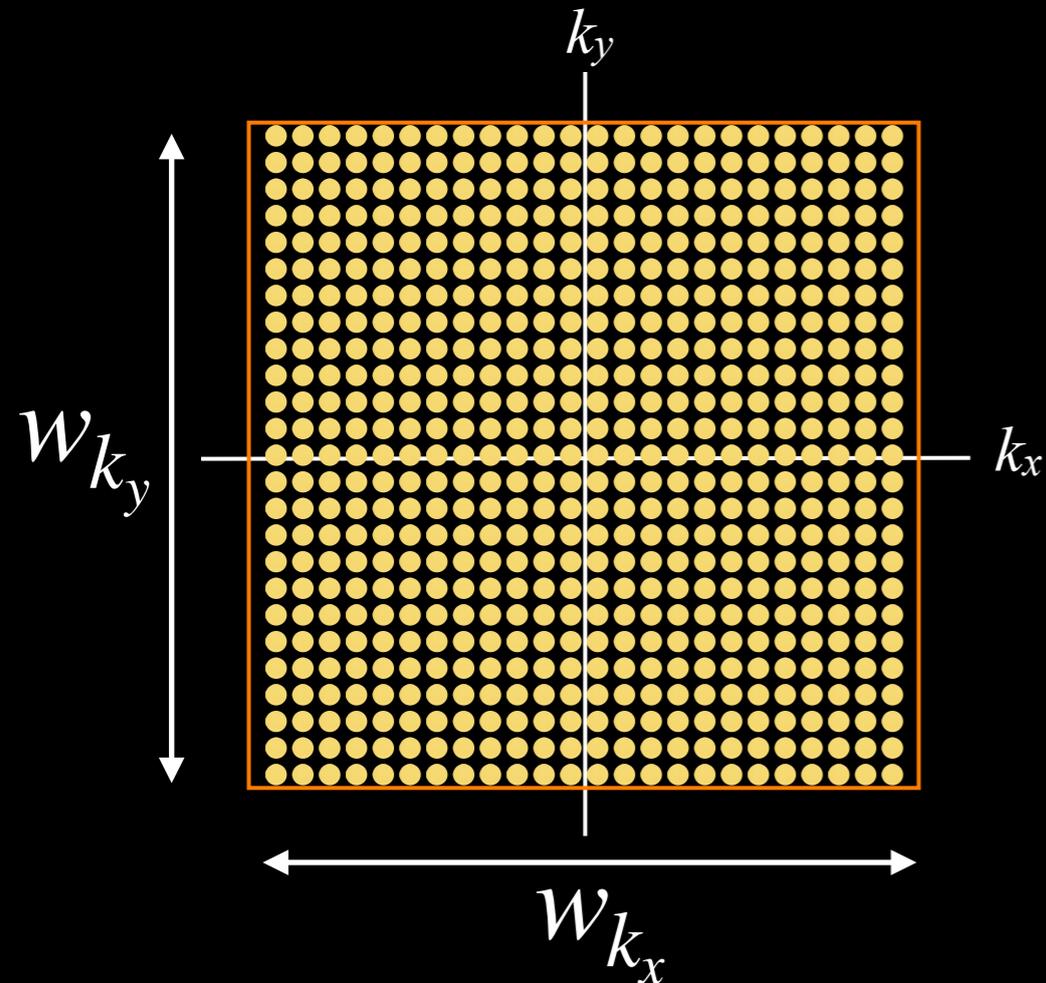


Number of  
Sample Points

$$I(x) = \Delta k \sum_{n=-N/2}^{N/2-1} S[n] e^{i2\pi n \Delta k x}, \quad |x| < \frac{1}{\Delta k} \quad \text{Eqn. 6.20}$$

This is the fundamental image reconstruction equation for MRI.

# Sampling Considerations



$$\Delta k_x = \frac{1}{FOV_x}$$

$$\Delta k_y = \frac{1}{FOV_y}$$

$$w_{k_x} = \frac{1}{\Delta x}$$

$$w_{k_y} = \frac{1}{\Delta y}$$

*Review Sampling Theorem*

*Review Lectures 9&10 on Spatial Localization*

# Noise Considerations

- Signal-to-Noise Ratio (SNR)
  - A fundamental measure of image quality

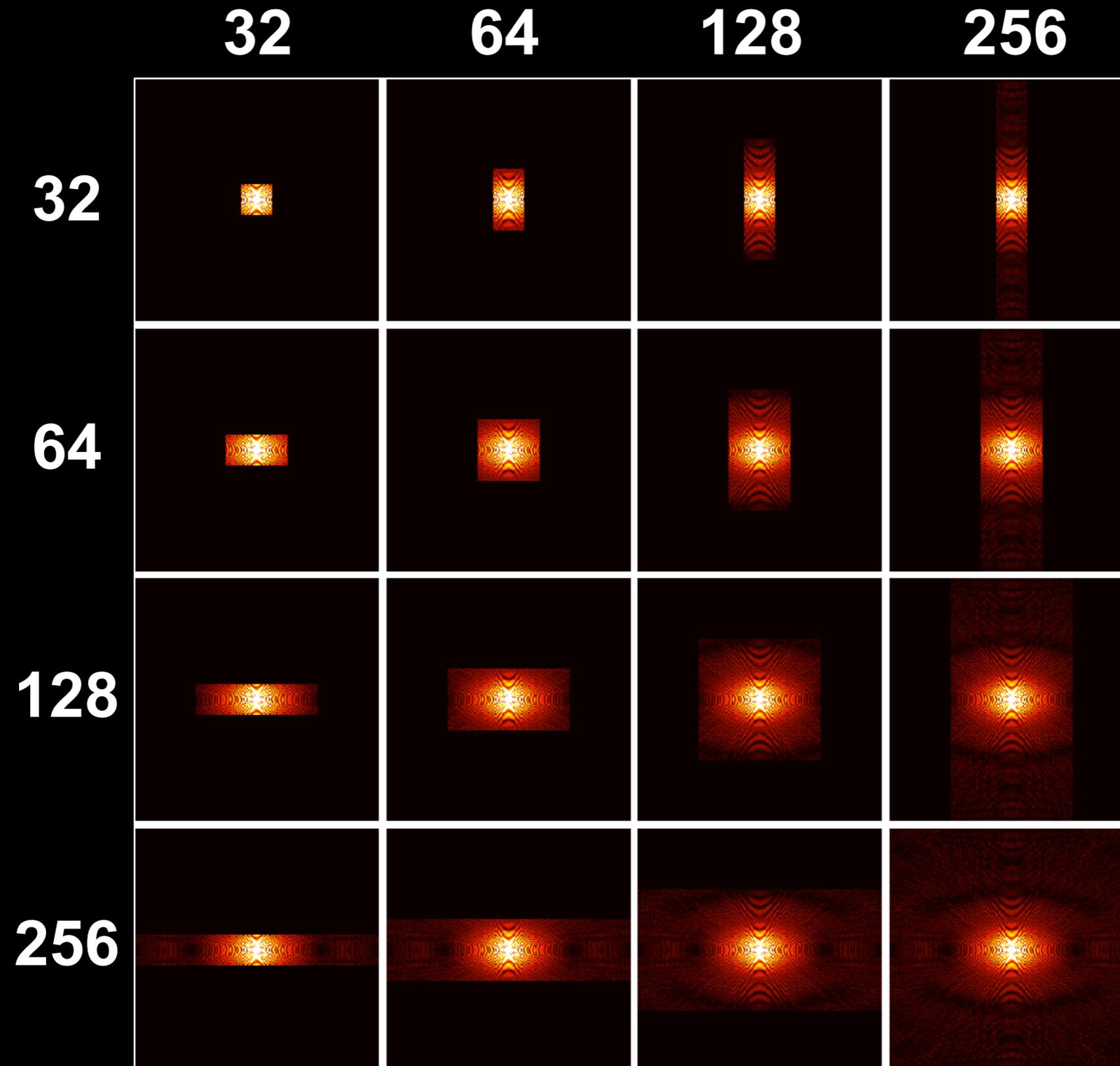
- $SNR \triangleq \frac{\text{signal amplitude}}{\sigma \text{ of noise}}$

- $SNR_{dB} = 20 \cdot \log(SNR)$

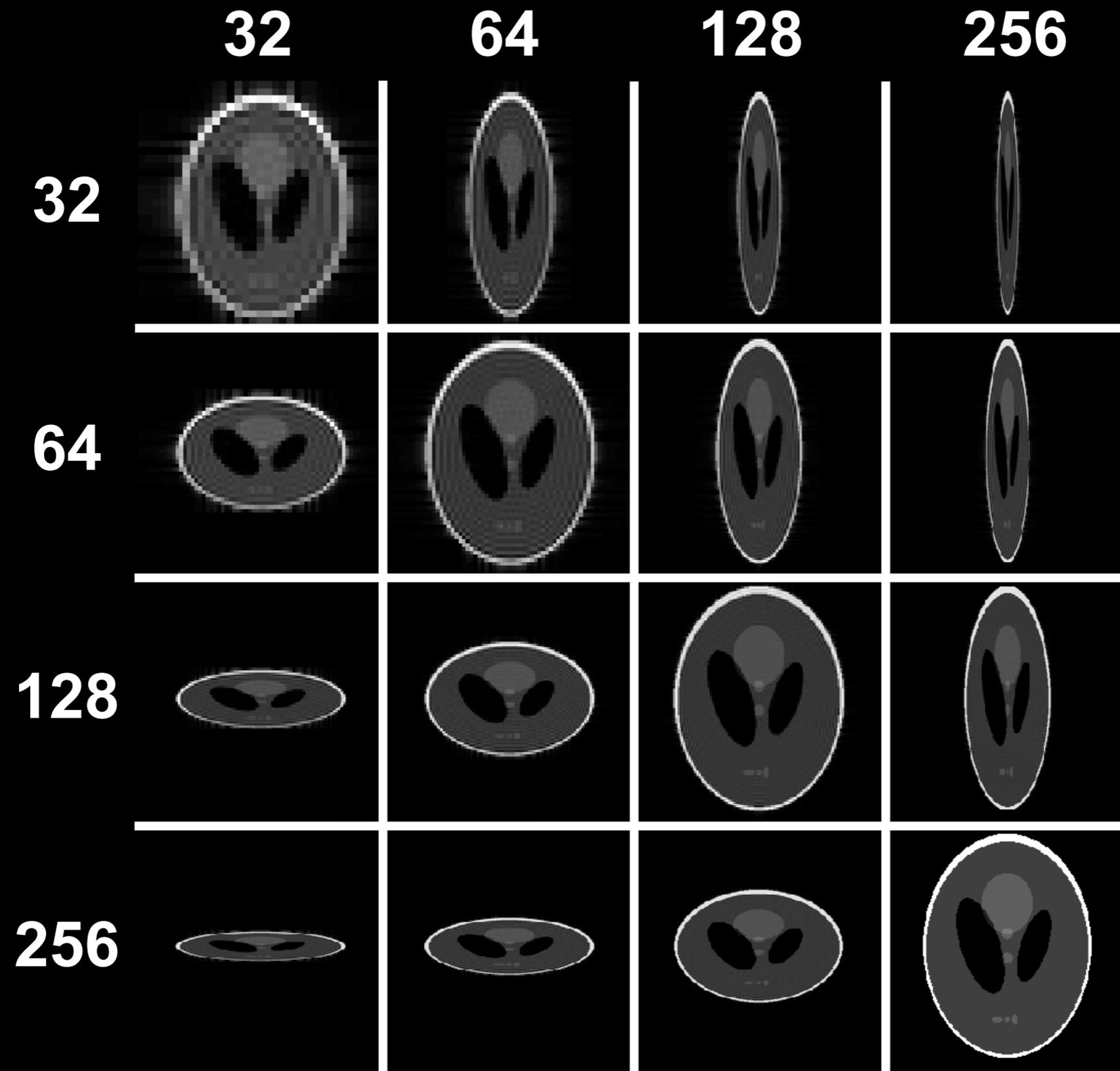
# Noise Considerations

- Summary of Acquisition Time Effects
  - $SNR \propto \sqrt{N_{ave} \cdot T_{read}}$
  - $SNR \propto \sqrt{\text{measurement time}}$
- Effect of Spatial Resolution
  - $SNR \propto (\delta_x)(\delta_y)(\delta_z)$
- Other factors
  - $SNR \propto f(\rho, T_1, T_2, \dots)$

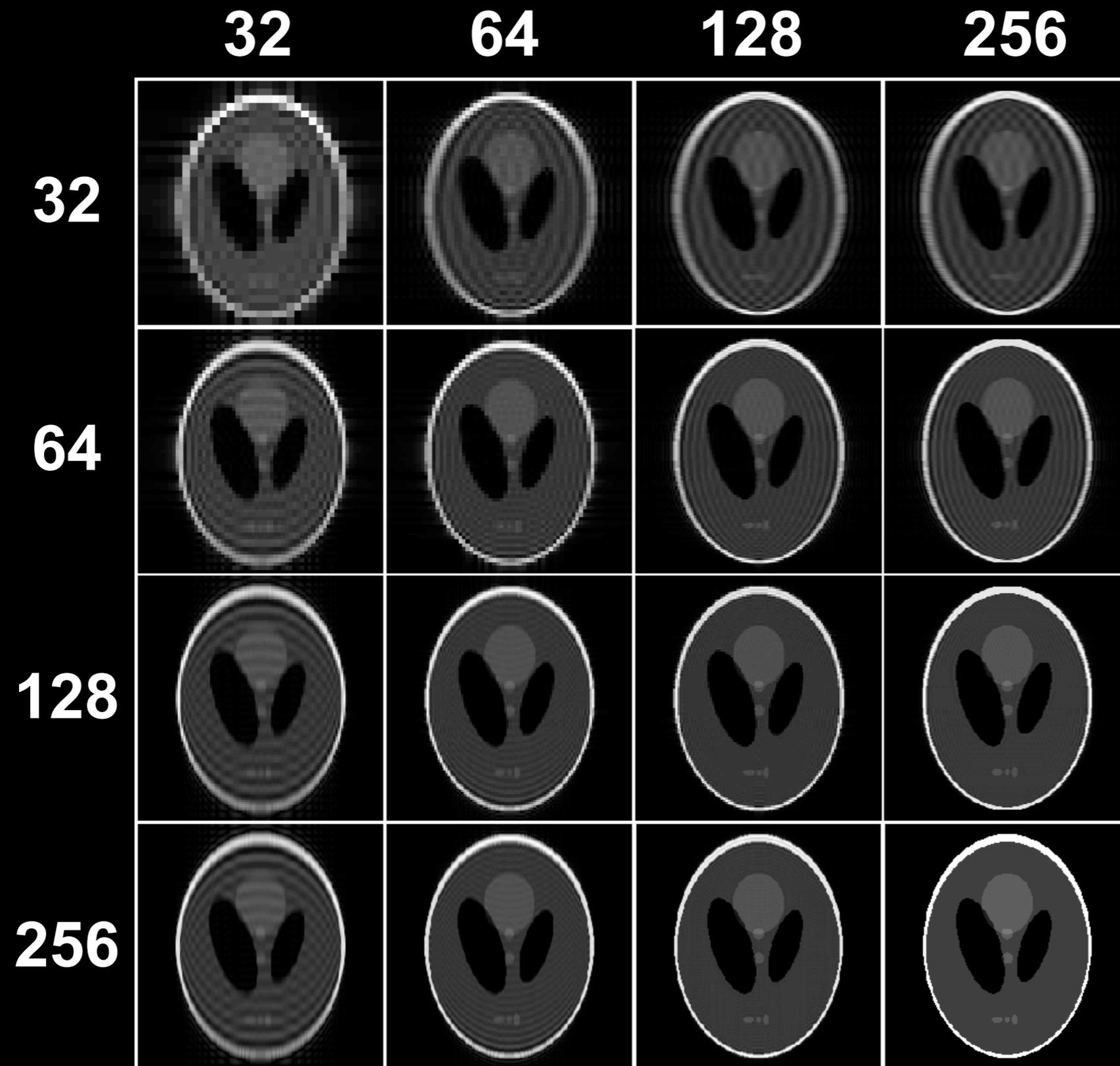
# Gibb's Ringing



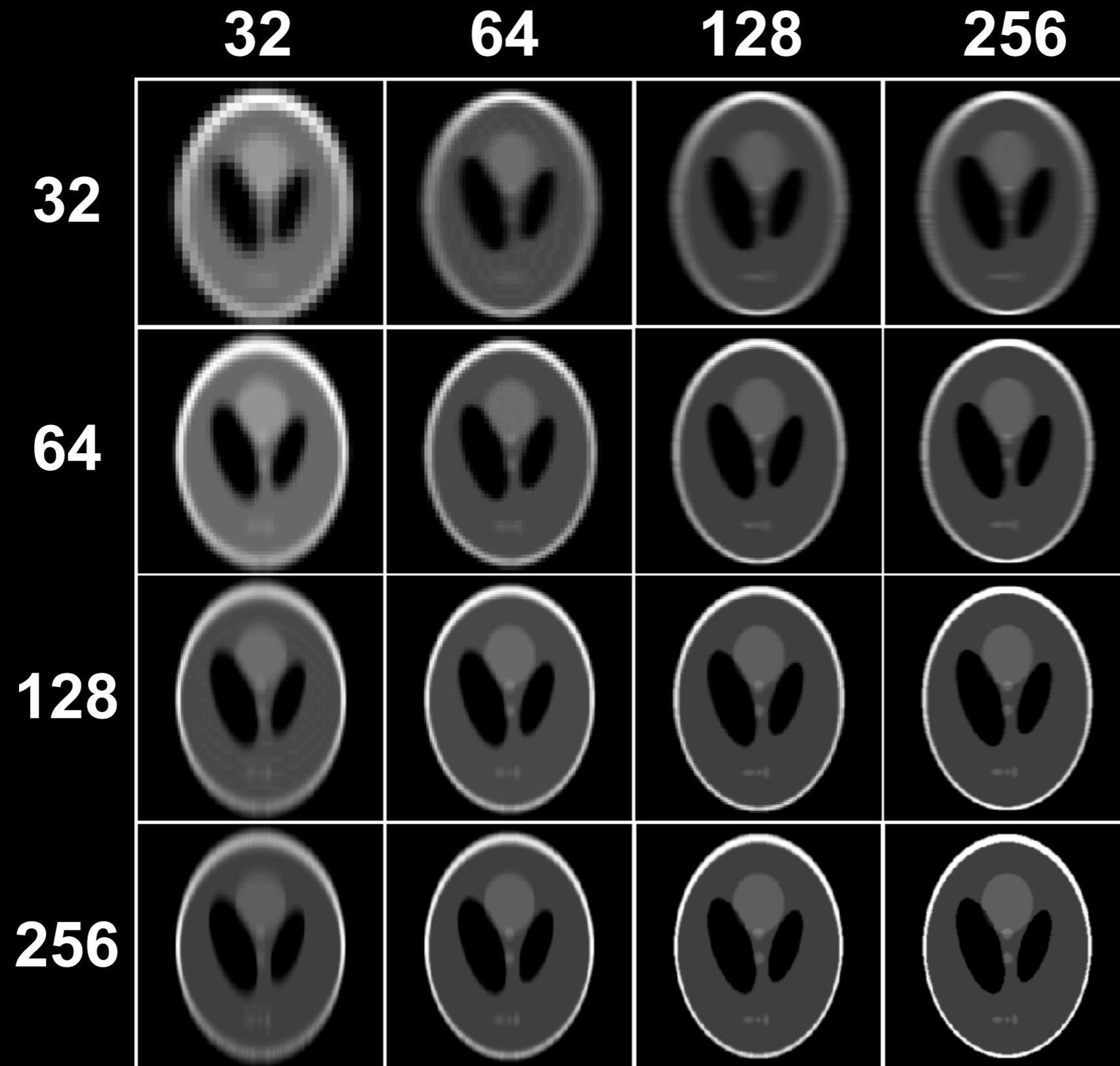
# Gibb's Ringing



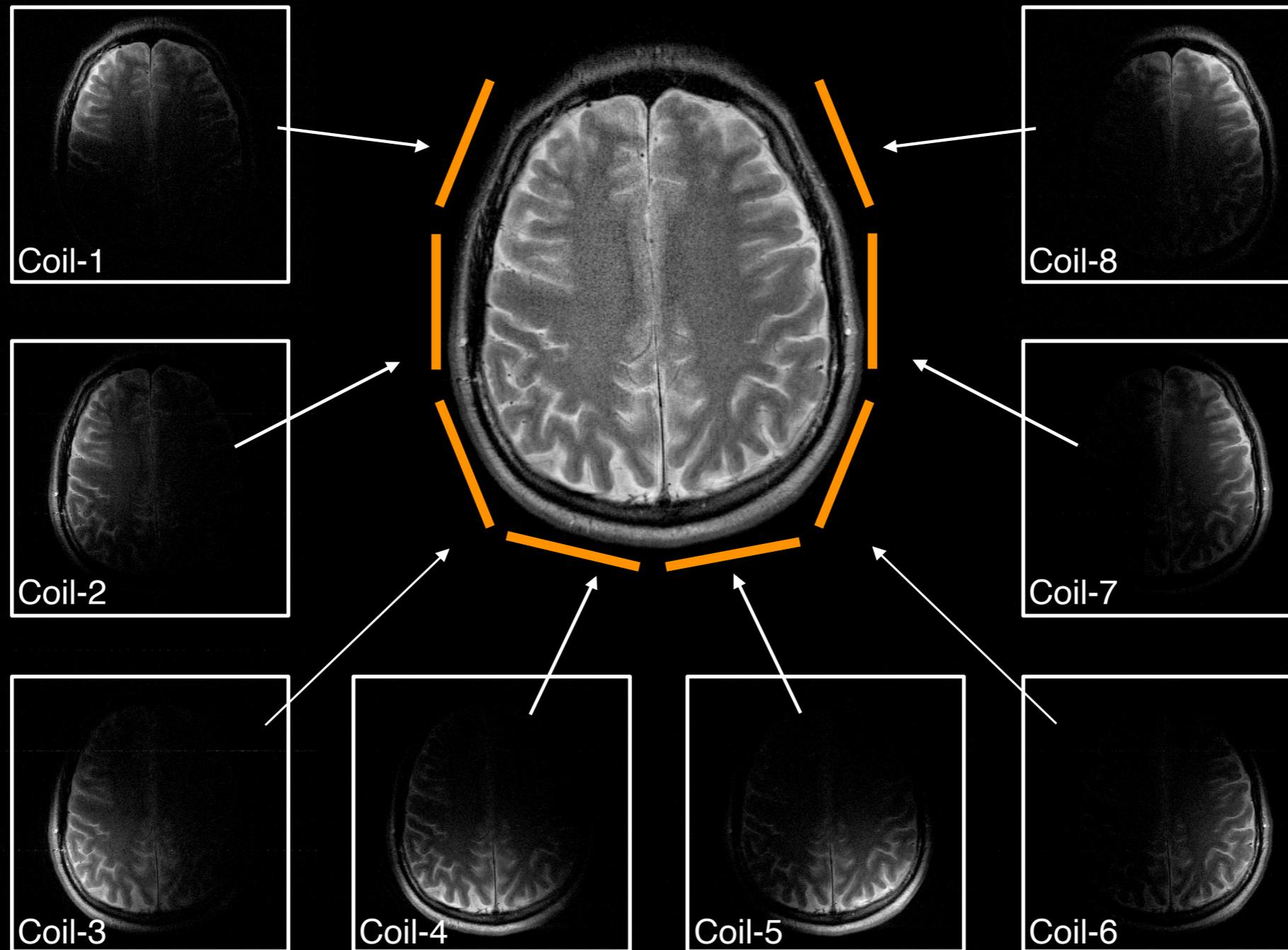
# Zero-Pad



# Hamming Window & Zero-Pad



# Multi-Coil Reconstruction



Each coil element (channel) has a unique sensitivity profile –  $\vec{B}_r(\vec{r})$

# Outline

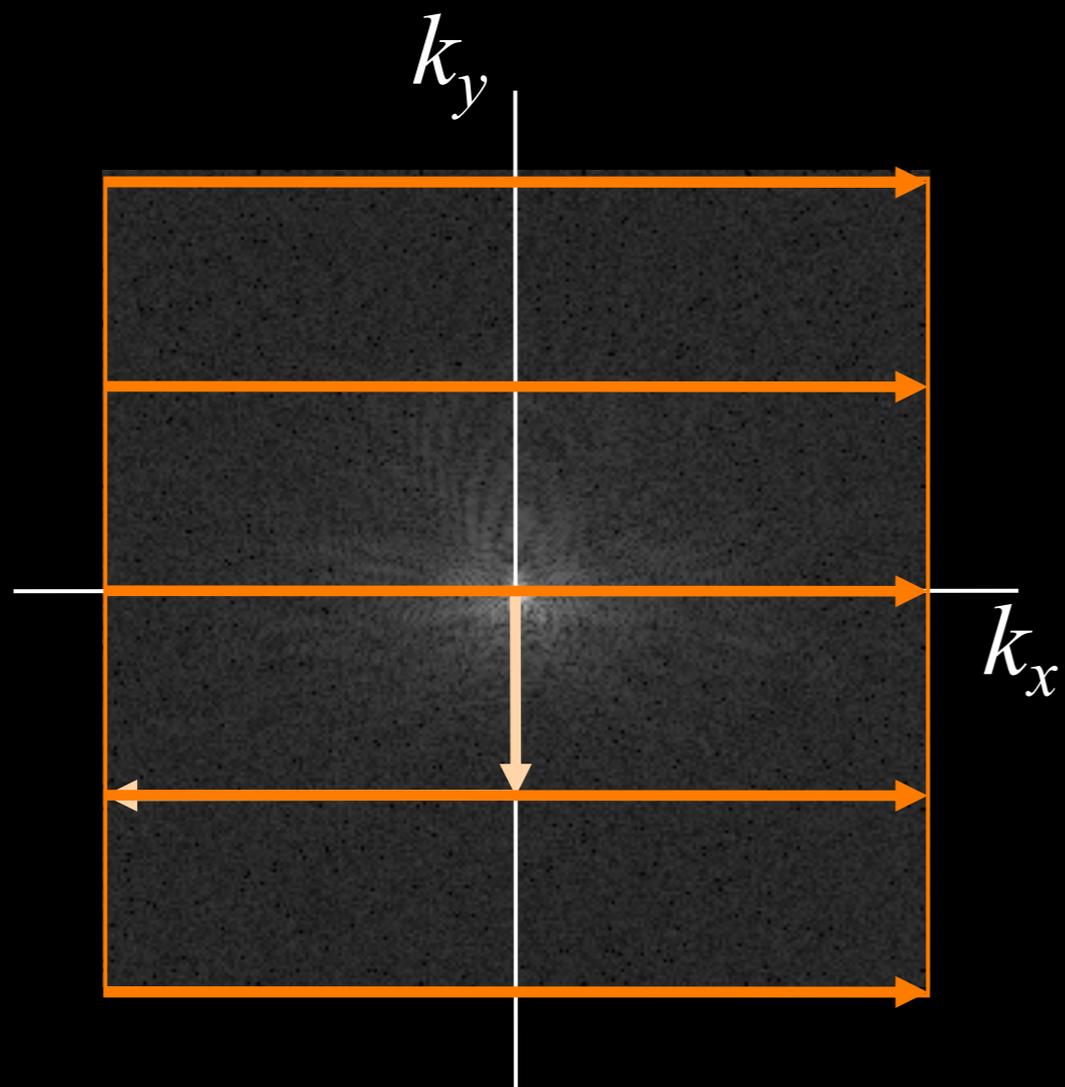
- Fast Imaging
  - Non-Cartesian MRI
  - Echo-planar imaging (EPI)
- Advanced MR Image Reconstruction
  - Parallel imaging
  - ... *and more in upcoming lectures*

# Overview

- Motivation
  - MRI is relatively slow; need to accelerate
- Strategies
  - Efficient pulse sequences
  - Fast k-space sampling trajectories
  - Data undersampling + advanced recon
- Many challenges and trade-offs
- Key drivers for MRI research

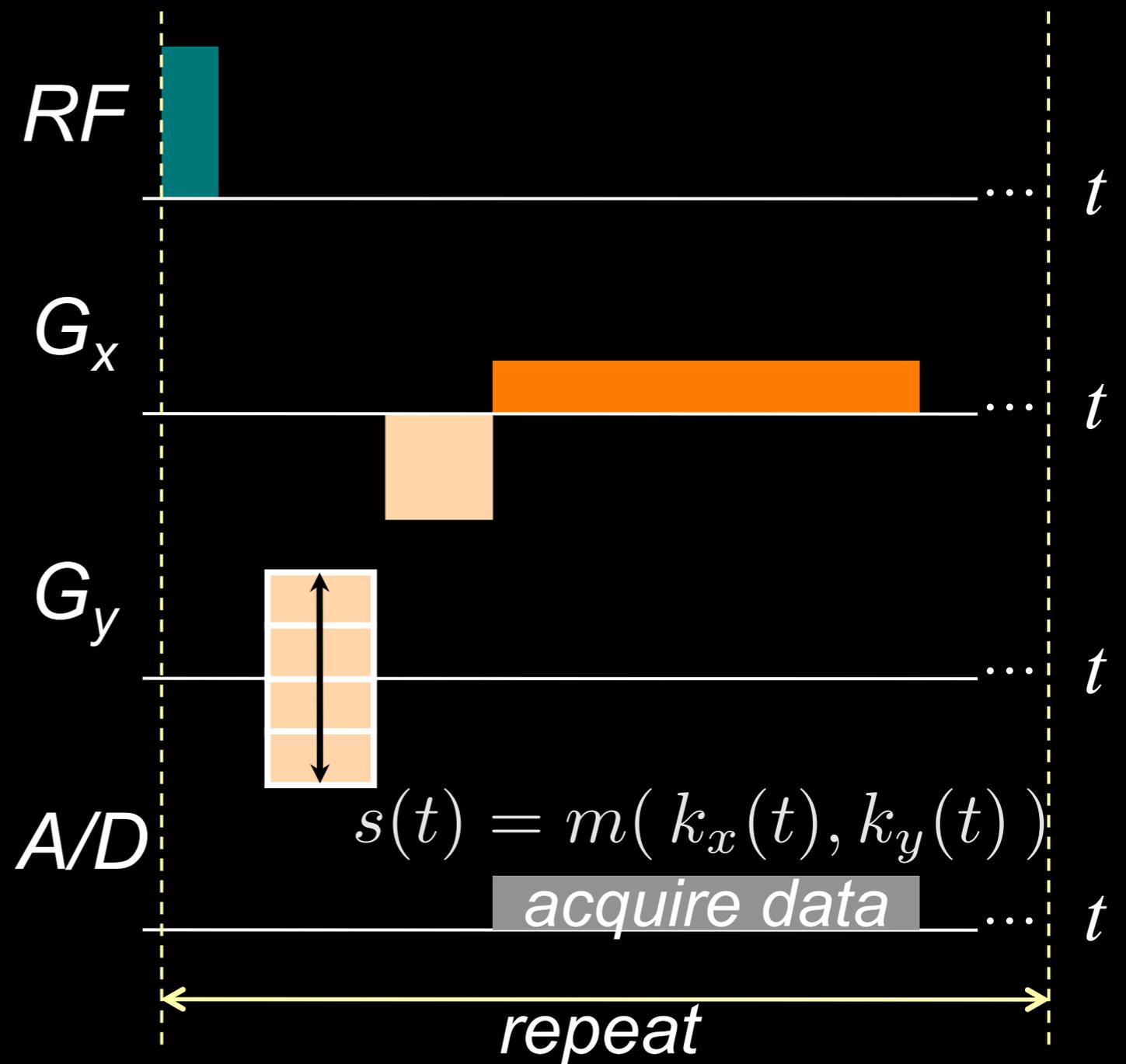
# Fast Imaging

# k-Space Sampling

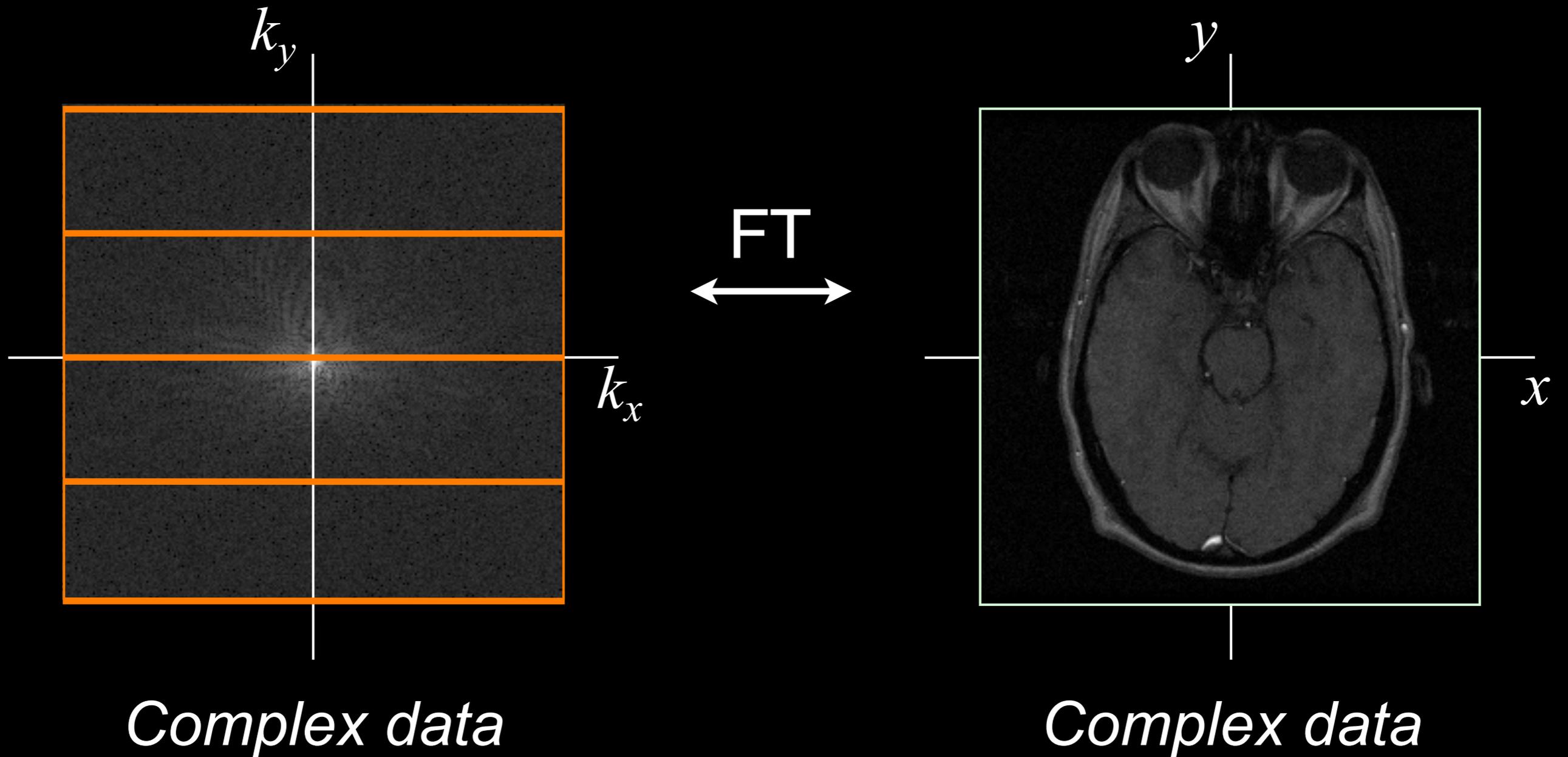


set of  $s(t)$  covers  $m(k_x, k_y)$

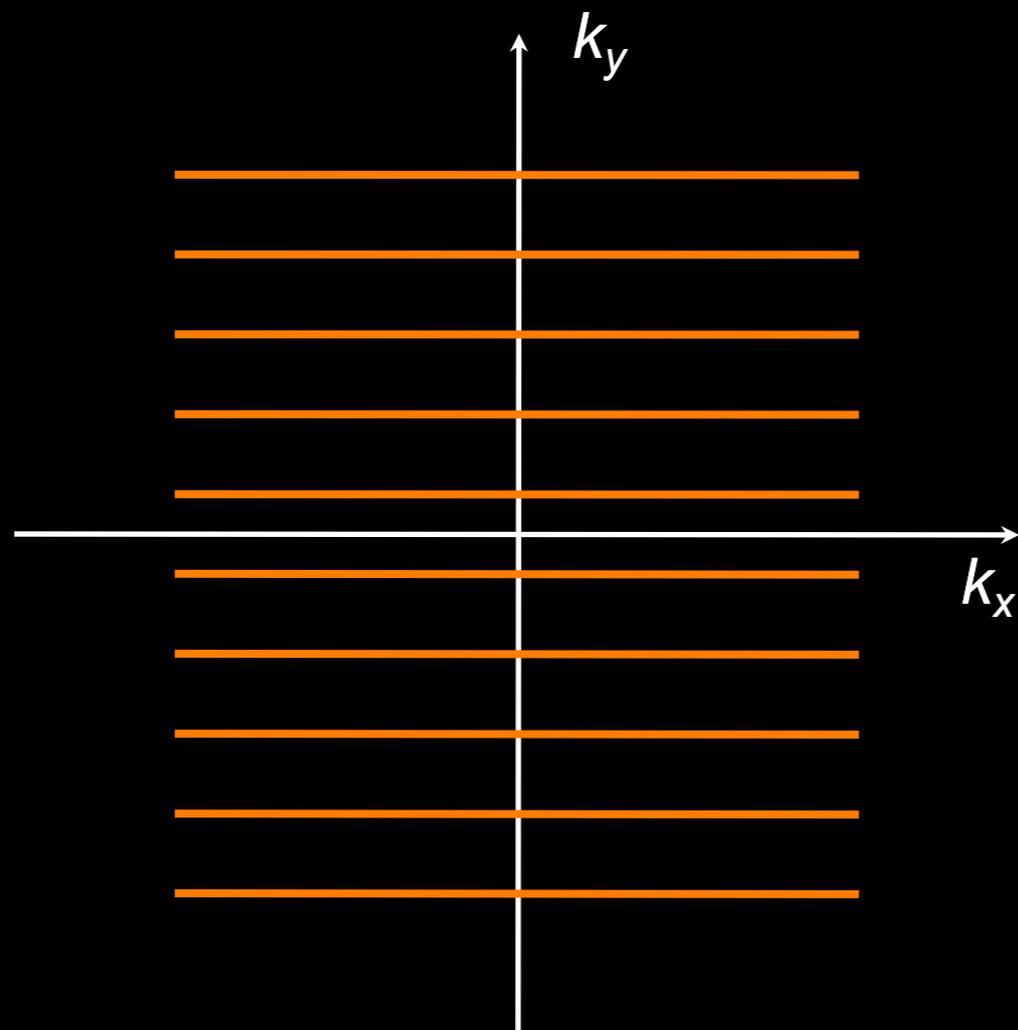
## Pulse Sequence Diagram



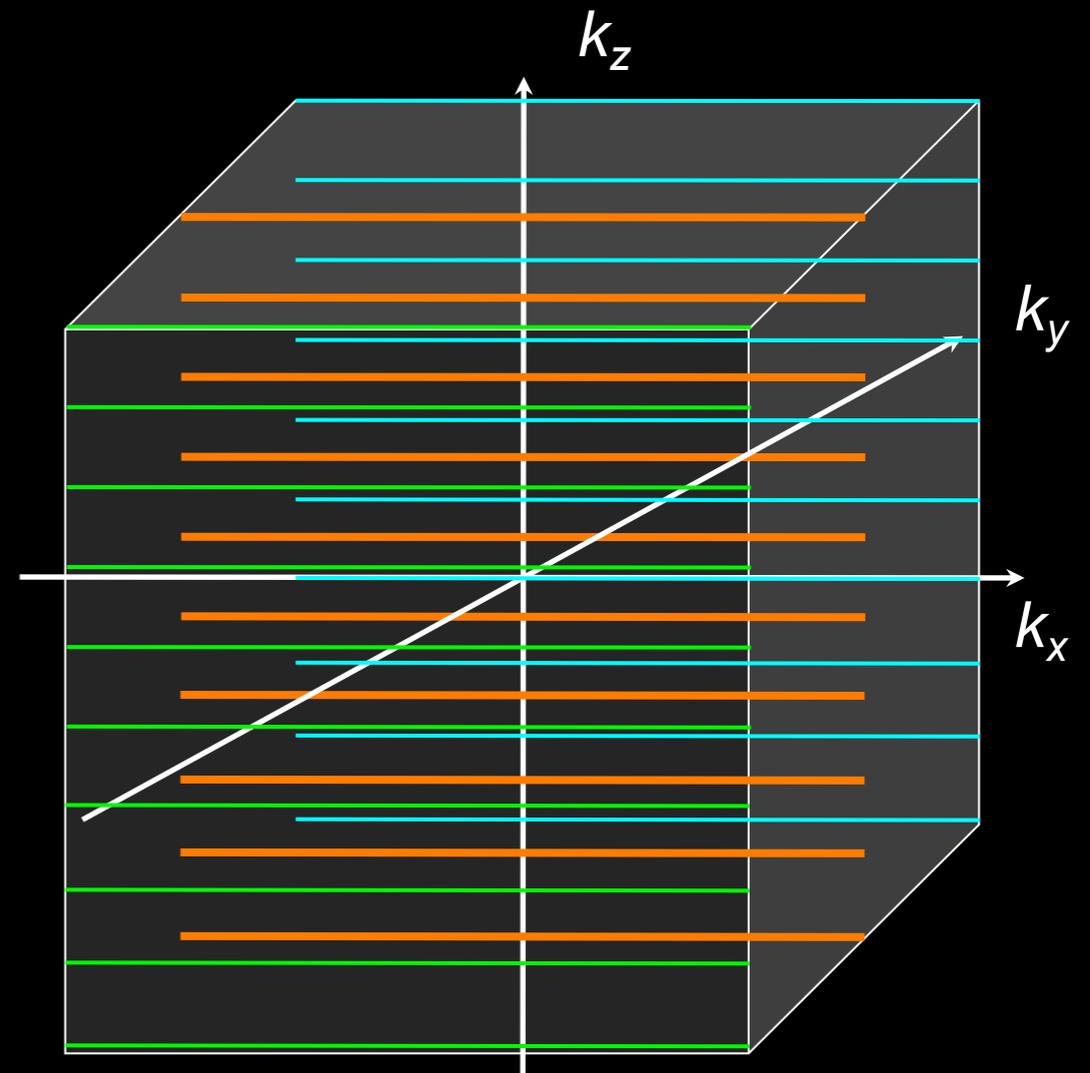
# Image Reconstruction



# Cartesian Sampling



Cartesian 2DFT



Cartesian 3DFT

# MR Signal Equation

$$s(t) = \iint_{X,Y} M(x, y) \cdot \exp(-i2\pi \cdot [k_x(t)x + k_y(t)y]) dx dy$$

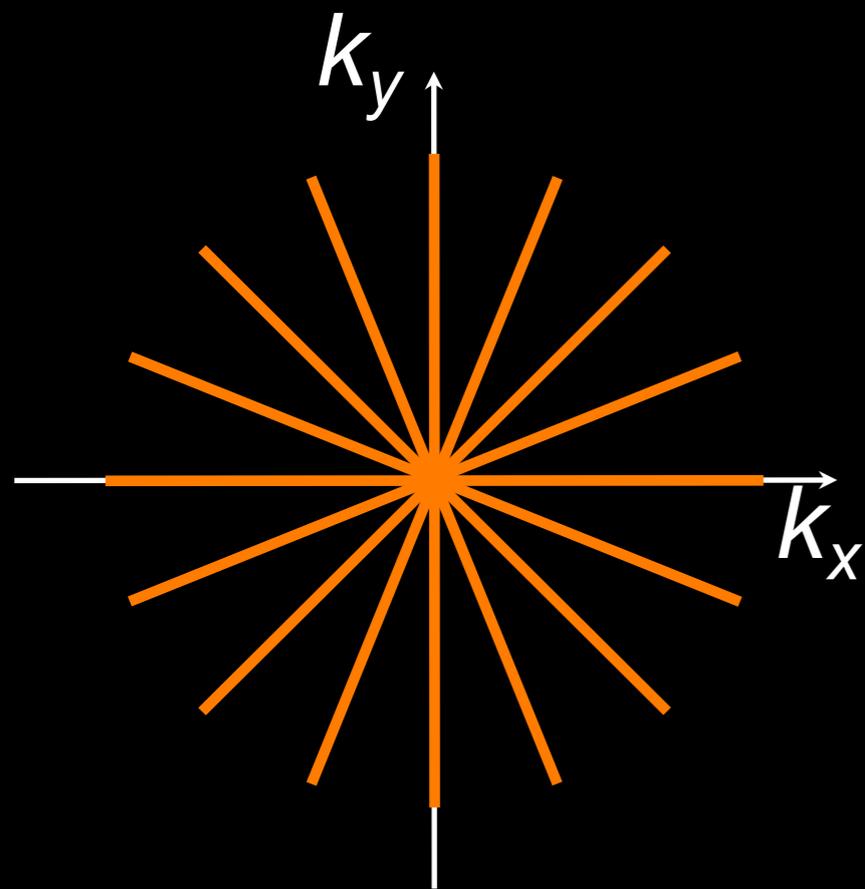
$$= m(k_x(t), k_y(t))$$

$$k_x(t) = \frac{\gamma}{2\pi} G_x t, \quad k_y(t) = \frac{\gamma}{2\pi} G_y t$$

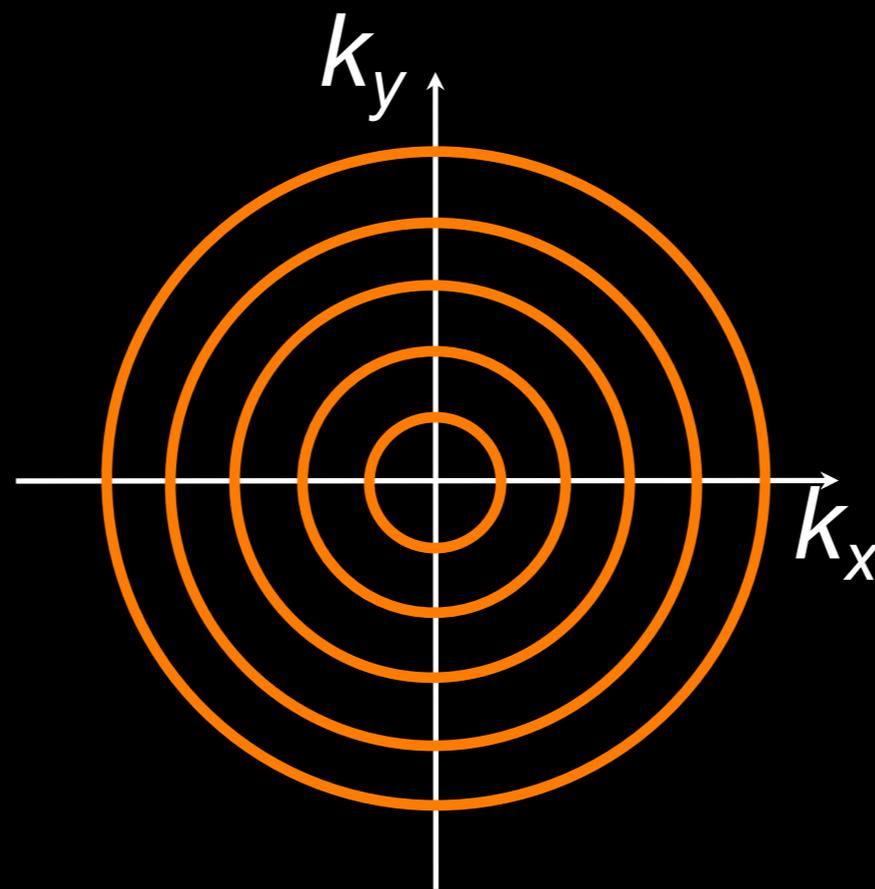
$$m = \mathcal{FT}(M(x, y))$$

$$k_x(t) = \frac{\gamma}{2\pi} \int_0^t G_x(\tau) d\tau, \quad k_y(t) = \frac{\gamma}{2\pi} \int_0^t G_y(\tau) d\tau$$

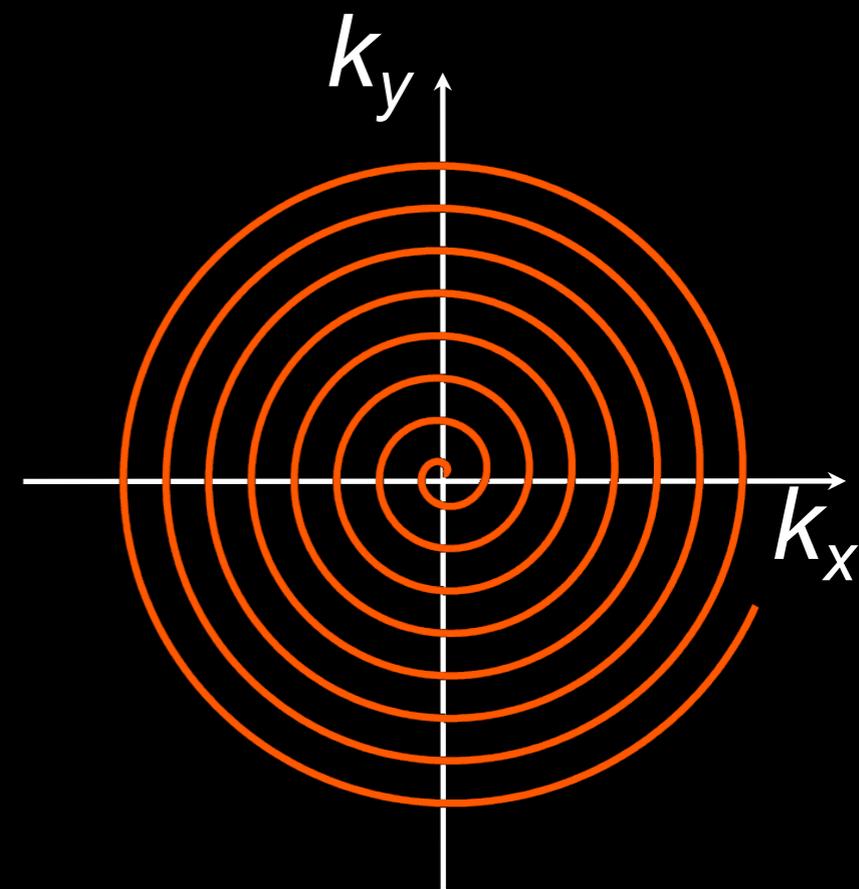
# Non-Cartesian Sampling



2D Radial



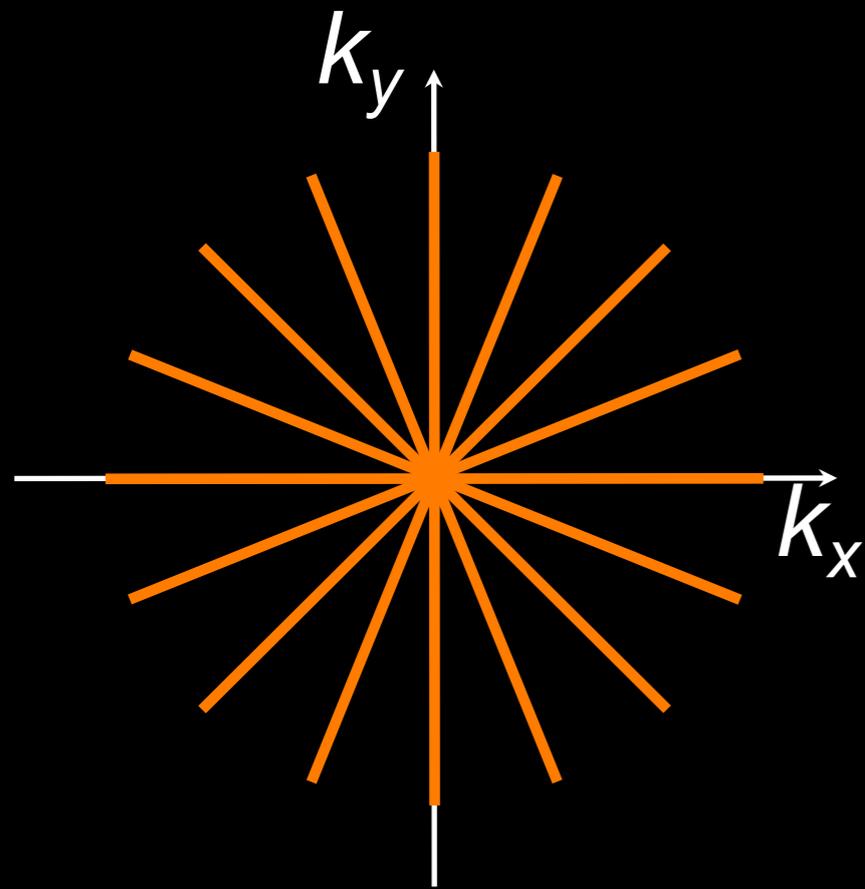
2D Concentric Rings



2D Spiral

*and much more ...*

# Radial: Pros and Cons



## Pros

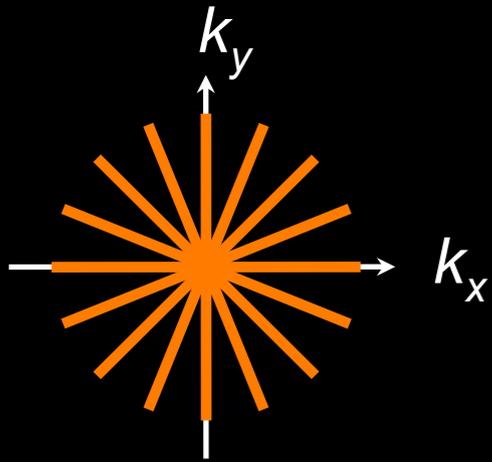
- Robust to motion (get DC every TR)
- Can tolerate a lot of undersampling
- Half-spoke PR has very short TE

## Cons

- SNR penalty (non-uniform density)
- May have mixed contrast
- Sensitive to gradient delays
- Sensitive to off-resonance effects

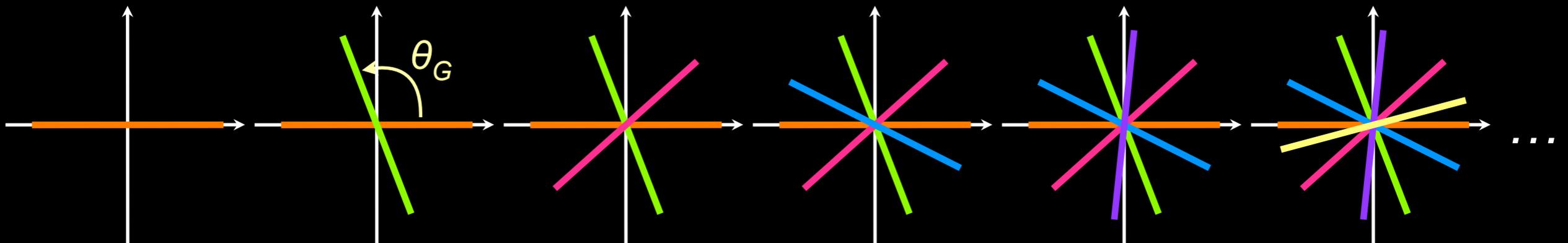
# Radial: Real-time MRI

## 2D Radial MRI



- Robust to motion (oversample center of k-space)
- Can tolerate a lot of undersampling

## Golden Angle Ordering



- Almost uniform sampling of  $k-t$  space
- Flexible choice of temporal frame location and width

# Radial: Real-time MRI

## Radial FLASH

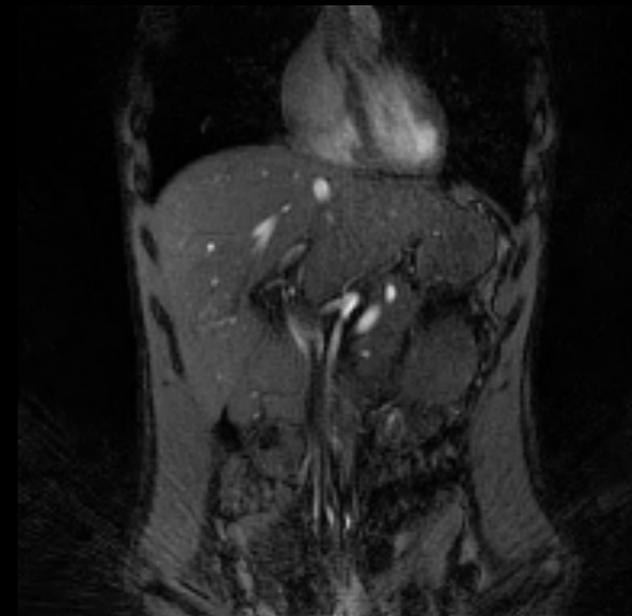
- golden-angle ordering
- 192 x 192 matrix
- TR = 3.1 ms  
(1 spoke per TR)
- 3.0 T

## Reconstruction

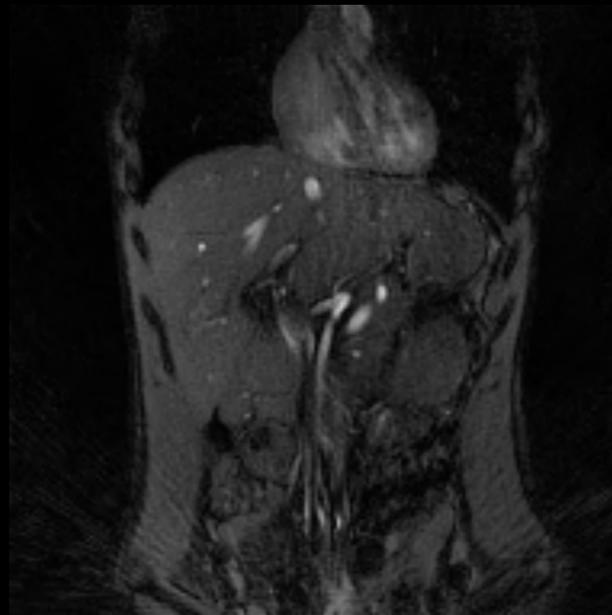
- sliding window of 20 TRs  
(display at 16 frames/sec)
- **parallel imaging (SPIRiT)**  
(300 spokes for Nyquist)



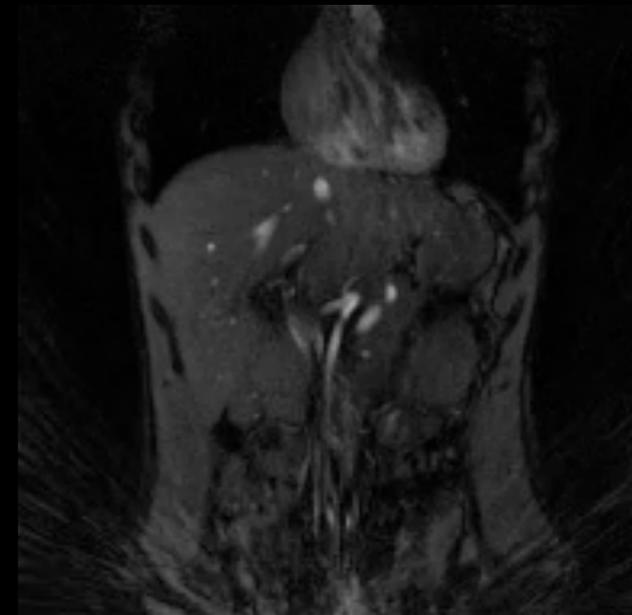
255 spokes/frame  
(791 ms/frame)



144 spokes/frame  
(446 ms/frame)



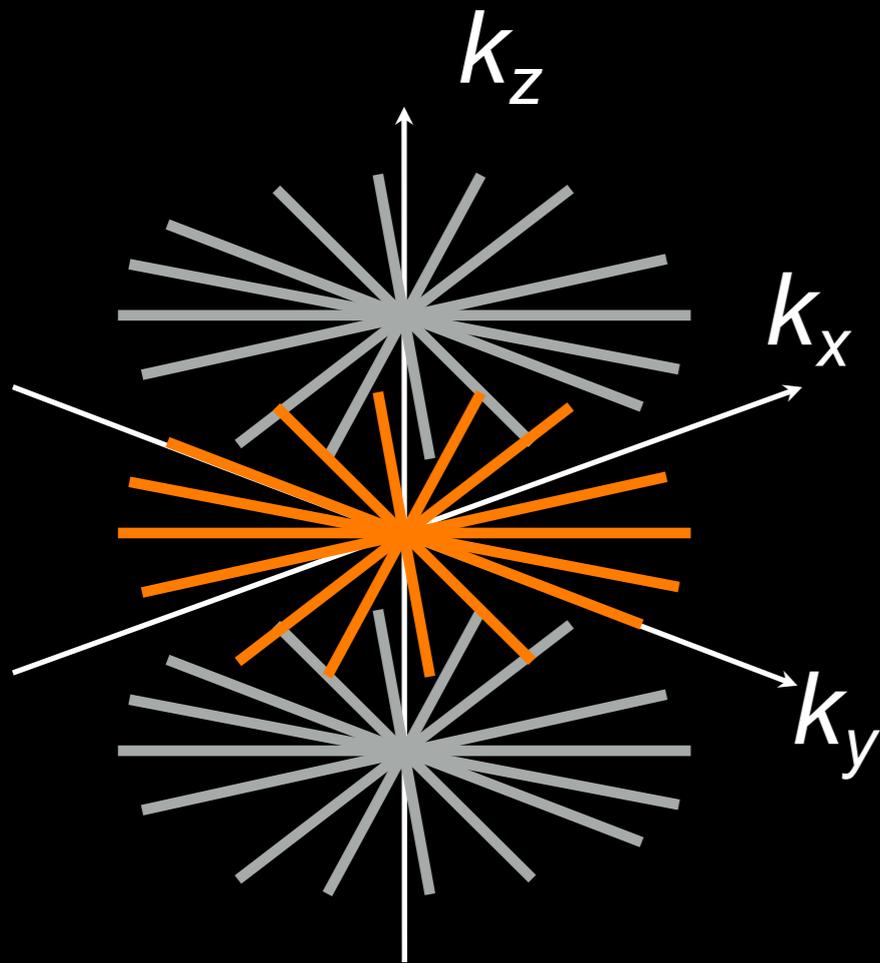
89 spokes/frame  
(276 ms/frame)



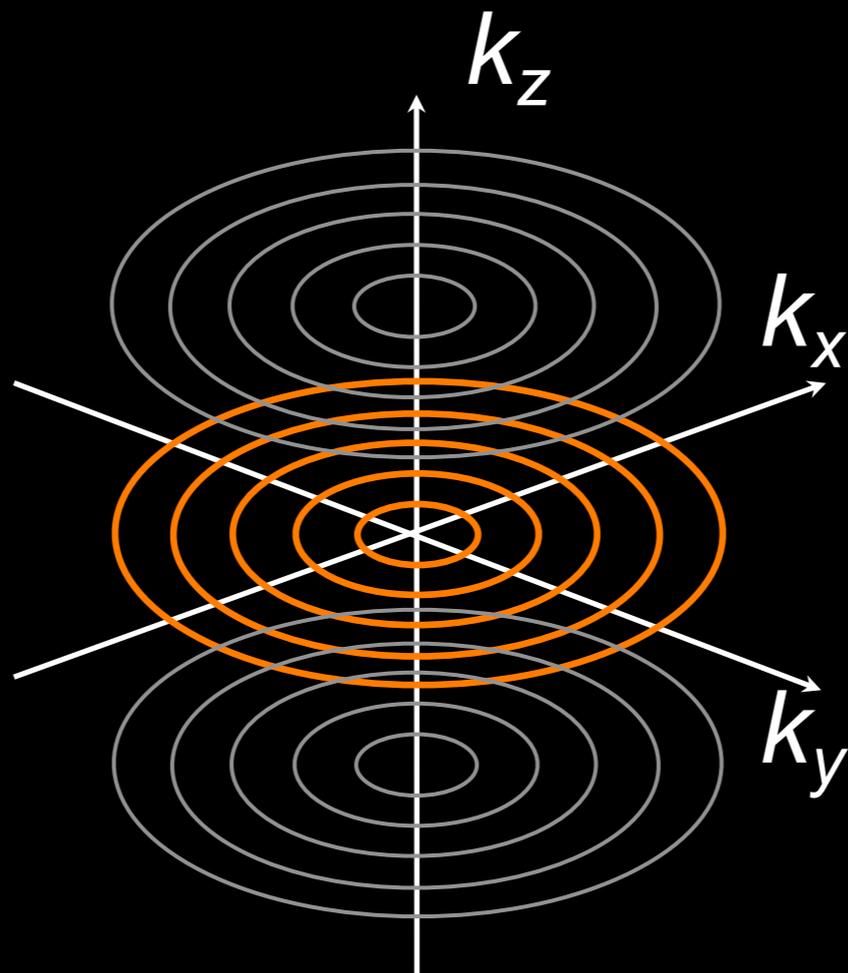
55 spokes/frame  
(171 ms/frame)

*courtesy of Samantha Mikael*

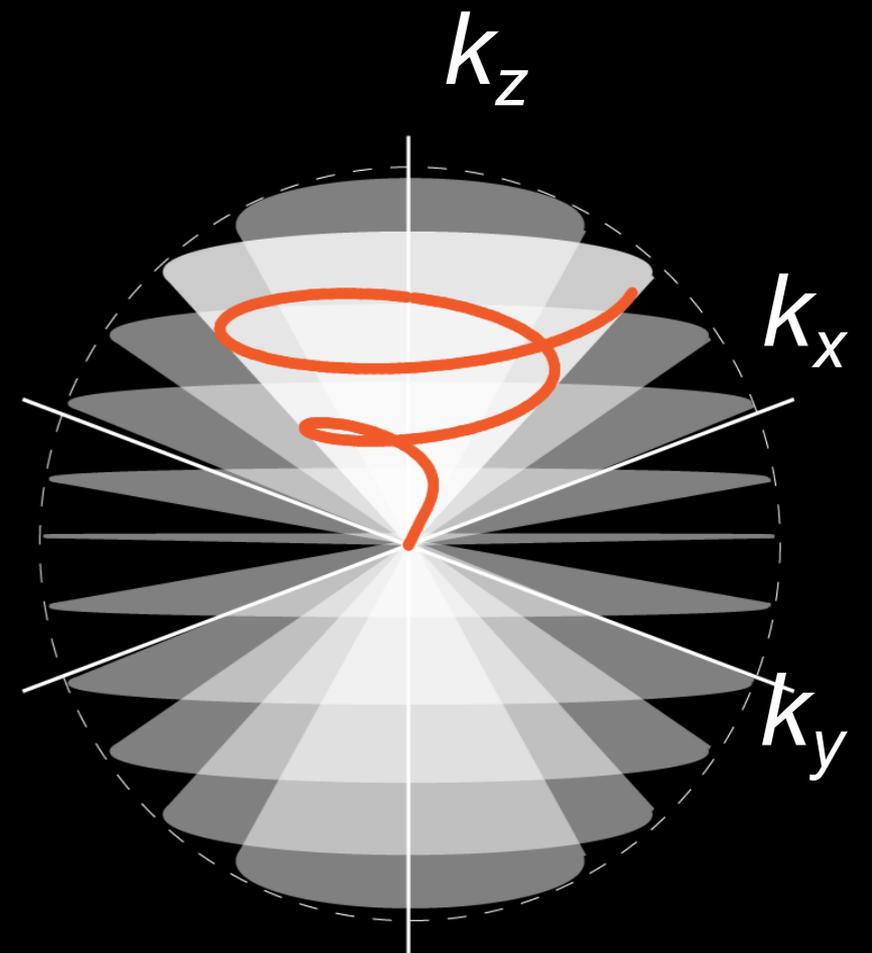
# Non-Cartesian Sampling



3D Stack of Stars



3D Stack of Rings

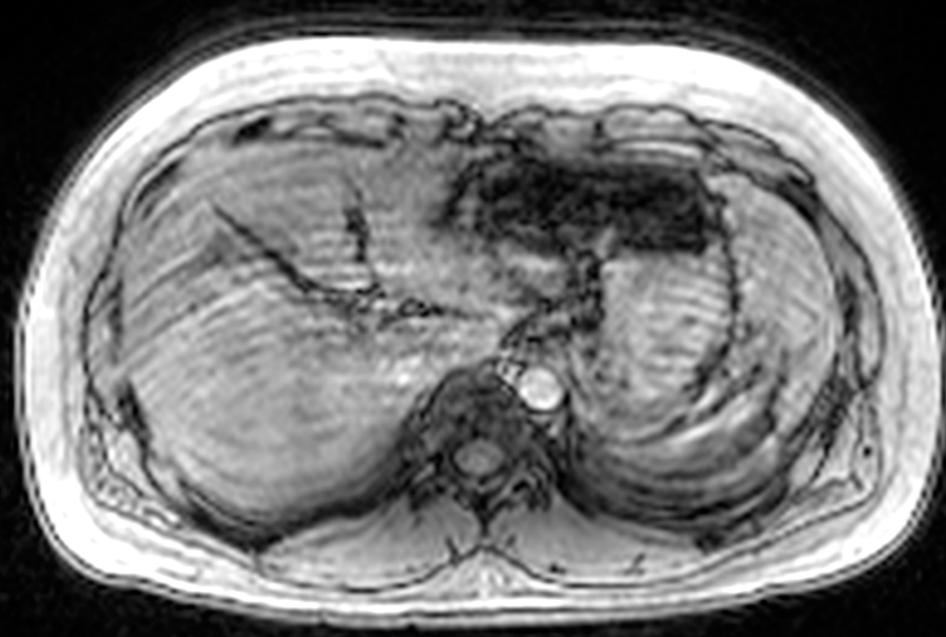


3D Cones

*and much more ...*

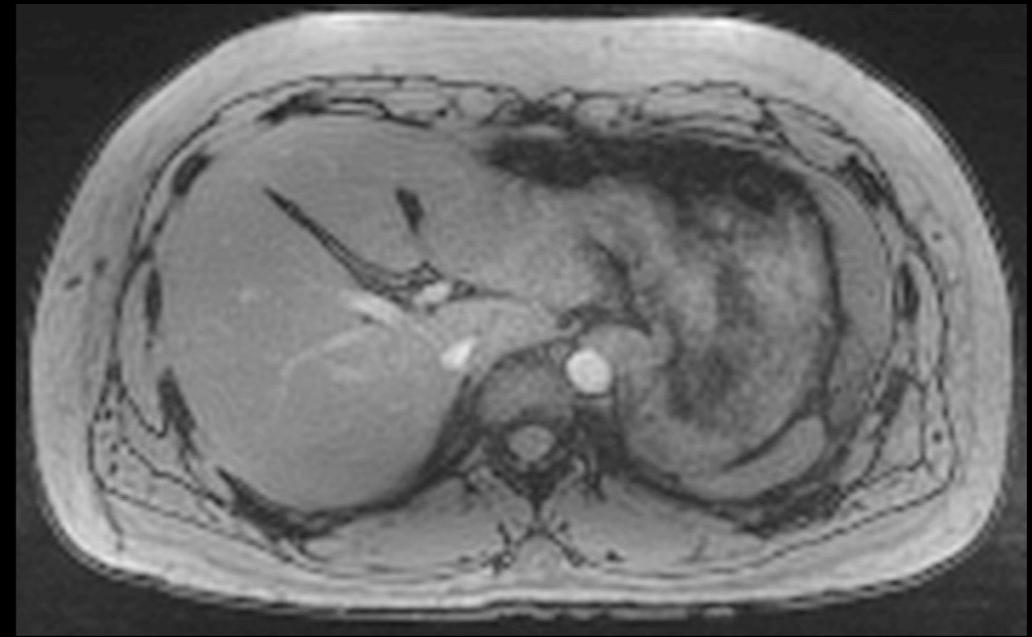
# 3D Stack-of-Radial: Liver MRI

3D Cartesian MRI

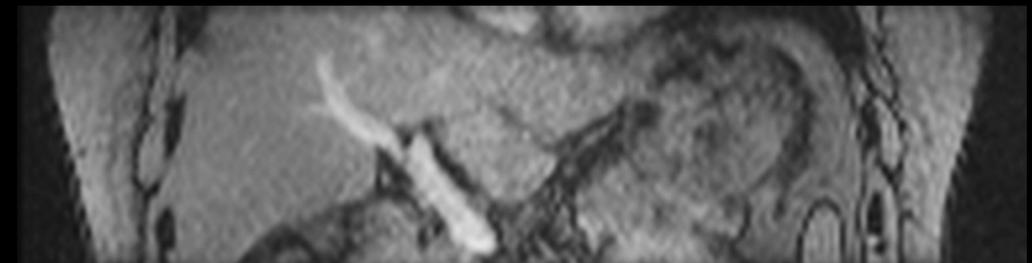


*Insufficient breath-holding*

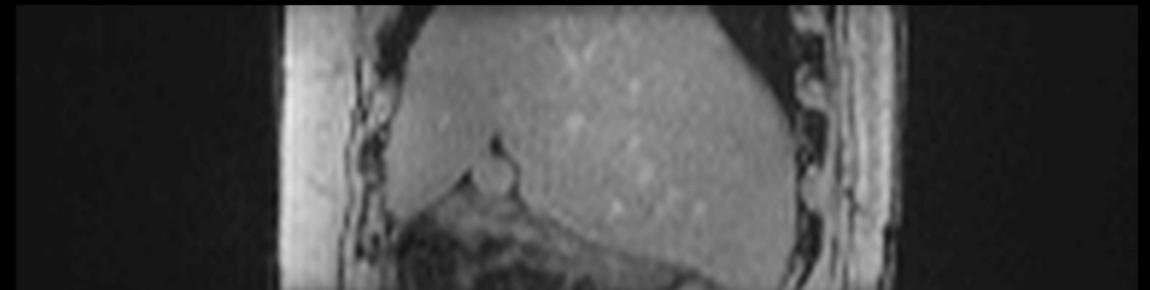
Free-breathing 3D Stack-of-Radial MRI



Axial



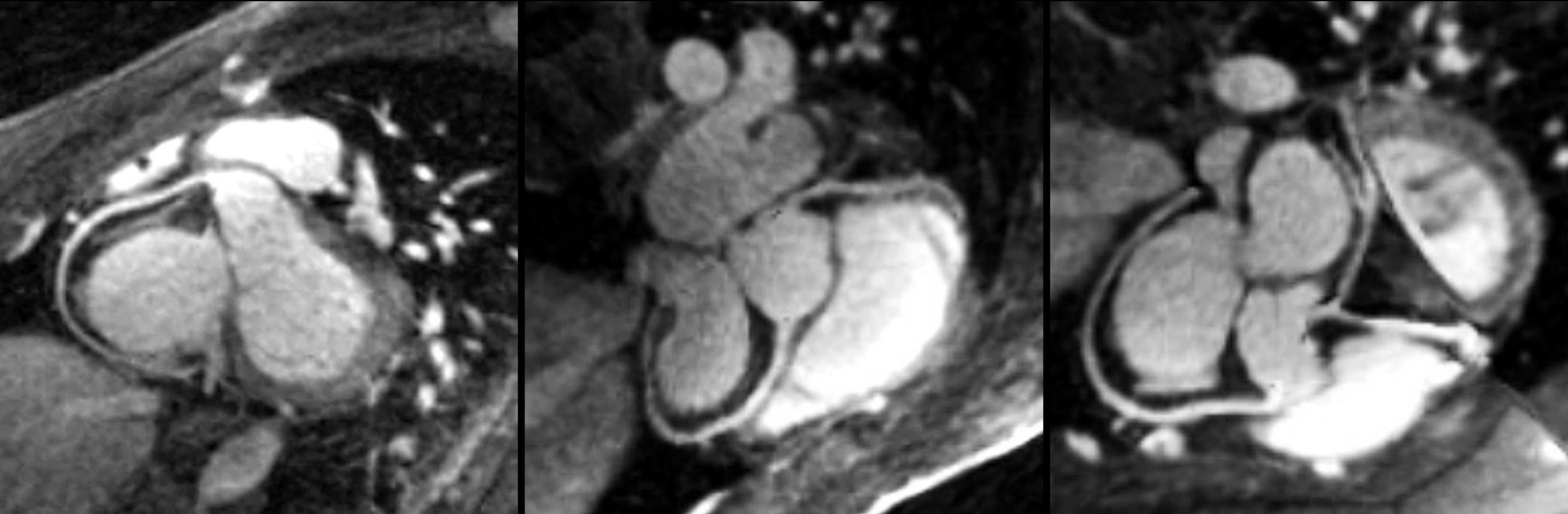
Coronal



Sagittal

# 3D Radial: Coronary MRA

Contrast-Enhanced MRA at 3.0T



ECG-gated, fat-saturated, inversion-recovery prepared spoiled gradient echo sequence  
(1.0 mm)<sup>3</sup> spatial resolution, 1D self navigation, CG-SENSE recon, 5.4 min scan time

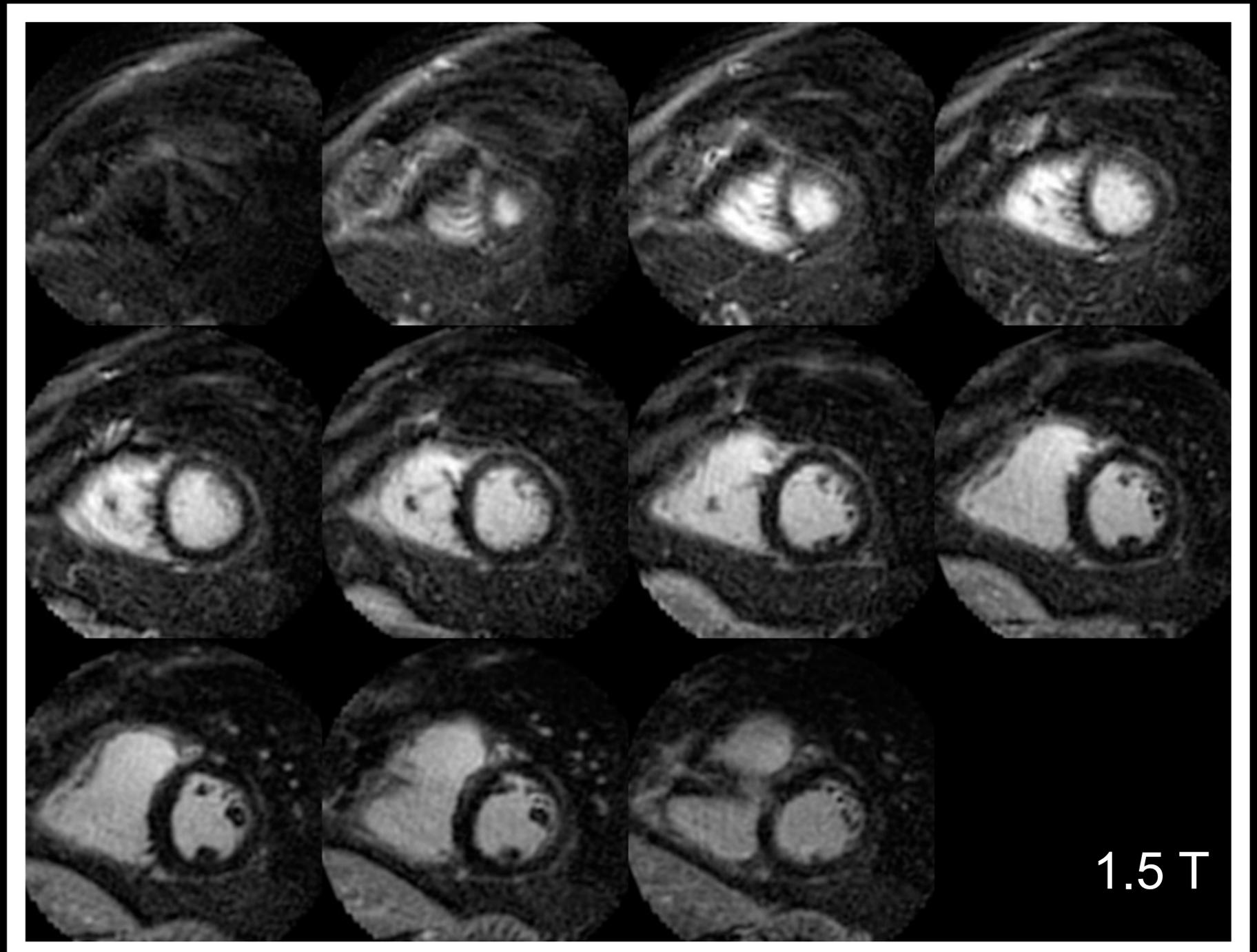
# 3D Stack-of-Spirals: LGE MRI

## 3D Spiral IR-GRE

- 6-interleaf VD spiral
- 7.5-ms readout
- 90 x 90 x 11 matrix
- outer volume suppr
- water-only RF exc
- TR = 15.48 ms
- 8-HB BH scan

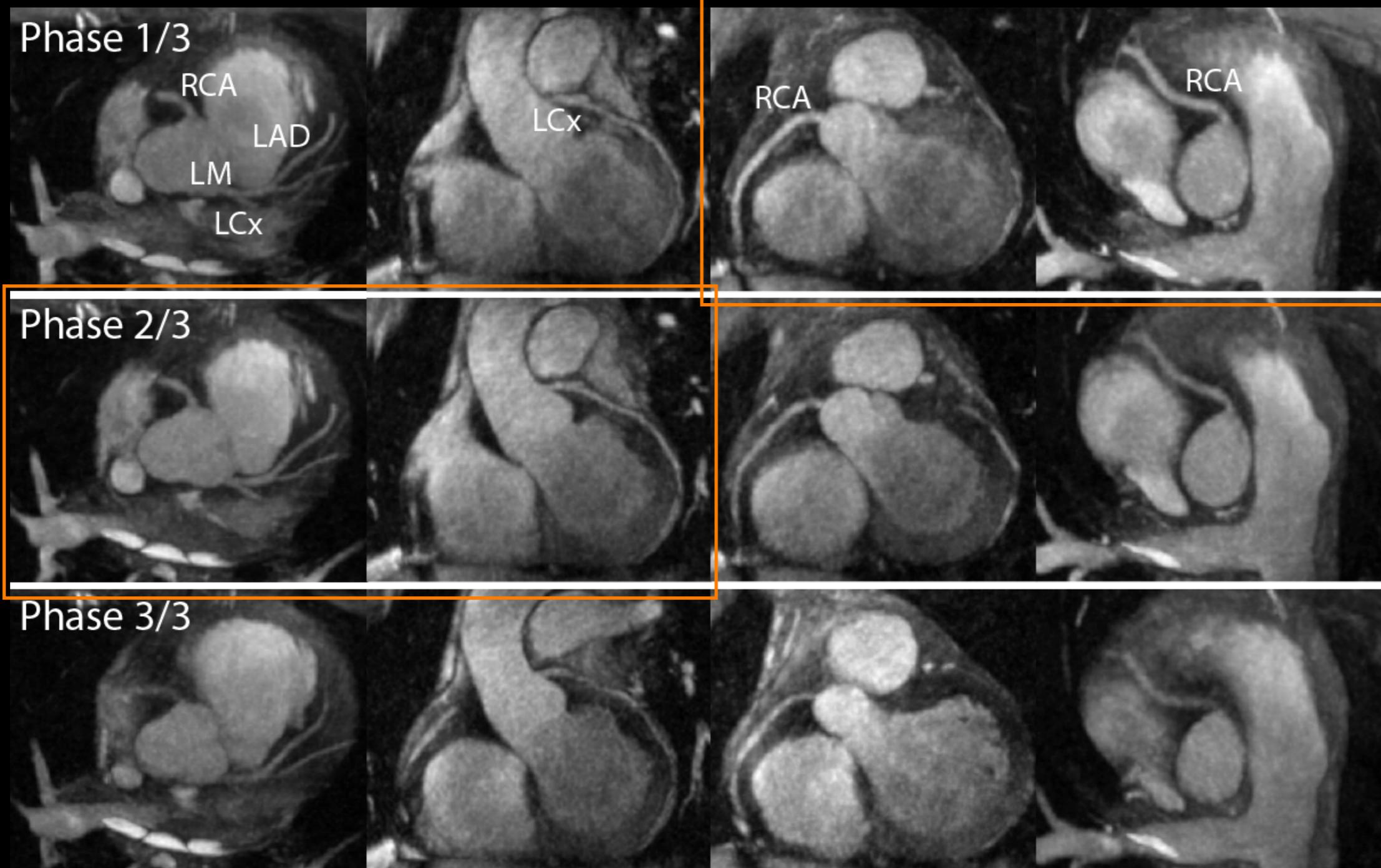
## Reconstruction

- SPIRiT ( $R = 2$ )
- ~5-sec recon



# 3D Cones: Coronary MRA

*Multi-Phase Thin-Slab MIP Reformats*

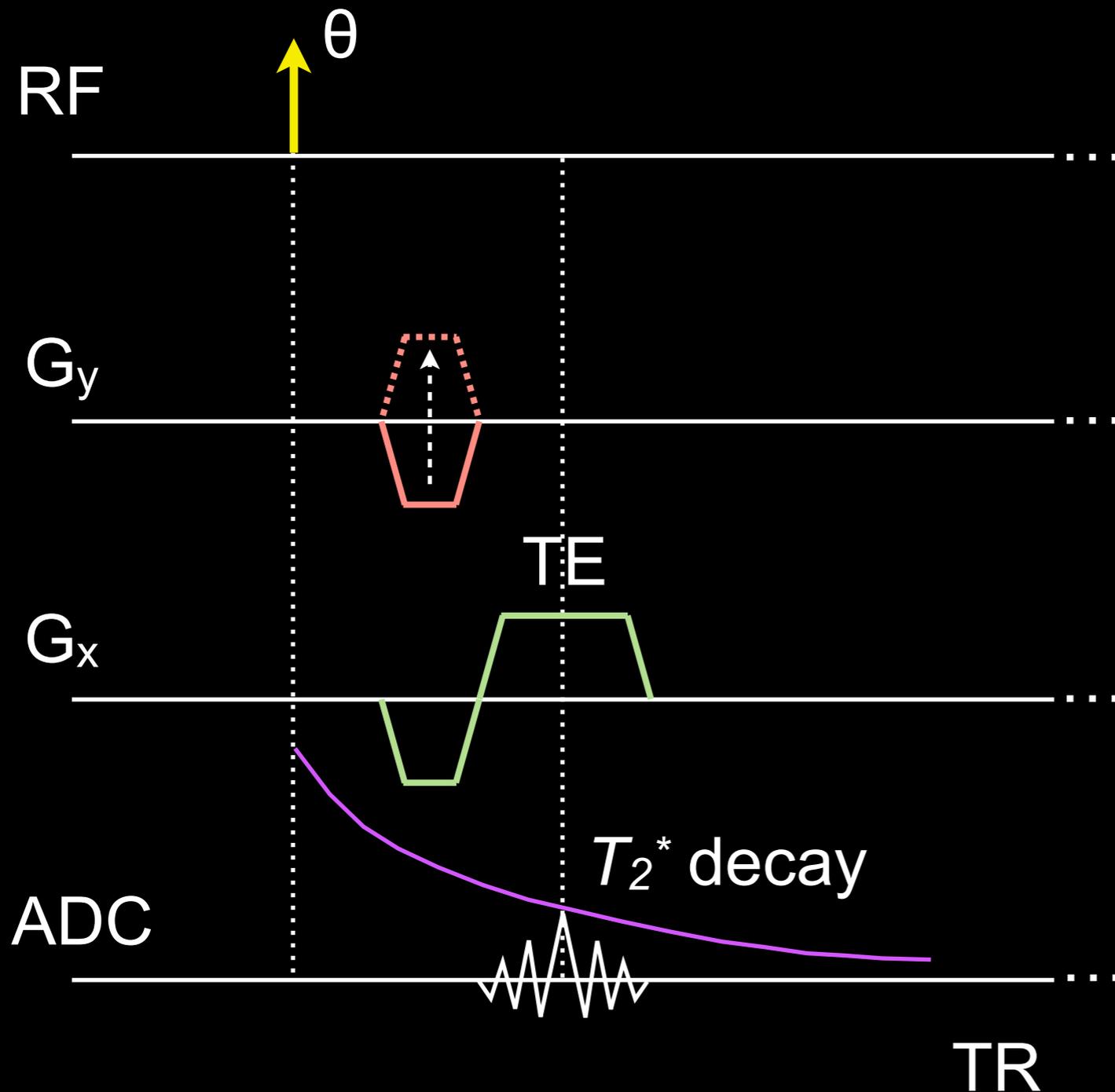


# Echo-Planar Imaging

- Echo-Planar Imaging (EPI)<sup>1</sup>
- Ultra-fast imaging (<100 ms/frame)
- Imperfections and artifacts
- Ongoing topic of rapid MRI research

<sup>1</sup>Mansfield P, *J Phys C: Solid State Phys* 1977

# Gradient Echo

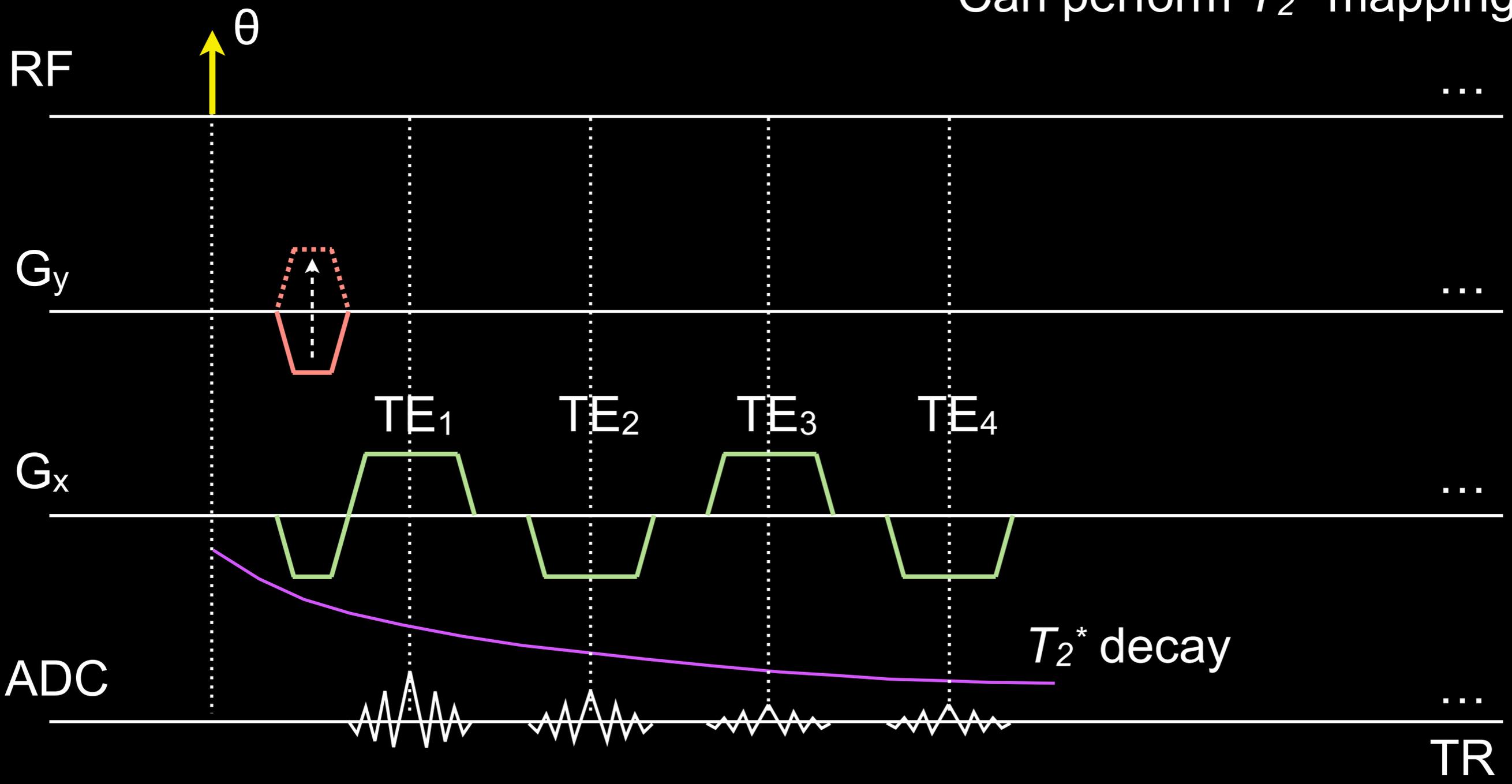


- Utilization of transverse magnetization
  - With  $T_s = 8 \mu s$  and  $N_x = 128$ ,  $T_{acq} = 1.024 ms$
  - $<2\%$  of  $T_2^*$  in brain at 3 T!<sup>1</sup>
- Scan time
  - $T_{GRE} = N_{pe} \times TR$
  - $TR = 10 ms$ ,  $N_{pe} = 256$ :  
 $T_{GRE} = 2.56 sec$

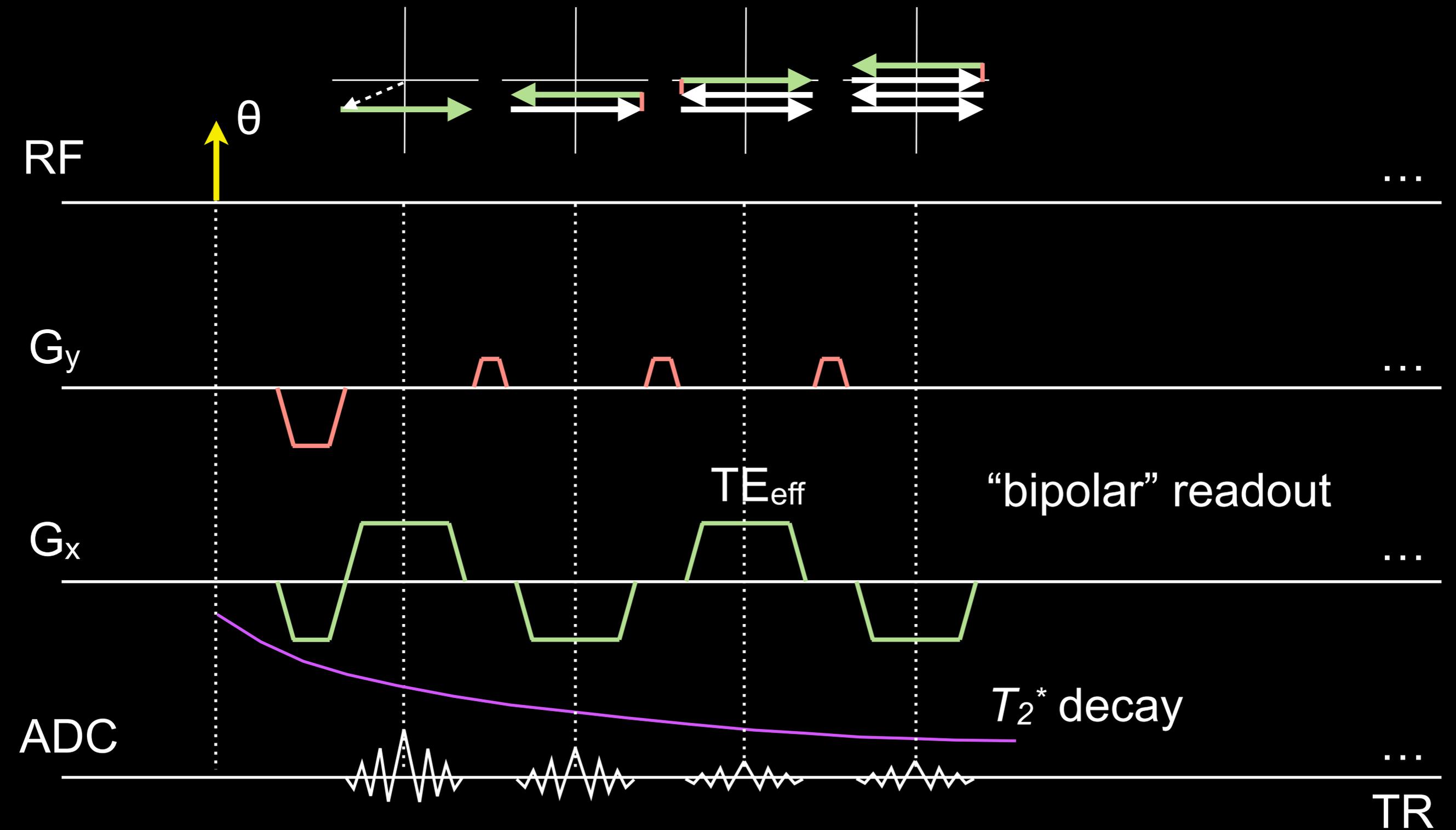
<sup>1</sup>Peters, et al., Proc ISMRM 2006

# Multi-echo Gradient Echo

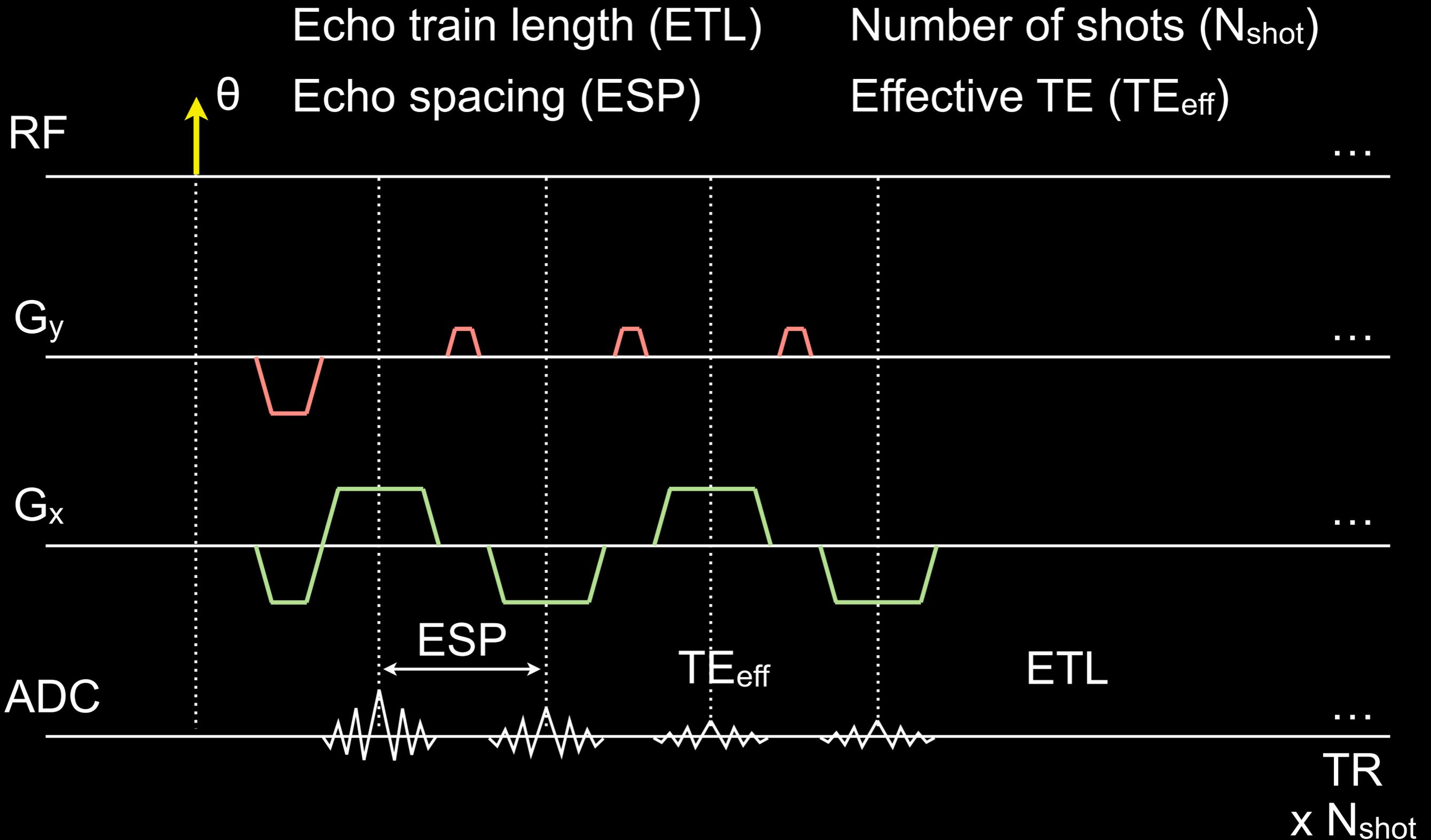
$\Delta TE$  can be non-uniform  
Can perform  $T_2^*$  mapping



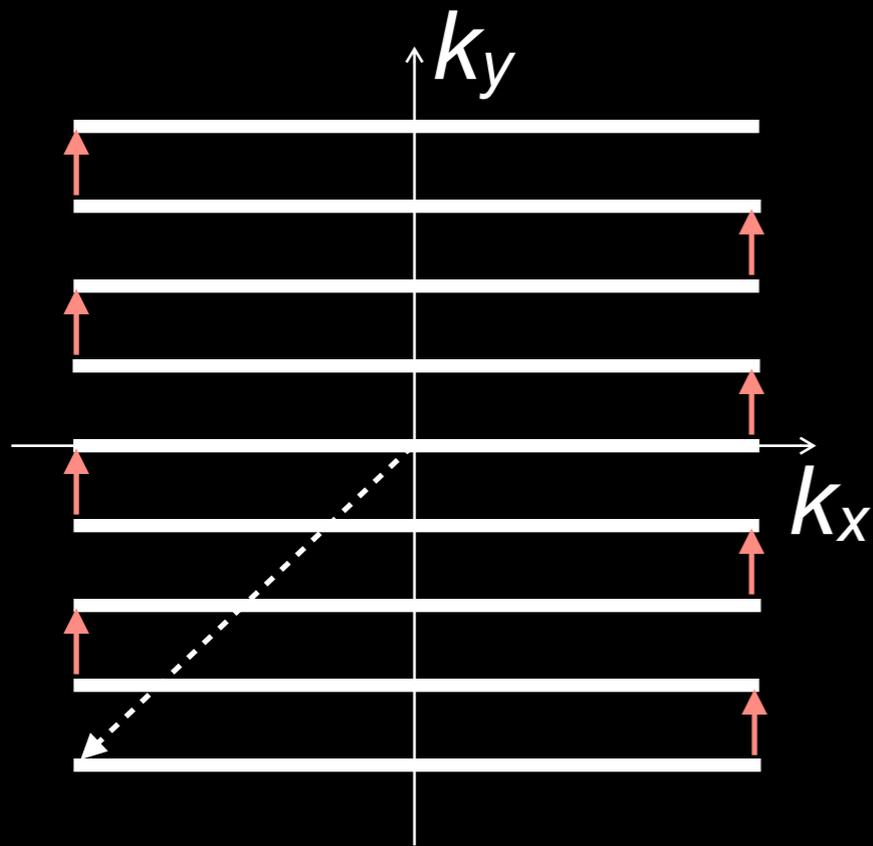
# Gradient-Echo EPI



# EPI Sequence Parameters

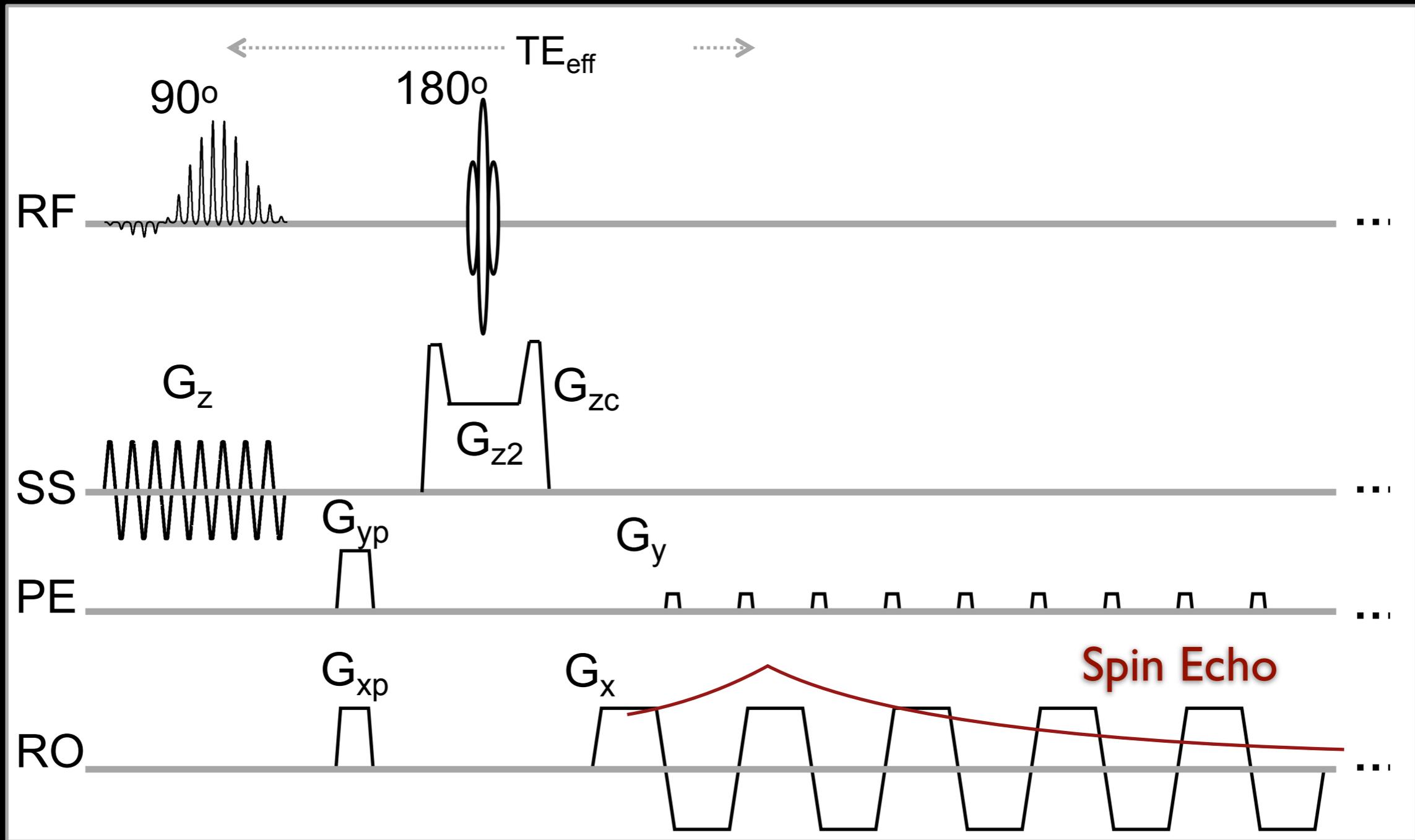


# EPI k-Space Sampling

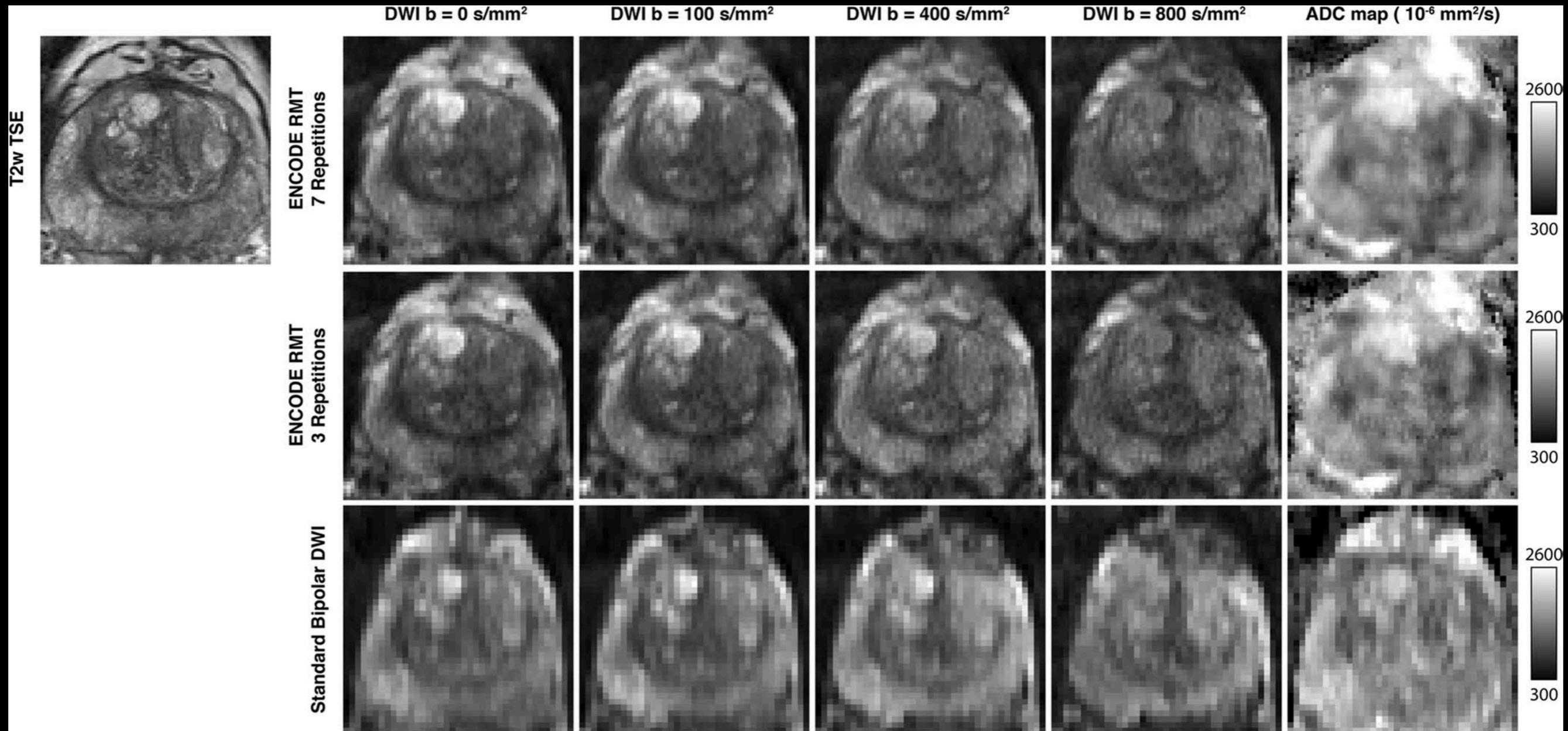


- ETL can be 4-64 or higher
  - Limited by  $T_2^*$  decay, off-resonance effects
  - aka “EPI factor”
- ESP typically  $\sim 1$  ms
  - Must accommodate RF, gradients, ADC
  - Short ESP facilitates high ETL

# Spin-Echo (SE) EPI

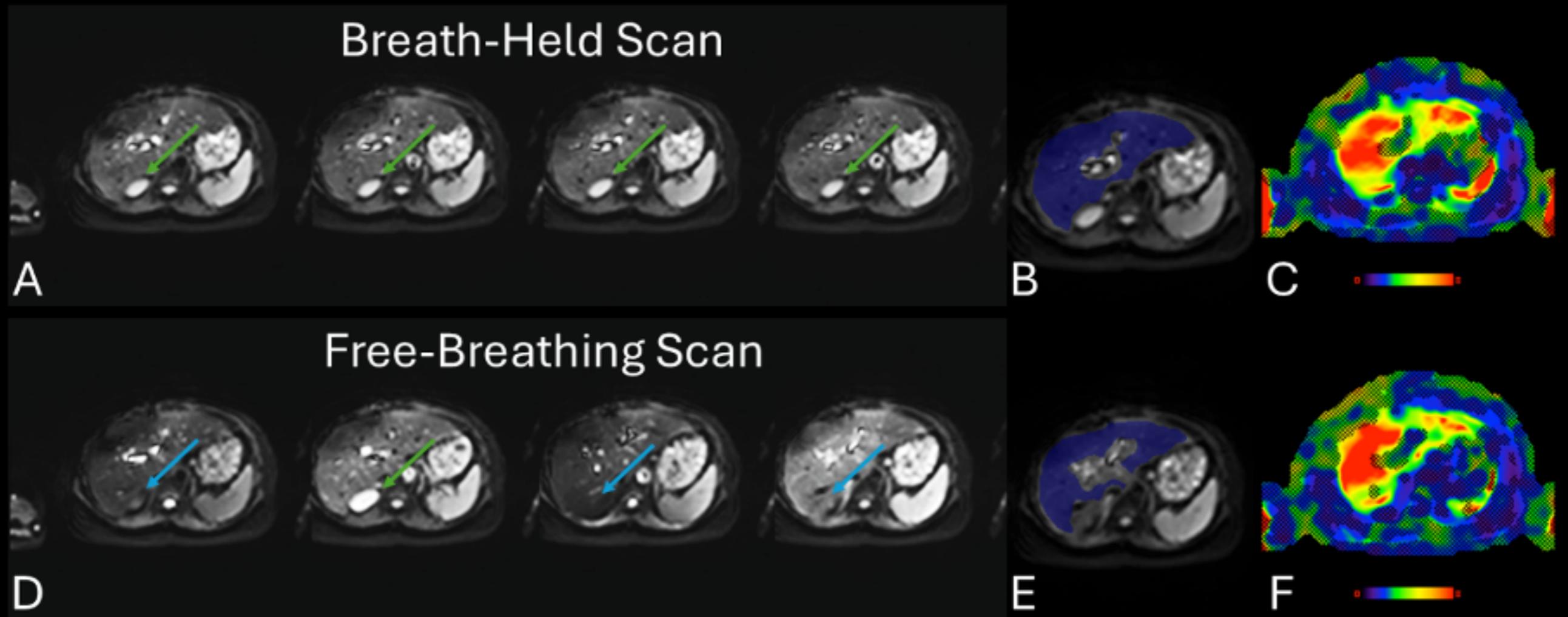


# SE-EPI: Prostate Diffusion MRI



ENCODE RMT: TR=4800 ms, 16 slices, 3 averages, parallel imaging R=2, scan time=2m 30s

# SE-EPI: Liver MR Elastography



SE-EPI MRE: TR=1000 ms, 4 slices, 4 wave encodings, parallel imaging R=2, scan time=11s

# Fast Imaging Challenges

- Trajectory and gradient design
- Hardware performance
- Gradient fidelity
- Off-resonance effects
- Reconstruction: non-uniform FT
- Methods have been developed!

# Fast Imaging Trajectories

- **Benefits**

- Reduced scan time
- Robustness to motion and flow
- Short echo time

- **Applications**

- Dynamic MRI
- Real-time MRI
- Cardiovascular MRI
- Short-TE MRI

- **Challenges**

- Hardware performance
- Gradient fidelity
- Off-resonance effects
- Design and implementation

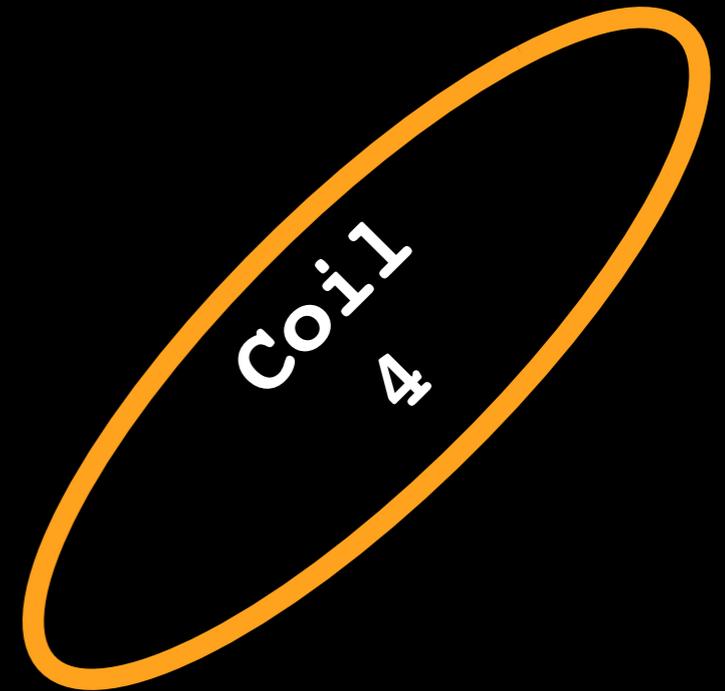
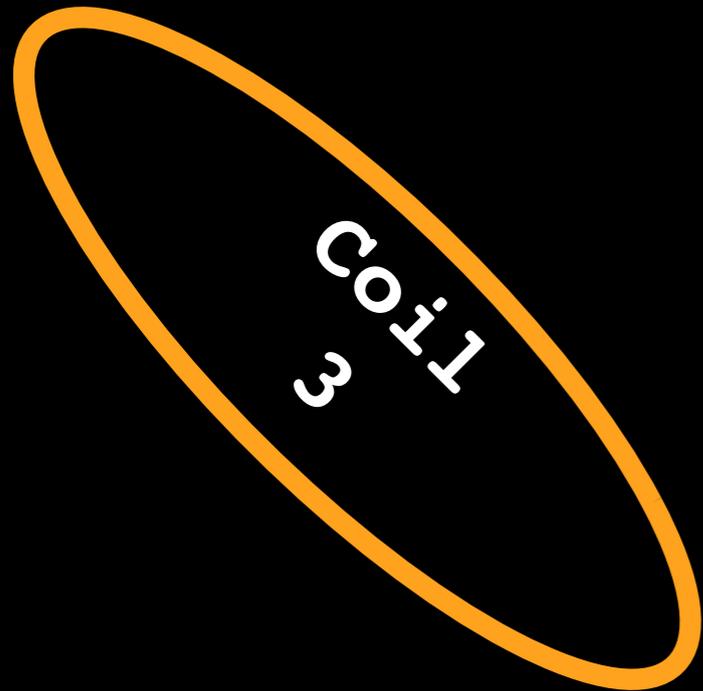
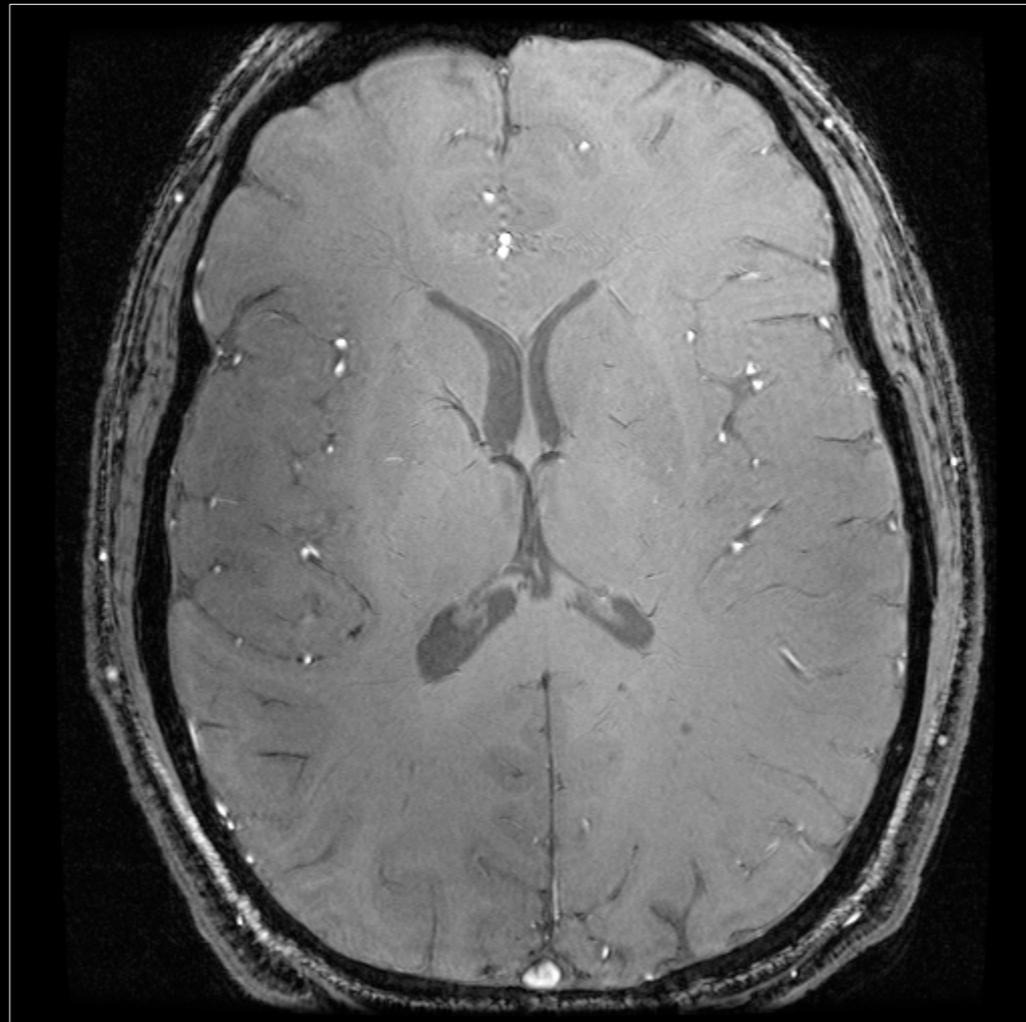
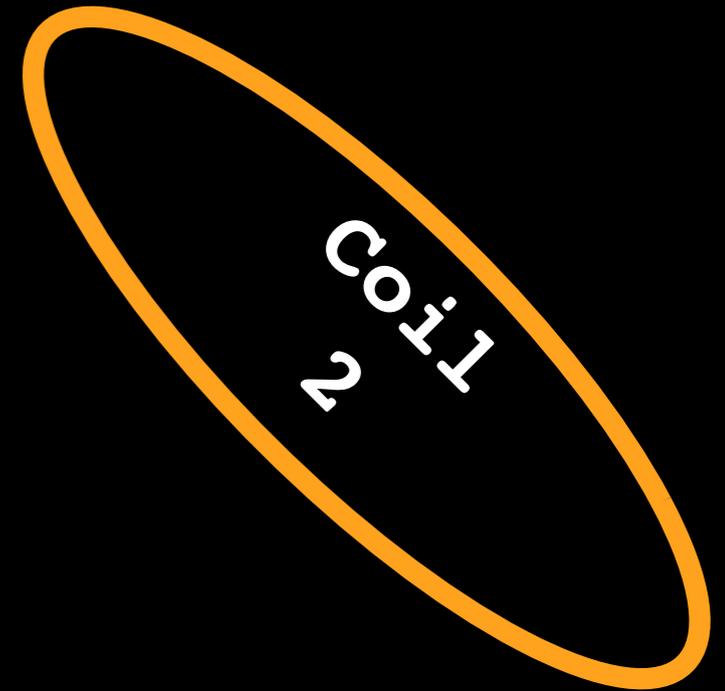
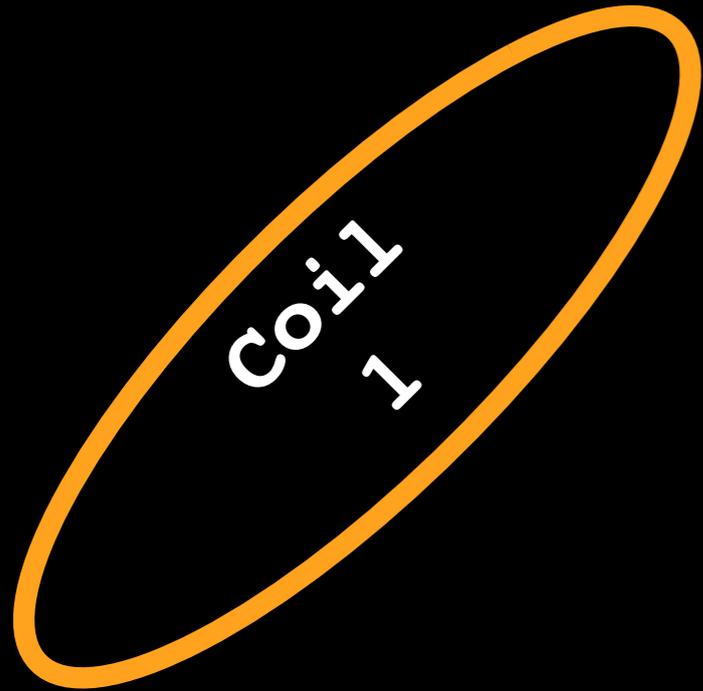
- **Challenges addressed**

- **On-going research**

- **Use judiciously!**

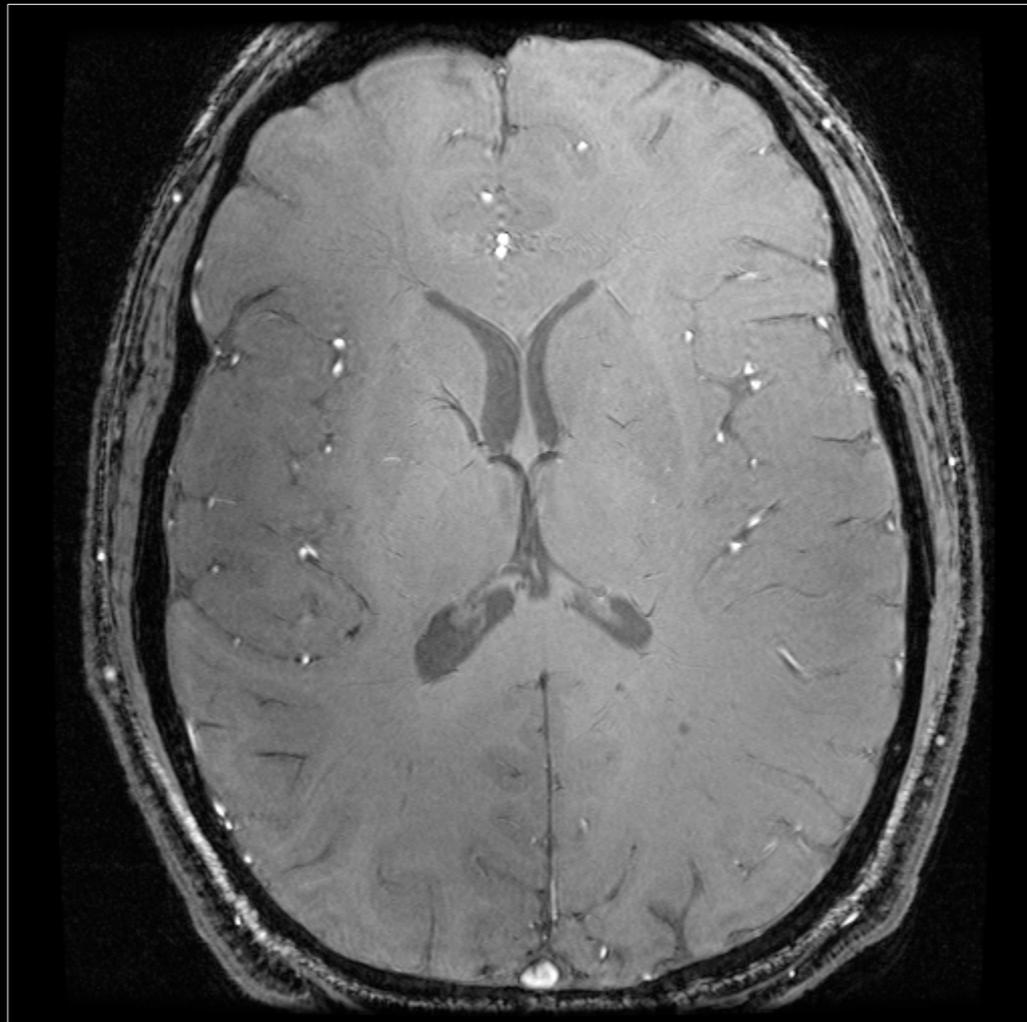
# Parallel Imaging

# Multi-coil Arrays



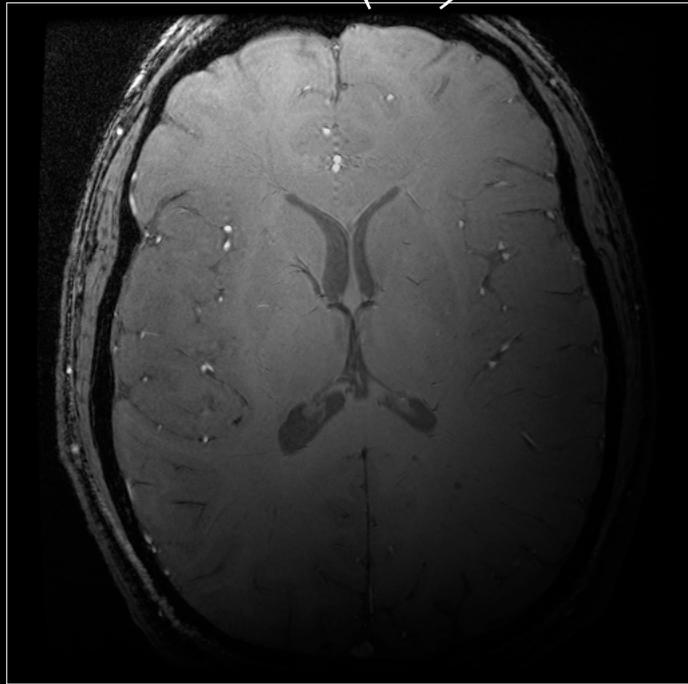
# Multi-coil Sensitivity

$$\| \vec{B}(\vec{r}) \|$$

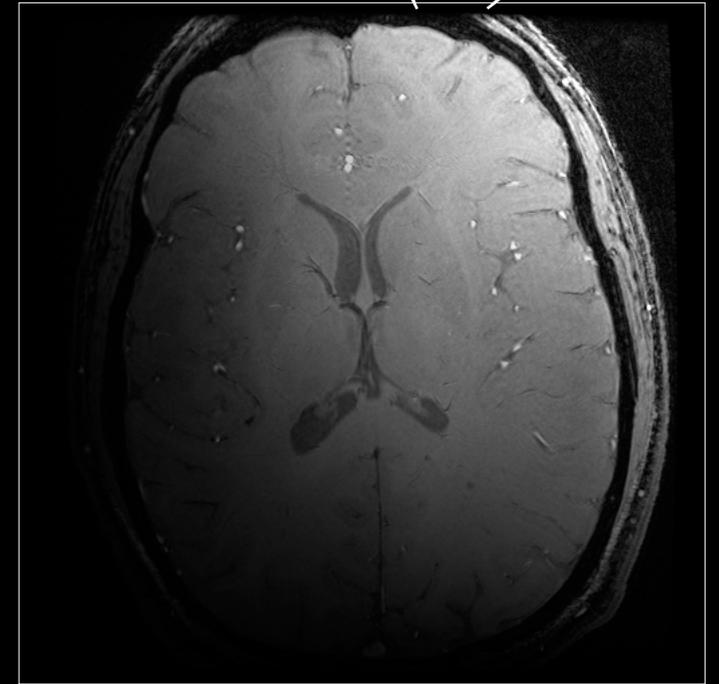


# Multi-coil Images

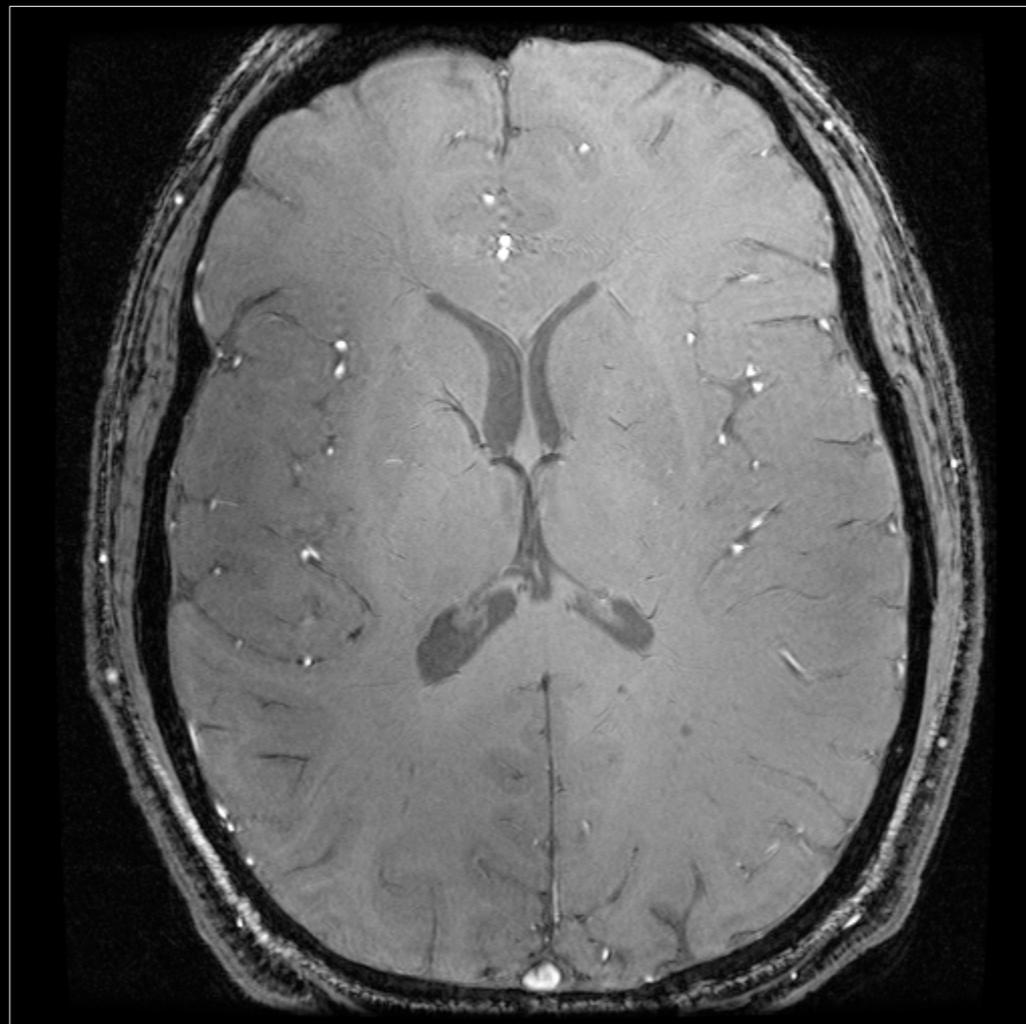
$m_1(x)$



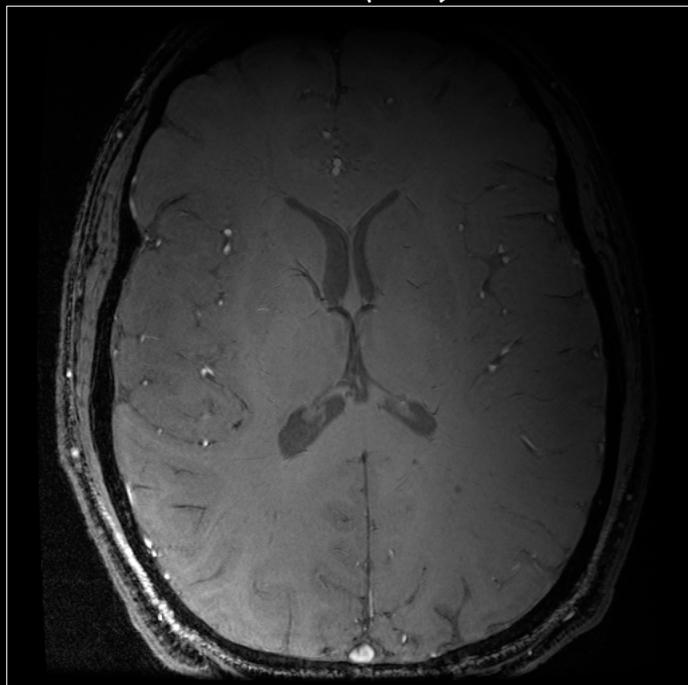
$m_2(x)$



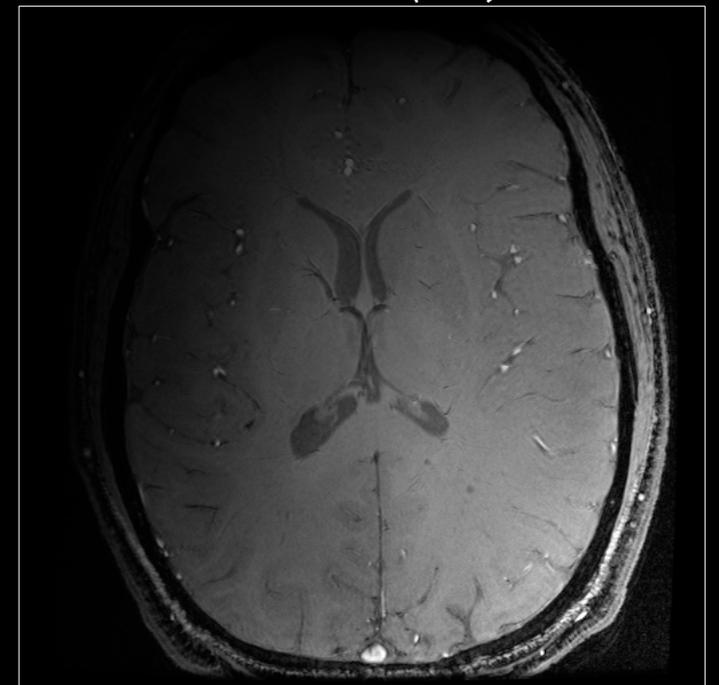
$m_s(x)$



$m_3(x)$



$m_4(x)$



# Multi-coil Reconstruction

- Each coil has a complete image of whole FOV and an amplitude and phase sensitivity

$$C_l(\vec{x}) \quad l = 1, 2, \dots, L$$

- Coils are coupled, so noise is correlated

$$E[n_i n_j] = \Psi$$

- Received data from coil  $l$ :

$$m_l(\vec{x}) = C_l(\vec{x})m(\vec{x}) + n_l(\vec{x})$$

- Given  $m_l(x)$ , how do we reconstruct  $m(x)$ ?

# Multi-coil Reconstruction

For a particular voxel  $\vec{x}$

$$\begin{pmatrix} m_1(\vec{x}) \\ m_2(\vec{x}) \\ \vdots \\ m_L(\vec{x}) \end{pmatrix} = \begin{pmatrix} C_1(\vec{x}) \\ C_2(\vec{x}) \\ \vdots \\ C_L(\vec{x}) \end{pmatrix} m(\vec{x}) + \begin{pmatrix} n_1(\vec{x}) \\ n_2(\vec{x}) \\ \vdots \\ n_L(\vec{x}) \end{pmatrix}$$

OR

$$\begin{array}{ccccc} \underline{m_s(\vec{x})} & = & \underline{C} & m(\vec{x}) & + & \underline{n} \\ \text{L} \times \text{1} & & \text{L} \times \text{1} & \text{1} & & \text{L} \times \text{1} \end{array}$$

# Minimum Variance Estimate

$$\hat{m}(\vec{x}) = \underbrace{(C^* \Psi^{-1} C)^{-1}}_{1 \times 1} \underbrace{C^* \Psi^{-1}}_{1 \times L} \underbrace{m_s(\vec{x})}_{L \times 1}$$

Covariance (variance)

$$COV(\hat{m}(\vec{x})) = C^* \Psi^{-1} C$$

What if  $\Psi$  is  $\sigma^2 I$ ?

$$\hat{m}(\vec{x}) = \underbrace{(C^* C)^{-1}}_{\text{Intensity}} \underbrace{C^*}_{\text{Phase}} m_s(\vec{x})$$

Intensity Correction      Phase Correction

# Approximate Solution

- Often we don't know  $C_l(x)$ , but we have

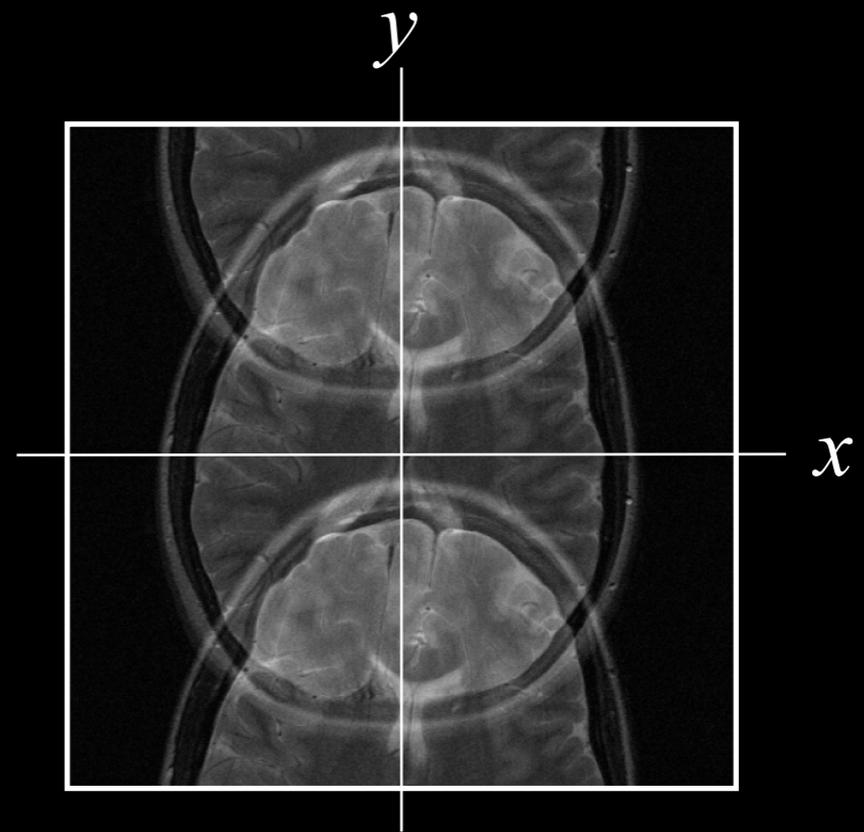
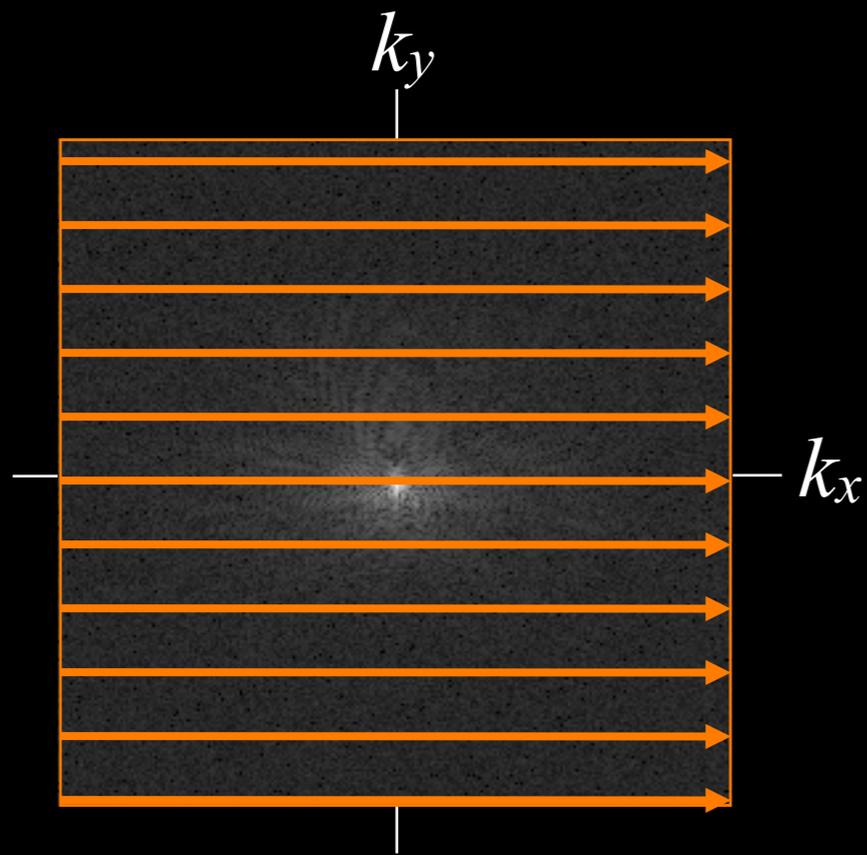
$$m_l(\vec{x}) = C_l(\vec{x})m(\vec{x})$$

- Approximate solution:

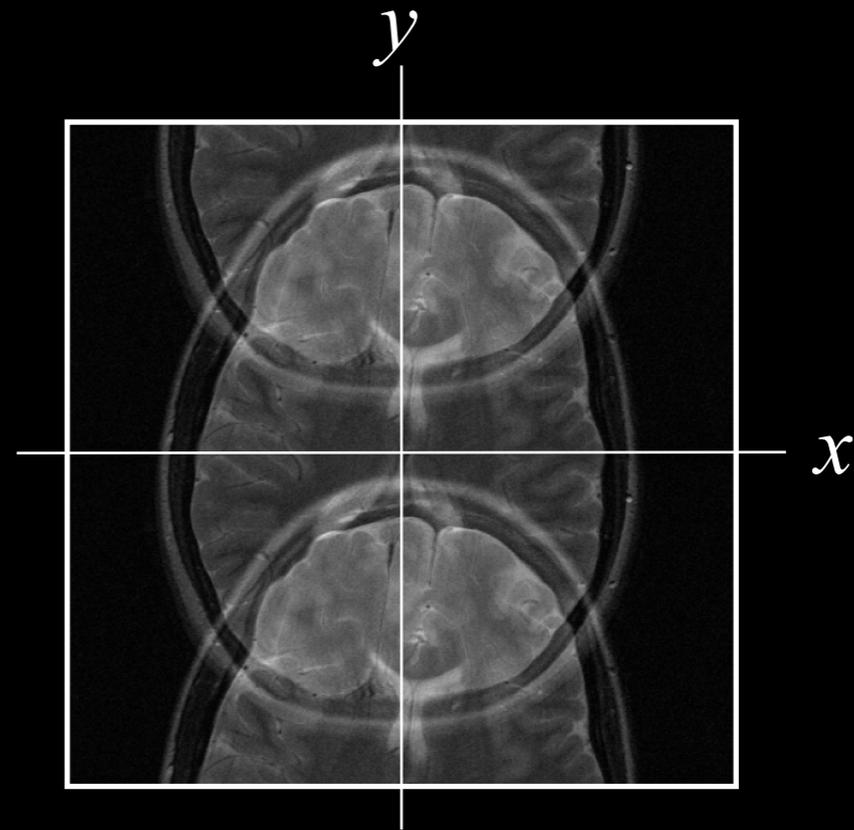
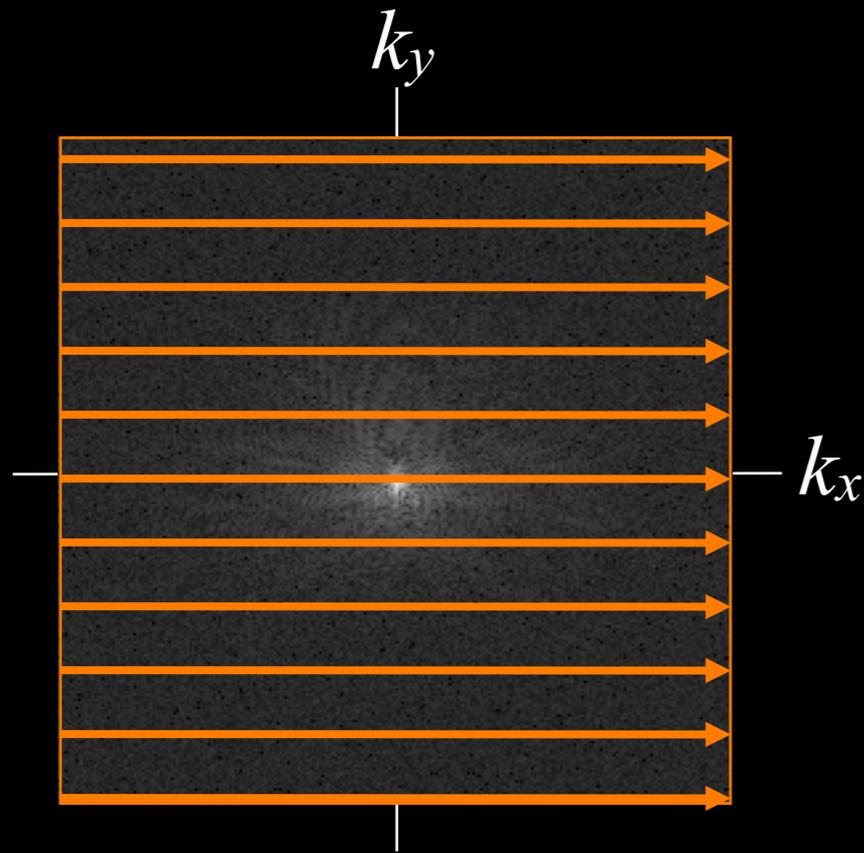
$$\hat{m}_{SS}(\vec{x}) = \sqrt{\sum_l m_l^*(\vec{x})m_l(\vec{x})}$$

- For SNR > 20, within 10% of optimal solution

# Accelerate Imaging with Array Coils



# Accelerate Imaging with Array Coils



- Parallel Imaging
  - Coil elements provide some localization
  - Undersample in k-space, producing aliasing
  - Sort out in reconstruction

# Parallel Imaging

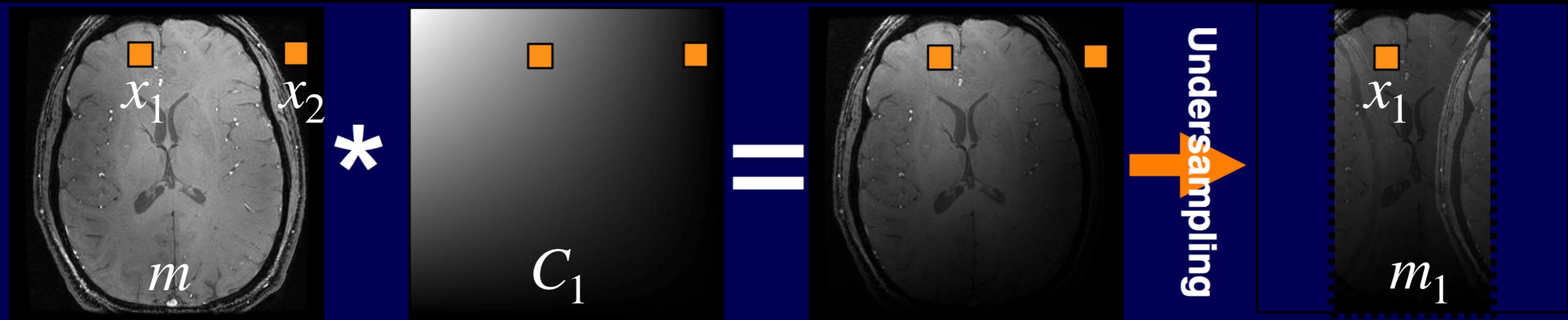
- Many approaches:
  - Image domain - SENSE
  - k-space domain - SMASH, GRAPPA
  - Hybrid - ARC
  
- We will introduce one:
  - SENSE: optimal if you know coil sensitivities

*Pruessmann et al. MRM 1999*

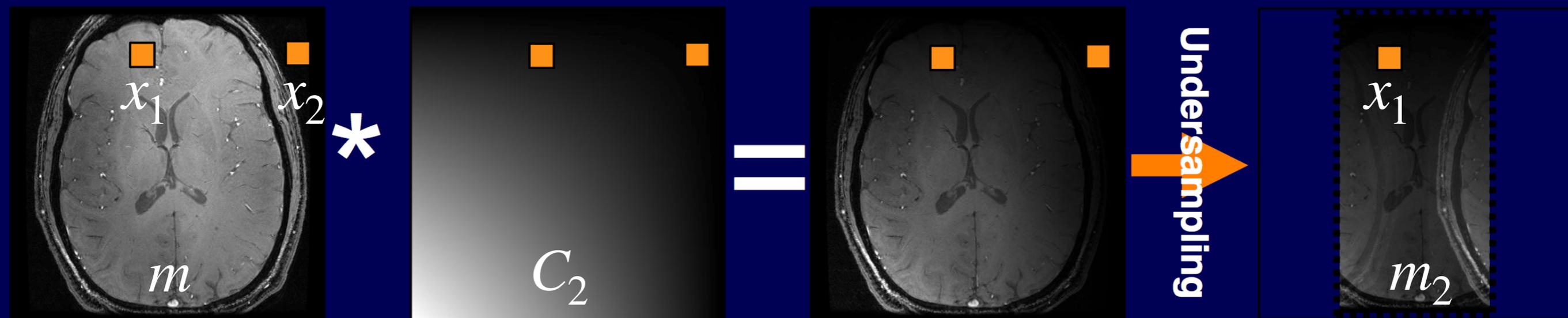
<https://pubmed.ncbi.nlm.nih.gov/10542355/>

# Cartesian SENSE

$$m_1(\vec{x}_1) = C_1(\vec{x}_1)m(\vec{x}_1) + C_1(\vec{x}_2)m(\vec{x}_2)$$



$$m_2(\vec{x}_1) = C_2(\vec{x}_1)m(\vec{x}_1) + C_2(\vec{x}_2)m(\vec{x}_2)$$



$$\begin{pmatrix} m_1(\vec{x}_1) \\ m_2(\vec{x}_1) \\ \cdot \\ \cdot \\ \cdot \\ m_L(\vec{x}_1) \end{pmatrix} = \begin{pmatrix} C_1(\vec{x}_1) & C_1(\vec{x}_2) \\ C_2(\vec{x}_1) & C_2(\vec{x}_2) \\ \cdot & \cdot \\ \cdot & \cdot \\ \cdot & \cdot \\ C_L(\vec{x}_1) & C_L(\vec{x}_2) \end{pmatrix} \begin{pmatrix} m(\vec{x}_1) \\ m(\vec{x}_2) \end{pmatrix} + \begin{pmatrix} n_1(\vec{x}_1) \\ n_2(\vec{x}_1) \\ \cdot \\ \cdot \\ \cdot \\ n_L(\vec{x}_1) \end{pmatrix}$$

Aliased Images
Sensitivity at Source Voxels
Source Voxels

OR

$$\begin{matrix} & & 2 \times 1 \\ m_s = & C & m & + & n \\ L \times 1 & L \times 2 & L \times 1 & & L \times 1 \end{matrix}$$

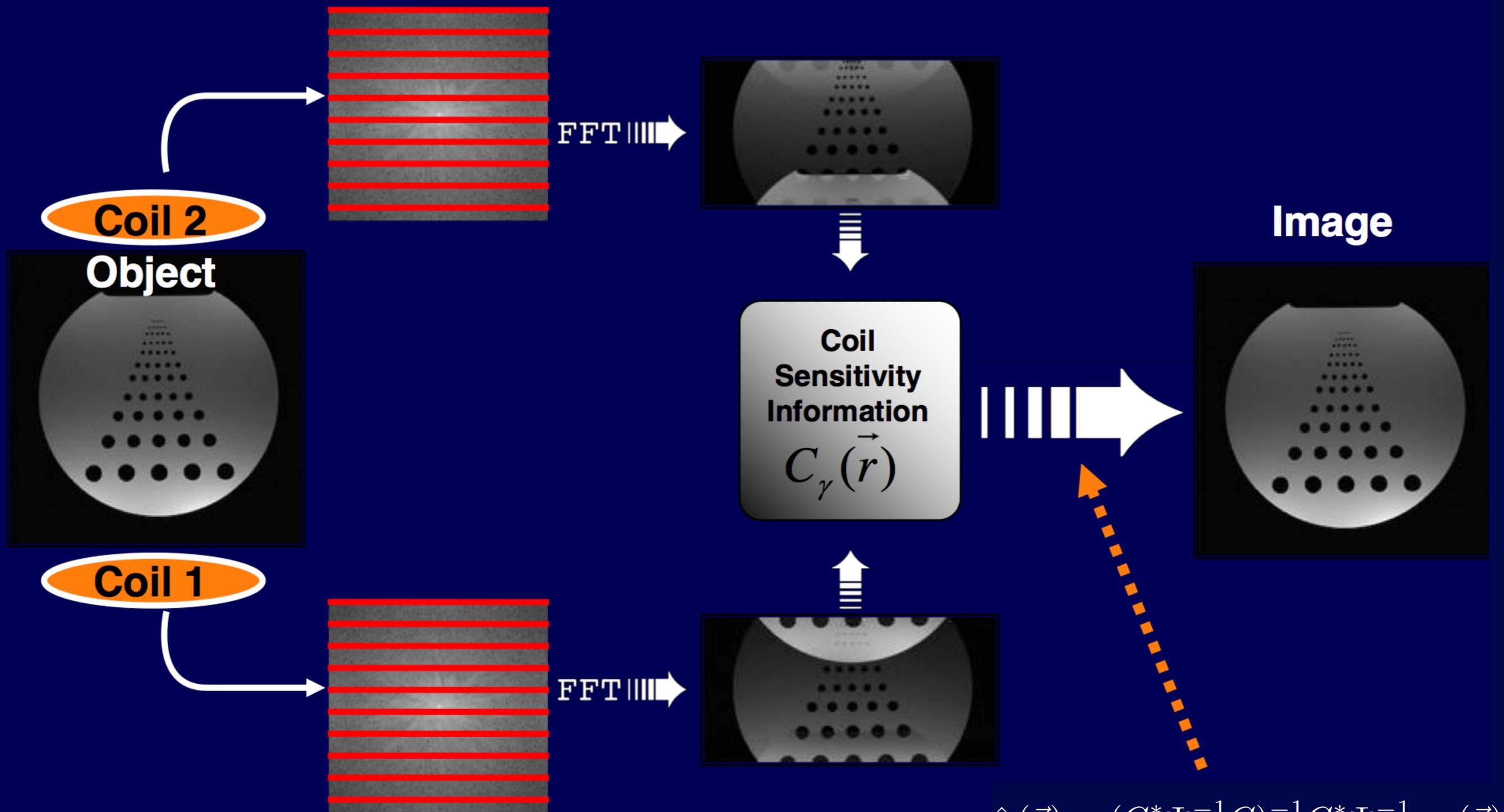
$$\hat{m}(\vec{x}) = \underbrace{(C^* \Psi^{-1} C)^{-1}}_{2 \times 2} \underbrace{C^* \Psi^{-1}}_{2 \times L} \underbrace{m_s(\vec{x})}_{L \times 1}$$

L aliased reconstruction resolves 2 image pixels

For an  $N \times N$  image, we solve  $(N/2 \times N)$   
 $2 \times 2$  inverse systems

For an acceleration factor  $R$ , we solve  $(N/R \times N)$   
 $R \times R$  inverse systems

# SENSE Reconstruction



$$\hat{m}(\vec{x}) = (C^* \Psi^{-1} C)^{-1} C^* \Psi^{-1} m_s(\vec{x})$$

**Unwrap fold over in image space**

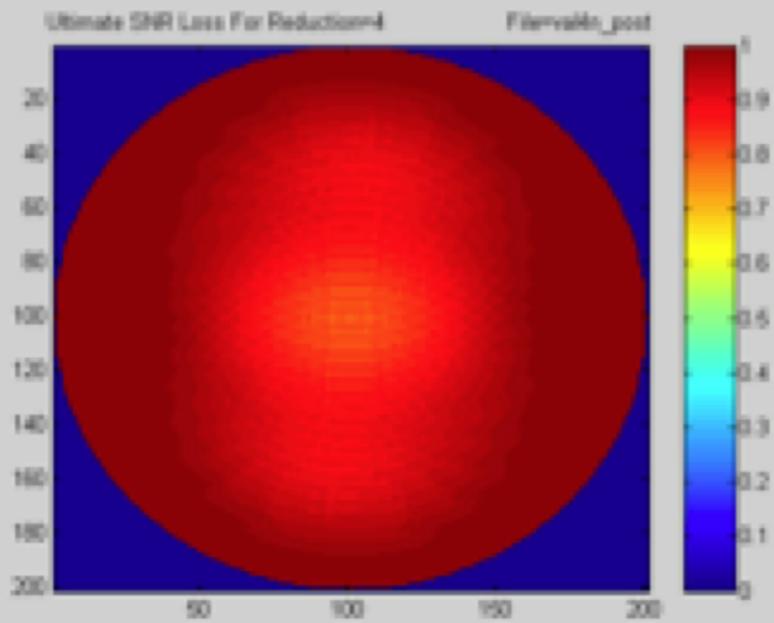
# SNR Cost

- How large can R be?
- Two SNR loss mechanisms
  - Reduced scan time
  - Condition of the SENSE decomposition
- SNR Loss

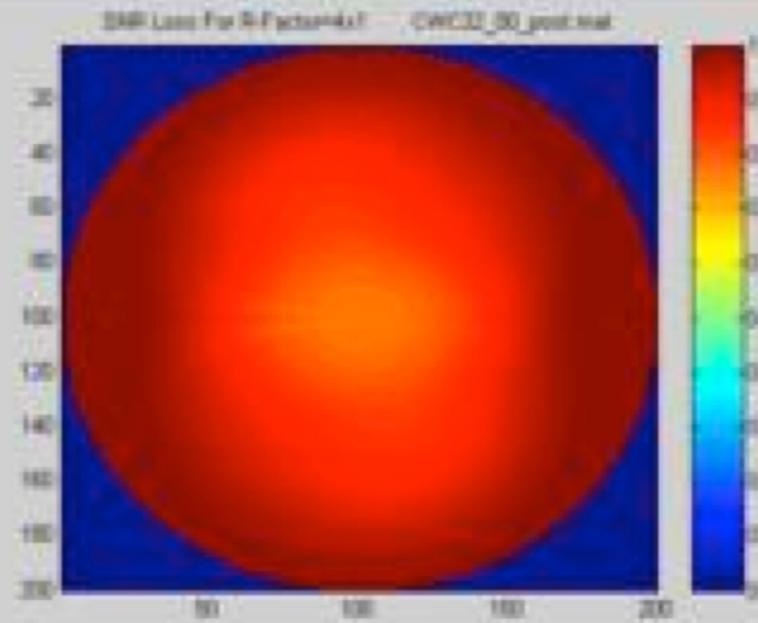
$$SNR_{SENSE} = \frac{SNR}{g\sqrt{R}}$$

Geometry Reduced  
Factor Scan Time

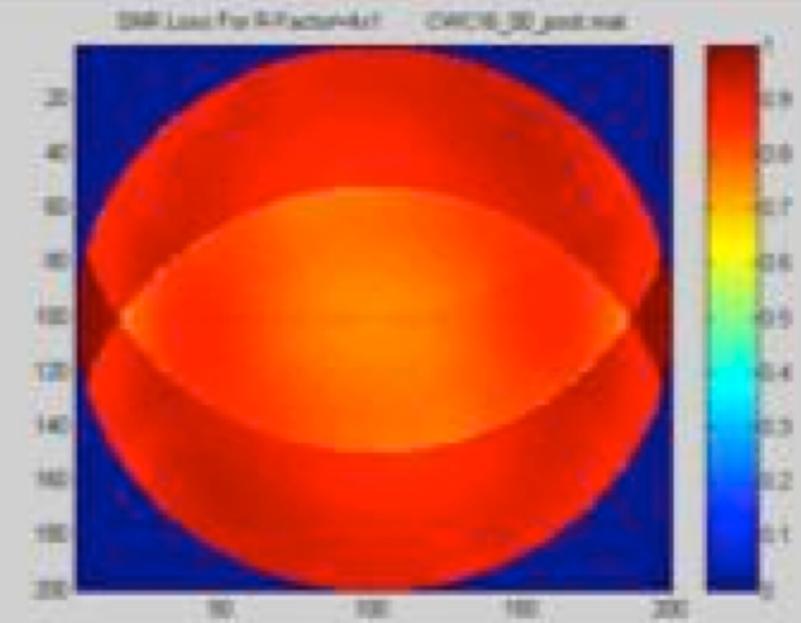
# 1/g-factor Map for R=4



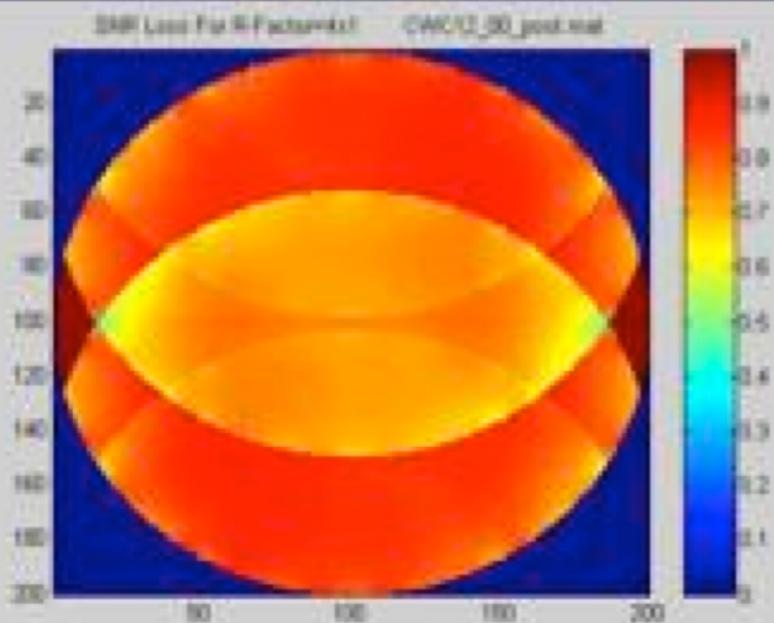
$\infty$  elements



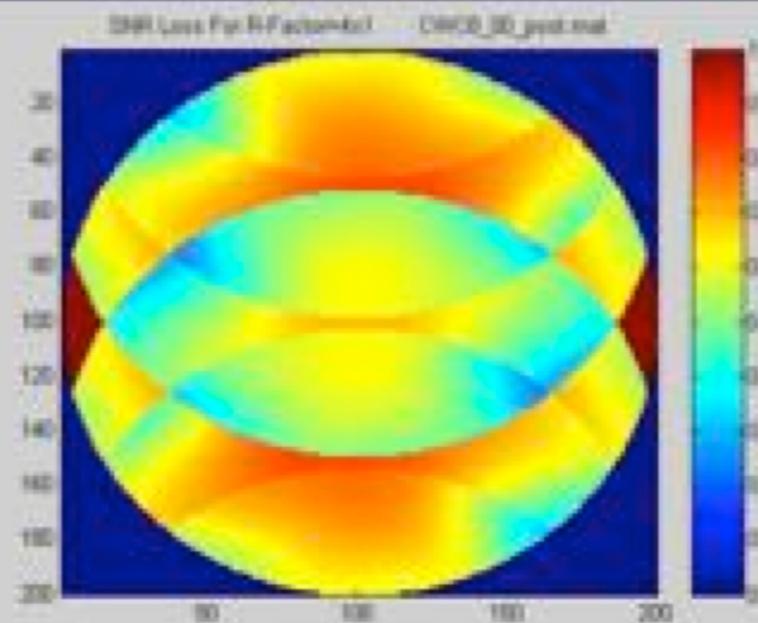
32 elements



16 elements



12 elements



8 elements

Relative  
SNR  
Scale

# g-factor and its Impact on Images

Rate 1

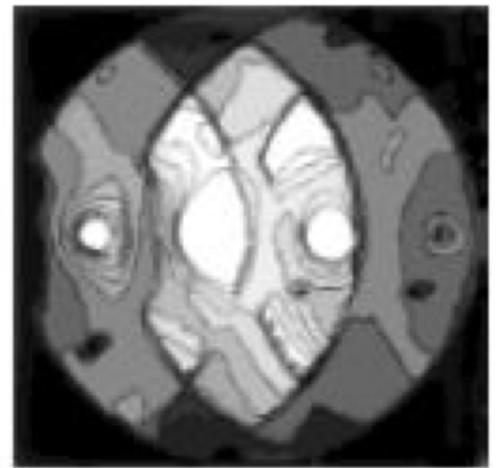
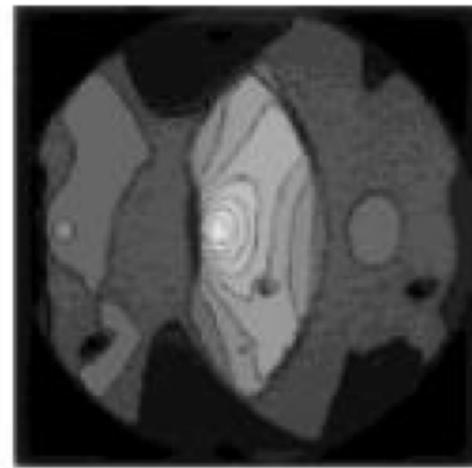
2

2.4

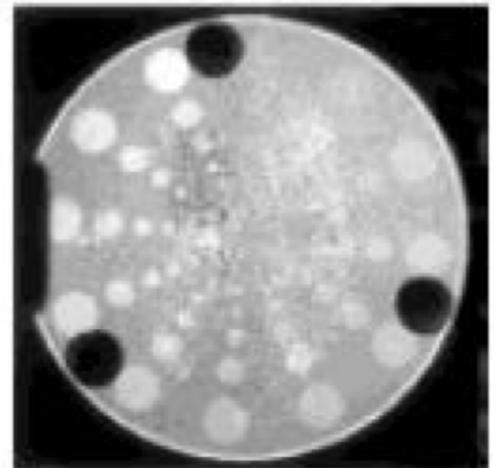
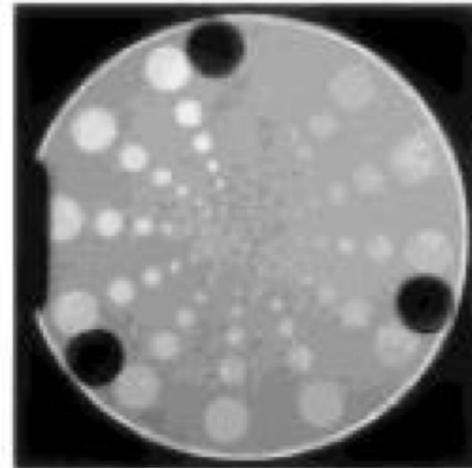
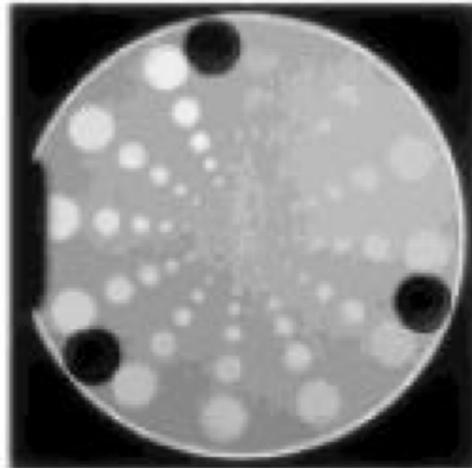
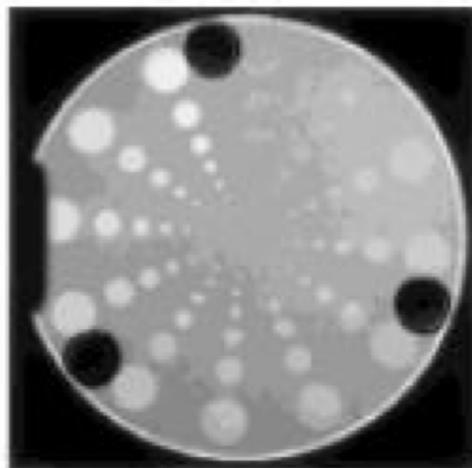
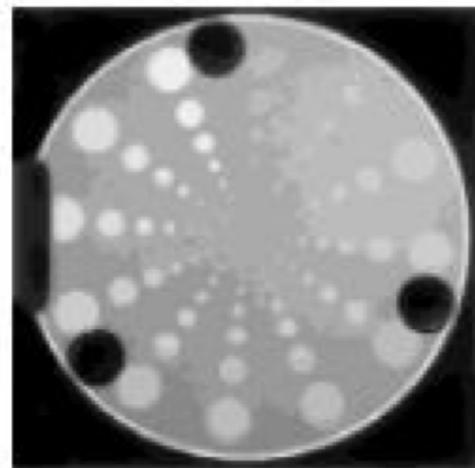
3

4

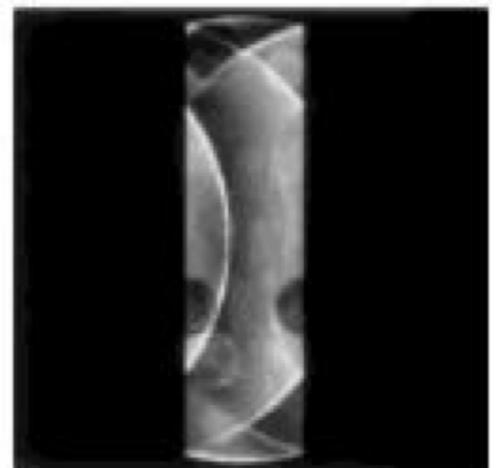
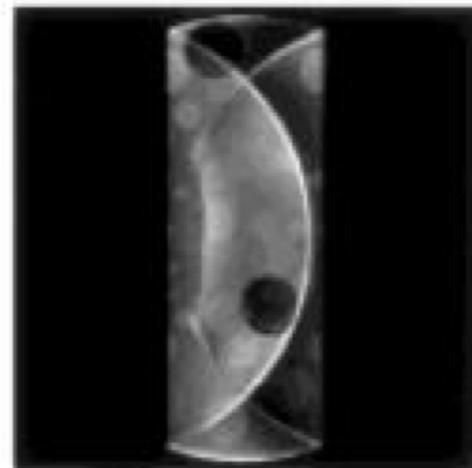
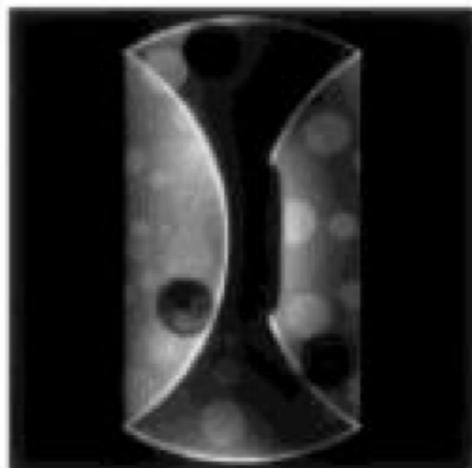
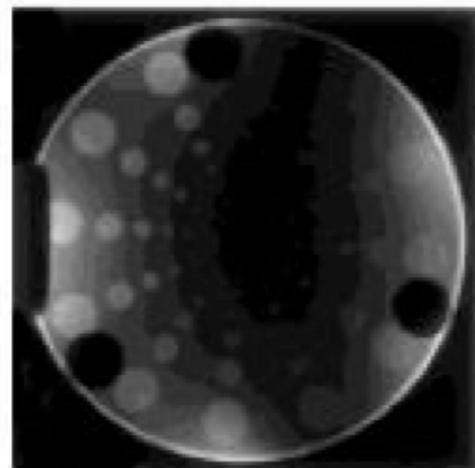
g-map



SENSE



aliased



# Parallel Imaging

- Utilizes coil sensitivities to increase the speed of MRI (typical  $R=2-4$ )
- Can be combined with other techniques
  - Efficient pulse sequences
  - non-Cartesian trajectories
  - Constrained reconstruction

# Parallel Imaging

- Cases for parallel imaging
  - Higher patient throughput
  - Real-time imaging/Interventional imaging
  - Motion suppression
- Cases against parallel imaging
  - Low SNR applications

# Thanks!

- Interested in more?
- M219 upcoming lectures
- M229 in Spring
  - Fast imaging sequences
  - Fast sampling trajectories
  - Parallel imaging
  - Constrained reconstruction
  - Deep learning-based methods

# Thanks!

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