

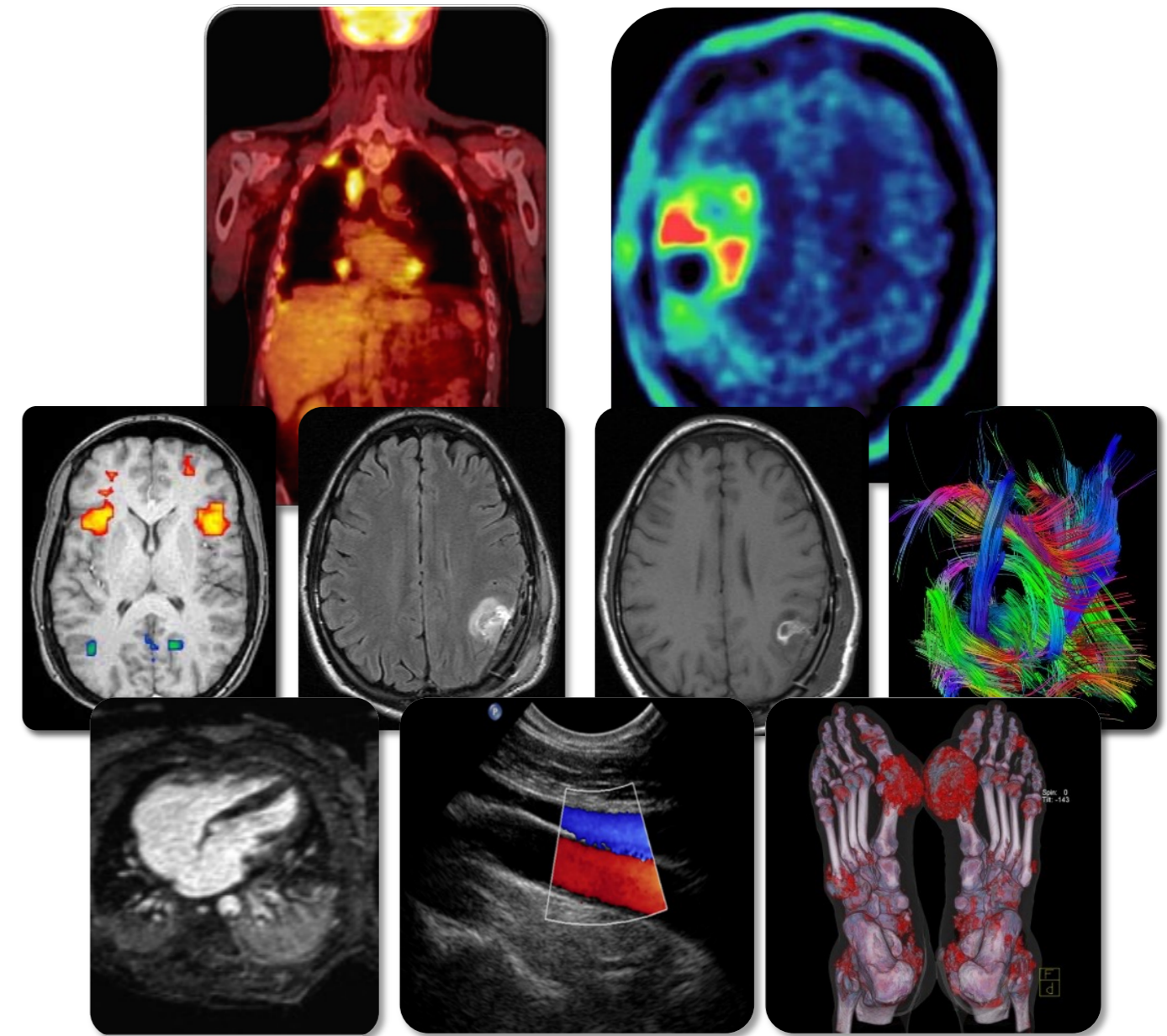
Advanced Application of MRI: Towards Quantitative Analysis & Biological Insights of Disease

William Hsu, PhD

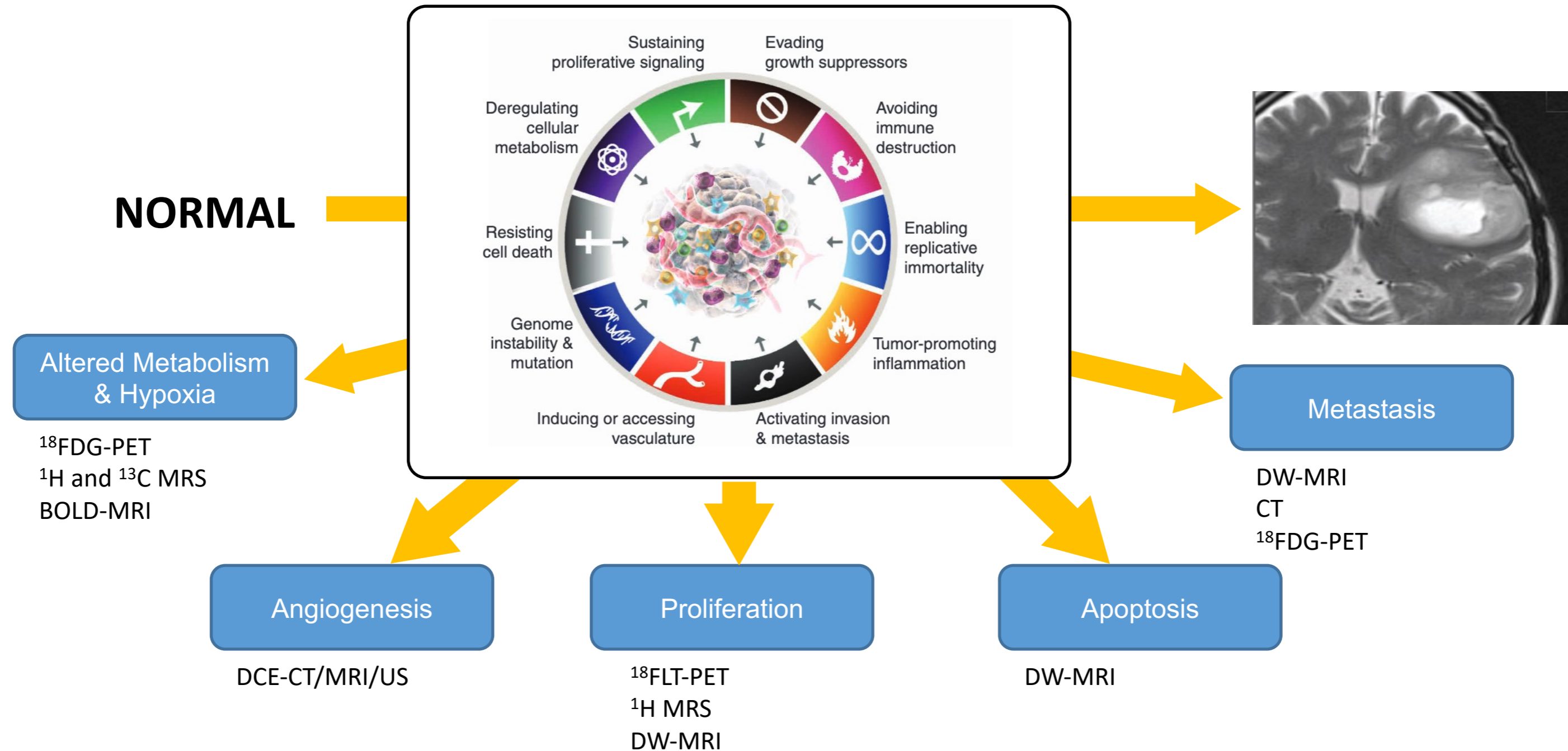
Associate Professor of Radiological Sciences,
Bioinformatics, and Bioengineering
Medical & Imaging Informatics

The role of multimodal imaging

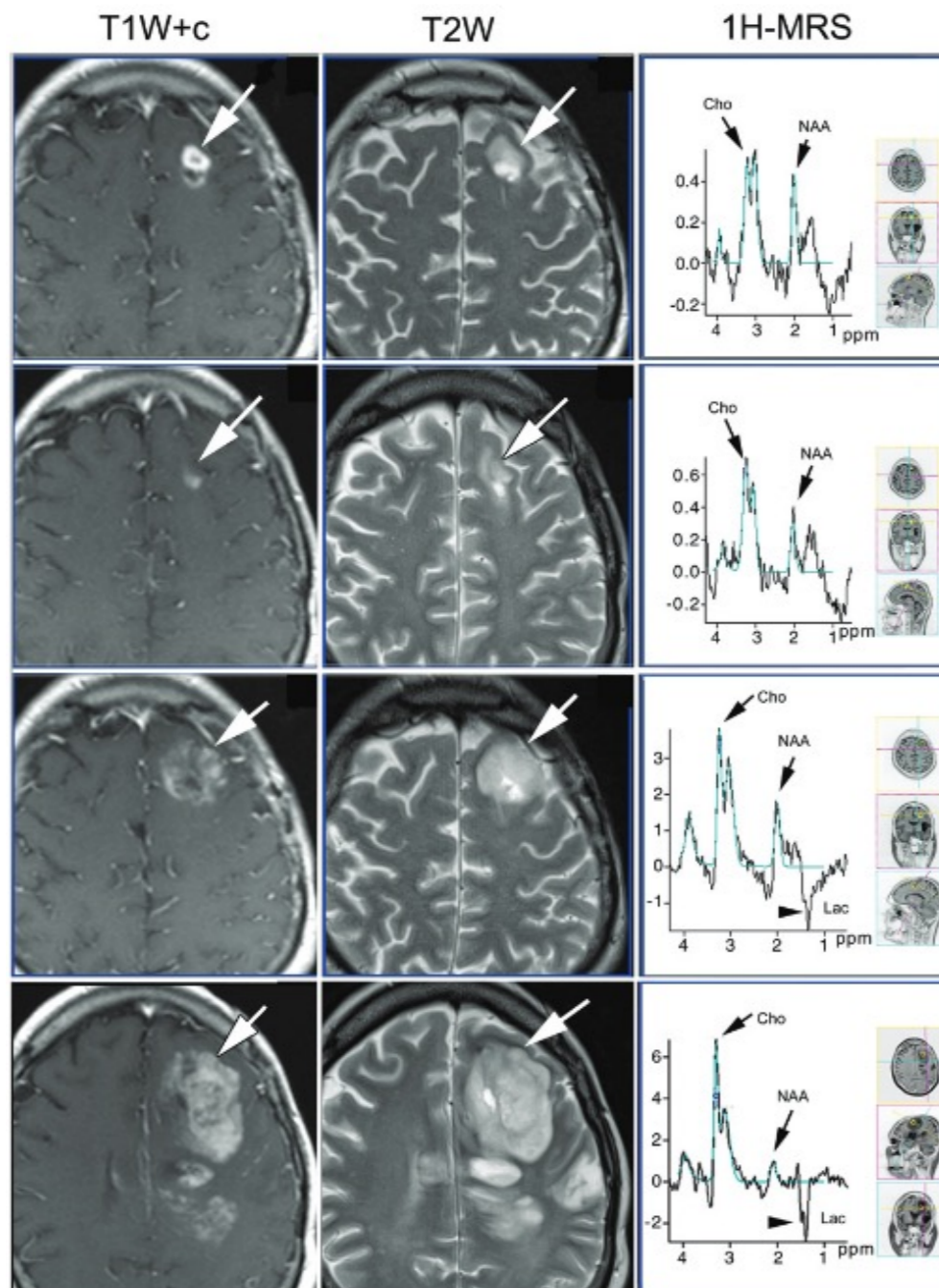
- Unique, in vivo, multi-scale view of anatomic and physiologic processes
- Utilized in the diagnosis, characterization, and clinical management of many diseases
- Biomarker of survival or treatment response
- A bridge between clinically observable level and lower biological scales



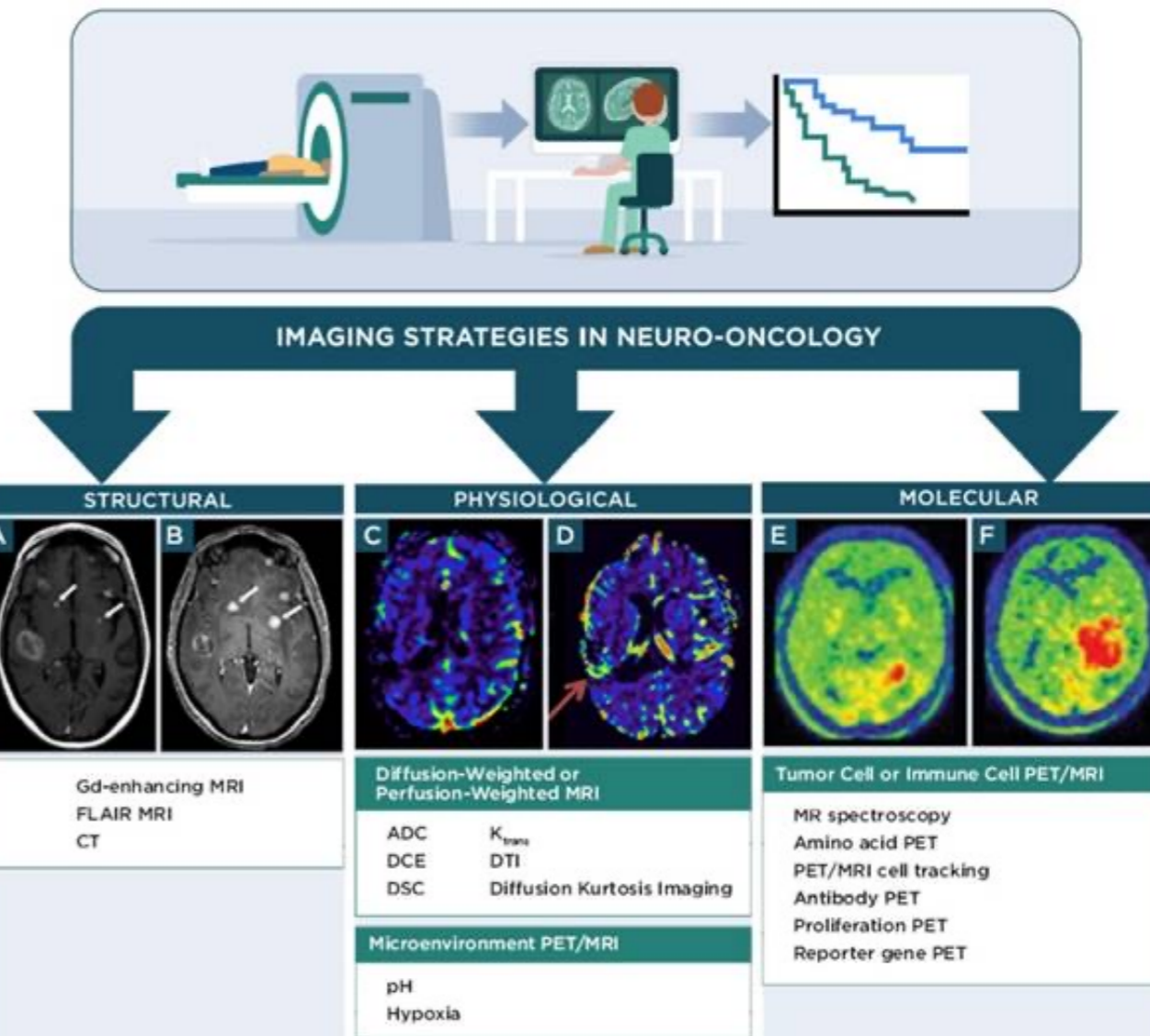
Imaging the “Hallmarks of Cancer”



Imaging treatment response

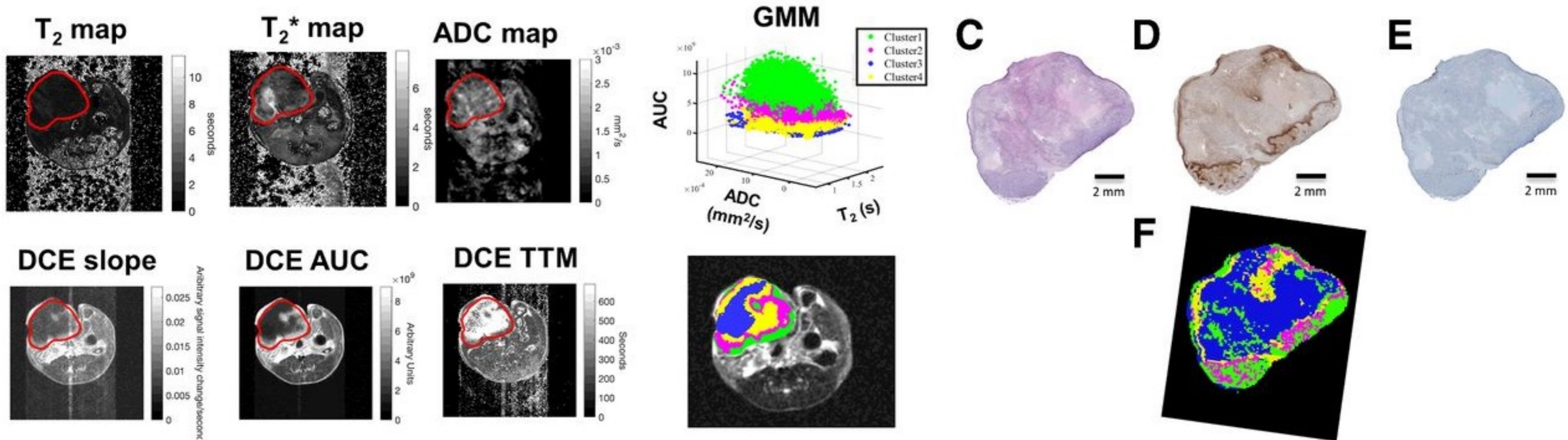


Padhani, A. R. & Miles, K. A. *Radiology* **256**, 348–364 (2010).



Kasten, B. B. *et al. Theranostics* **9**, 5085–5104 (2019).

Habitat maps combining MRI and histopathology



Driving questions

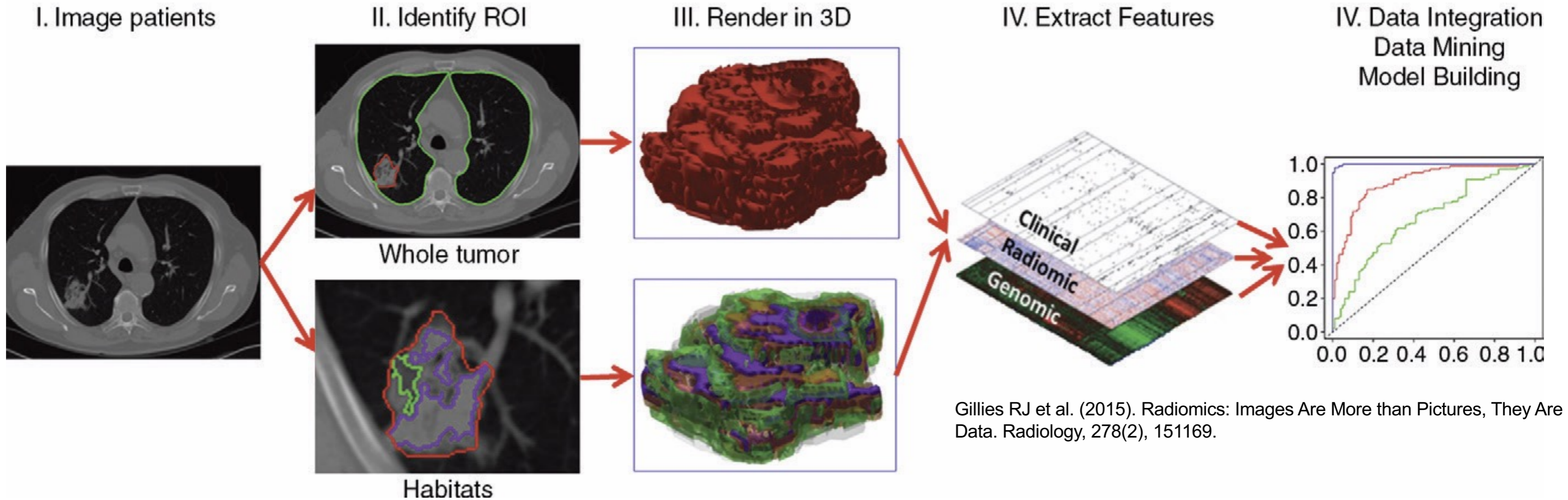
- What techniques exist for extracting biological knowledge using quantitative analysis of (MR) images?
- What barriers need to be addressed before biological insights can be reliably obtained?
- What role does imaging informatics play in the integration and analysis of biological information?

Outline

- Radiomics
- Mitigating variability due to image acquisition
- Spatially registering multimodal images
- Multimodal data fusion
- Ongoing efforts and concluding thoughts

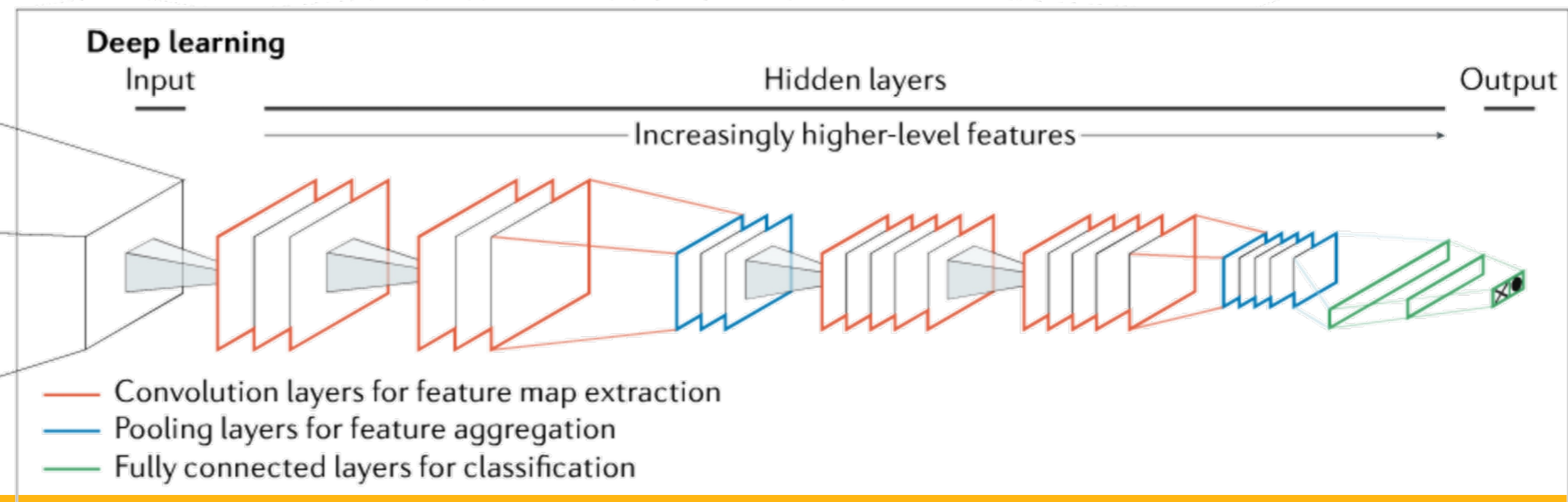
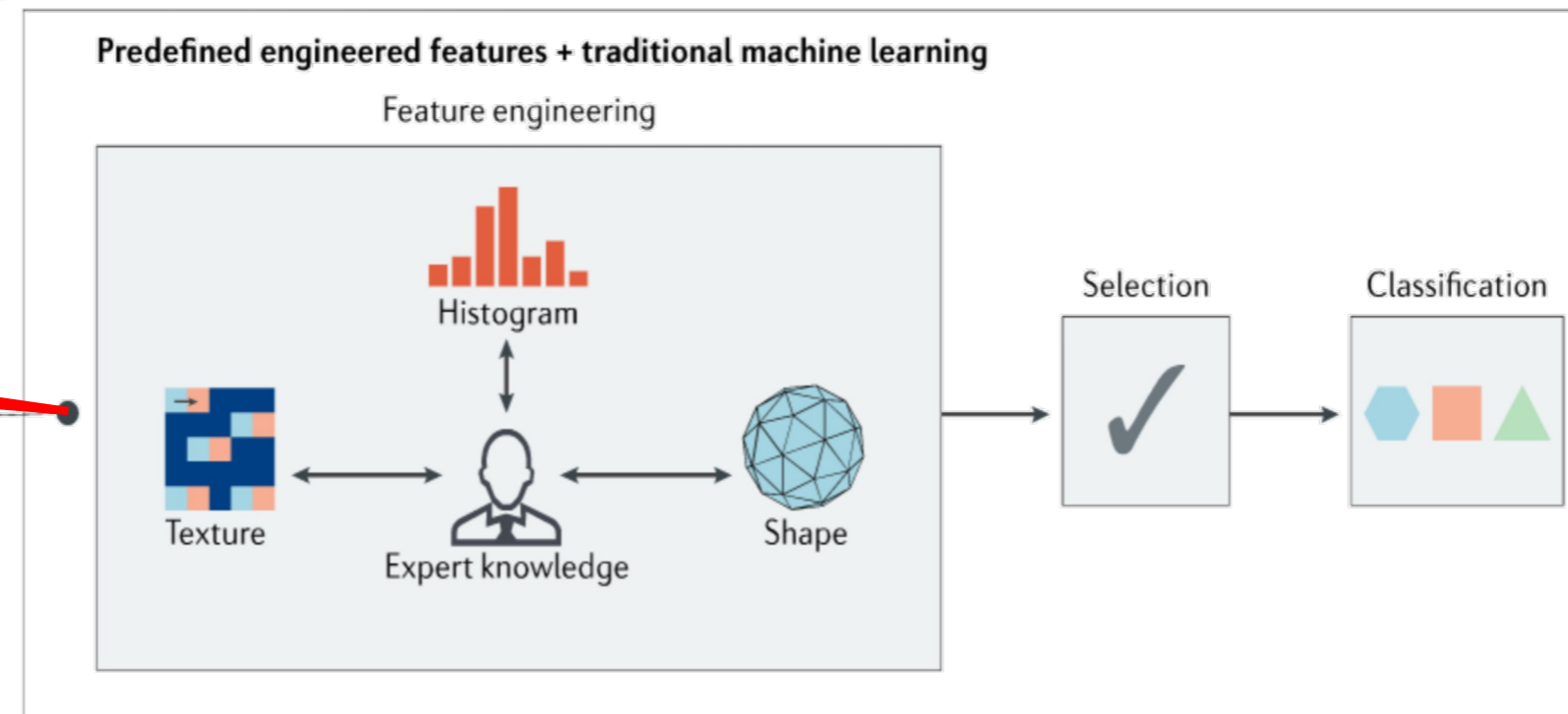
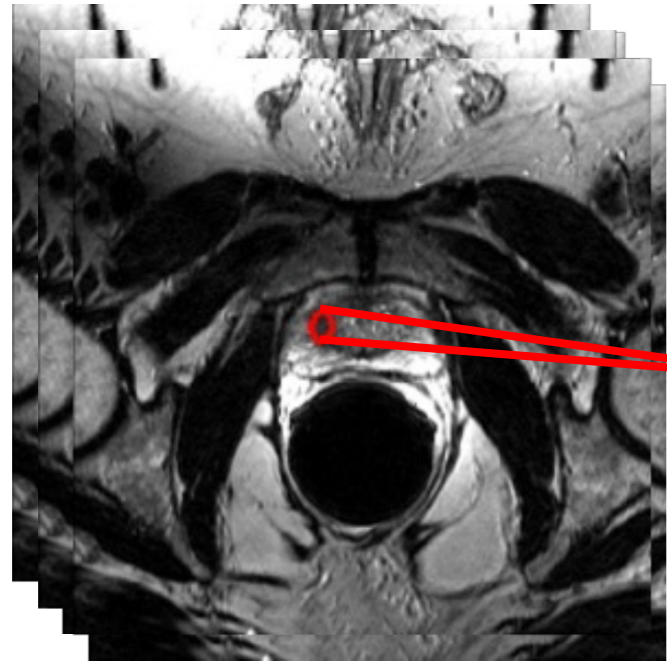
Radiomics

What is radiomics

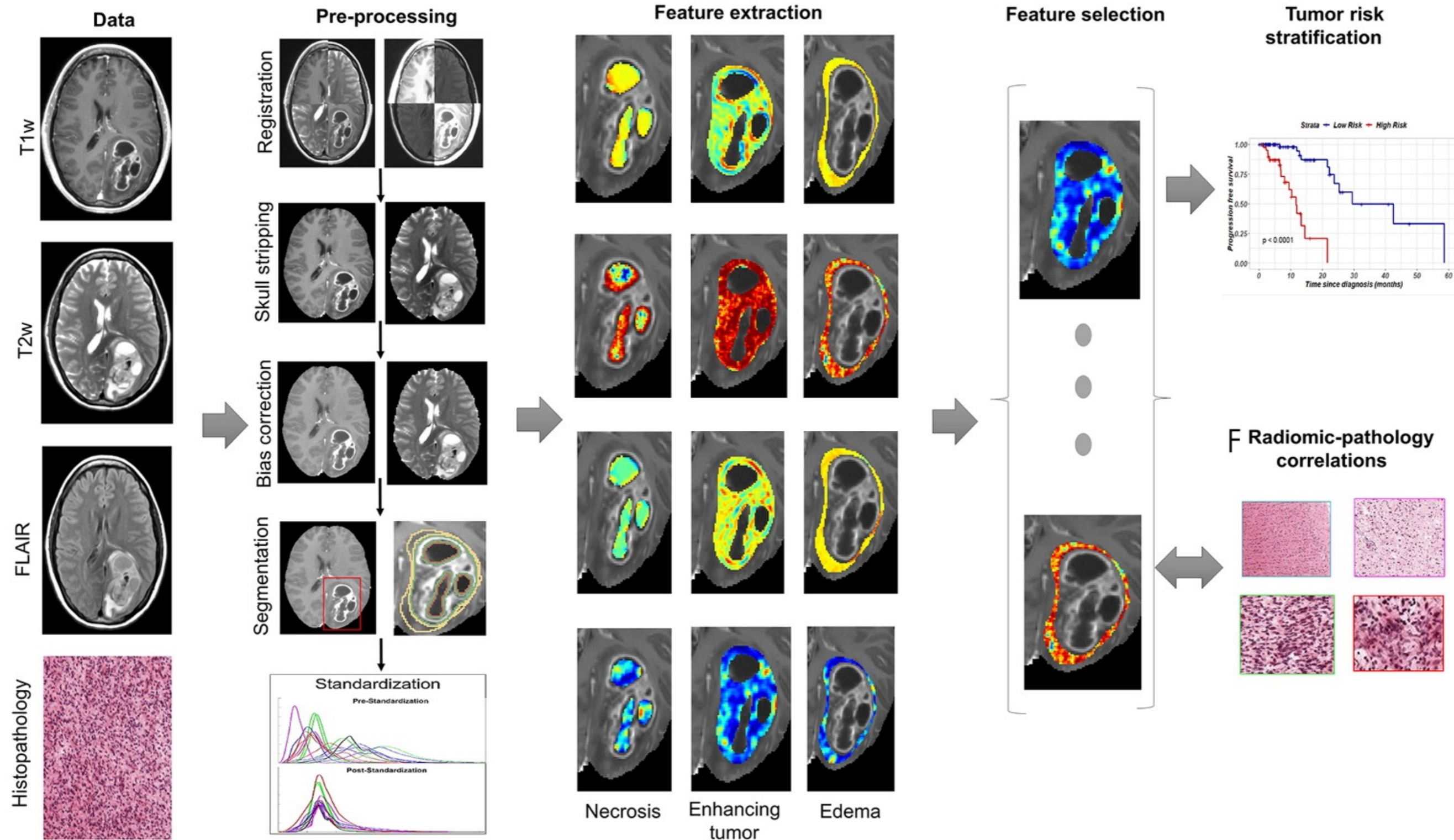


Gillies RJ et al. (2015). Radiomics: Images Are More than Pictures, They Are Data. *Radiology*, 278(2), 151169.

Radiomic vs deep features



Typical radiomic analysis pipeline



Families of radiomic features

Feature family	count	ROI mask		
		morph.	int.	discr.
morphology	29	✓	✓	×
local intensity	2	×	✓ ^a	×
intensity-based statistics	18	×	✓	×
intensity histogram	23	×	✓	✓
intensity-volume histogram	5	×	✓	✓ ^b
grey level co-occurrence matrix	25	×	✓	✓
grey level run length matrix	16	×	✓	✓
grey level size zone matrix	16	×	✓	✓
grey level distance zone matrix	16	✓	✓	✓
neighbourhood grey tone difference matrix	5	×	✓	✓
neighbouring grey level dependence matrix	17	×	✓	✓

- Number of features in the document
- The required input of a morphological (morph.) and/or intensity (int.) ROI mask
- Requirement of image discretization (discr.)

^a The entire image volume should be available when computing local intensity features

^b Image discretization for the intensity-volume histogram is performed with finer discretization than required for e.g. textural features

Discretization

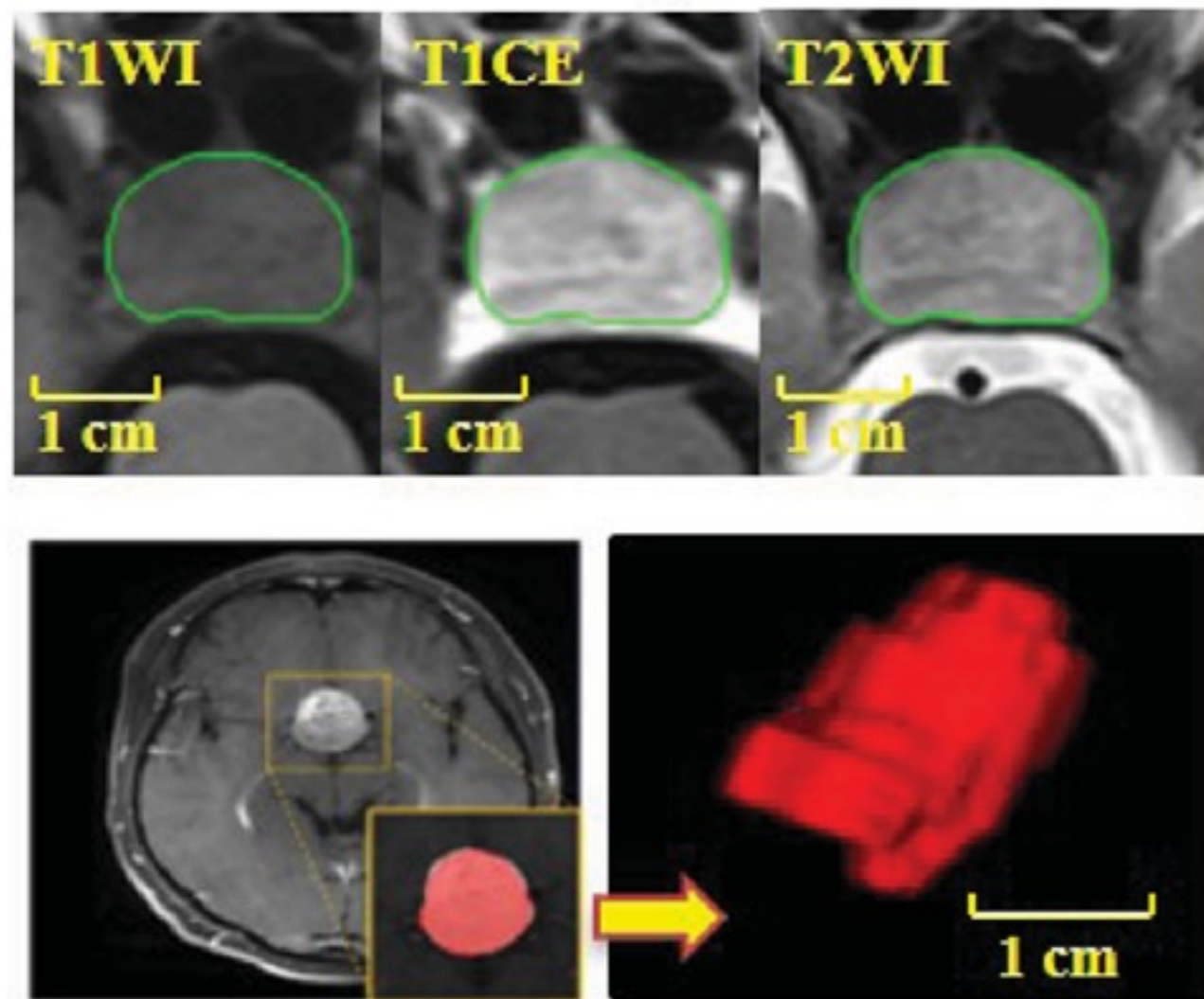
- Intensity-resampling step applied to the image before computing features (used widely in intensity and texture features)
 - Matrix dimensions are determined by the number of intensity values obtained after this resampling
 - One approach: assign intensity value to bin based on:

$$I_B = B \times \frac{I - I_{min}}{I_{max} - I_{min}}$$

B = number of bins (8, 16, 32, 64...)

I_{min} , I_{max} = min/max intensity values in image

Morphology



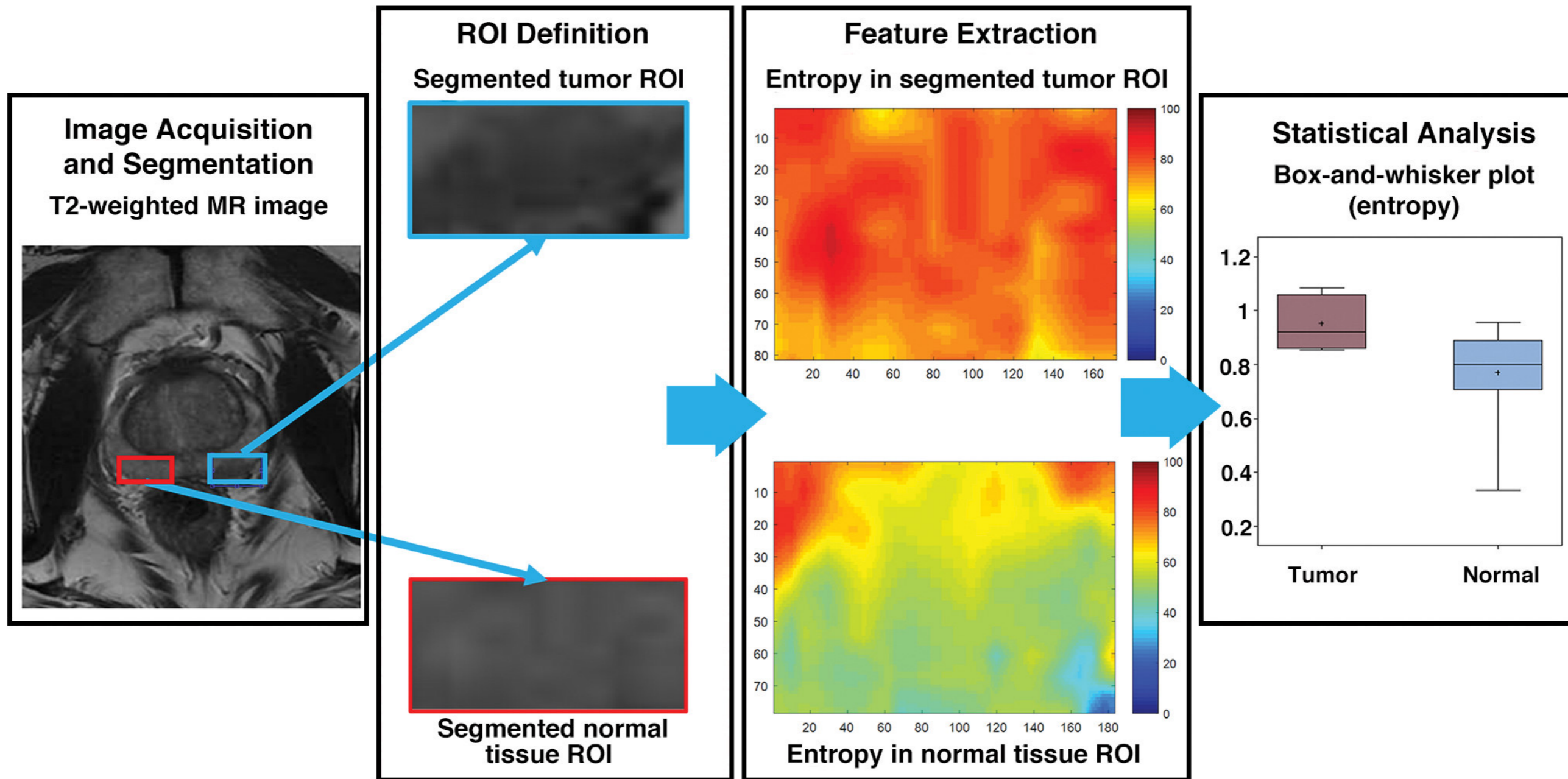
- Volume
- Surface area
- Sphericity
- ...

Source: <https://onlinelibrary.wiley.com/doi/10.1002/jmri.27930>

Intensity

- **Local intensity features**: computed from voxel intensities within a defined neighborhood around a center voxel
- **Intensity-based statistical features**: description of how intensities within an ROI are distributed
- **Intensity histogram features**: characterization of the histogram profile after discretizing the original intensity distribution into bins
- **Intensity-volume histogram features**: description of the relationship between a defined discretized intensity bin and the fraction of the ROI that have voxel intensities within this bin

Texture



Co-Occurrence Matrix

- **Co-occurrence matrix** is defined over an image to be the distribution of co-occurring values at a given offset
 - How combinations of (discretized) grey levels of neighboring pixels or voxels in a 3D volume are distributed along one of the image directions
- **Grey Level Co-occurrence Matrix (GLCM aka Harlick features)** calculates how often a pixel with grey-level value i occurs either horizontally, vertically, or diagonally to adjacent pixels with the value j
 - Relationship between the reference and neighboring pixel (e.g., second order feature)

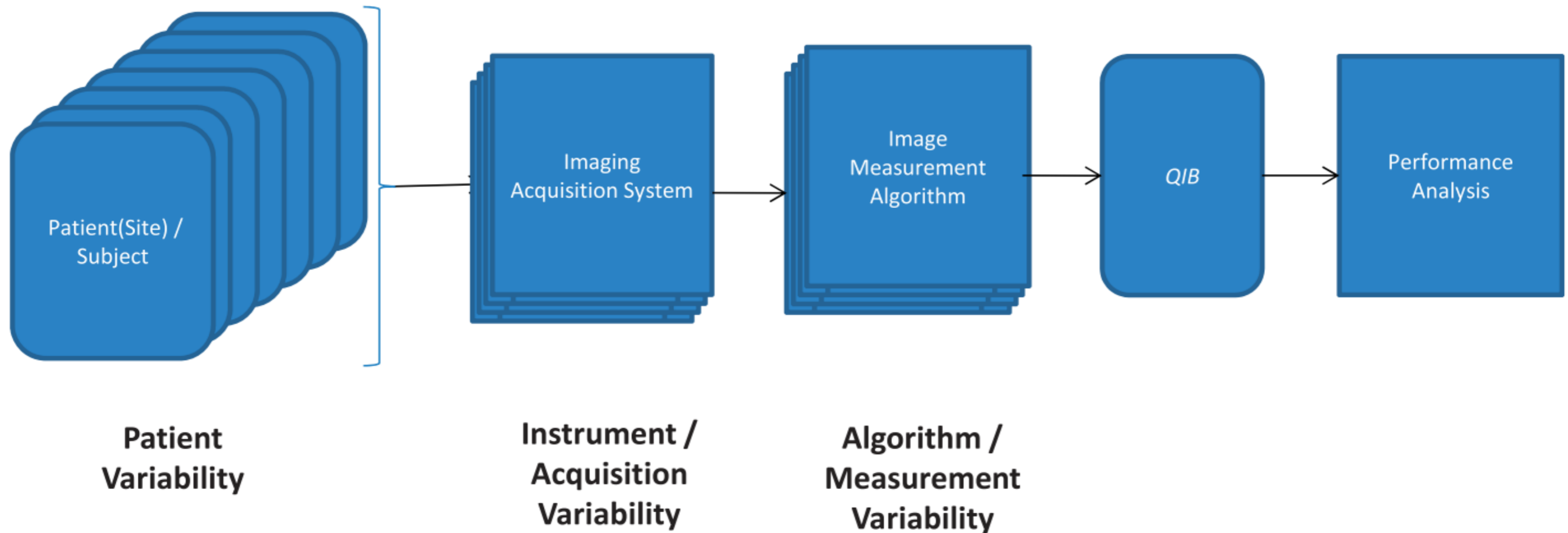
Calculating GLCM

0	0	1	1
0	0	1	1
0	2	2	2
2	2	3	3

1. Discretize the image
2. Create a framework matrix
3. Decide on the spatial relation between the reference and neighbor
4. Count the occurrences and complete the framework matrix
5. Add the matrix to its transpose to make it symmetrical
6. Normalize the matrix

Mitigating variability due to image acquisition

Sources of variability



Repeatability vs reproducibility

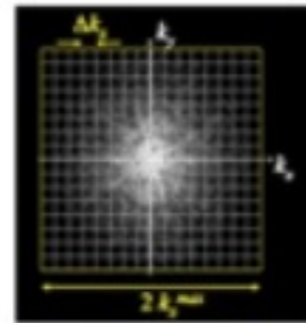
- **Repeatability** refers to “variability of the quantitative image biomarker when repeated measurements are acquired on the same experimental unit under identical or nearly identical conditions” to determine the measurement error
- **Reproducibility** refers to “variability in the quantitative image biomarker measurements associated with using the imaging instrument in real-world clinical settings”

Factors that influence radiomics stability

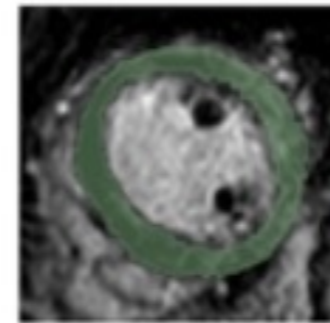
Image acquisition



Reconstruction



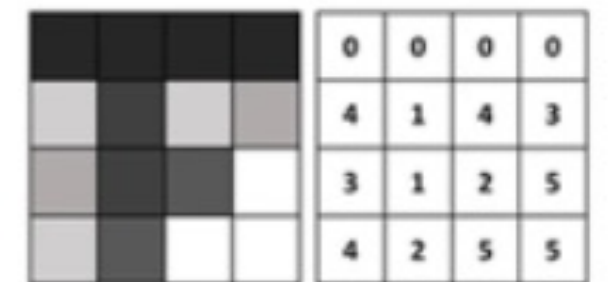
Segmentation



Post-processing



Feature extraction



MRI

- Field strength
- Sequence design
- Matrix size (acquired)
- Field of view
- Slice thickness
- Acceleration techniques
- Vendor
- Contrast timing
- Movement

- Matrix size (reconstructed)
- Reconstruction technique

- Manual 2D
- Manual 3D
- Semi-automated 2D
- Semi-automated 3D
- Automated 2D
- Automated 3D
- Size of the ROI

- Image interpolation ('resampling' / 'rescaling')
 - Grid alignment
 - Pixel sizing
- Intensity discretisation ('rebinning')
- Normalisation

- Mathematical formula
- Post-processing platform

Measuring agreement

- Intraclass correlation (ICC)

$$Y_{ij} = \mu + \alpha_j + \varepsilon_{ij},$$

$$\frac{\sigma_{\alpha}^2}{\sigma_{\alpha}^2 + \sigma_{\varepsilon}^2}.$$

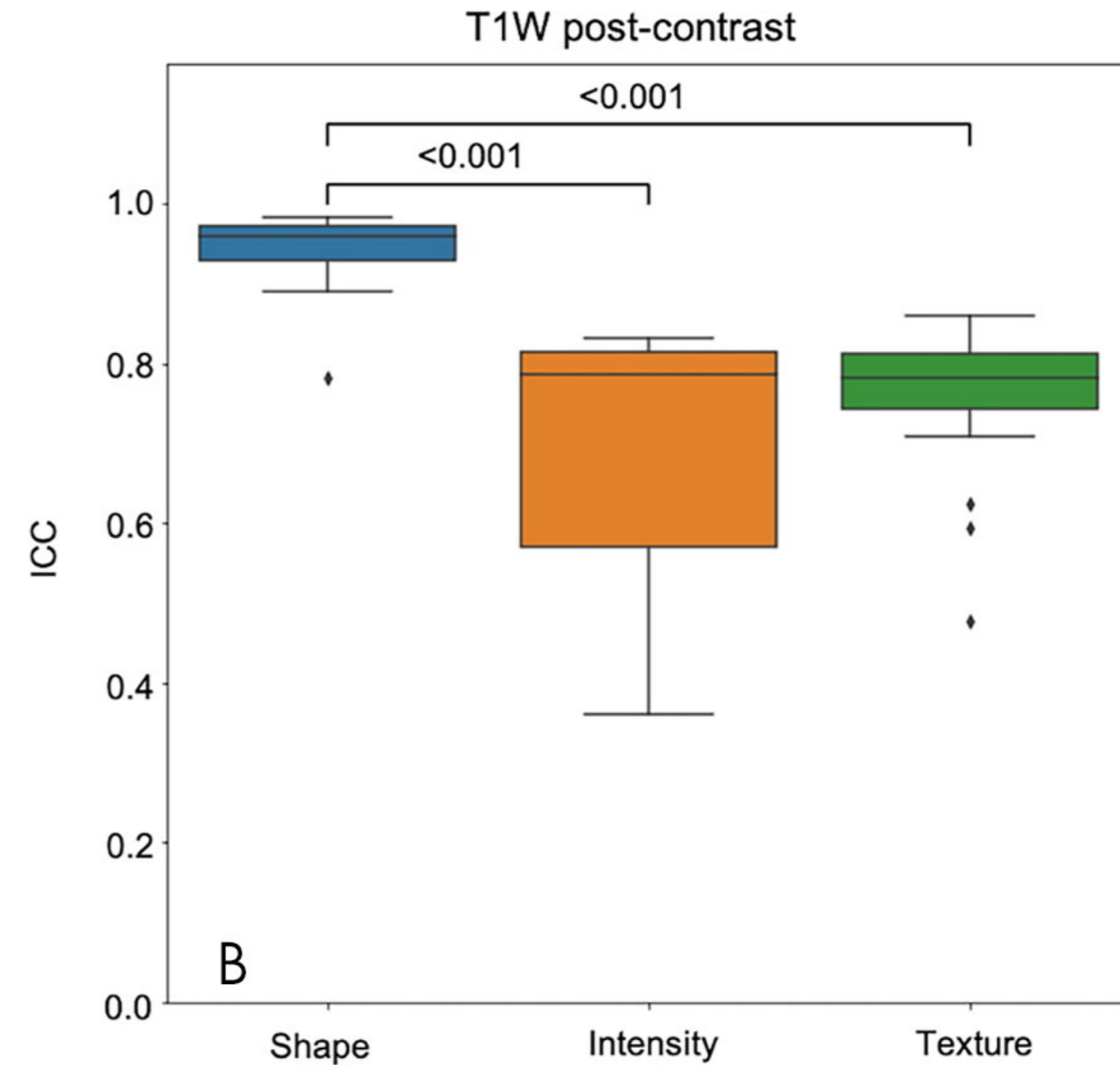
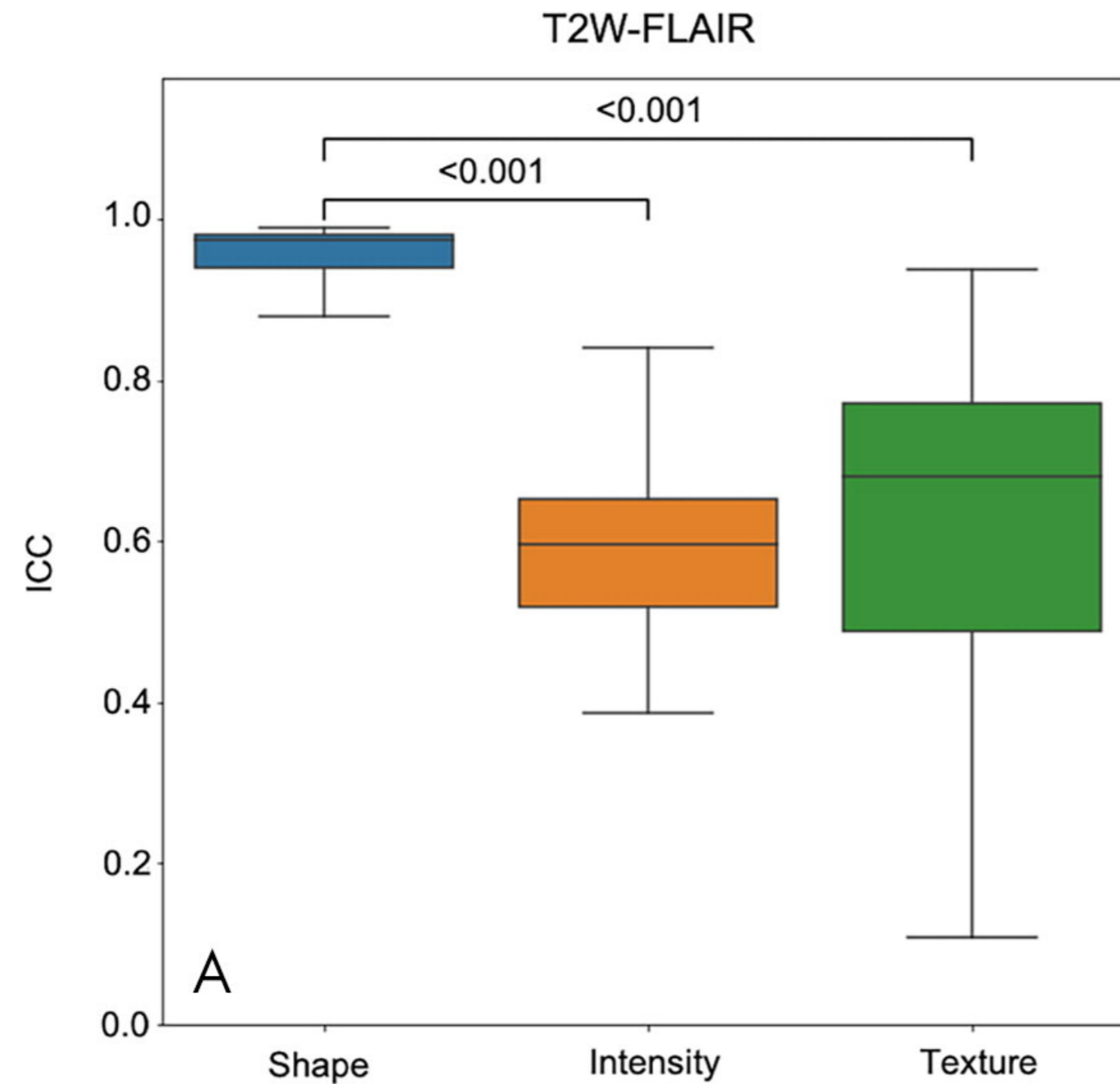
- Assumes linear relationship between variables
- Takes into account differences in the means of the measures being considered
- Can be generalized to multiple readers

- Concordance correlation (CCC)

$$P_{CCC} = \frac{2\sigma_{12}}{\sigma_{\beta}^2 + \sigma_{\beta}^2 + (\mu_1 - \mu_2)^2}.$$

- No statistical model is assumed in the definition
- Does not assume a common mean for judges' ratings
- Applies to only two judges at a time

ICC values from scan/rescan of same patient



Normalization techniques

- Z score normalization

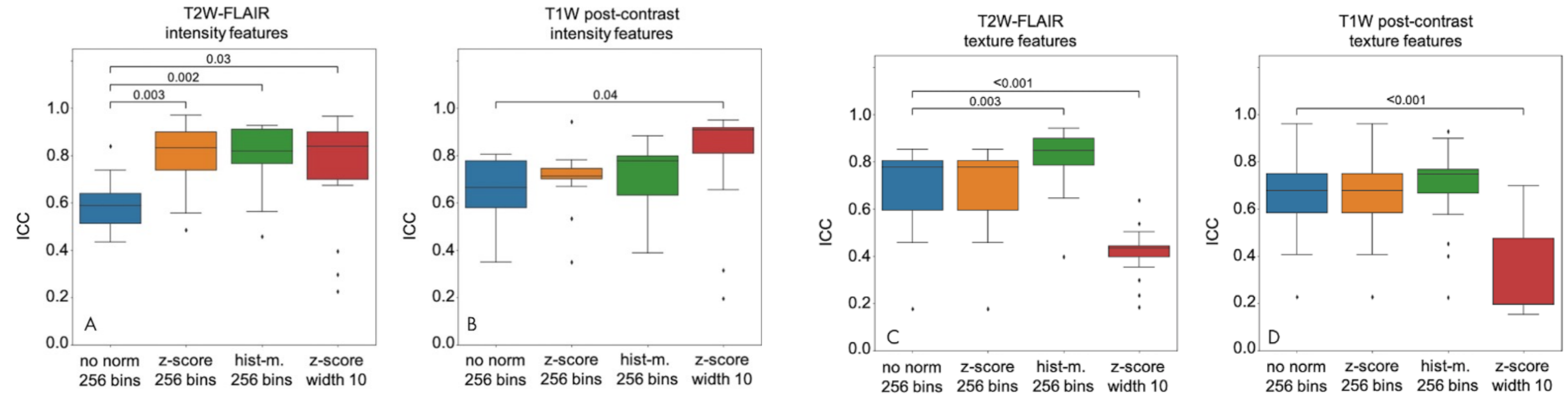
- Subtract the mean intensity of the entire image or a region of interest from each voxel value and dividing it by the corresponding standard deviation
- Mean of the voxel intensity distribution is centered at zero with unit variance

- Histogram matching

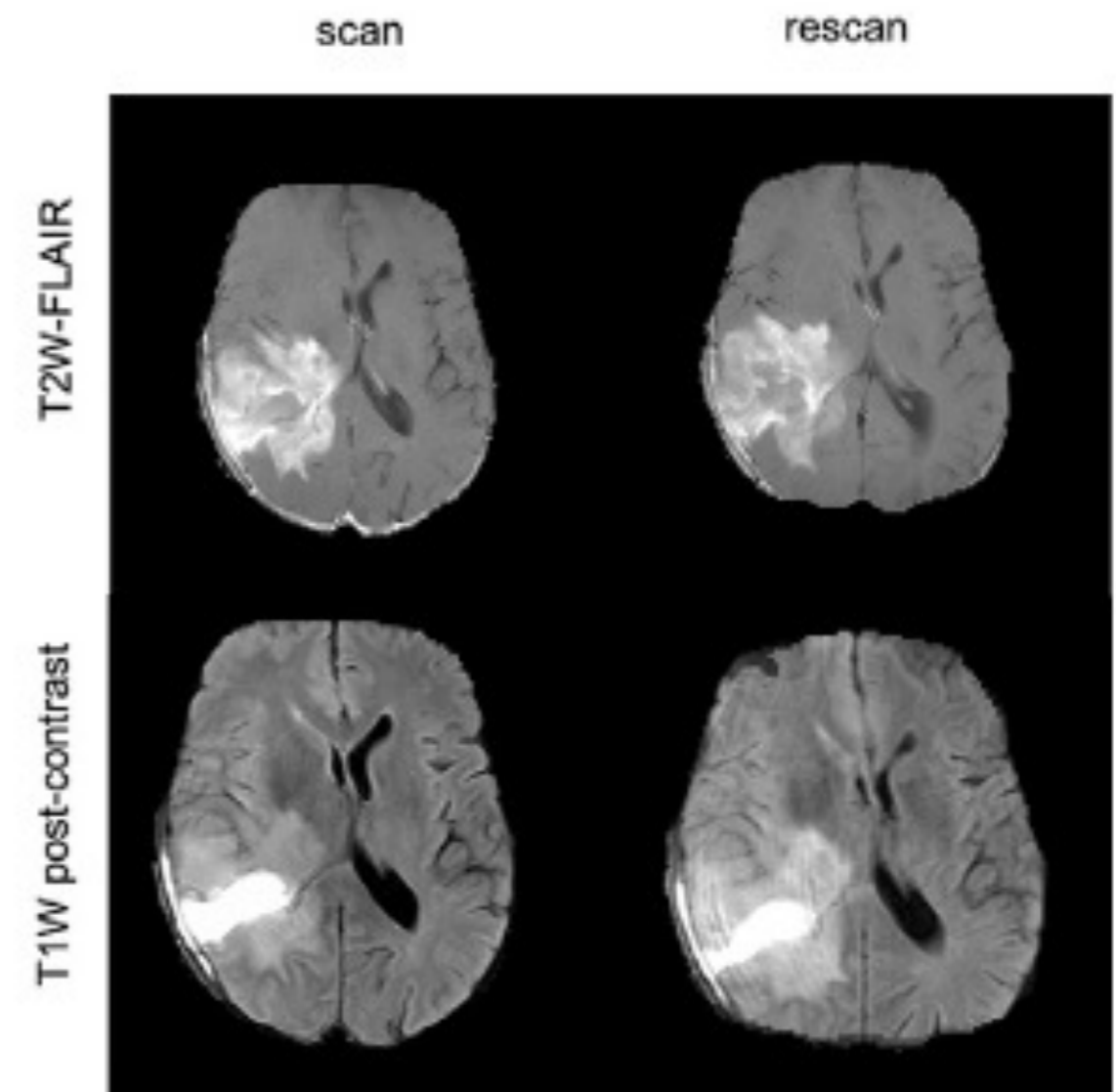
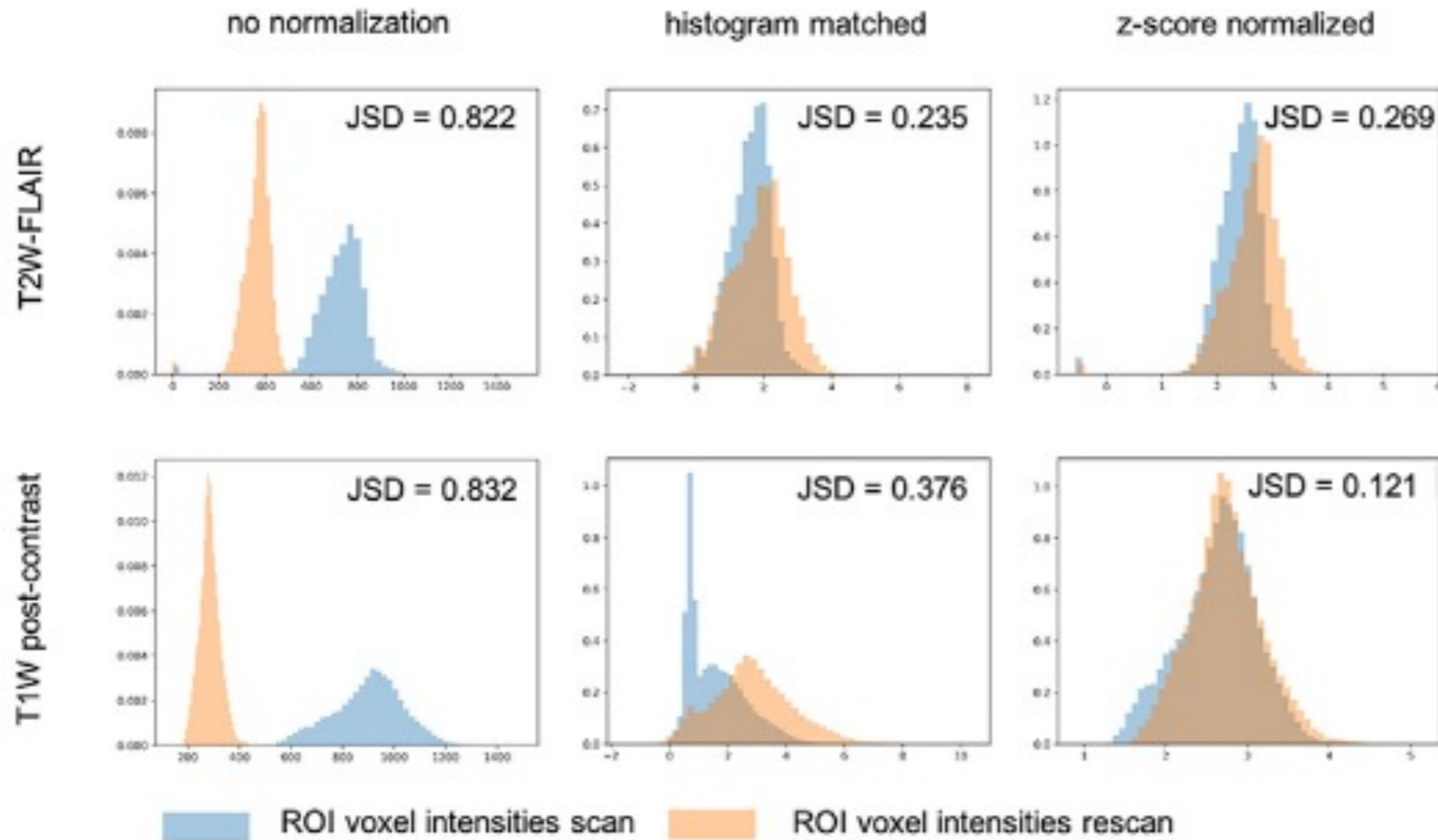
- Modify the contrast level of one scan according to another
- Piecewise linear transformation is applied such that the histogram of a source image is matched to that of a chosen reference image

Nyúl LG, Udupa JK. On standardizing the MR image intensity scale. Magn Reson Med 1999;42(6):1072–1081.

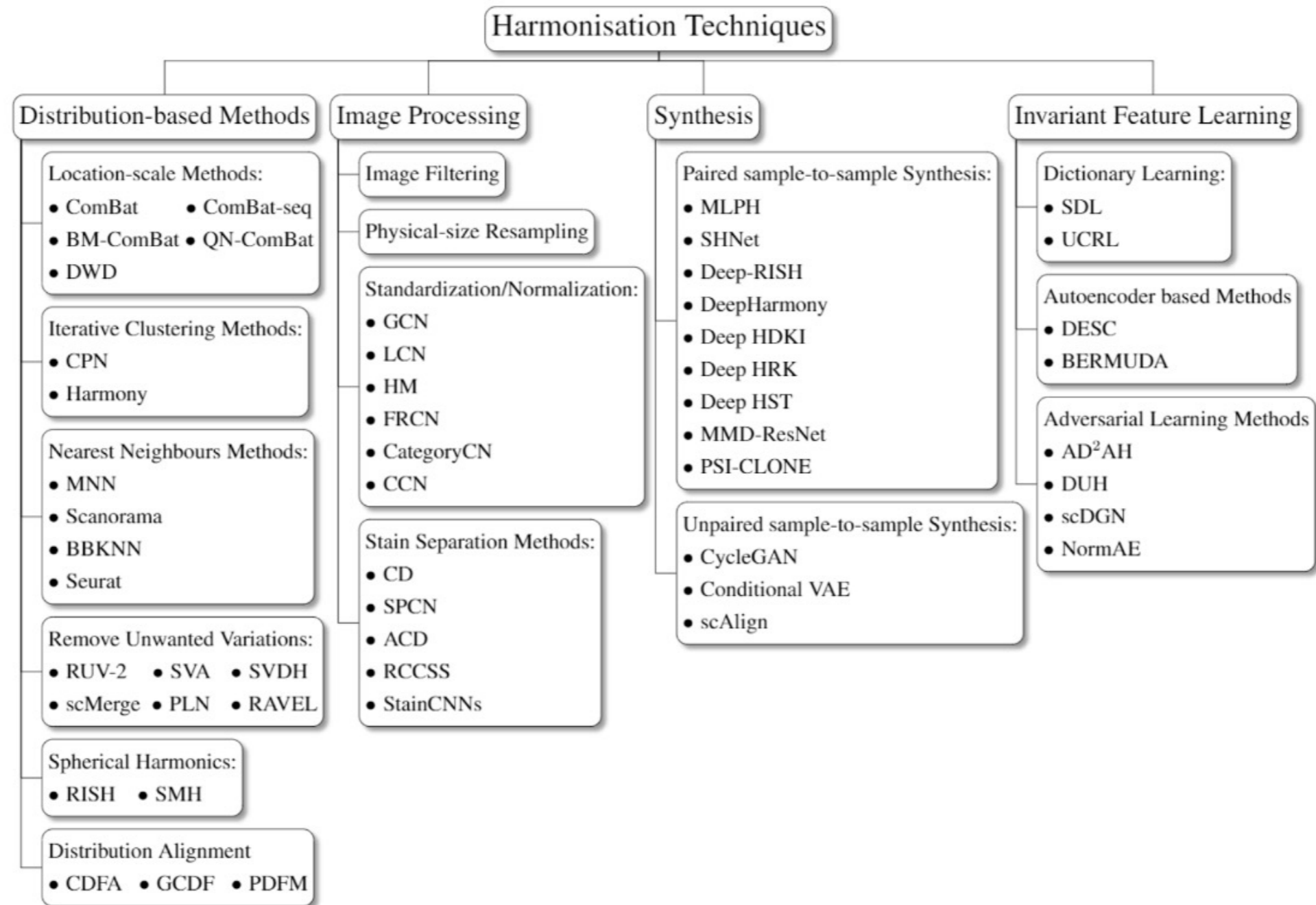
Effect of normalization



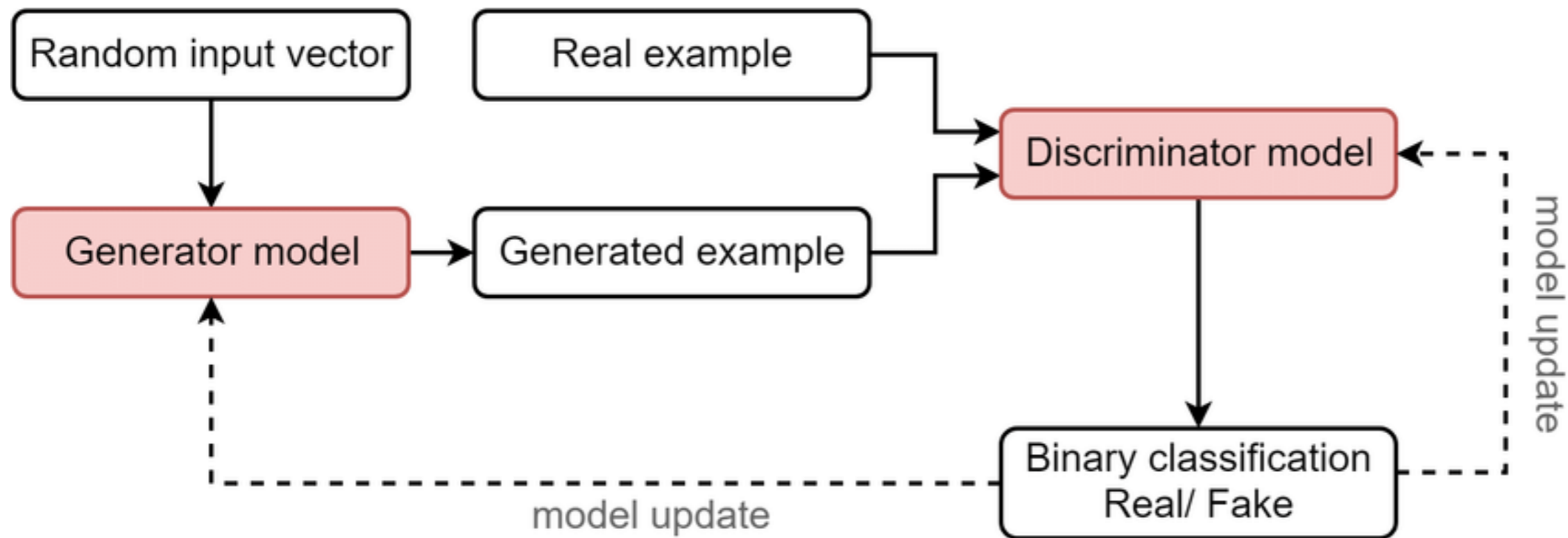
Effect of normalization



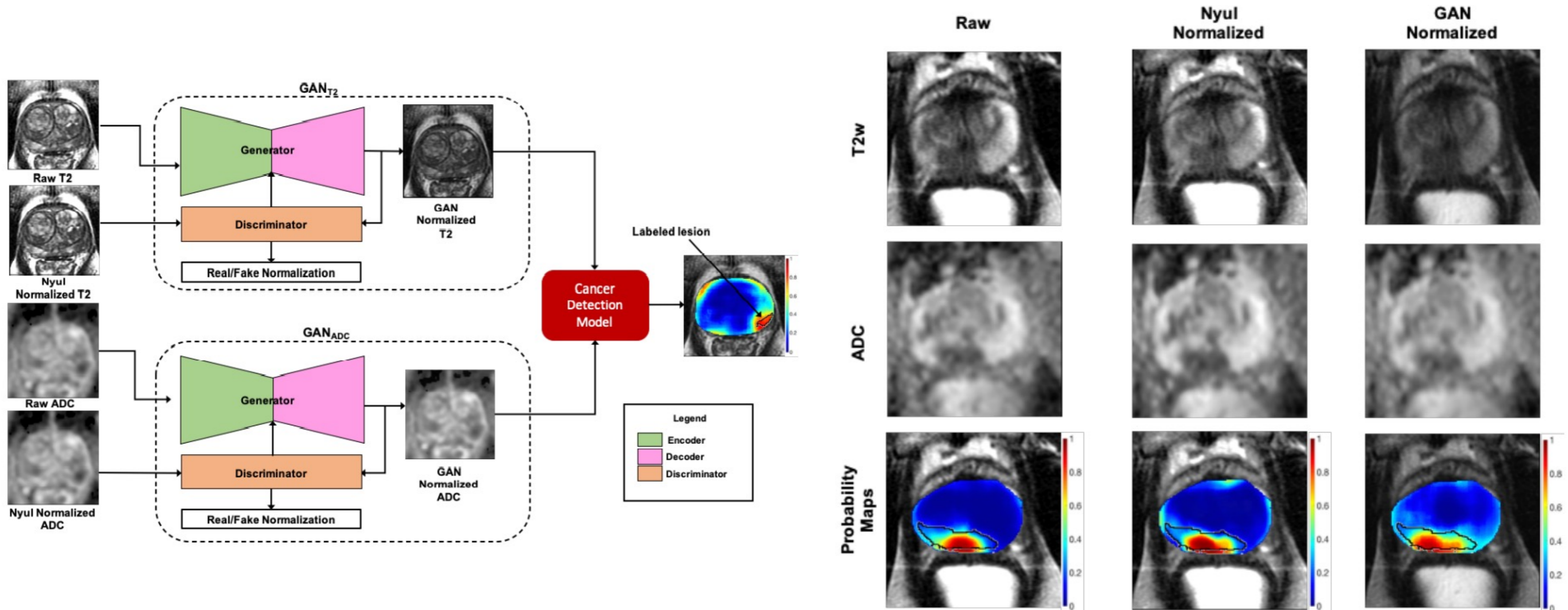
Methods for normalization



Normalization via synthesis

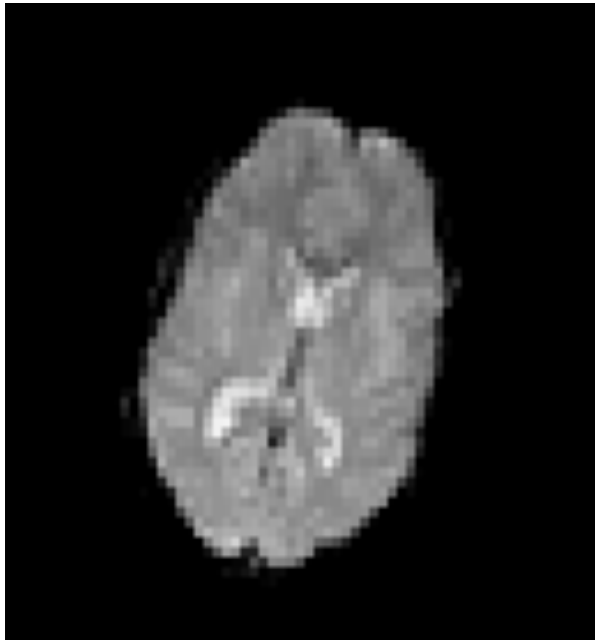


GAN-based normalization example

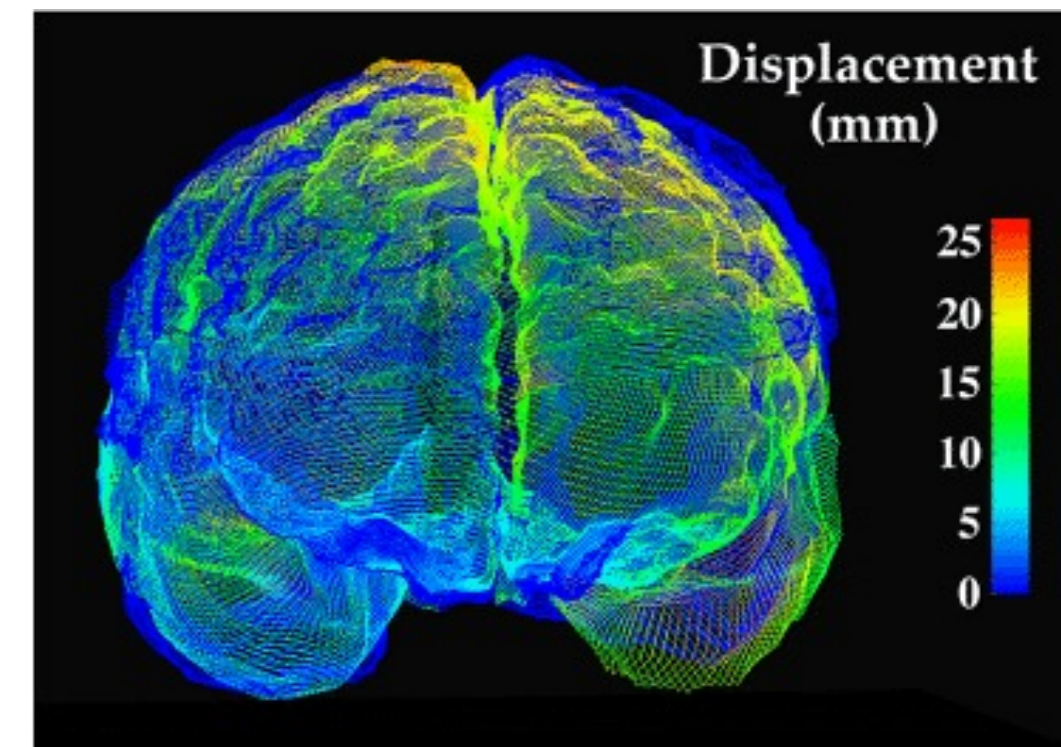


Spatially registering multimodal images

The need for spatial registration

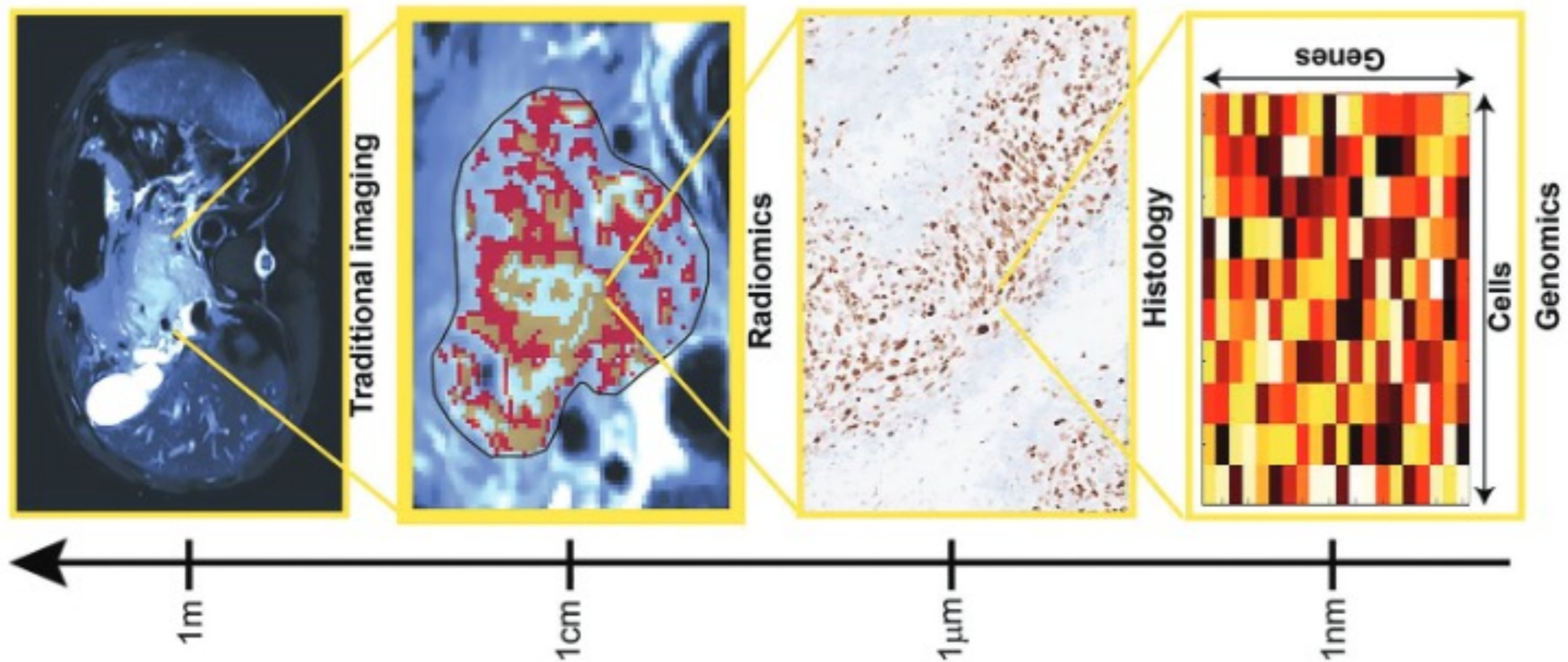


- Two or more images of the same or different patients that you wish to spatially align with each other
 - << Multiparametric images of the same patient
 - Imaging studies from a cohort of patients from which you wish to build an atlas >>

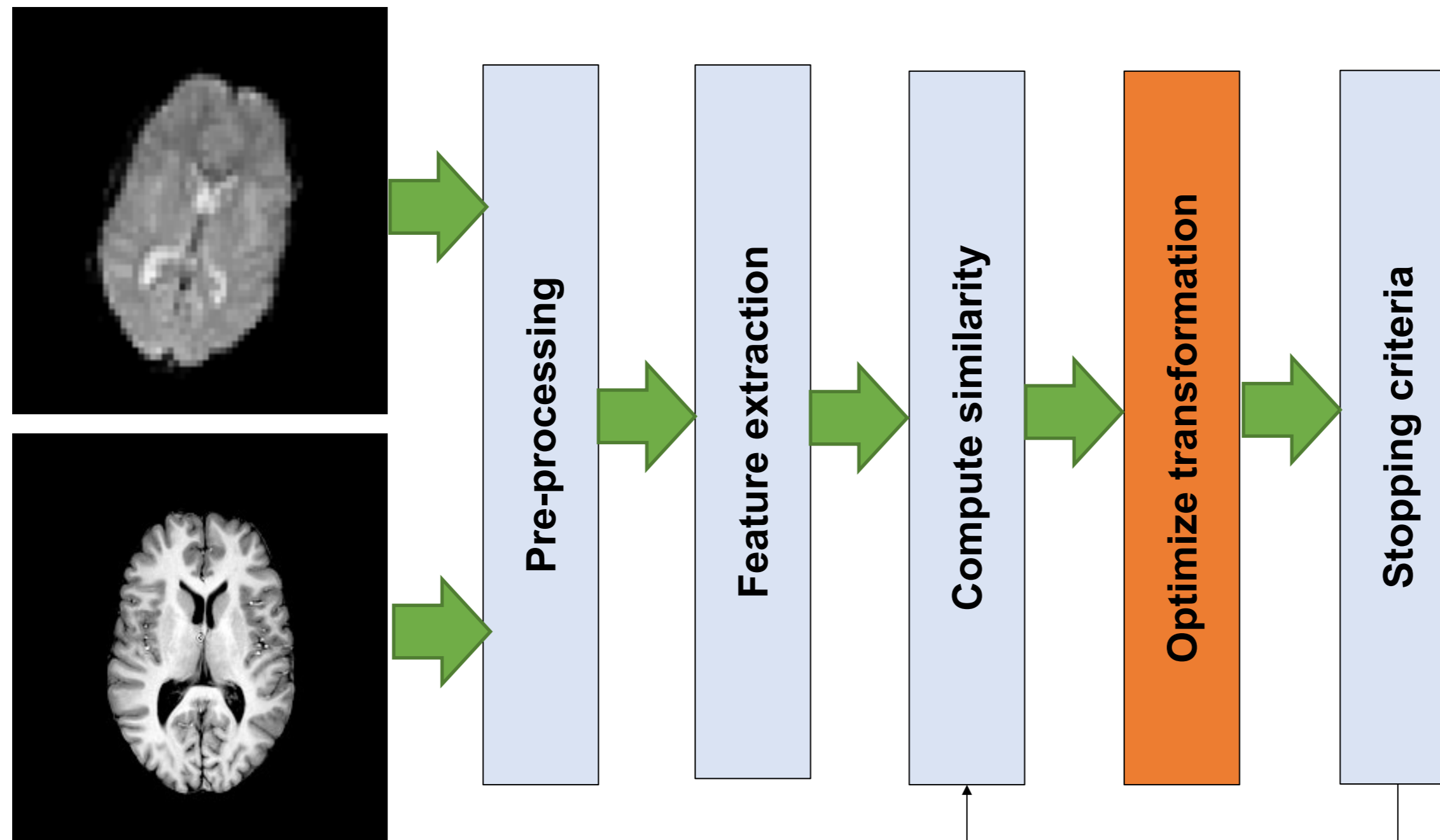


Source:
<http://users.loni.usc.edu/~thompson/hbm97abs.html>

Aligning modalities

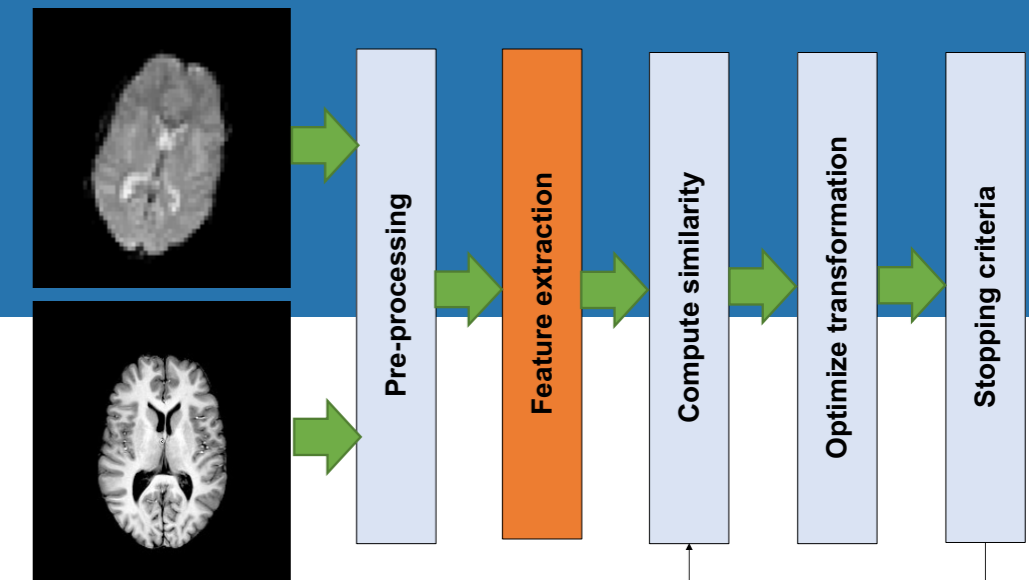


Registration framework



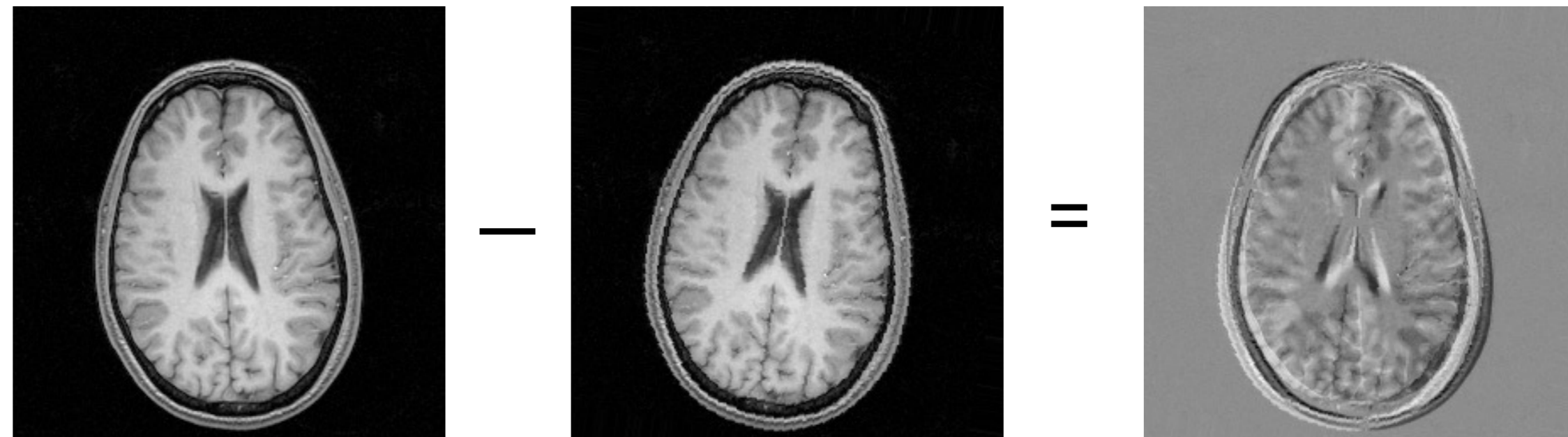
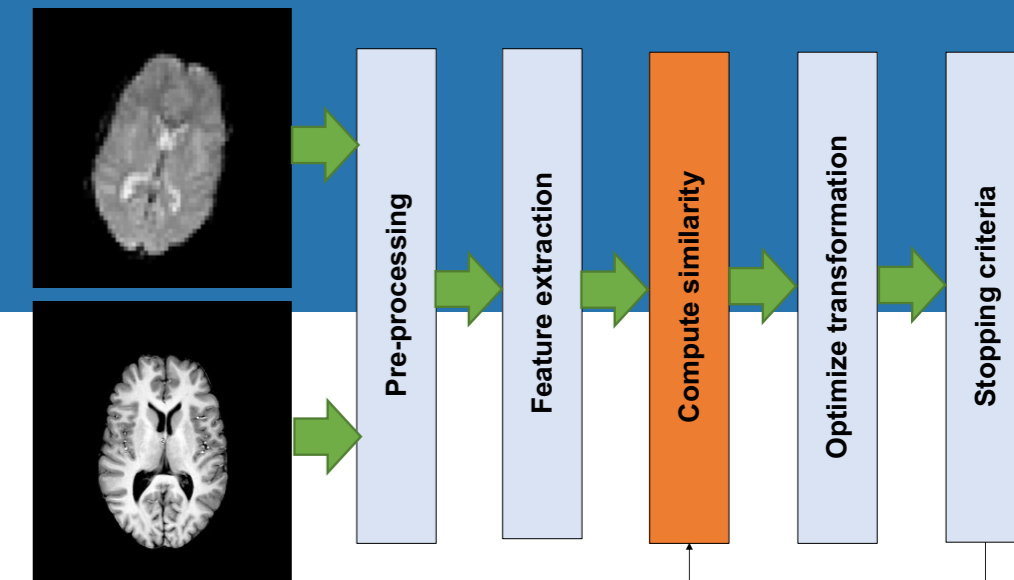
Feature extraction

- Raw intensity values
- Edges
- Salient features
 - Points of locally maximum curvature on contour line
 - Centers of windows having locally maximum variance
 - Line intersections
- Statistical features
 - Moment invariants
 - Centroid/principal axes
- Higher level features
- Matching against models
 - Anatomic atlas

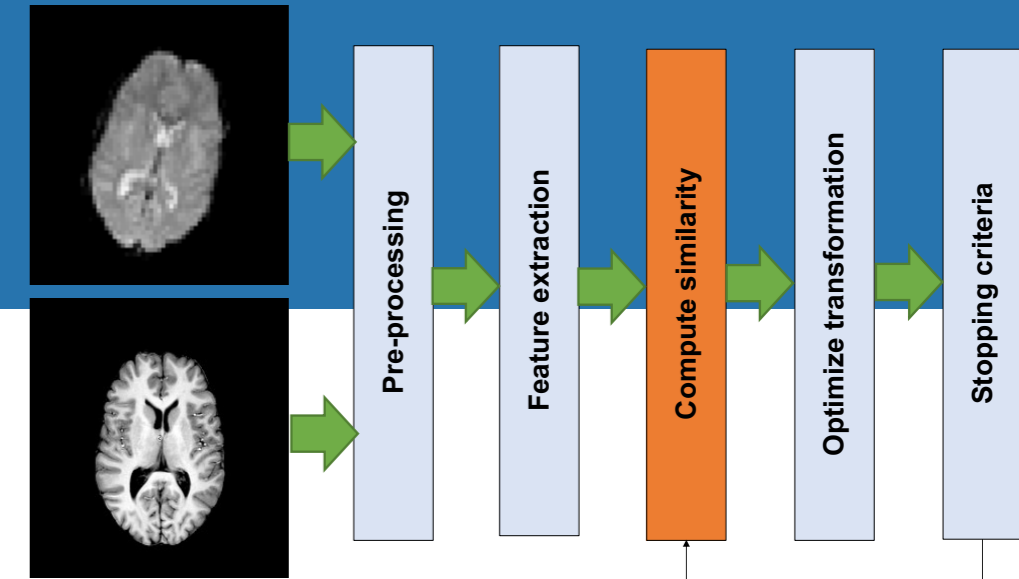


Compute similarity

- Similarity measure: maximum when images are perfectly aligned
 - Mutual information
 - Gradient correlation
 - Correlation coefficient
- Distance measure: minimum when images are perfectly aligned
 - Sum of squared differences
 - Sum of absolute differences



Compute similarity



- Feature Similarity

- Point to point distances

$$D = \sum_i \sum_j \|x_i - y_j\|^2$$

- Image Similarity

- Cross Correlation (Matched Filter, Template Matching)
- Sum of squared differences
- Ratio image uniformity
- Mutual Information

$$CC = \sum_i \sum_j I_1(i, j) I_2(i - u, j - v)$$

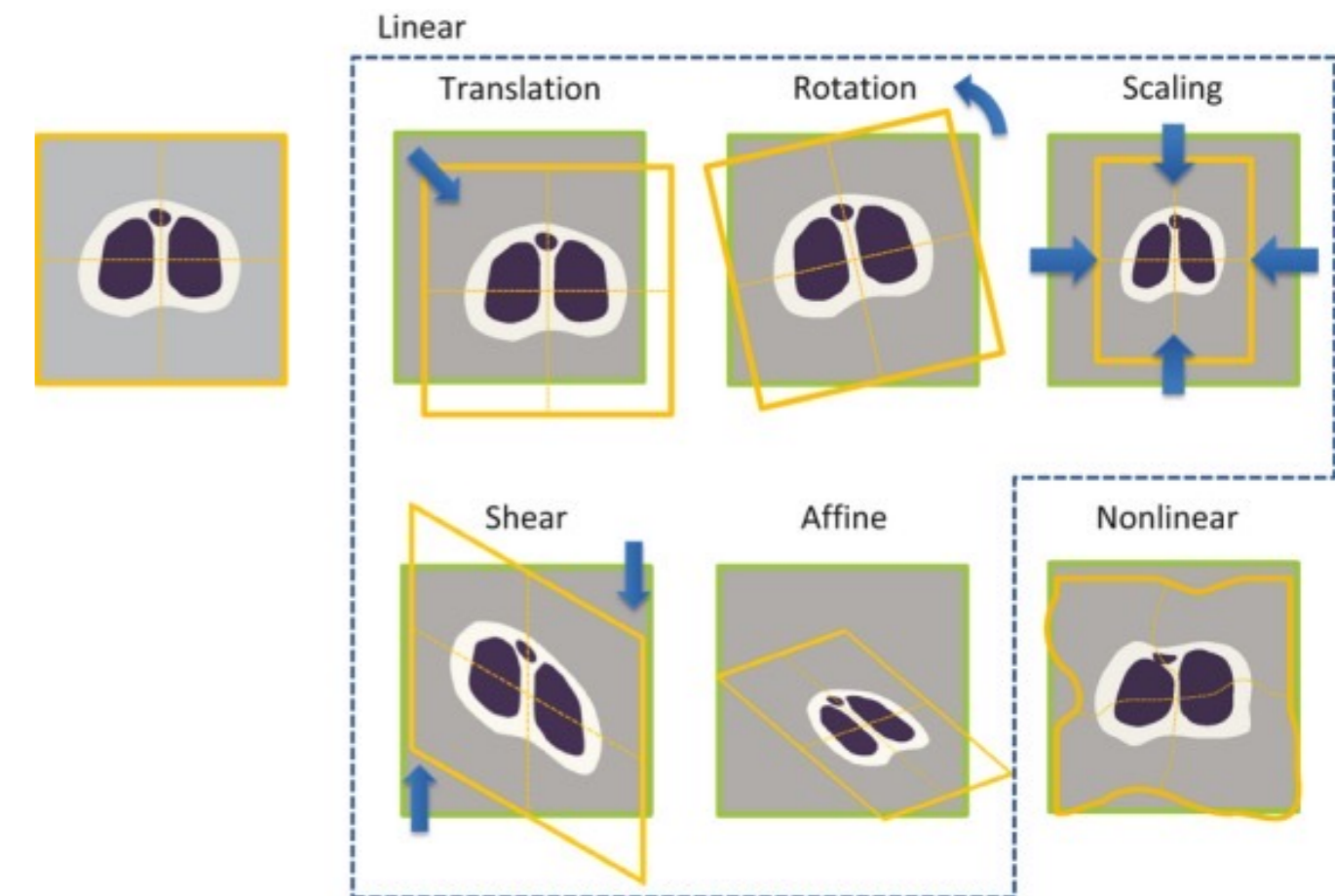
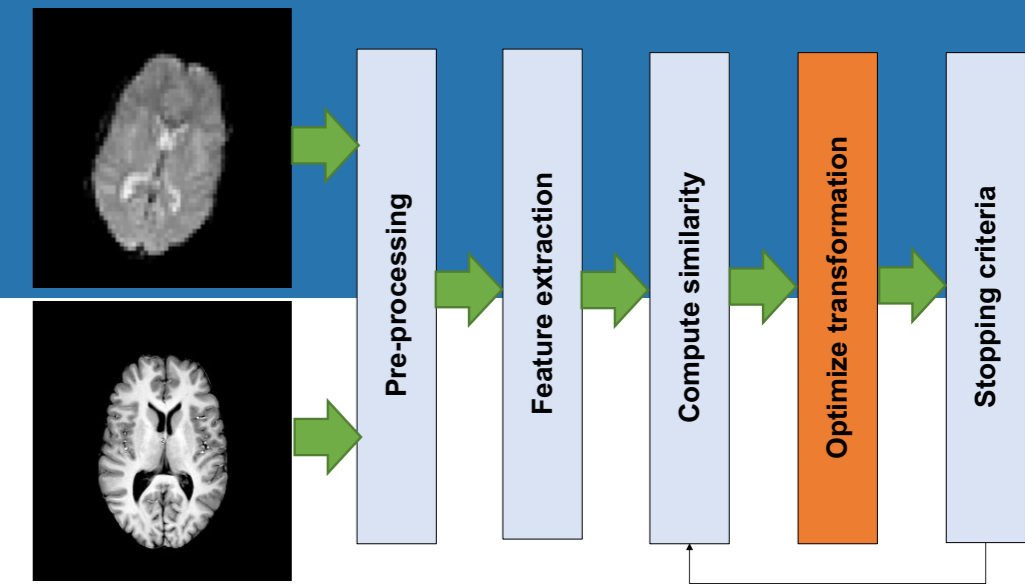
$$SSD = \sum_i \sum_j (I_1(i, j) - I_2(i - u, j - v))^2$$

$$RIU = \frac{\sigma_R}{\mu_R} \quad \text{where } R(i, j) = \frac{I_1(i, j)}{I_2(i, j)}$$

$$MI = - \sum_{g_1} \sum_{g_2} p(g_1, g_2) \log \left\{ \frac{p(g_1, g_2)}{p(g_1) p(g_2)} \right\}$$

Transformations

- For images to become aligned, they must be **transformed**
- Maps points in the “moving” image to new locations on the “transformed” image
- **Degrees of freedom (DOF)**
 - Rigid body (6 DOF)
 - Affine (12 DOF)
 - Non-linear/deformable (>12 DOF)

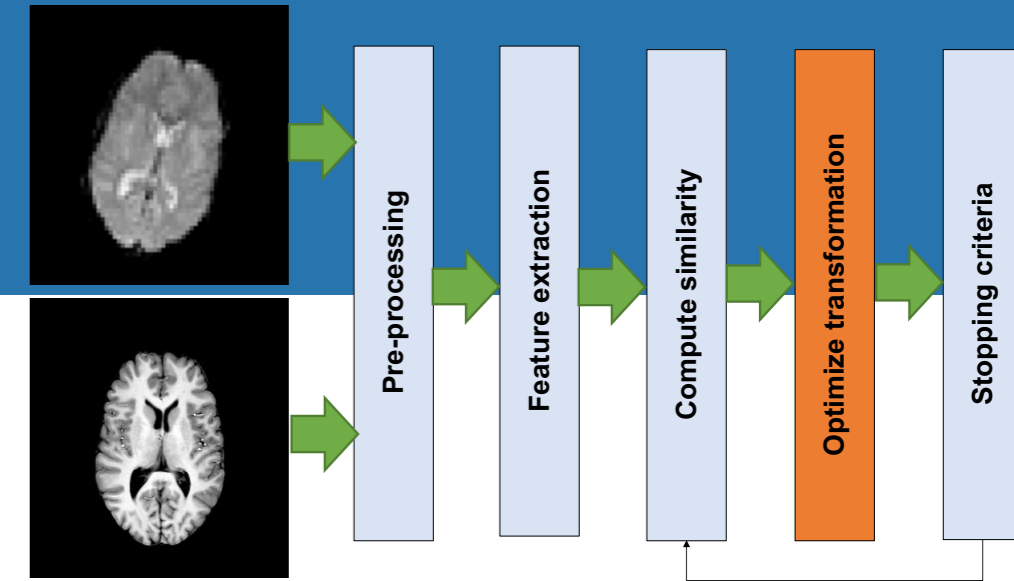


Optimize transformation

- Iterative Closest Point (ICP) Algorithm

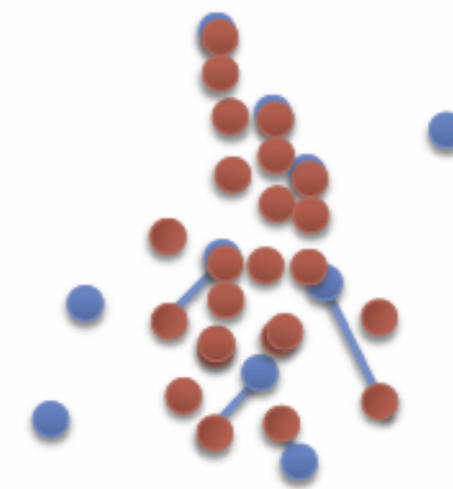
- Initial transformation is identity matrix
- Repeat
 - For each point in A, find closest point in B
 - Estimate the combination of rotation and translation that will best align each source point to its match
 - Compute mean squared error

$$MSE = \frac{1}{N} \sum_{i=1}^N \|p_{A,i} - R(p_{B,i}) - T\|^2$$



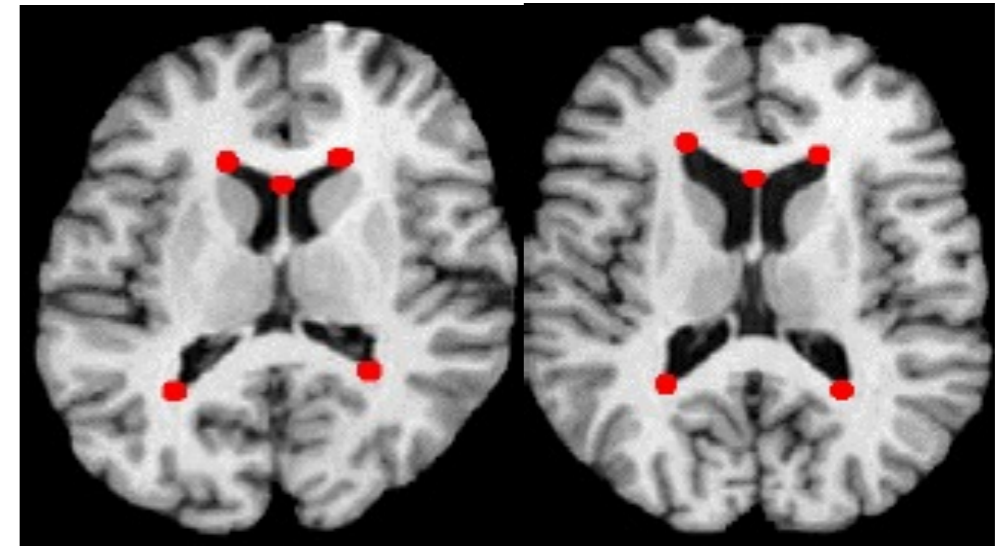
A and *B* are unstructured point clouds with unknown correspondence of points

A is the smaller set



Landmark based

- Identifying corresponding points in the images and inferring the image transformation
- Types of landmarks (fiducial marker)
 - Extrinsic
 - artificial objects attached to the patient
 - Intrinsic
 - internal anatomical structures
- Compute the average or “centroid” of each set of points → translation
- Rotate this point set about the new centroid difference between images is minimized



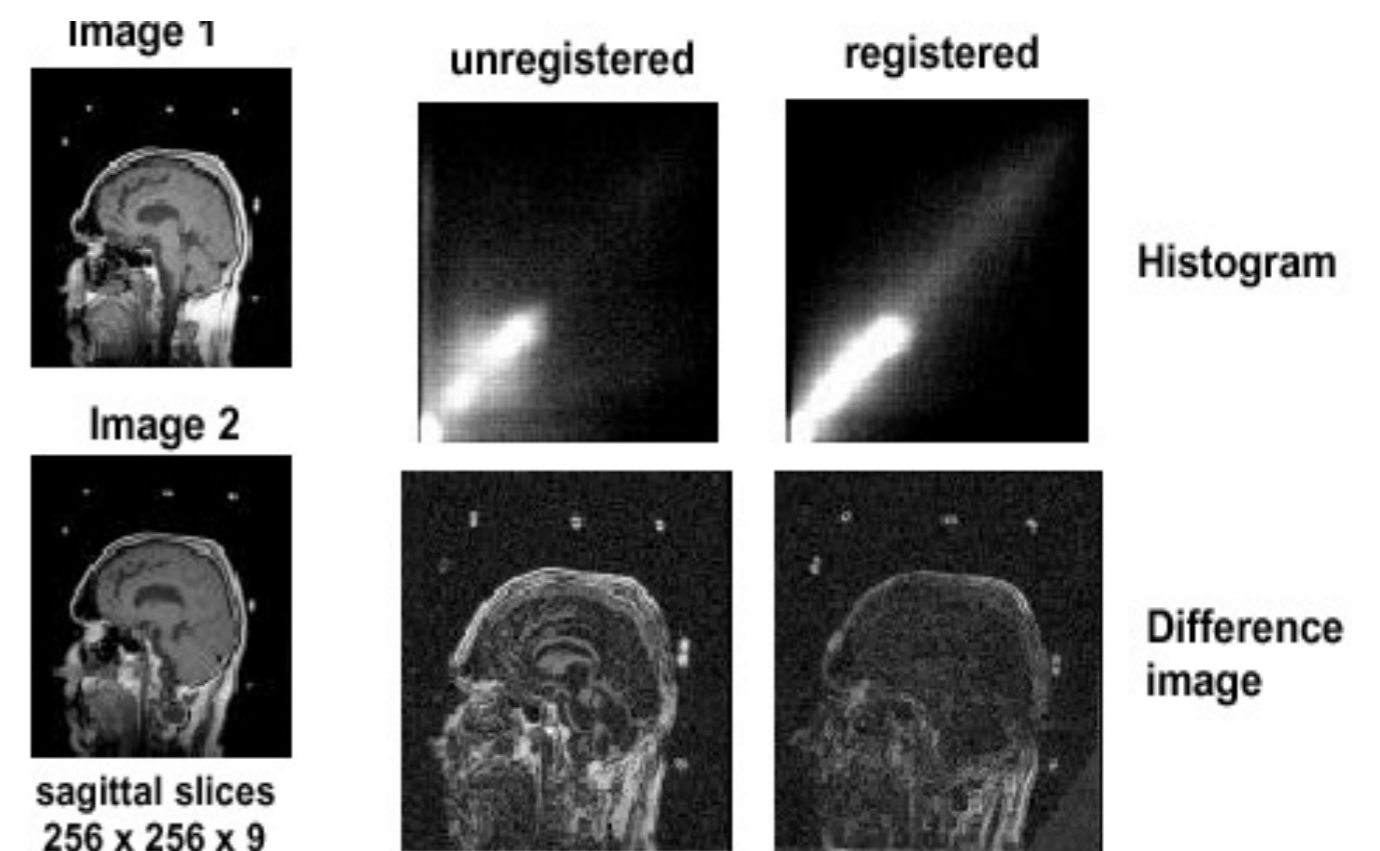
Voxel intensity based

- Method

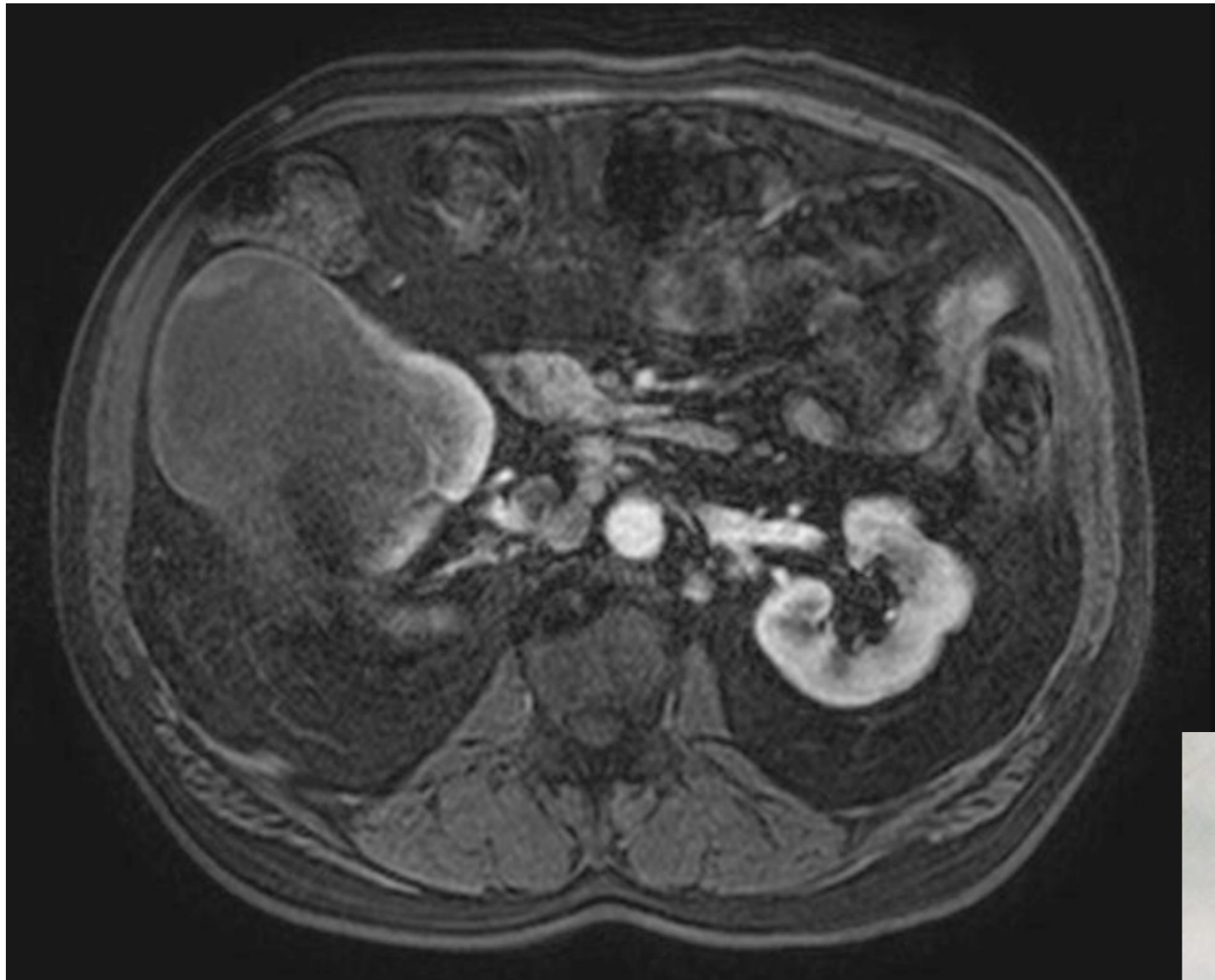
- Calculate the registration transformation by optimizing some measure derived from the voxel values in the image

- Algorithms used

- Registration by minimizing intensity difference
- Correlation techniques
- Ratio image uniformity
- Partitioned Intensity Uniformity

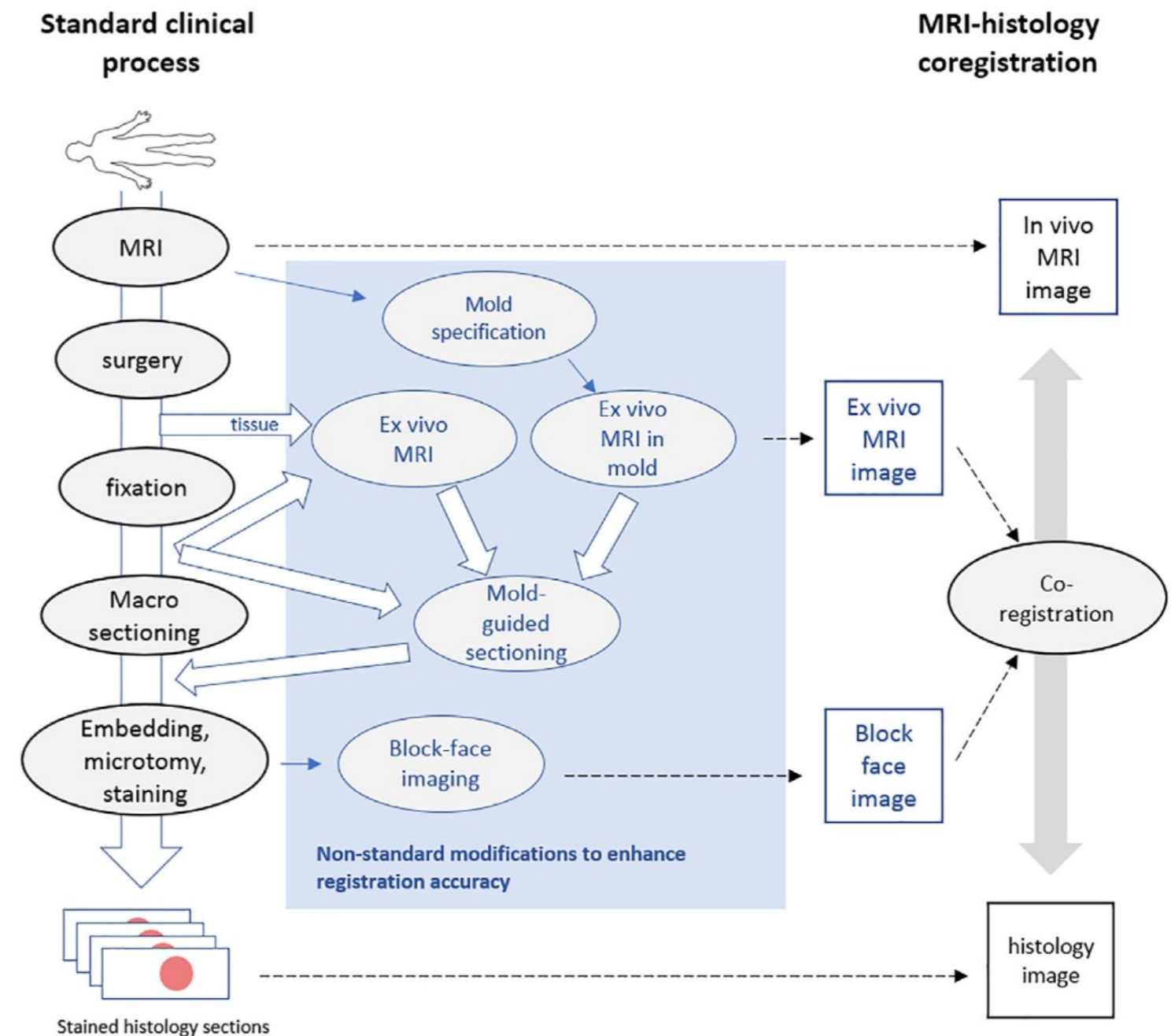


Radiology to pathology matching

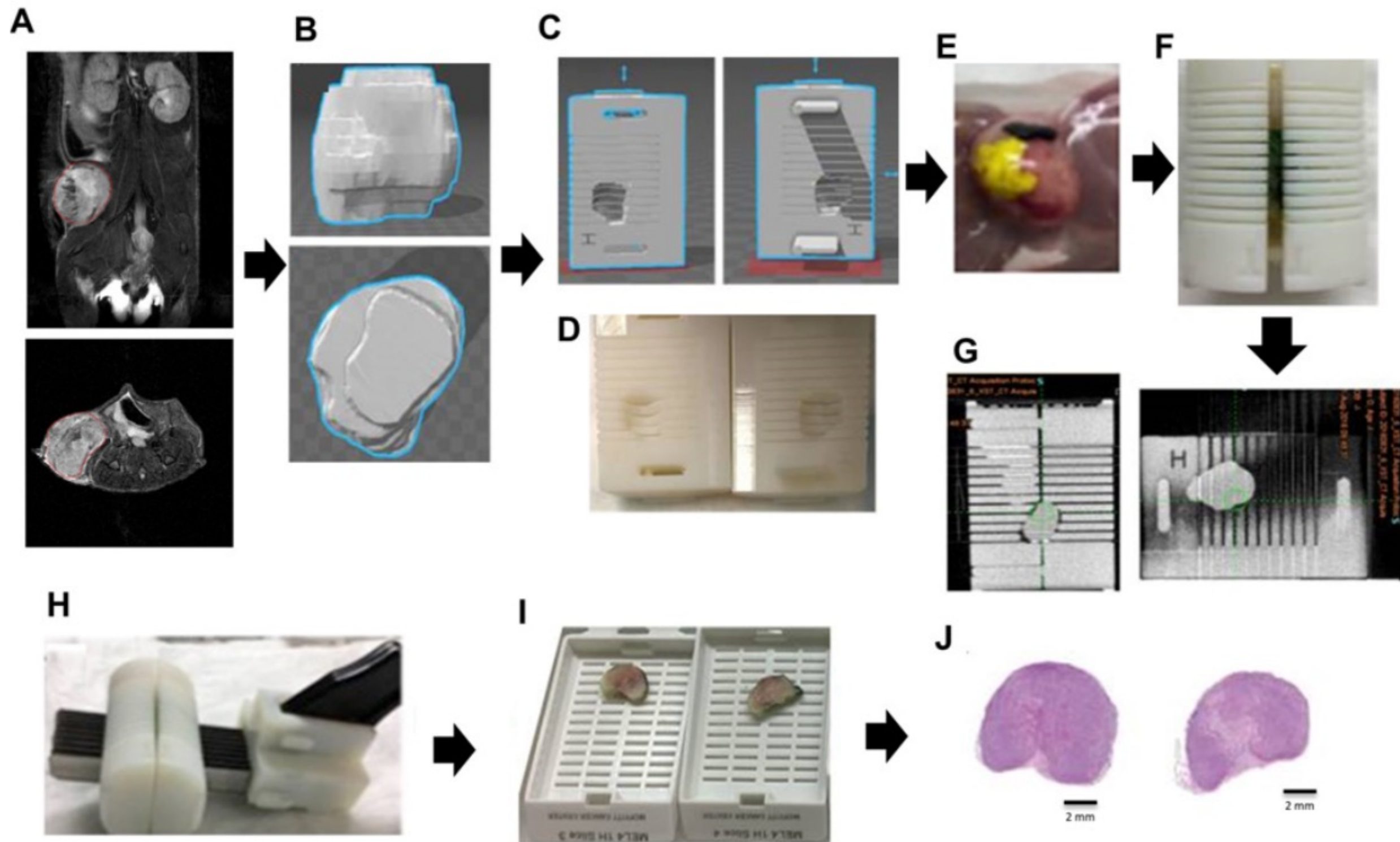


Matching MRI to pathology: Challenges

- Deformation of resected tissue
- Devascularization
- Difficulty orientating amorphous specimens
- Tissue shrinkage
- Thin-sectioning compression,
- Misalignment of macroscopic tissue sections
- Subdivision of macro tissue sections
- Slice thickness mismatch between sections prepared for light microscopy

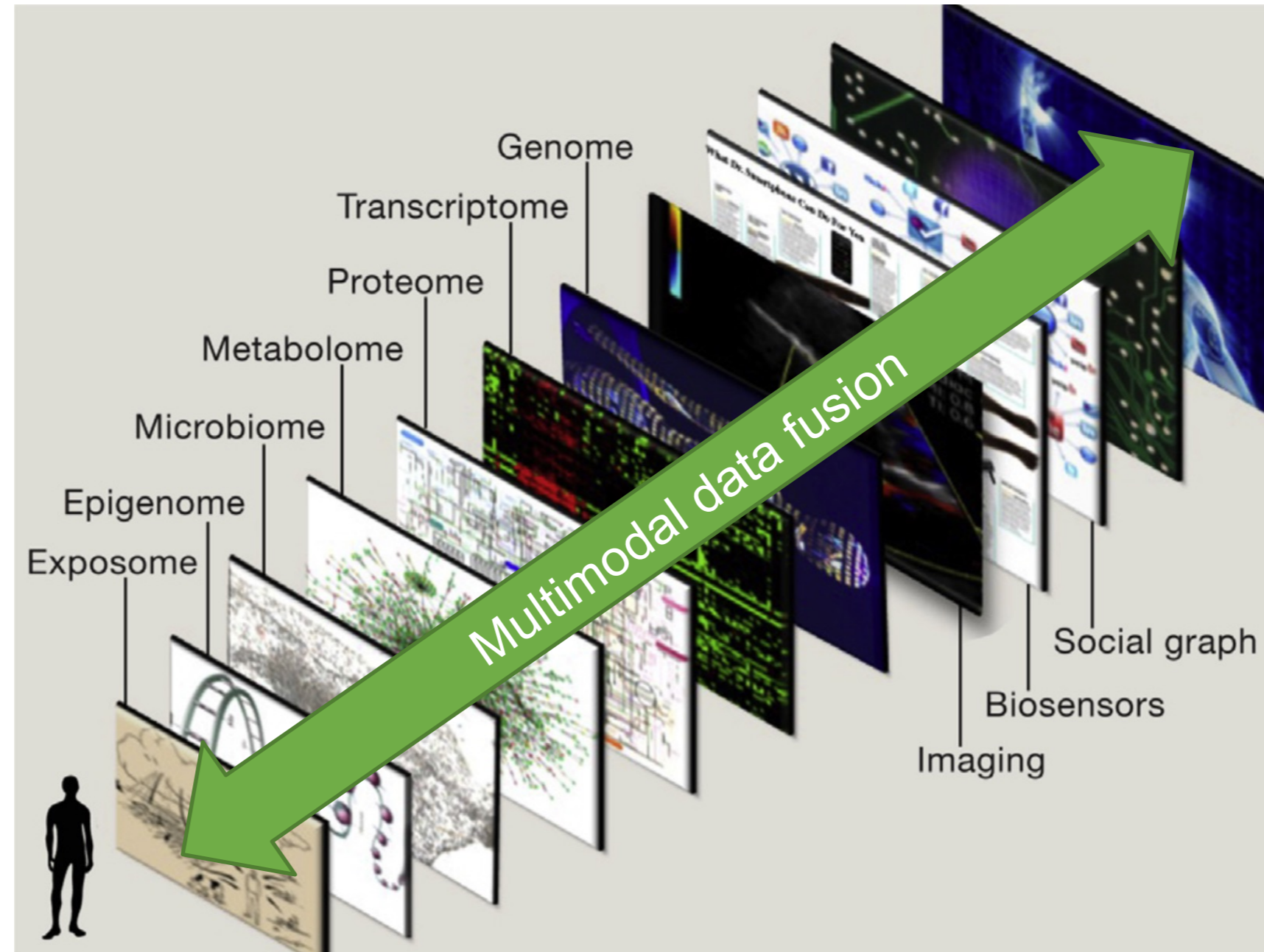


Registering in vivo and histopathology images



Multimodal data fusion

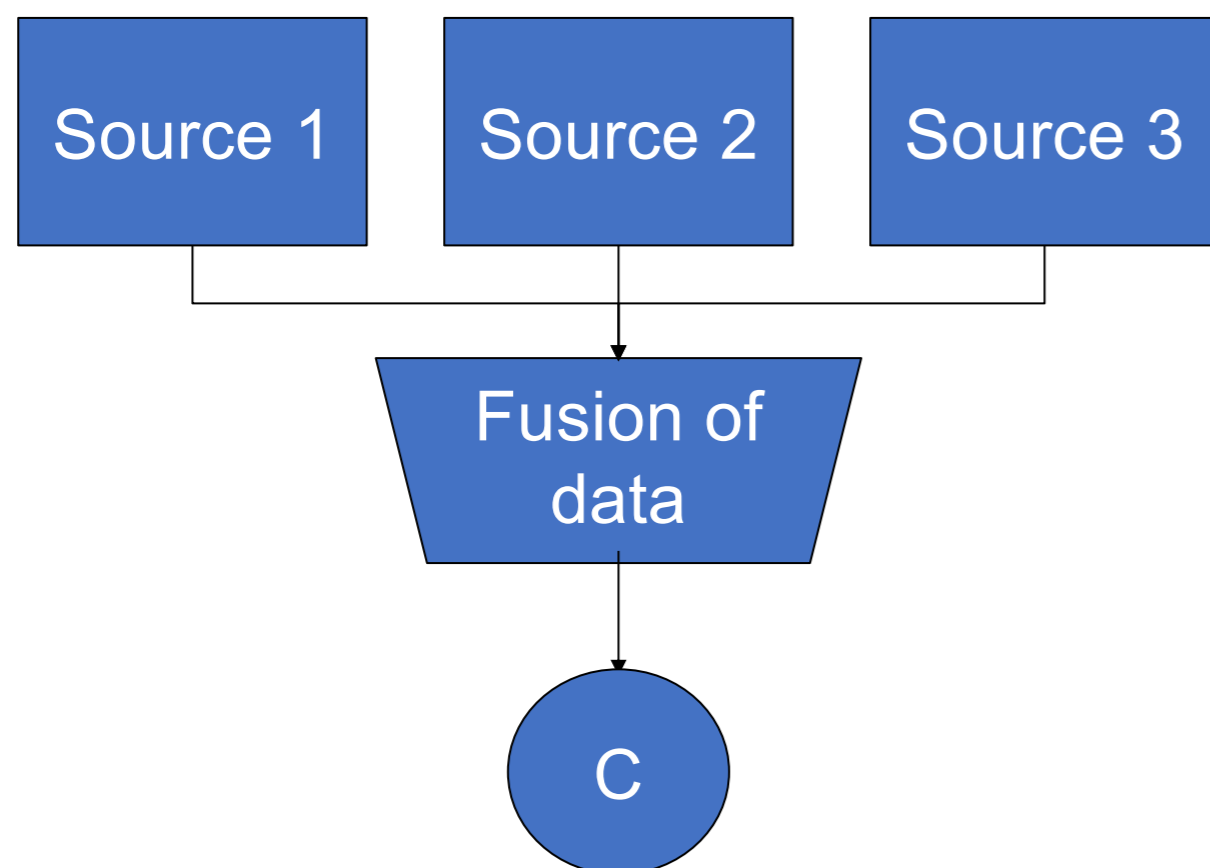
Motivation



Basic types of multimodal fusion

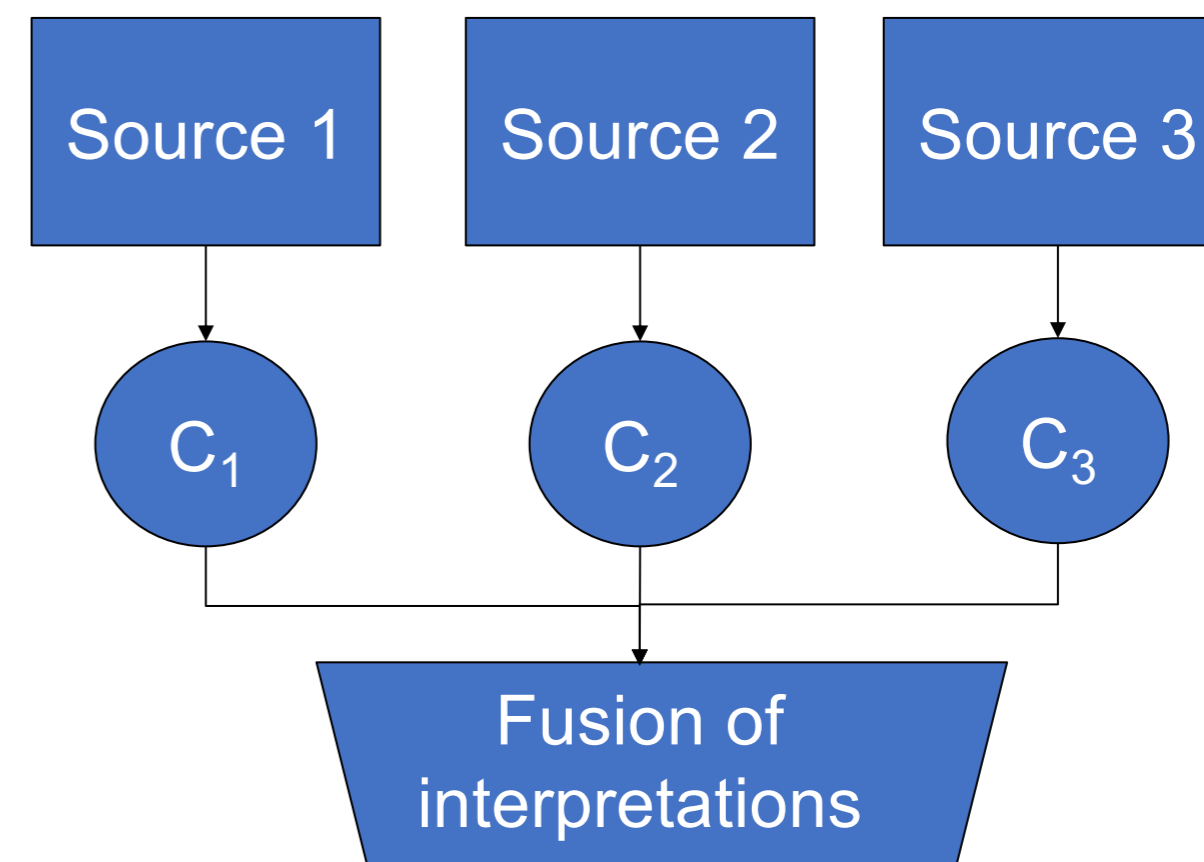
Combination of data (CoD):

Combine features across sources to generate a single feature vector for classification

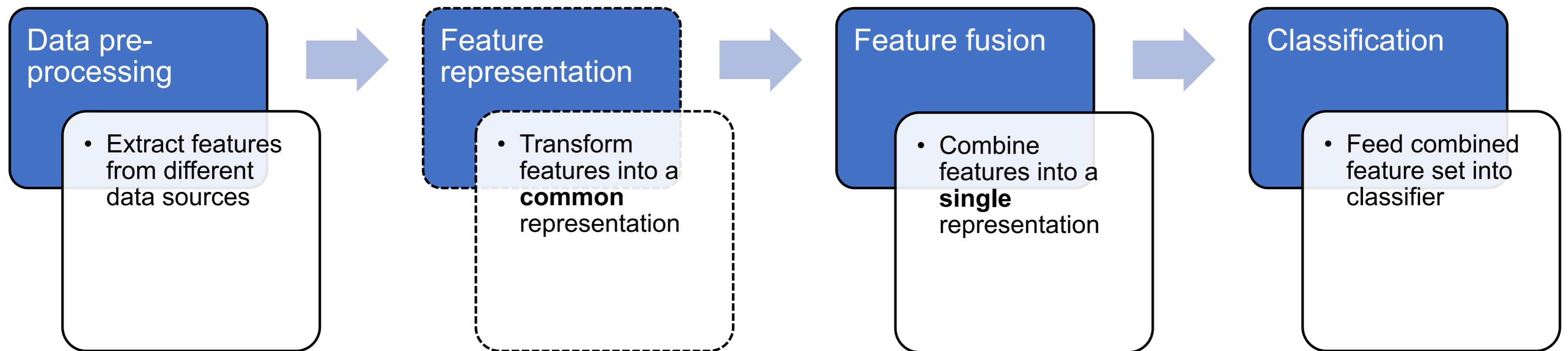


Combination of interpretations (CoI):

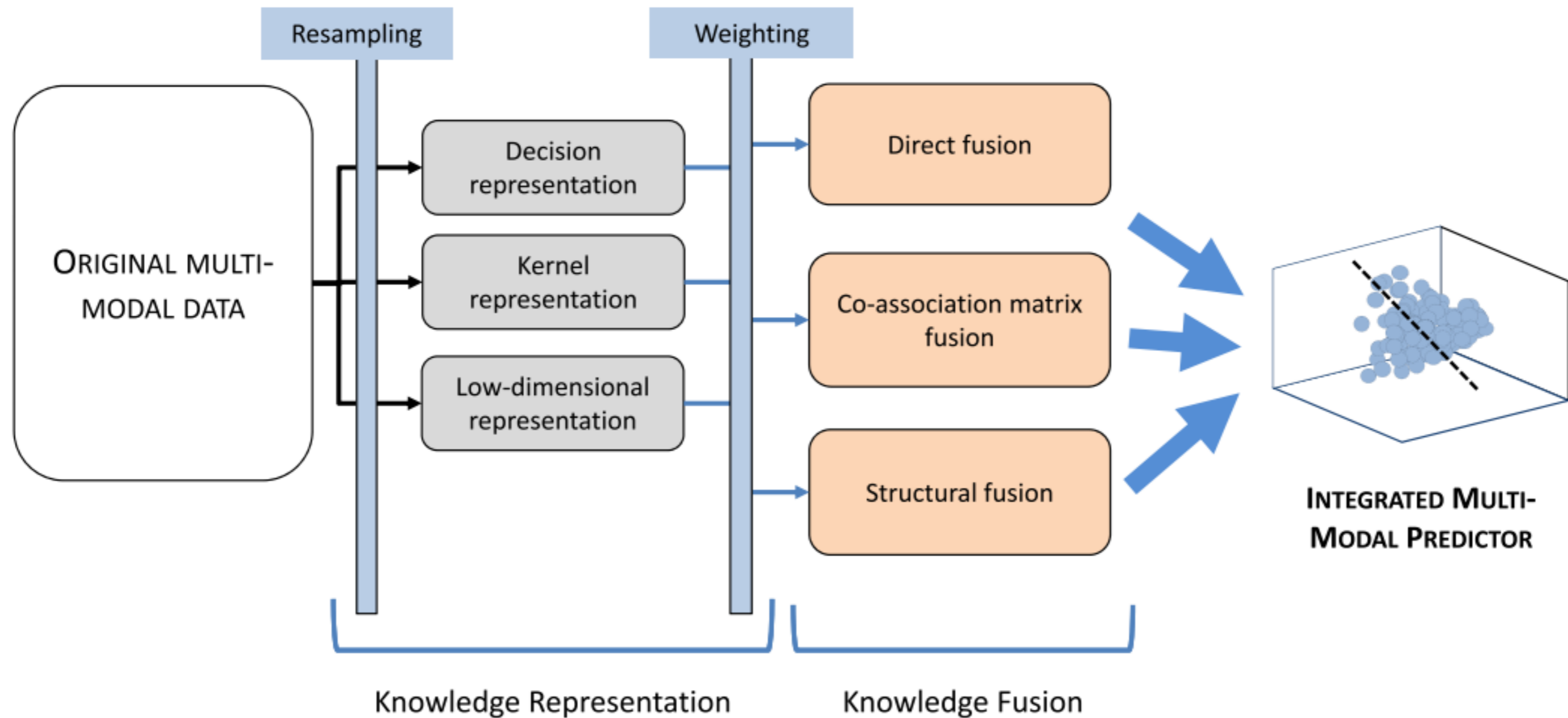
Classify data from each source independently then aggregate the results



General approach

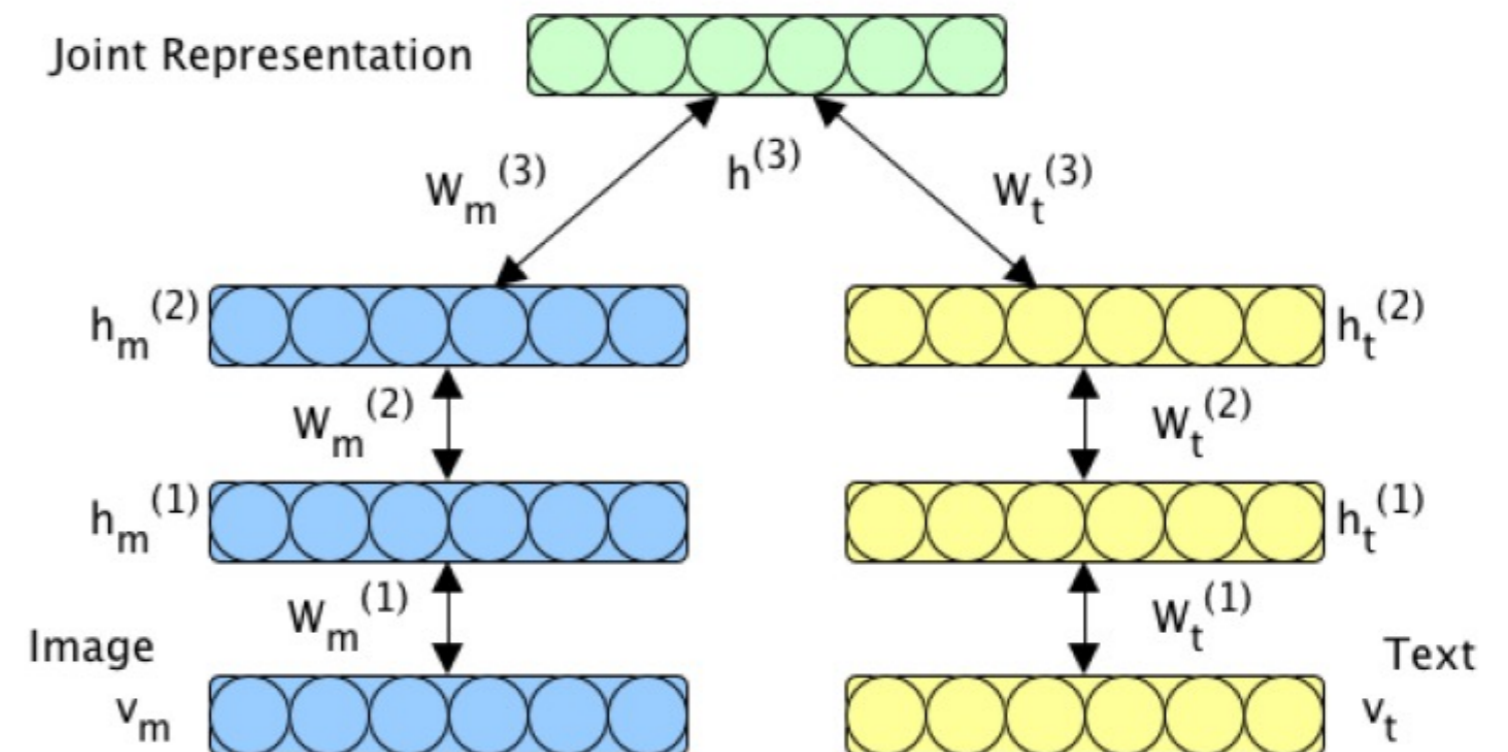
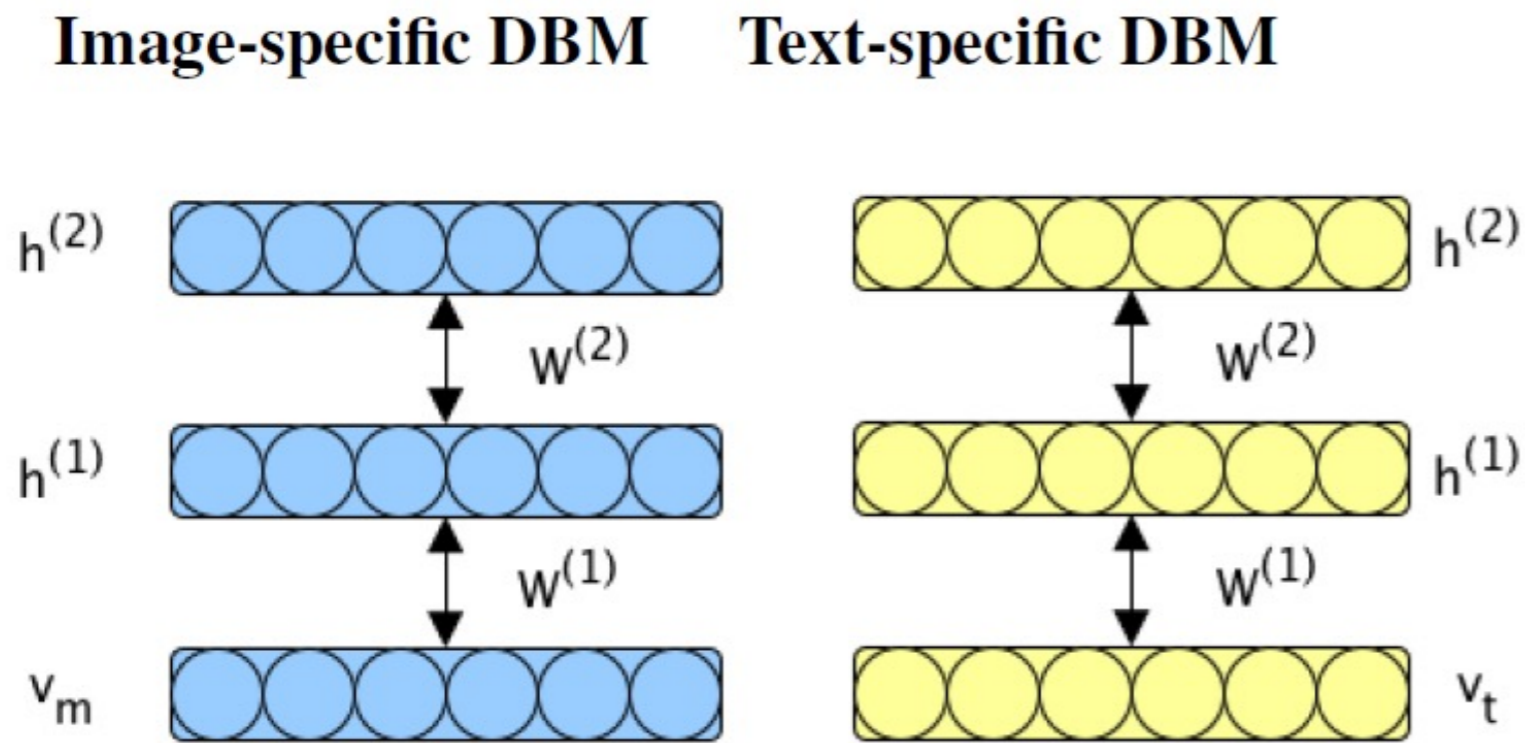


Examples of approaches

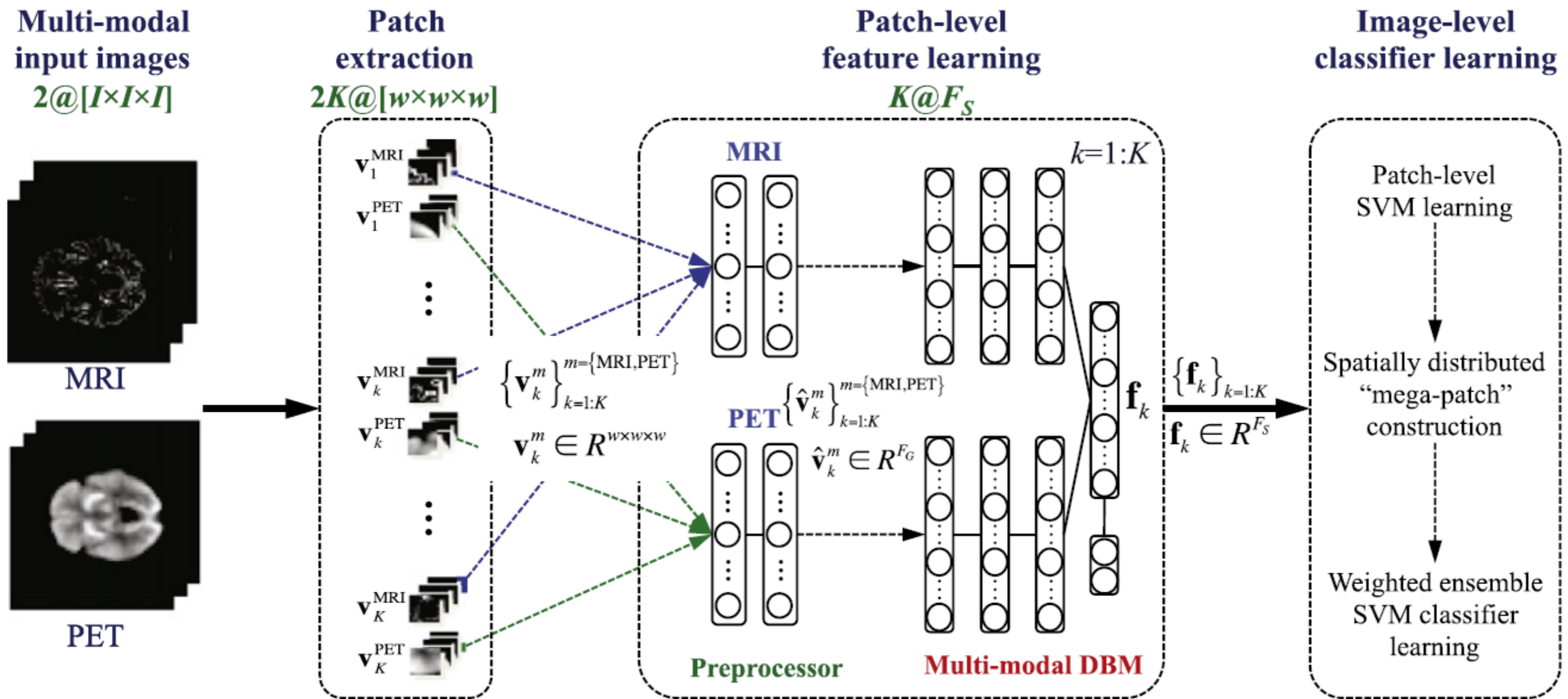


Examples of approaches

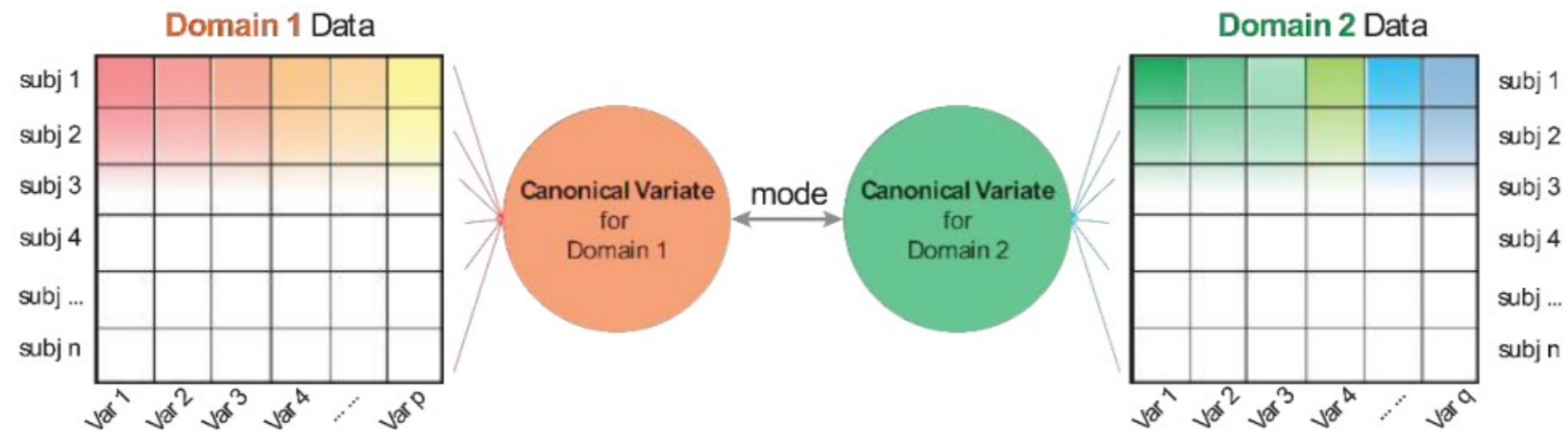
Multimodal DBM



Examples of approaches



Examples of approaches



C

Original Variables Canonical Vector

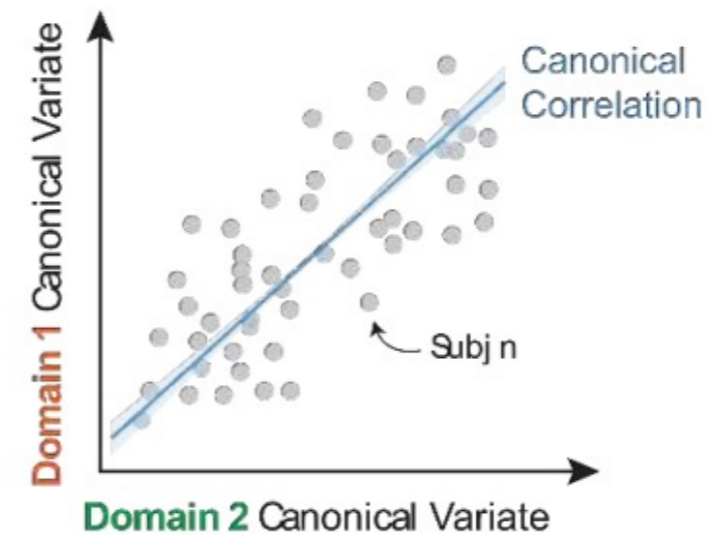
Var 1	x	0.4
Var 2	x	0.2
Var 3	x	0
Var 4	x	-0.1
⋮		
Var p	x	0.3

Canonical Variate

Var 1
+
Var 2
+
Var 4
+
Var p

=

Mode 1



Ongoing efforts & concluding thoughts

Integrated Diagnostics Shared Resource

Mission: Catalyze innovative research and tool development through data integration and curation to improve early detection, diagnosis and treatment of cancer

By systematically collecting



Clinical and Outcomes Data



Imaging Data



Pathology Data



Prospective biospecimens

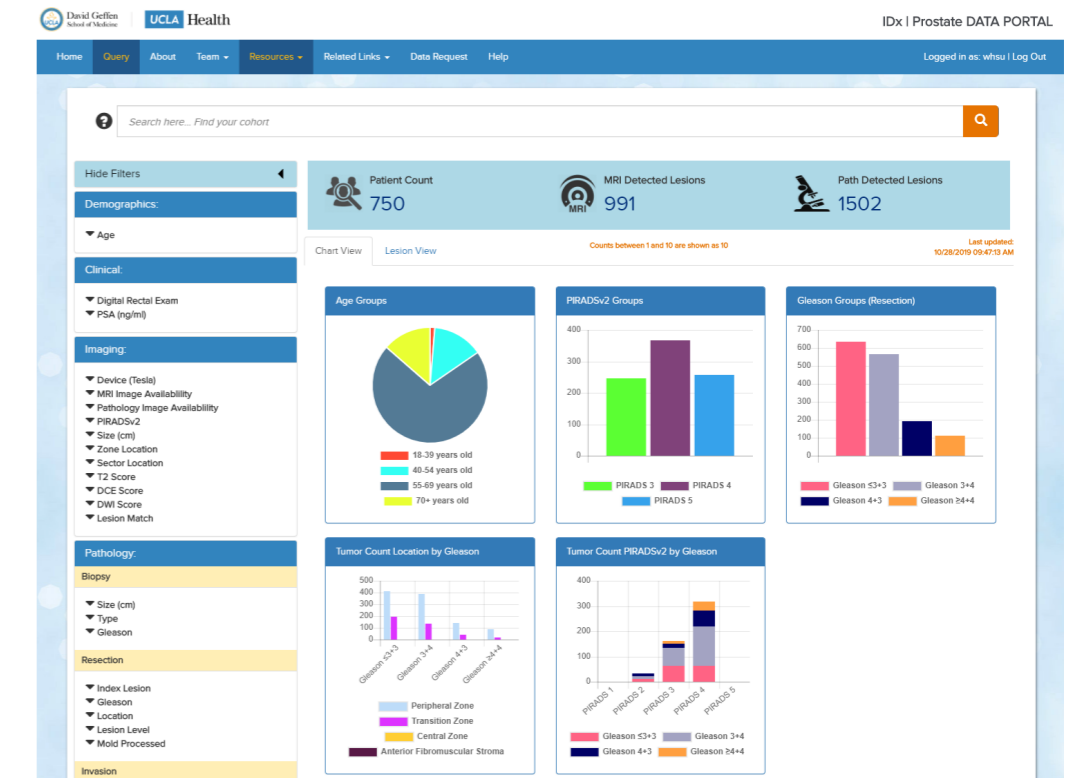
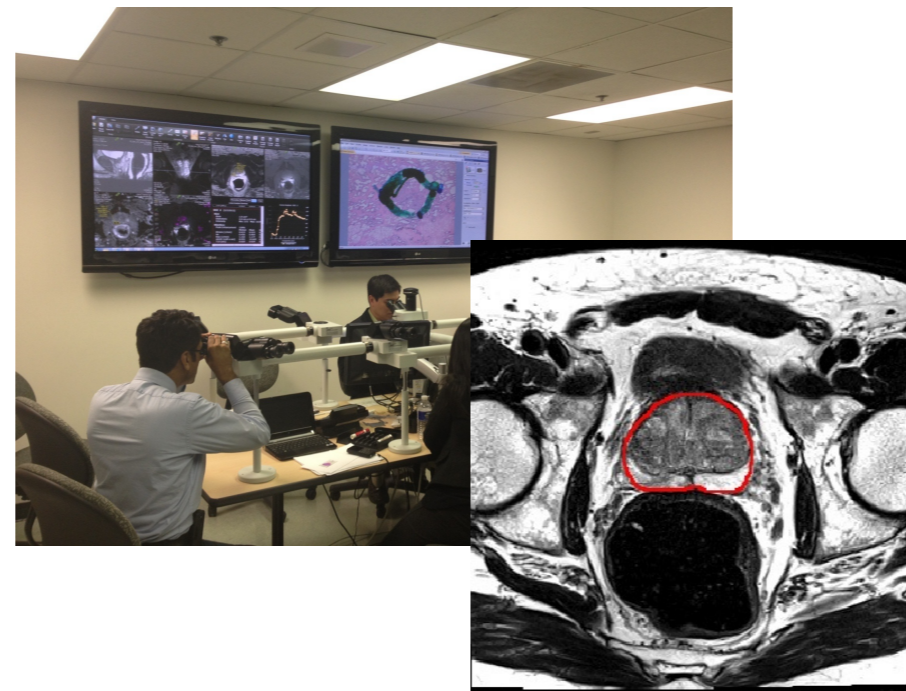


Multi-omics Data

With the goal of

1. Developing and validating of novel AI/ML algorithms and imaging biomarkers to assist clinicians with cancer diagnosis and treatment
2. Generating new biological knowledge through the lens of imaging
3. Discovering actionable information that can inform clinical management of patients

Functions of the shared resource

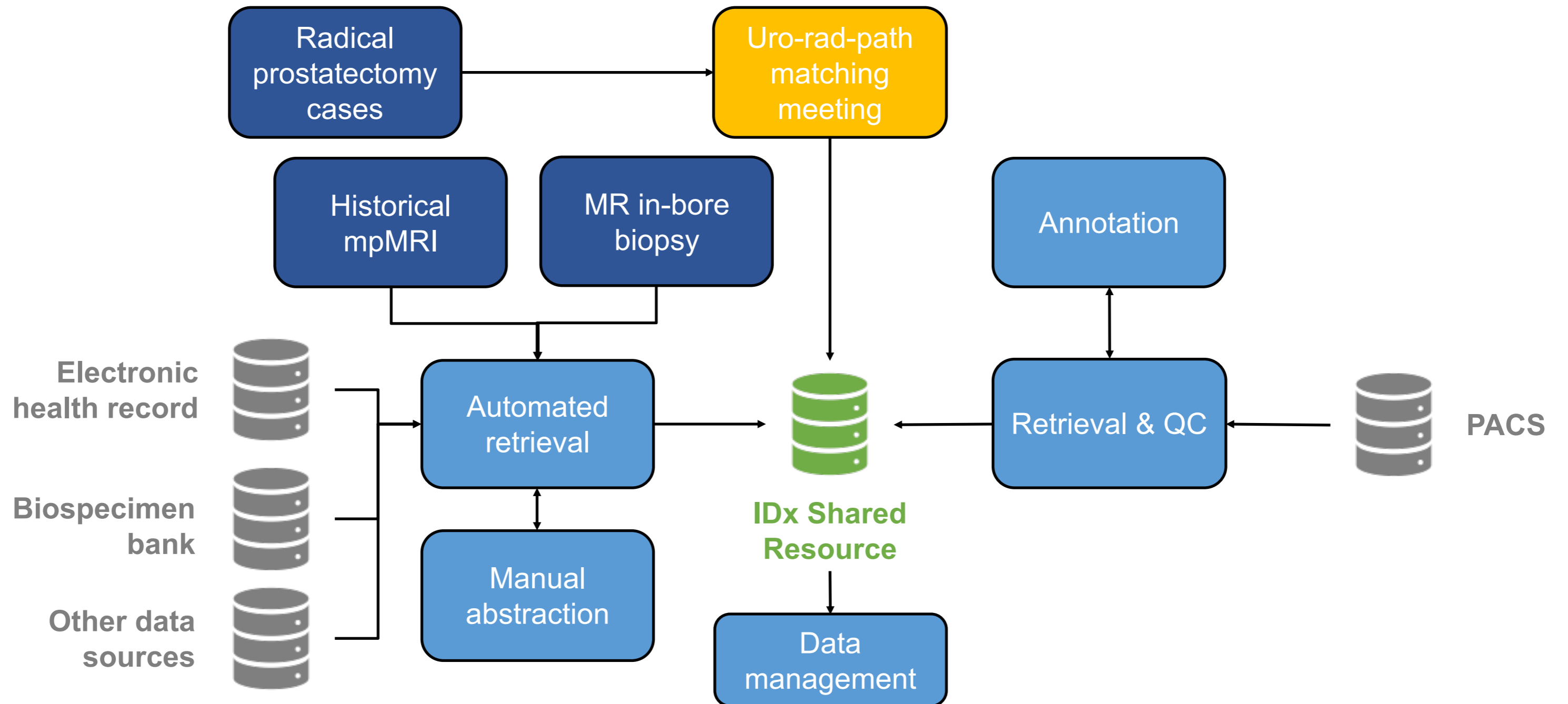


Data and specimen collection

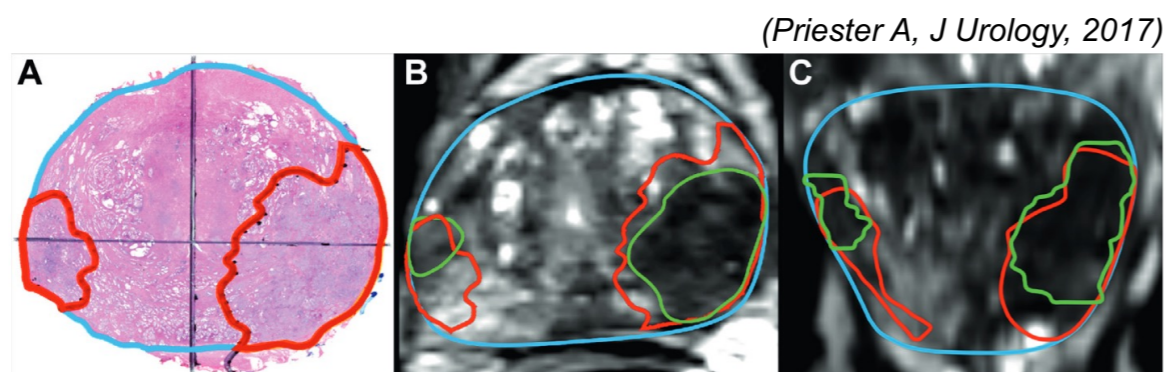
Annotation and data curation

Data delivery and knowledge discovery

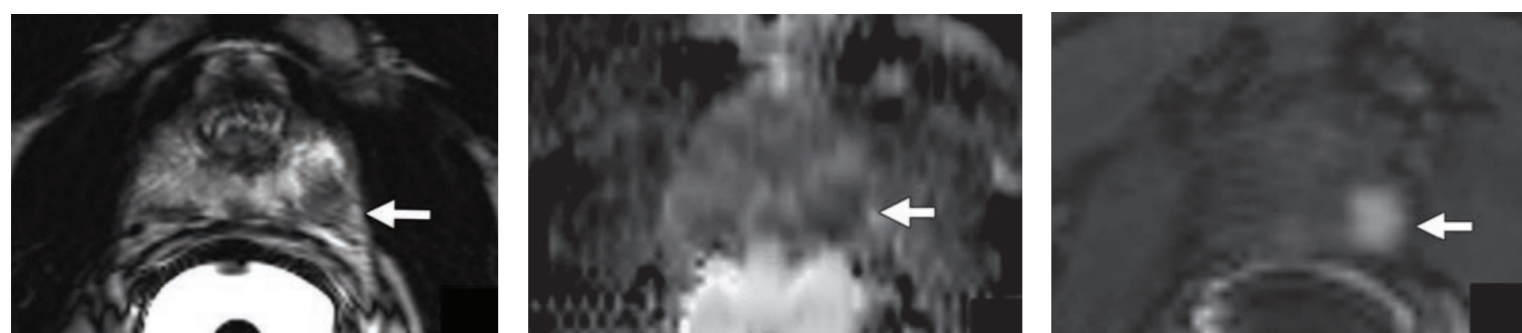
Database architecture



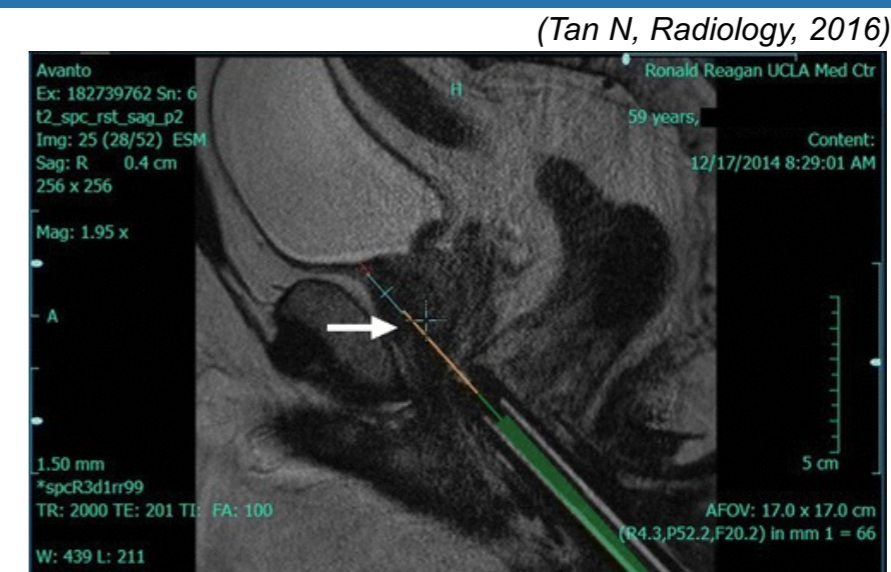
Example: IDx Prostate



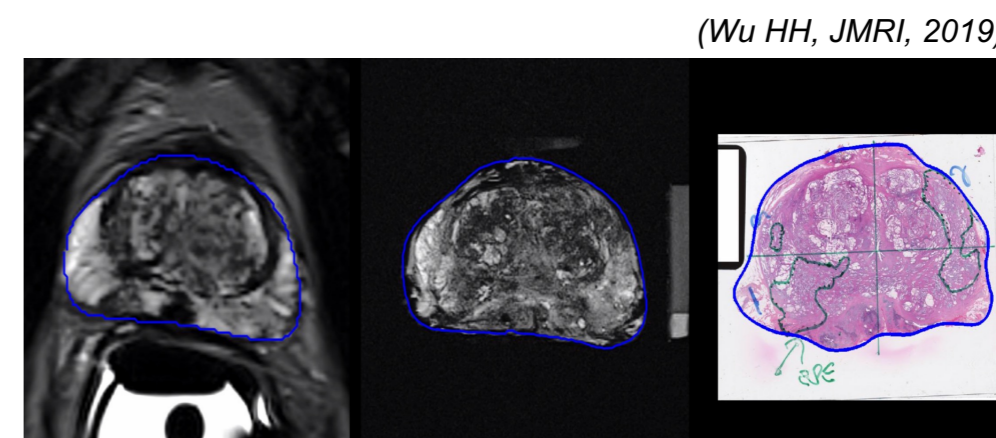
Resection cases N = 750
Archived images N = 741
Annotations N = 491



Historical mpMRI cases N = 4,071

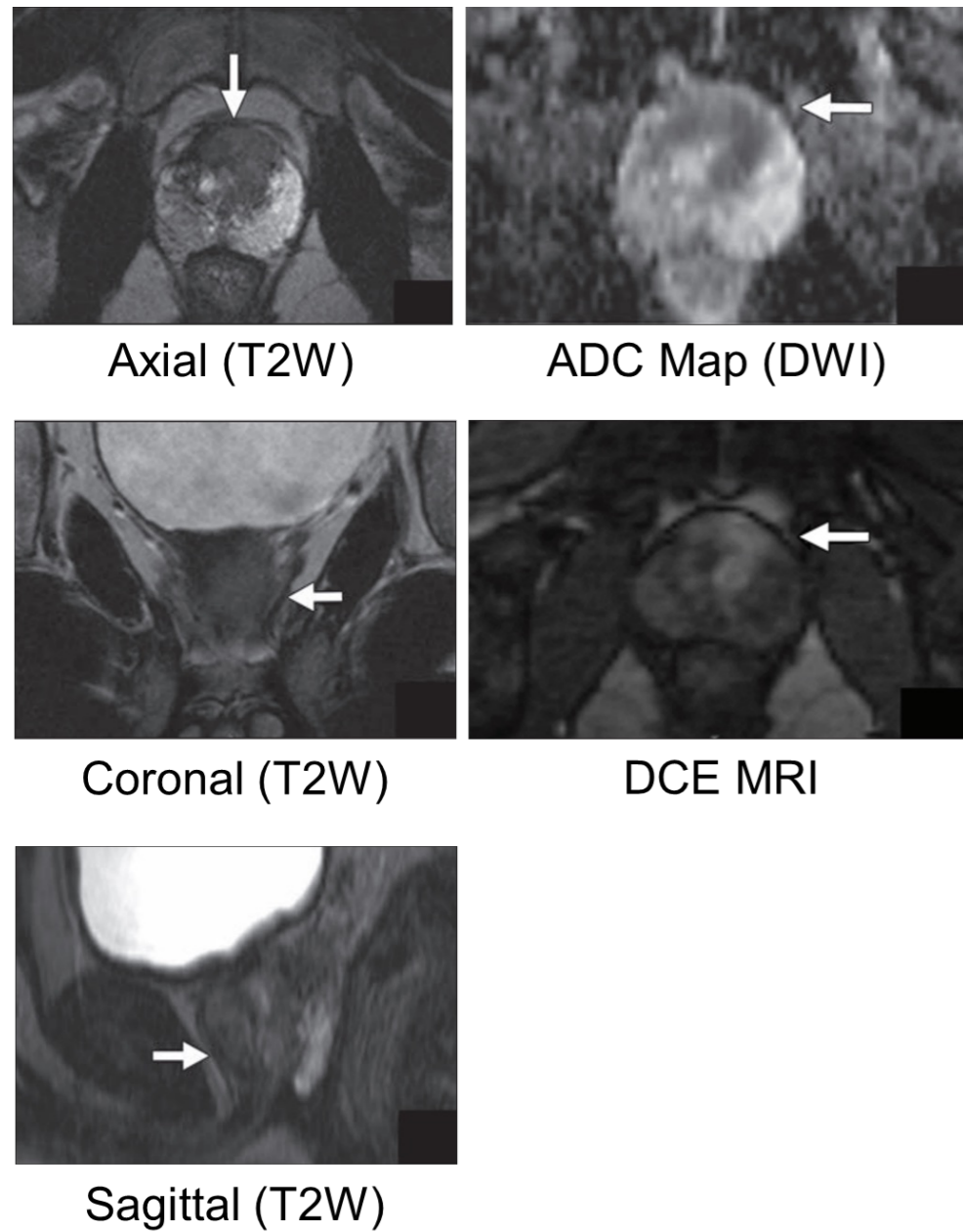


MR-guided Targeted Biopsy N = 254
Archived Images (biopsy + pre) N = 219
Annotations (pre) N = 150
Banked specimens N = 219

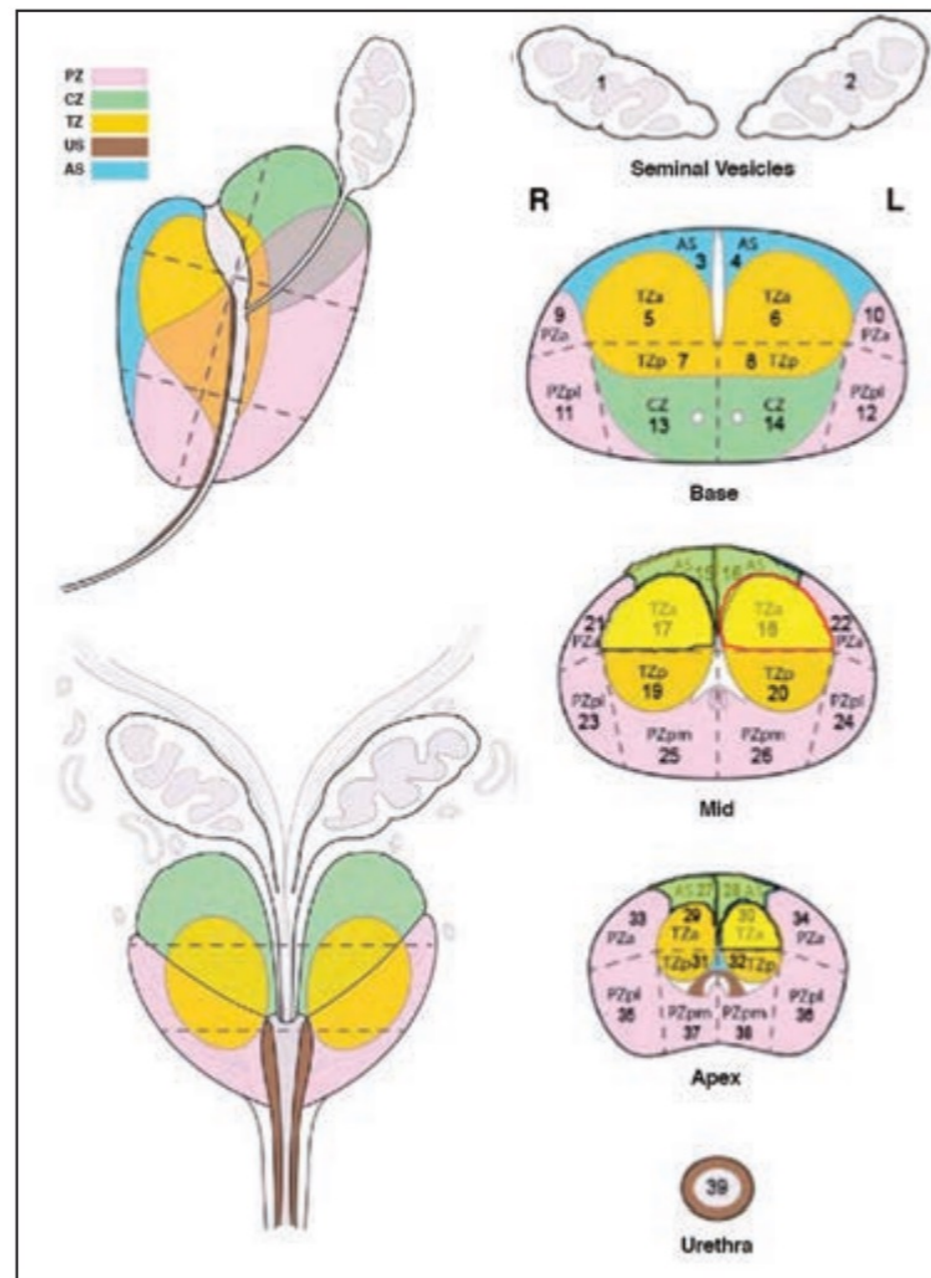


Ex vivo cases N=60+

Precise MRI to whole mount correlation



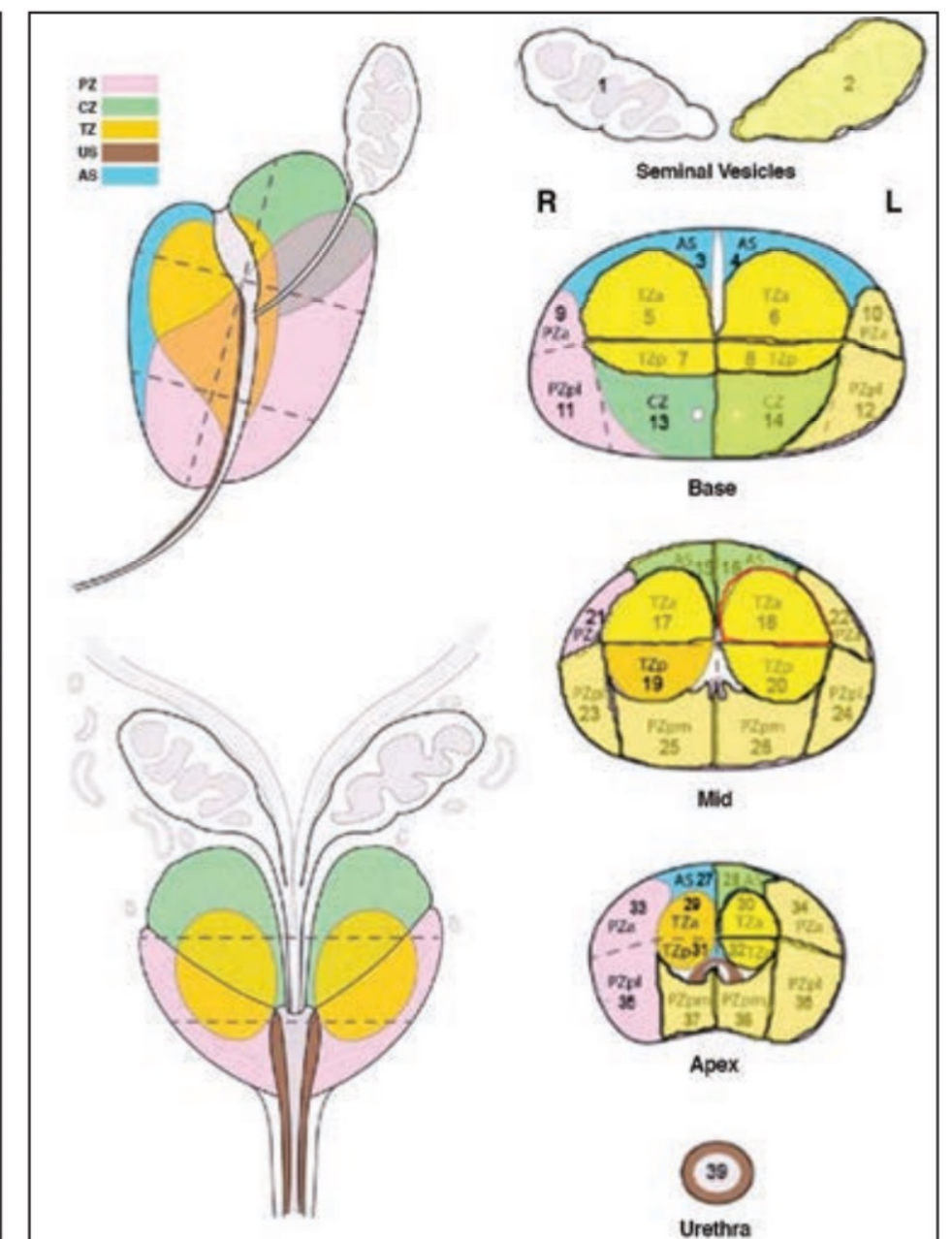
mpMRI images



Radiology Sector Map

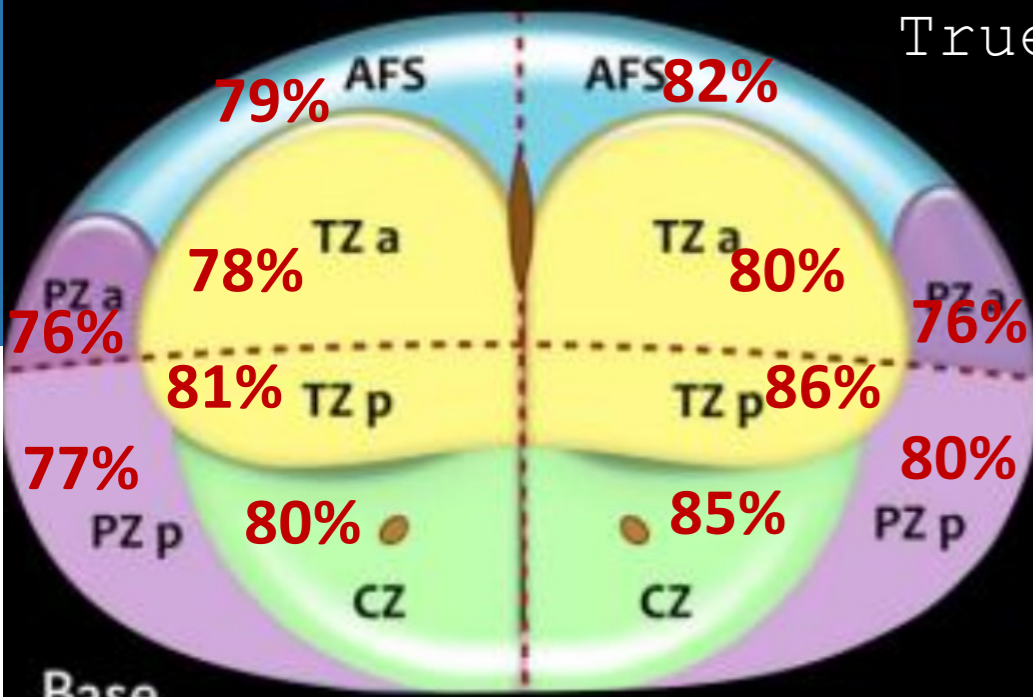


WM images

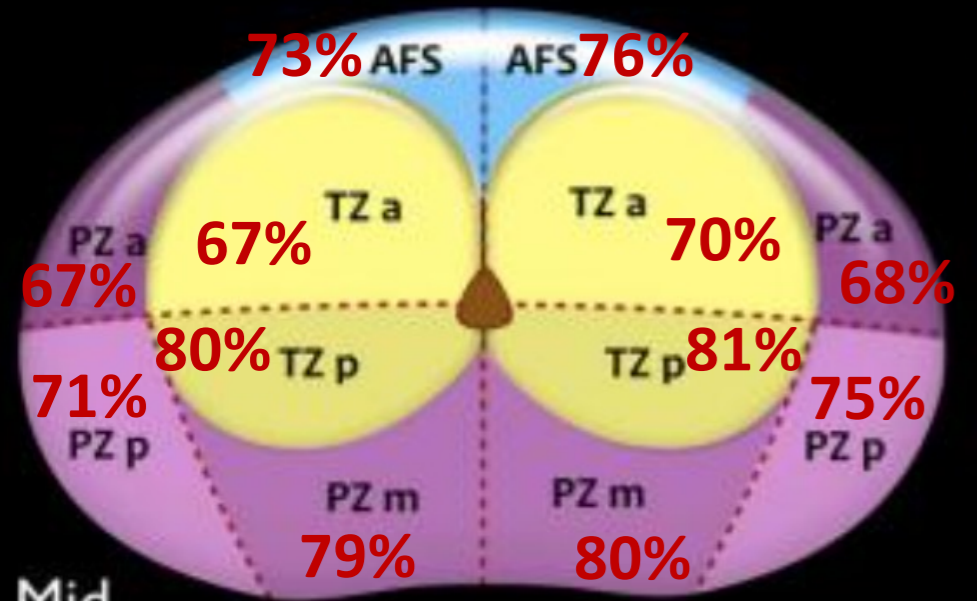


Pathology Sector Map

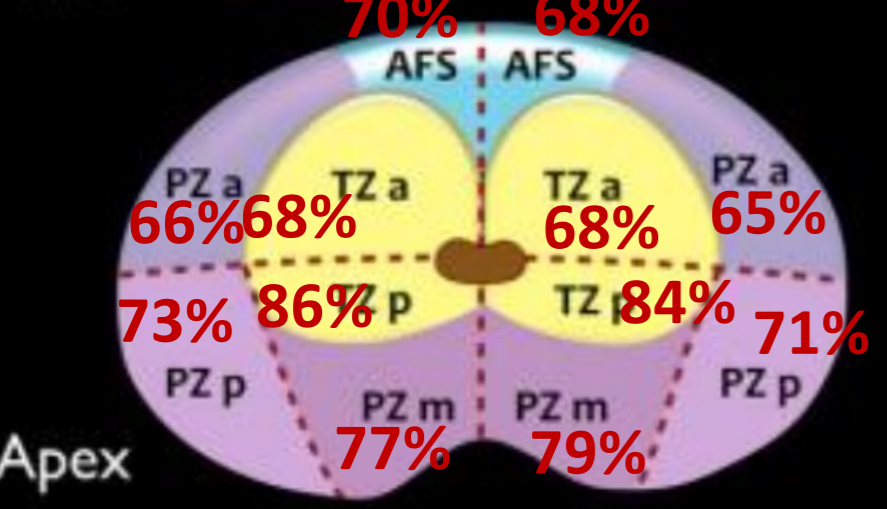
True Positive Rate



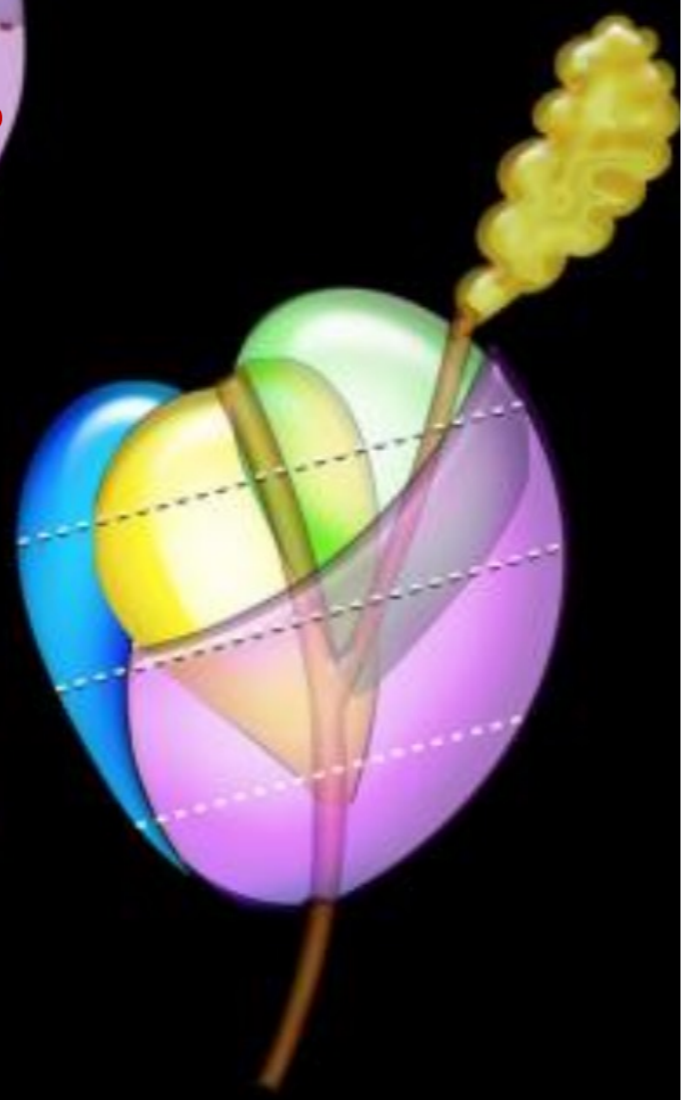
Base



Mid

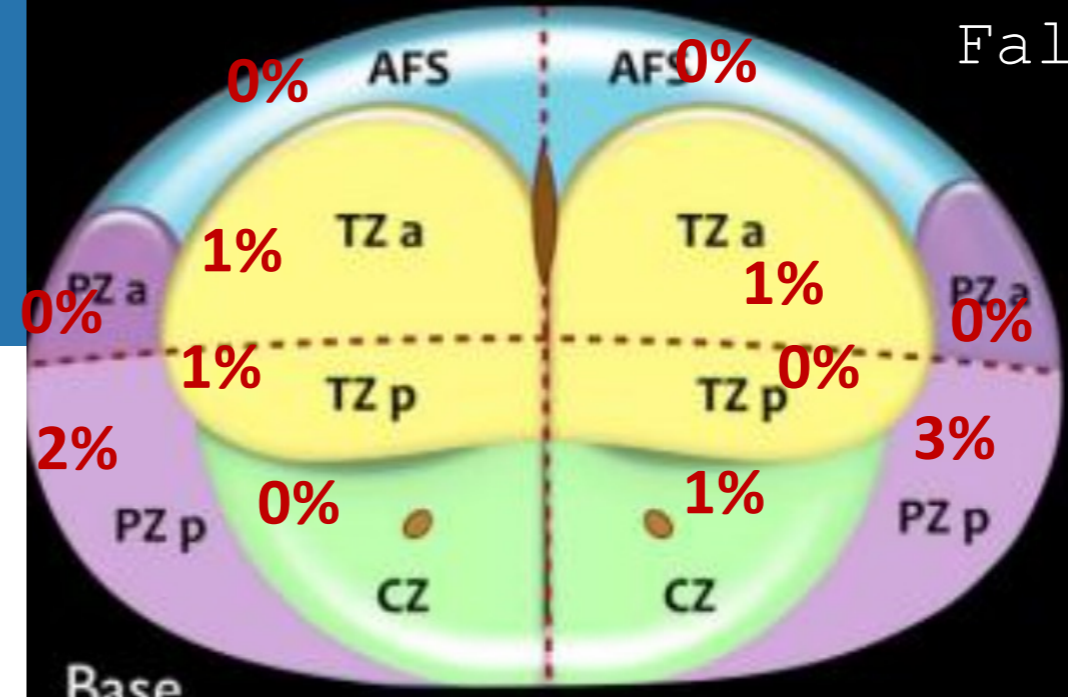


Apex

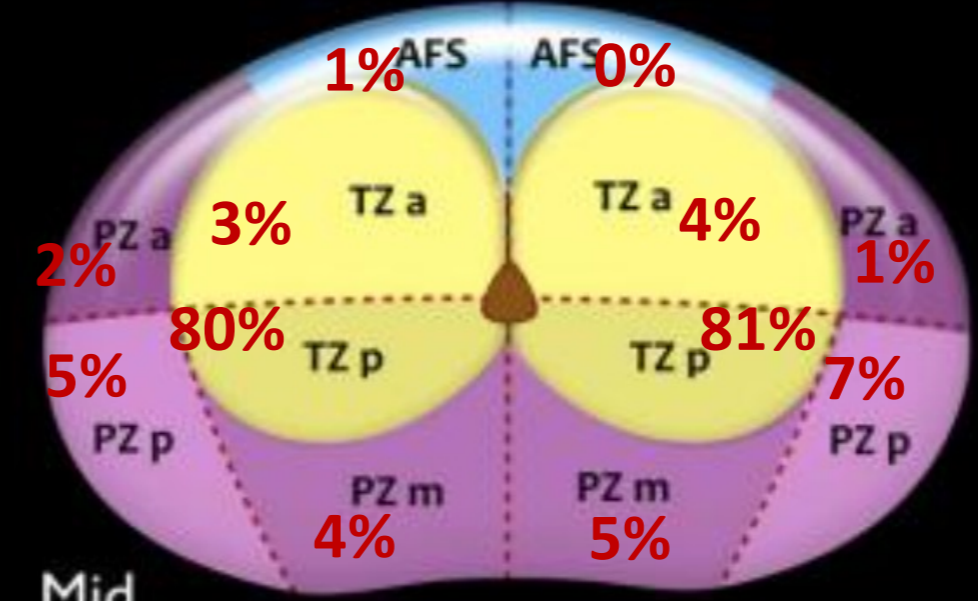


39 ROIs
Fisher's Exact test
All p<0.001

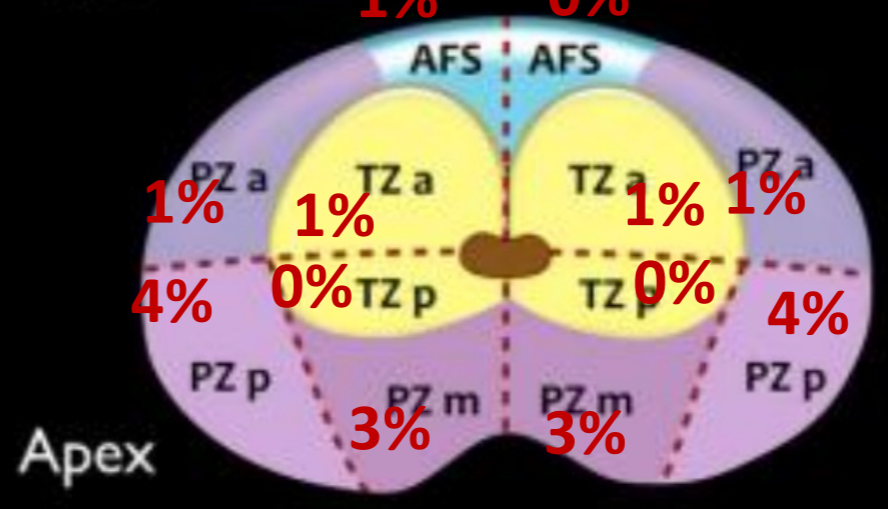
False Positive Rate



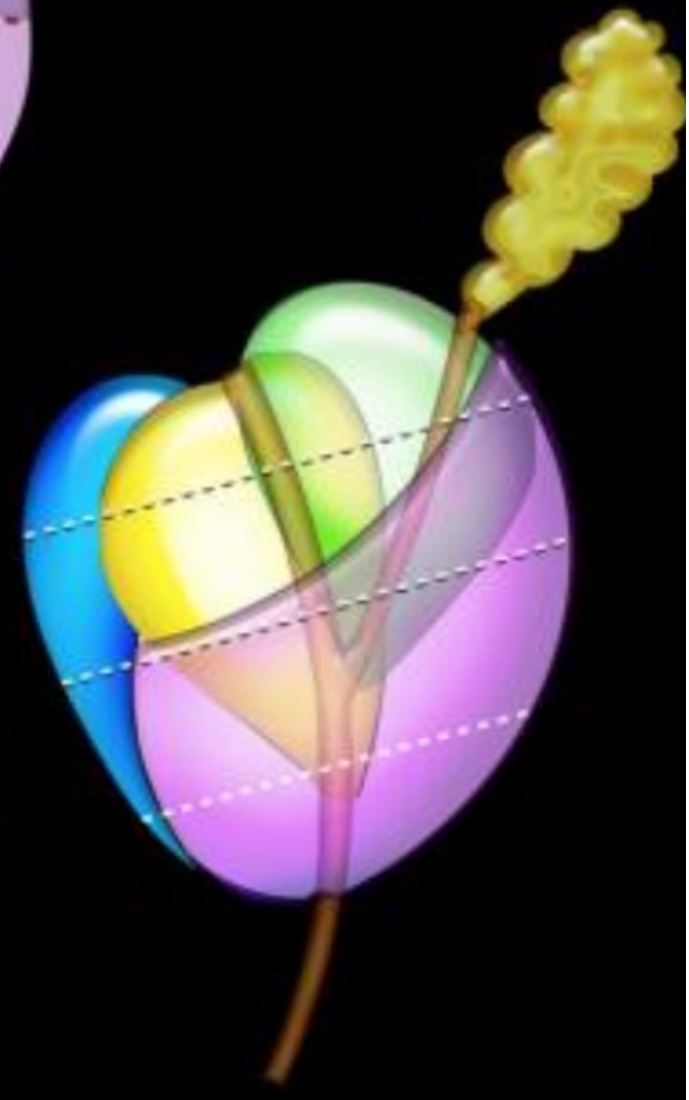
Base

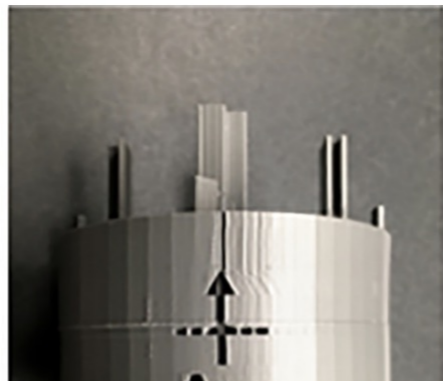
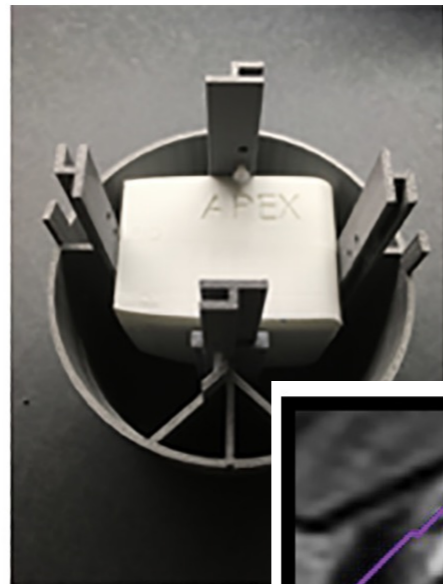
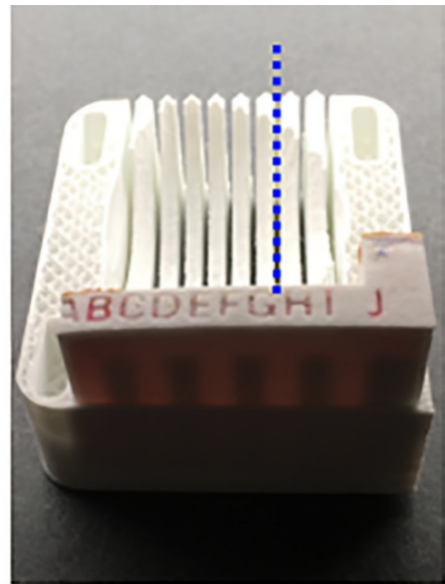


Mid



Apex

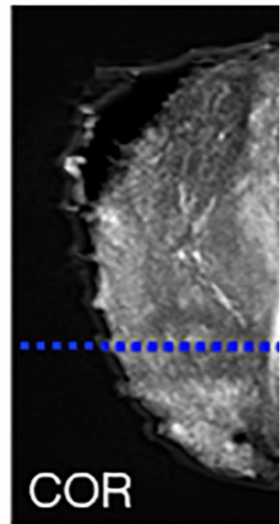




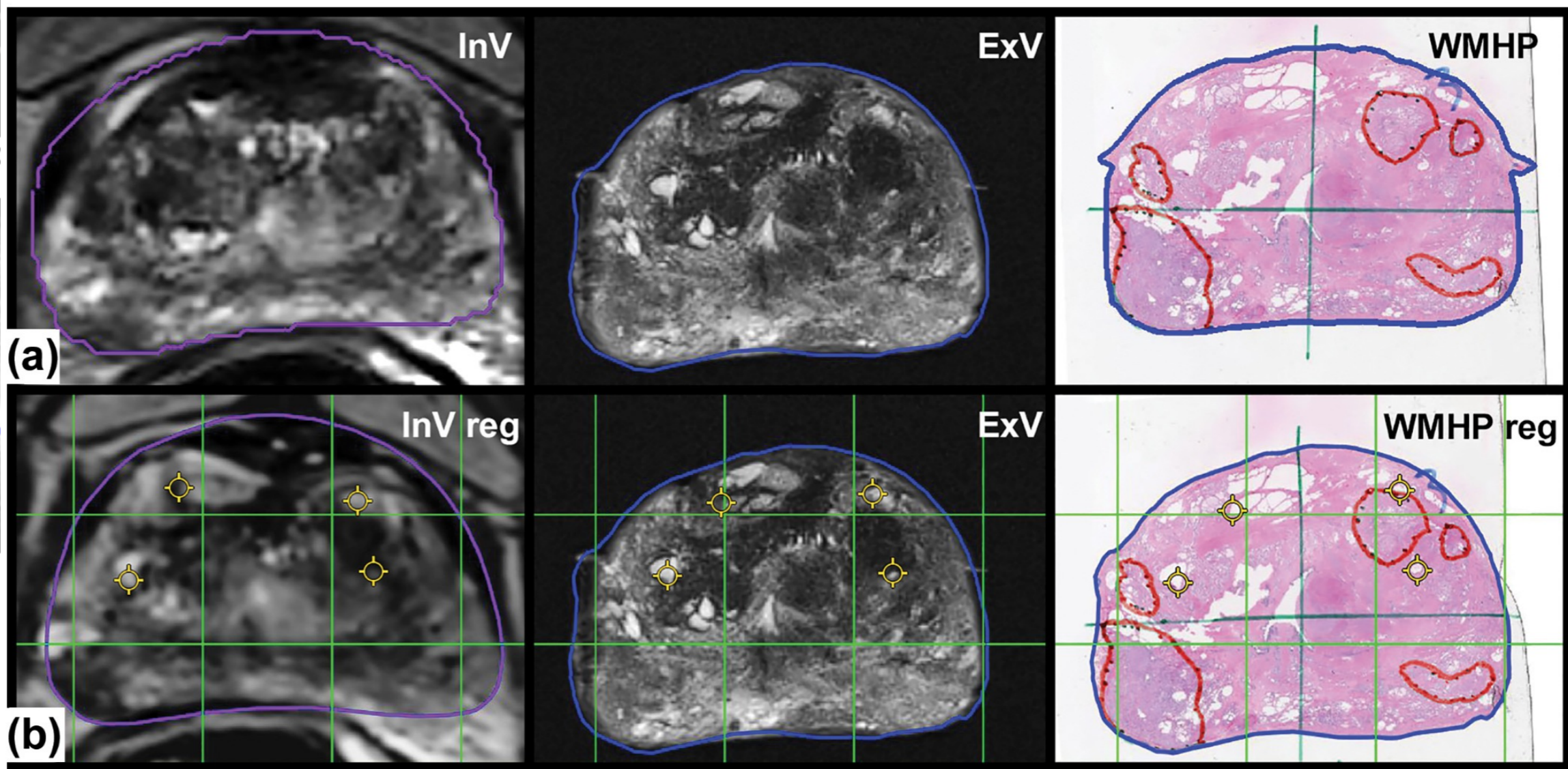
(a) Fiducials

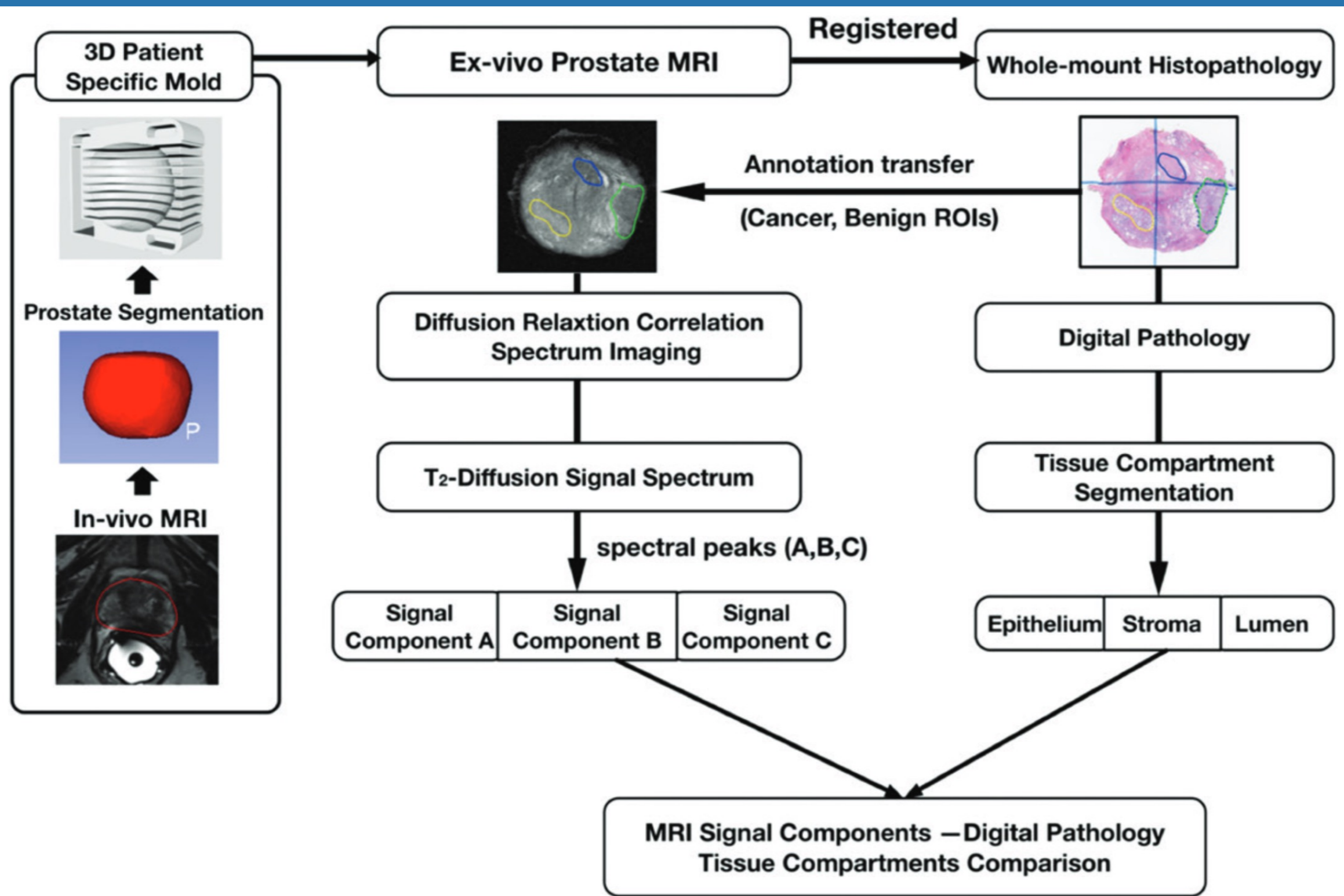
3D Mold (half)

Mold h

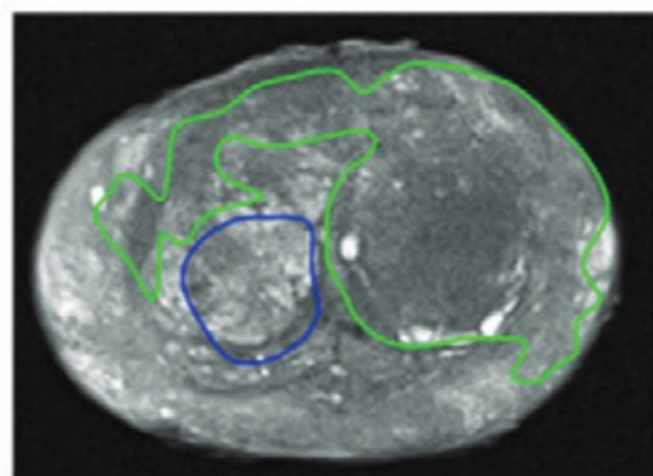


(b) 3T MRI with 15-ch knee coil

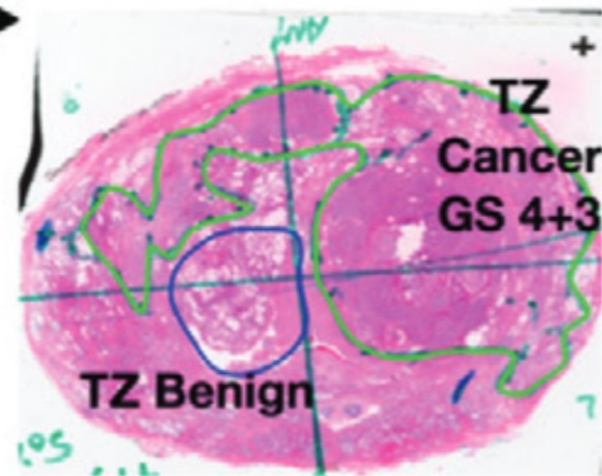




MRI

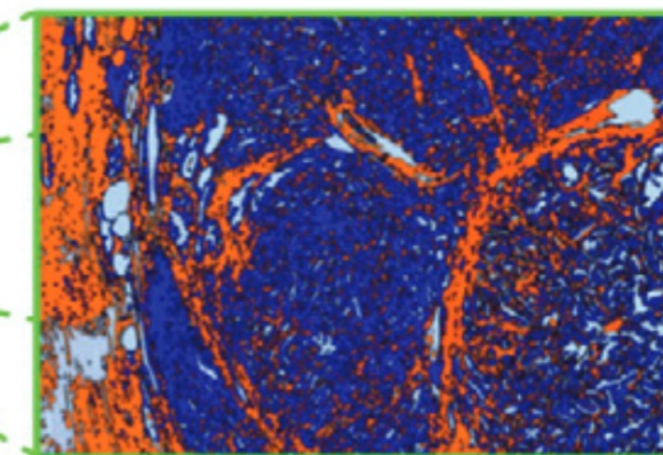
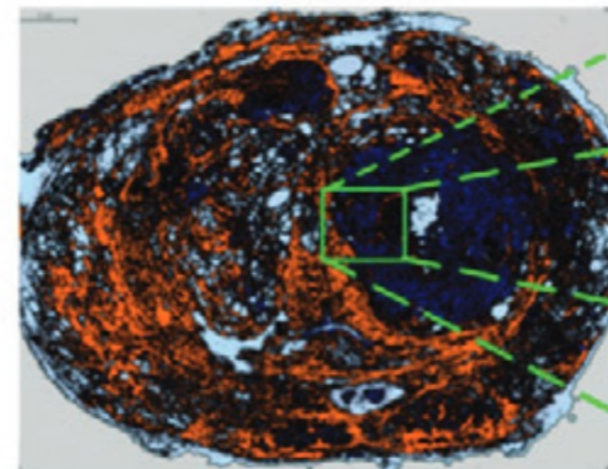


Registered



WMHP

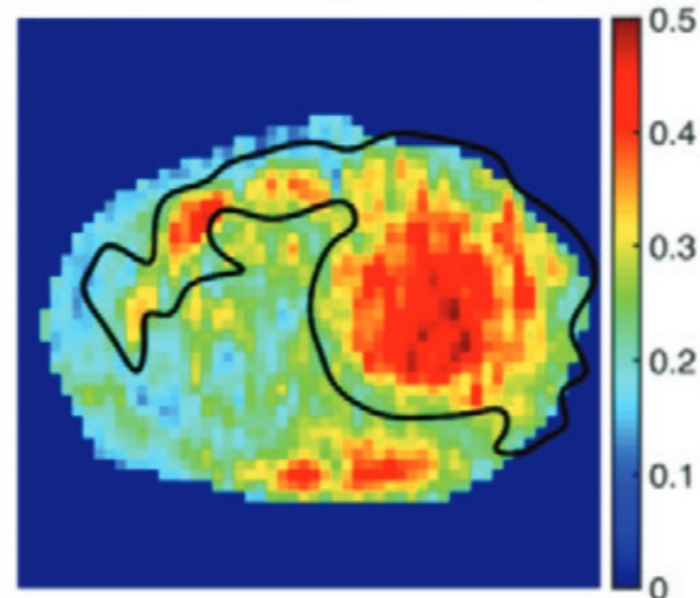
Digital Histopathology: Tissue Compartment Segmentation



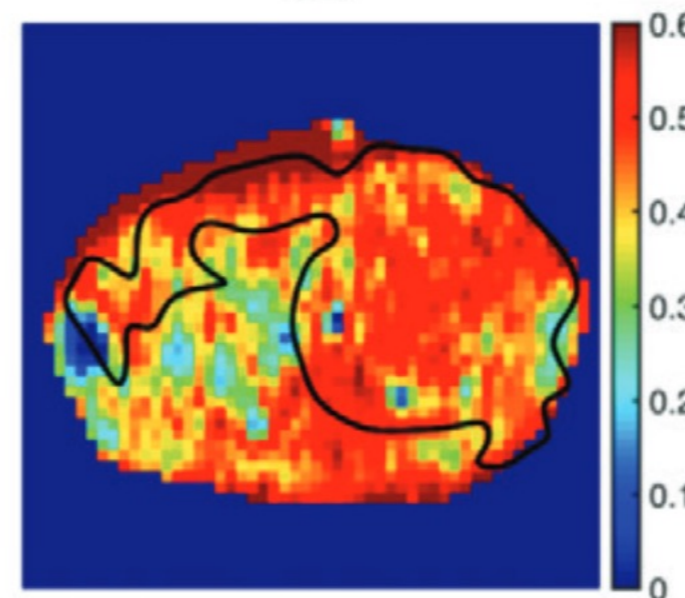
- Stroma
- Epithelium
- Lumen

DR-CSI signal component fraction maps

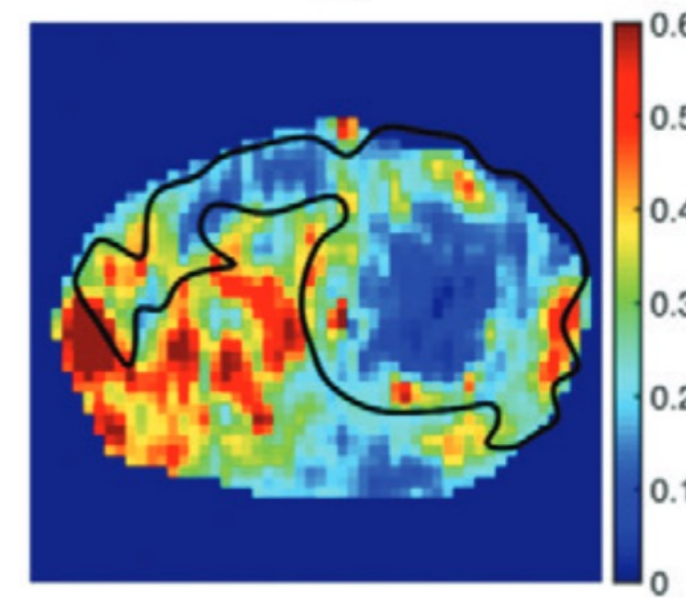
f_A



f_B

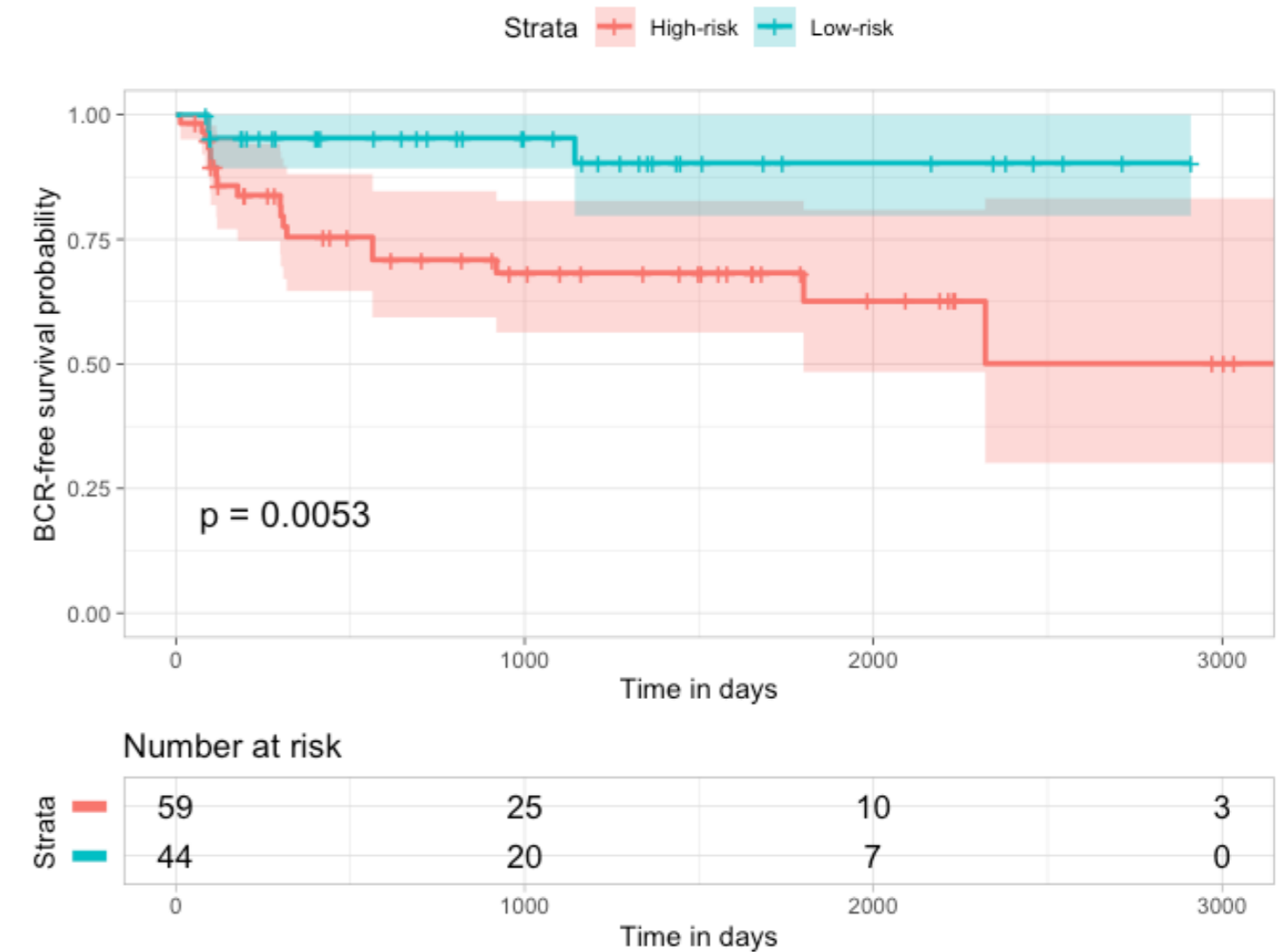
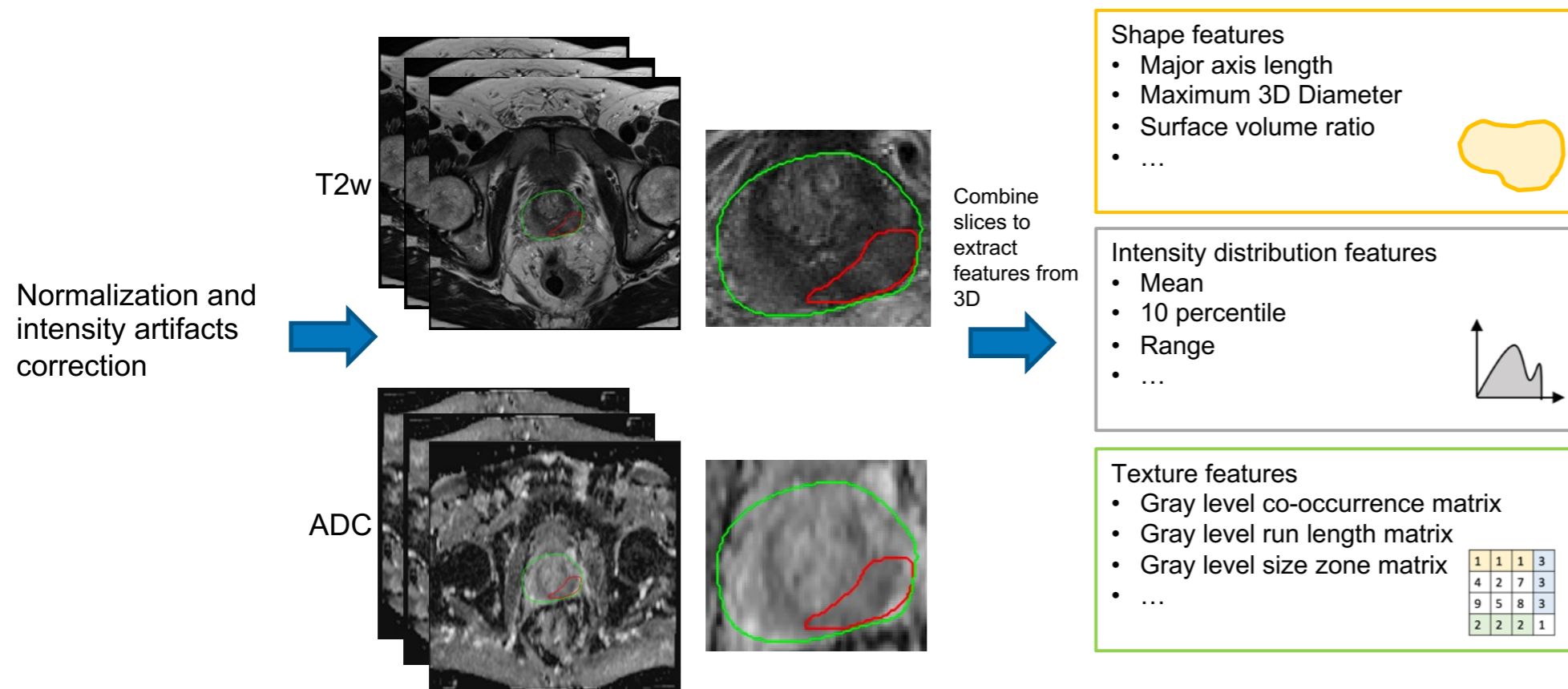


f_C



Radiomic analysis to predict outcomes

MRI slices with annotations (red: tumor; green: prostate)



Current domains

Prostate

- 960+ resection cases
- 64 ex vivo cases
- 5,000+ mpMRI cases
- 310+ MR-guided biopsies

Kidney

- 1,020+ retrospective RCC cases
- 80+ CT/US-guided biopsies

Liver

- 1,700+ ablation cases
- 110+ CT/US-guided biopsies

Lung

- 3,500+ screening cases
- 990+ CT-guided biopsies

Breast

- 240+ US-guided biopsies

Patient data



Data integration



Disease trajectory

inputs

modeling

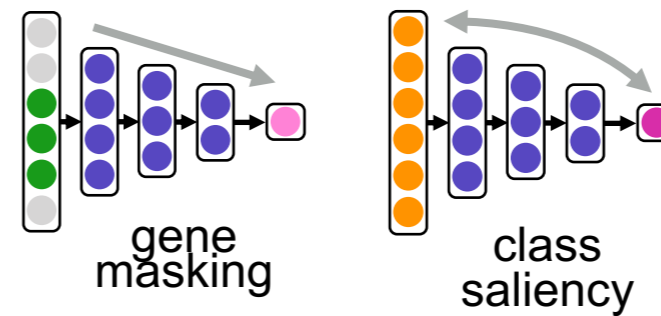
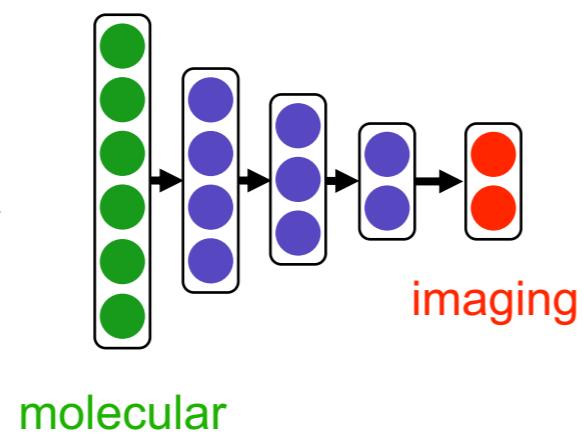
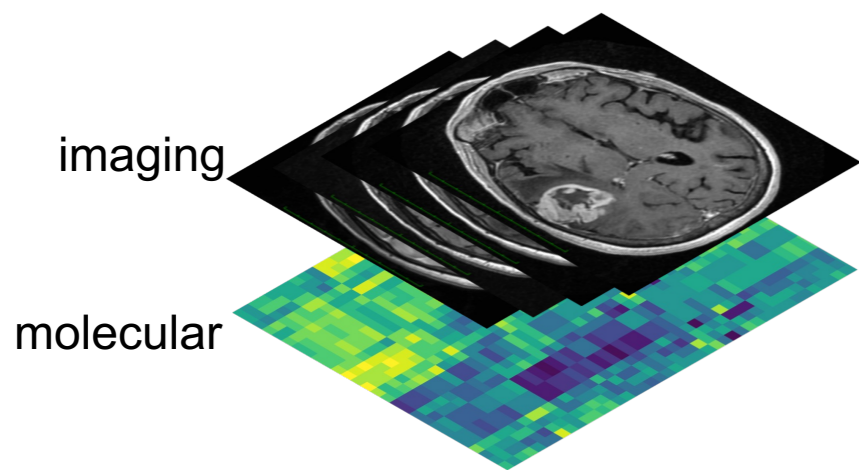
interpretation

outcomes

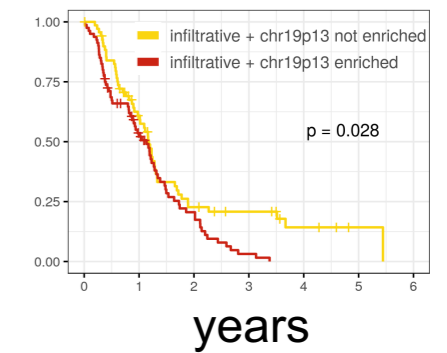
radiogenomic mapping

interpretability methods

- progression-free survival
- overall survival



probability of survival



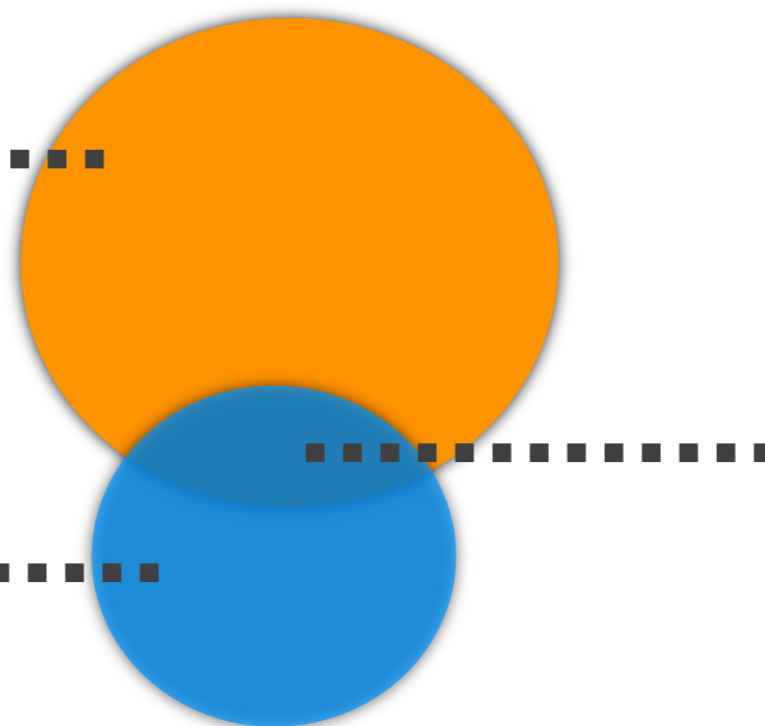
Data

The Cancer Genome Atlas (TCGA)

n = 528 GBM patients
microarray
untreated, primary tumors

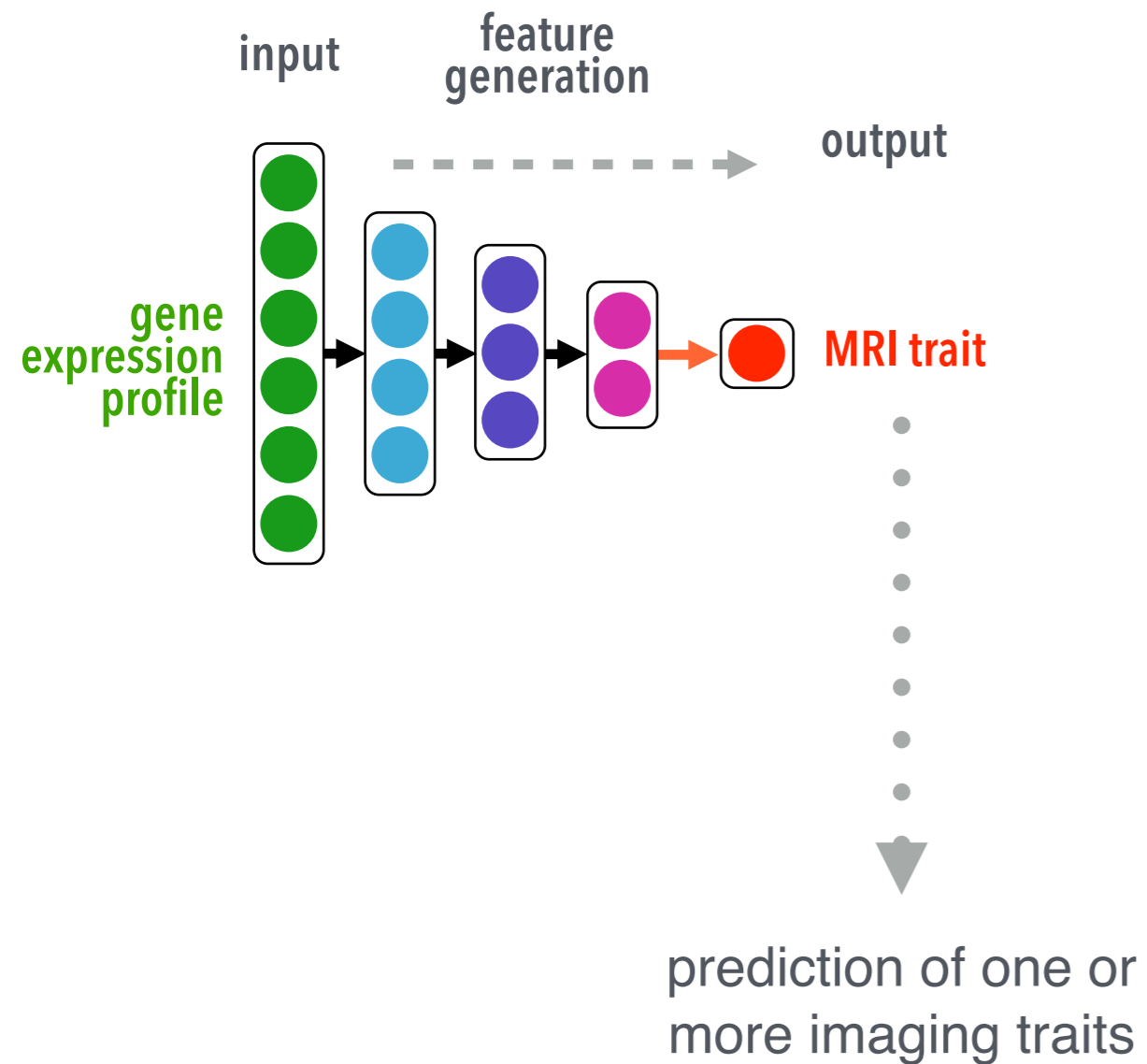
The Cancer Imaging Archive (TCIA)

n = 262 GBM patients
multiple image modalities



- n = 109 paired, radiogenomic samples
- gene expression profile *and* pre-operative MR imaging

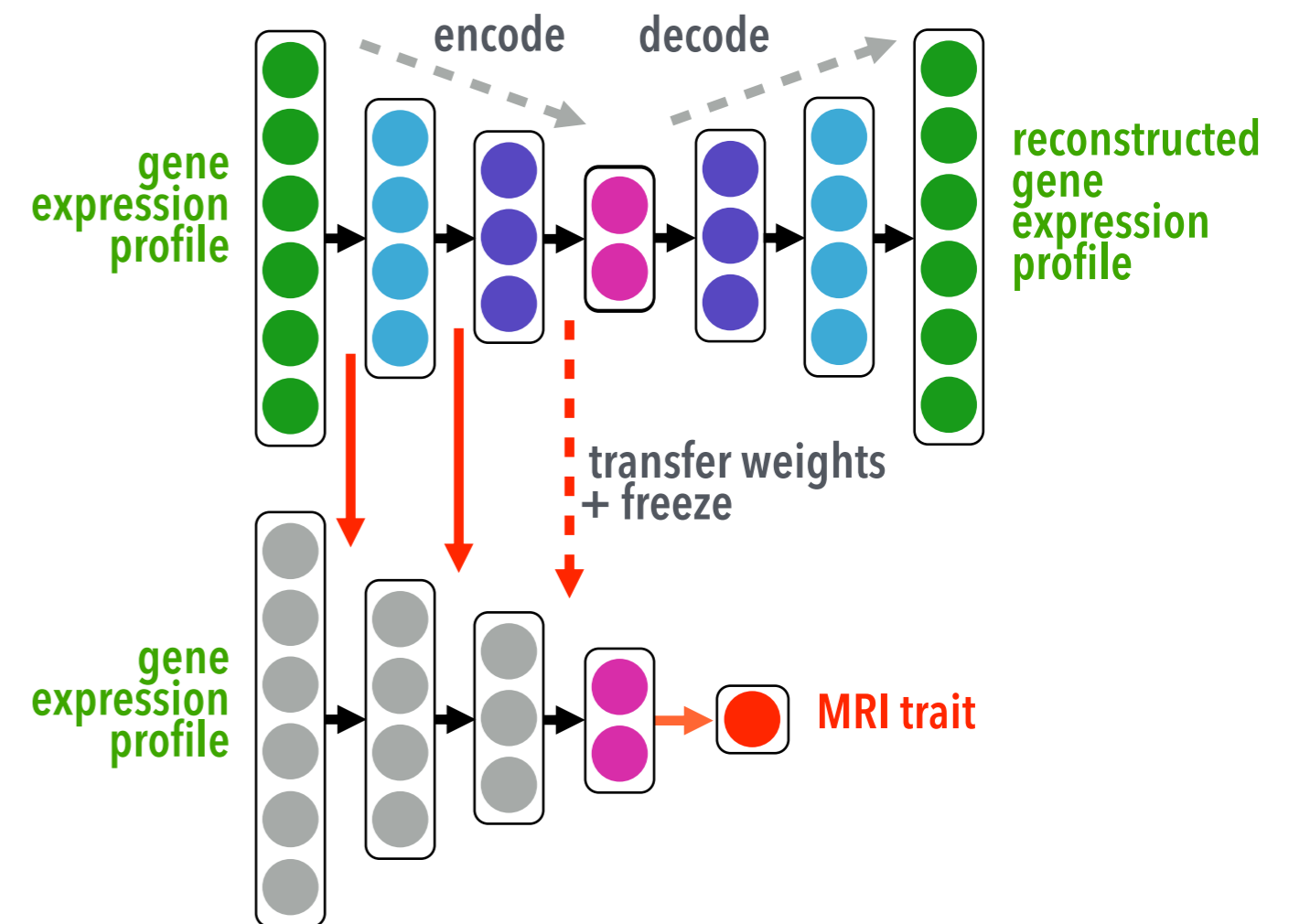
Radiogenomic neural network

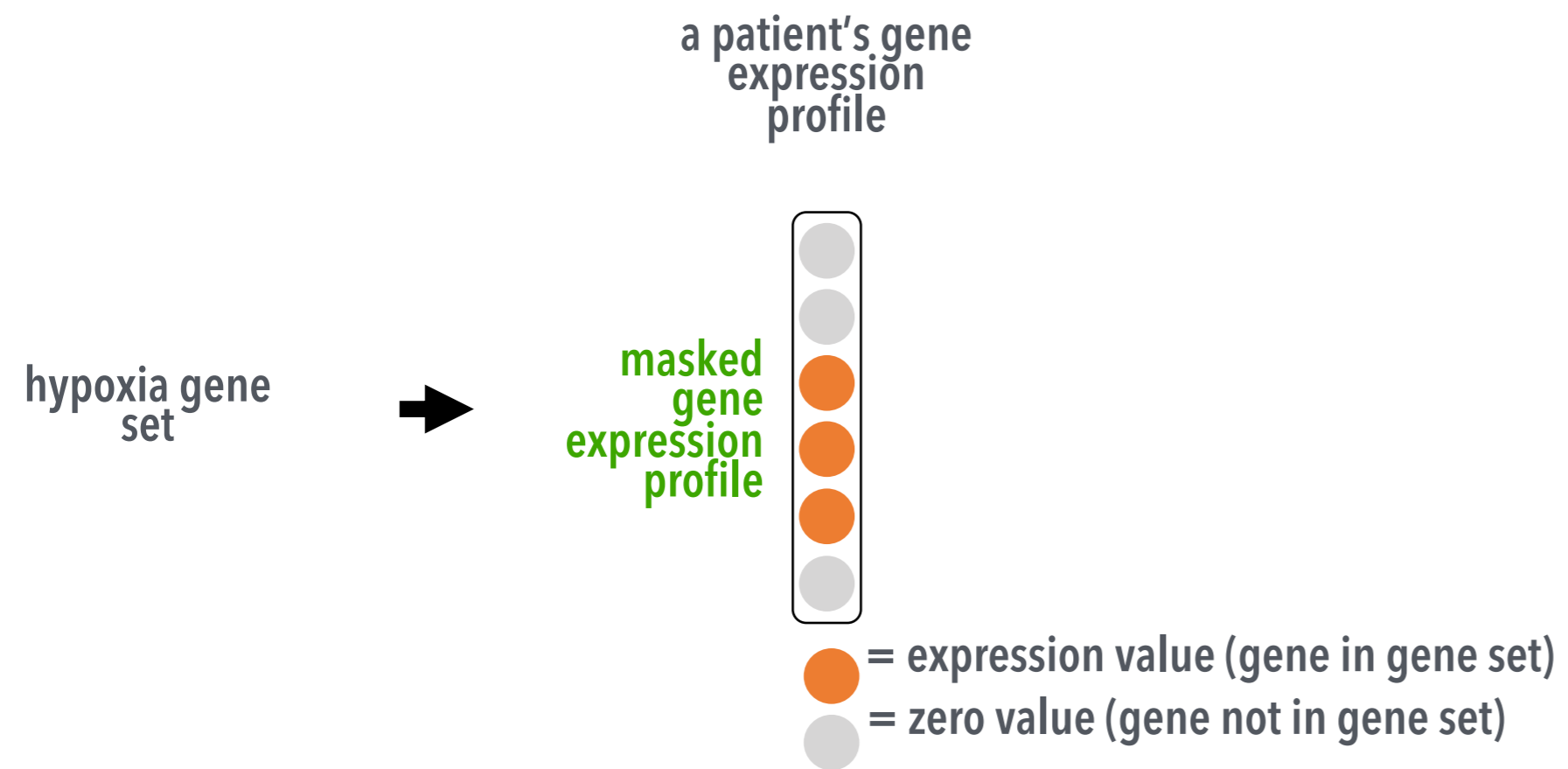


Training:

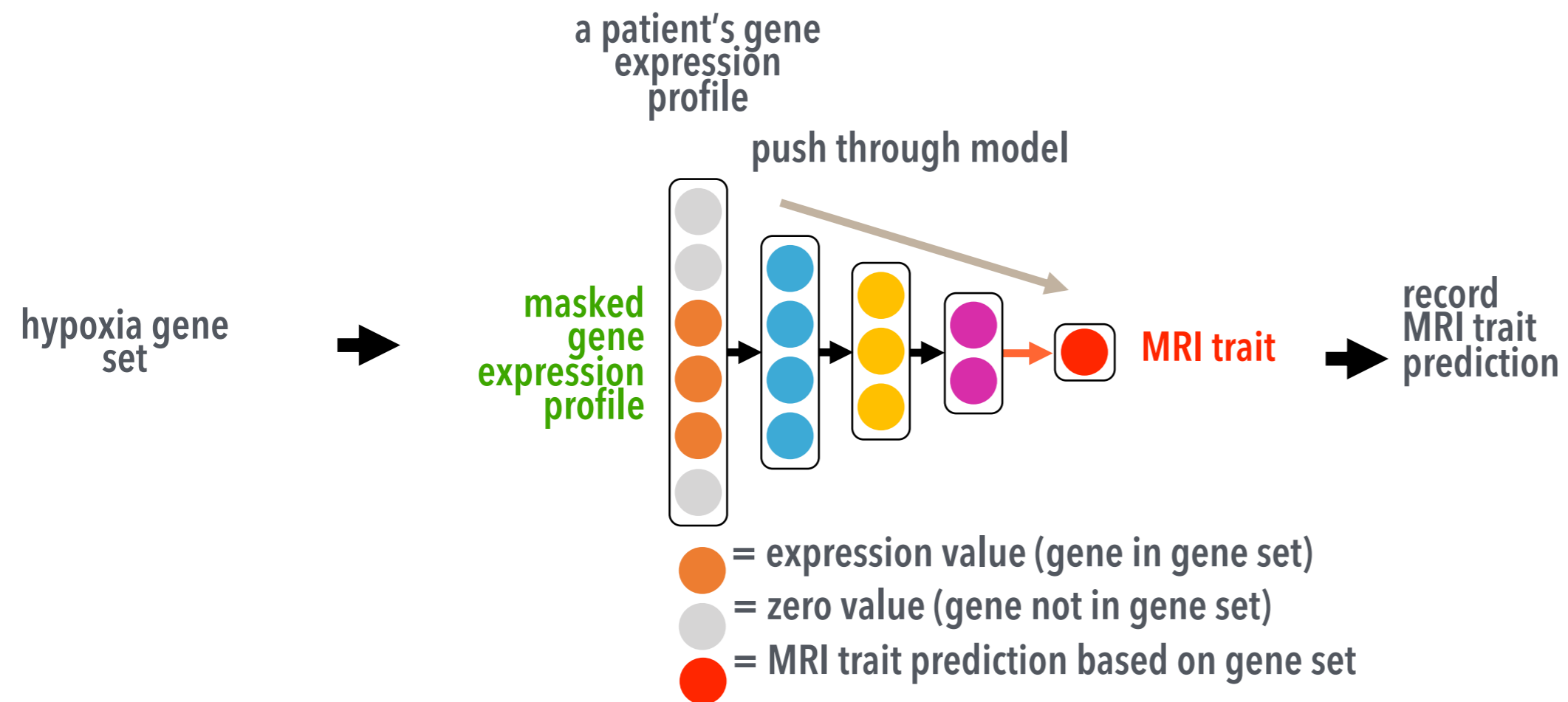
transcriptomic autoencoder

fine tune radiogenomic model

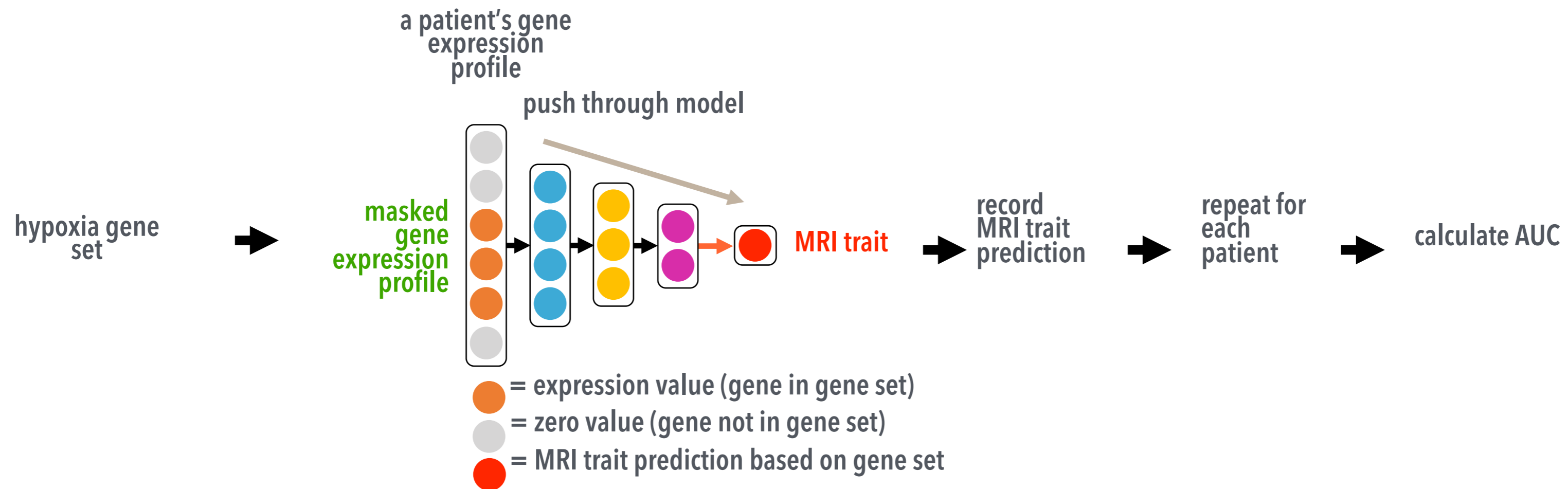




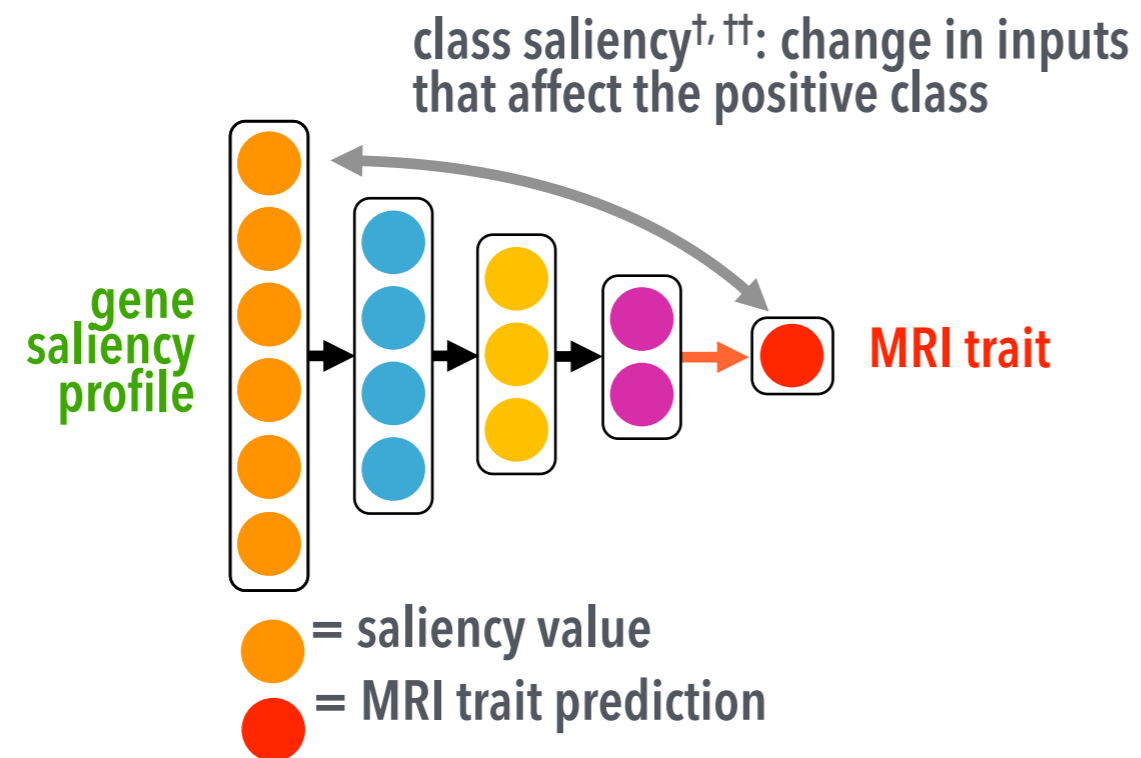
- mask the input



- mask the input
- measure the output



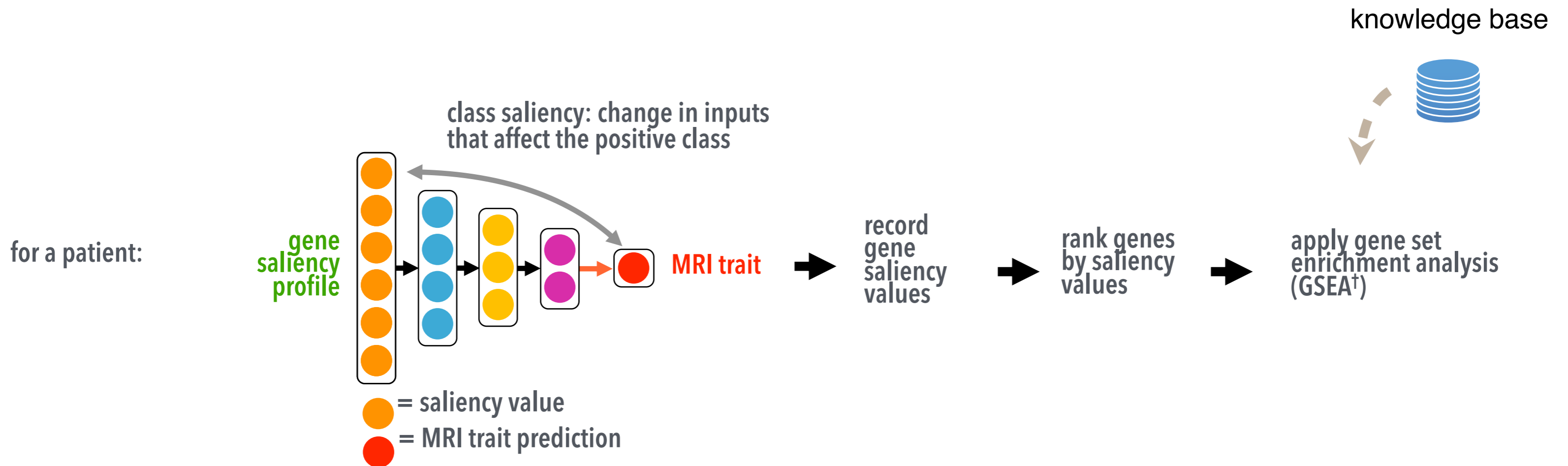
- measures performance of model when only using genes from a gene set
- use AUC as strength of association



- attach weights to genes based on their importance in predicting a class label

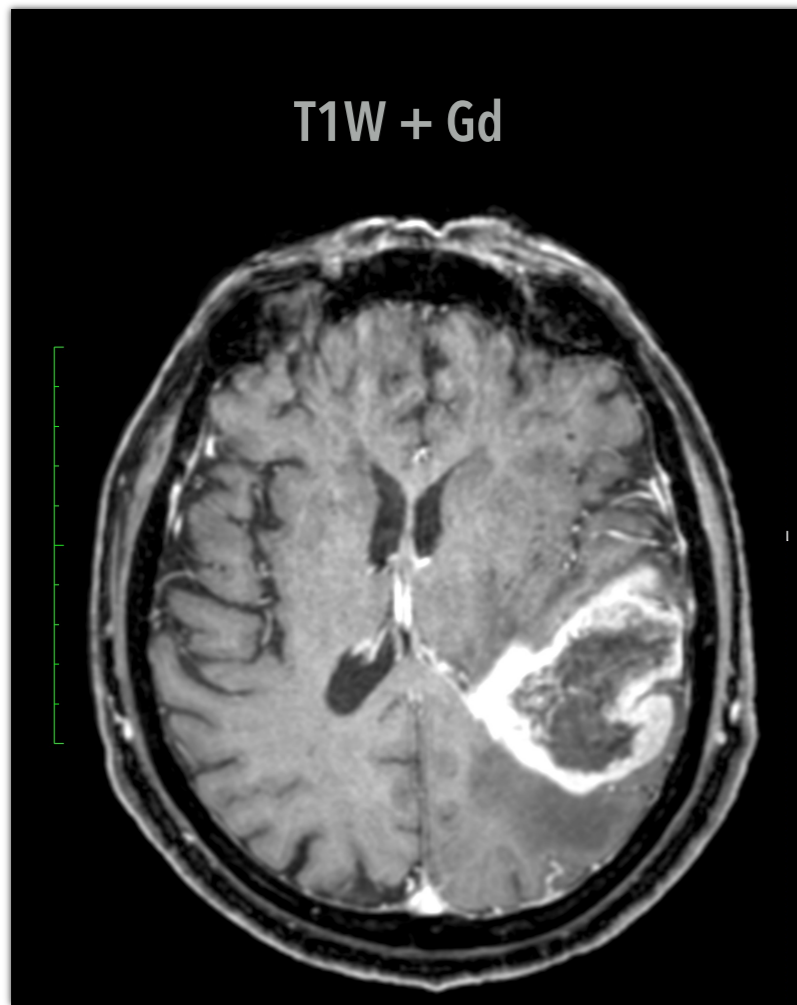
[†] Simonyan, Karen, Andrea Vedaldi, and Andrew Zisserman. "Deep inside convolutional networks: Visualising image classification models and saliency maps." *arXiv preprint* (2013)

^{††} Kotikalapudi, Raghavendra, et al. "keras-vis." (2017)



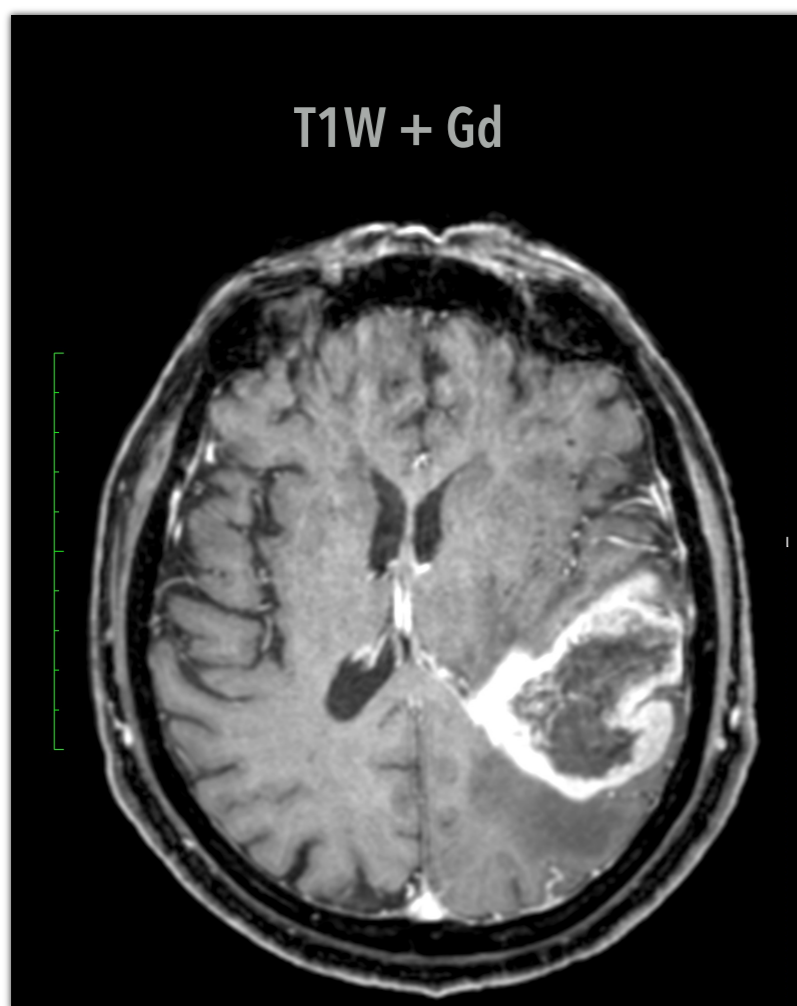
- attach weights to genes based on their importance in predicting a class label
- use of GSEA to determine what gene sets (pathways, biological processes etc.) were at the top of ranked genes

Model interpretation using gene masking



- high grade, aggressive tumor
- abnormal, leaky blood vessels
- disrupted blood-brain barrier

Model interpretation using gene masking



- high grade, aggressive tumor
- abnormal, leaky blood vessels
- disrupted blood-brain barrier

transcriptomic drivers					
MRI trait	theme	gene set (collection*, query†)	AUC	AP	see also
enhancing	growth/death	growth (GO, <i>PTEN</i>)	0.86	0.84	
		sensory organ development (GO, <i>EGFR</i> , <i>KCNK3</i>)	0.85	0.84	[JDB14, GCH13]
	immune system	IL2/STAT5 signaling (H)	0.77	0.76	
		complement system (H)	0.79	0.75	
		activation of immune response (GO, <i>PTEN</i>)	0.90	0.89	
		leukocyte & lymphocyte activation (GO, <i>PIK3R1</i>)	0.86, 0.85	0.85, 0.83	
	hormones	immune effector process (GO, <i>PIK3CA</i>)	0.87	0.84	
		early & late responses to estrogen (H)	0.79, 0.78	0.73, 0.73	
		response to steroid hormone (GO, <i>RBI</i>)	0.88	0.88	
	ECM	regulation of hormone levels (GO, <i>PARK2</i>)	0.87	0.84	
related to ECM proteins (C, ECM)		0.77–0.84	0.73–0.76	[DNW08]	
vasculature	apical junction (H)	0.80	0.75		
	heme metabolism (H)	0.77	0.65		
kinases activity	multiple (GO, <i>EGFR</i> , <i>LTBP1</i>)	vasculature & heart development (GO, <i>LTBP1</i>)	0.81, 0.78	0.80, 0.77	[JDB14]
		all 0.87	all 0.85	[JDB14, GCH13]	

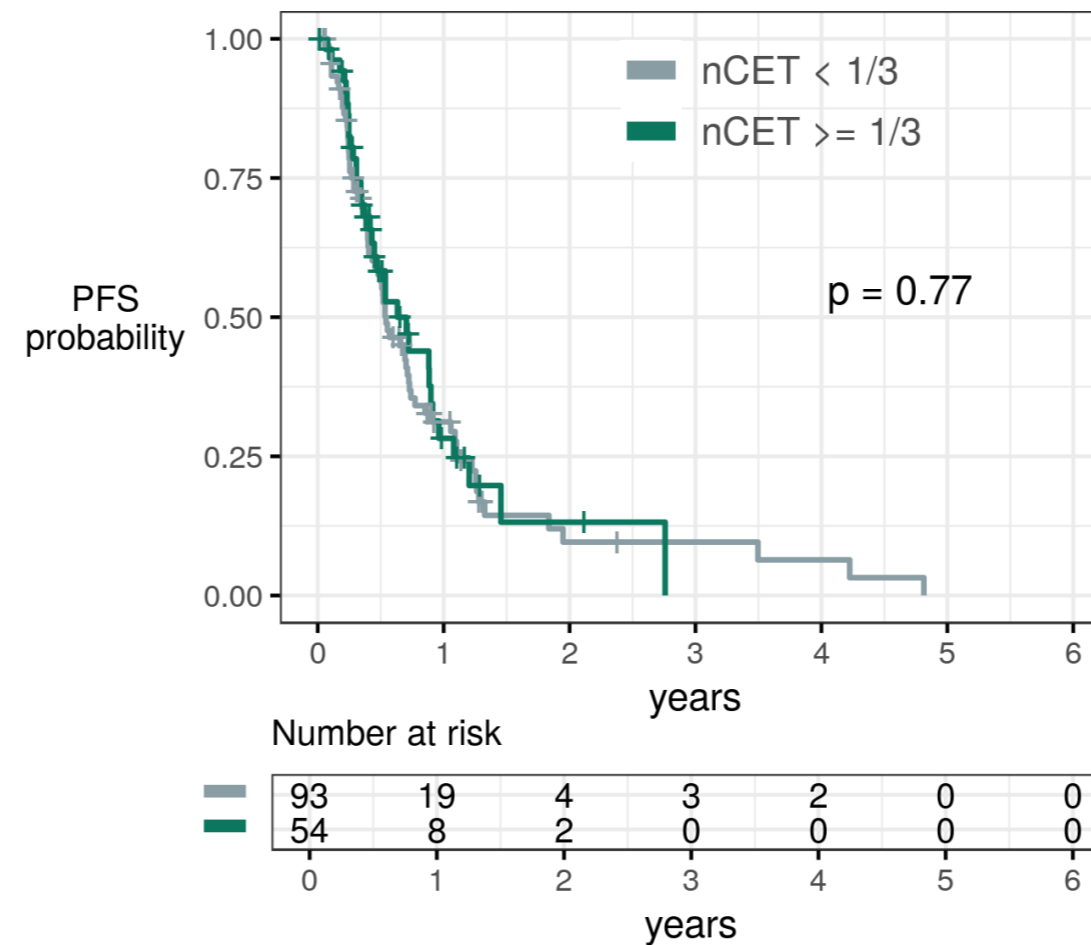
- identified the most predictive gene sets
- gene sets are related to growth, vasculature, immune system processes, and involved *EGFR*
- gene sets associated with prior radiogenomic work
- repeated analysis for all VASARI traits

Using class saliency to predict progression

- identify radiogenomic traits using class saliency
- Kaplan Meier survival curves
- **radiogenomic traits were able to differentiate progression free survival better than imaging traits alone**

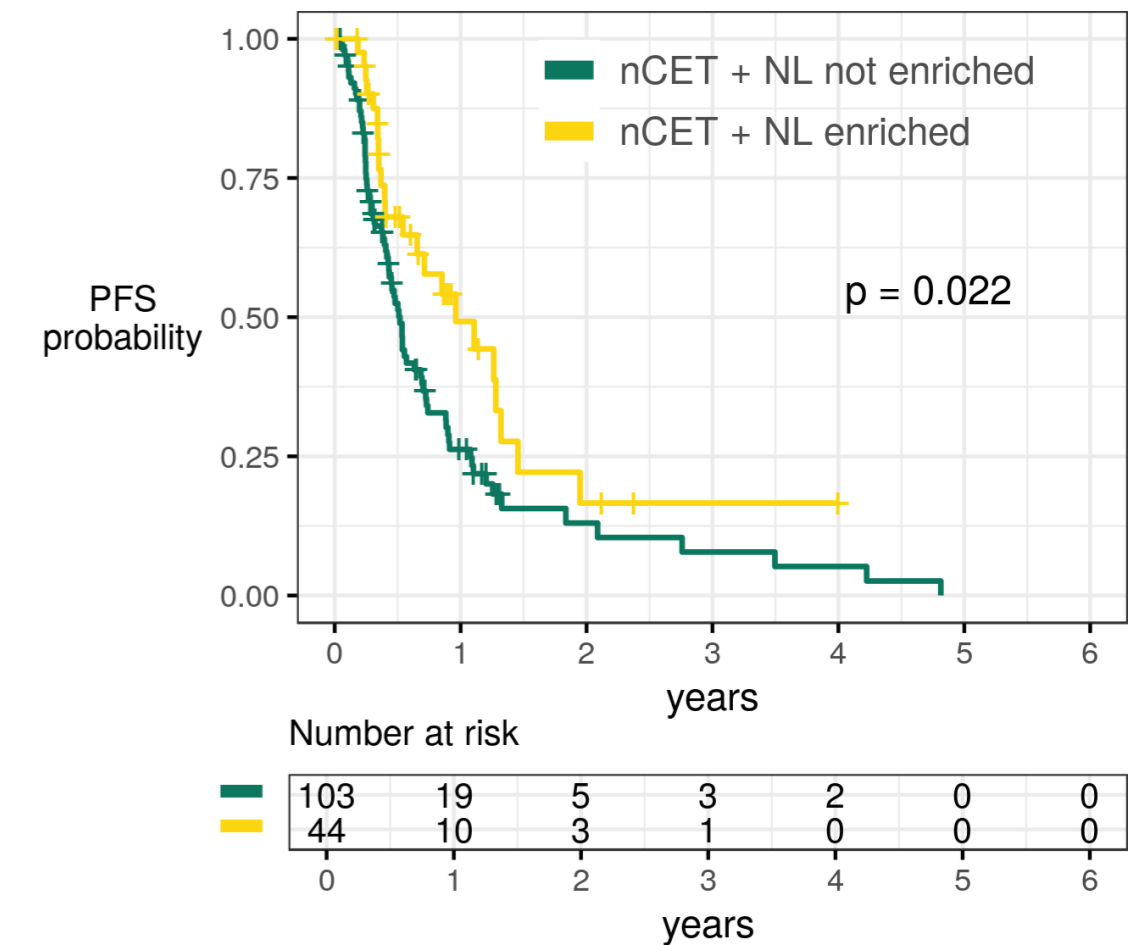
imaging trait

proportion of non-contrast enhancing tumor (nCET)



radiogenomic trait

prediction of nCET involved neural (NL) subtype genes



Concluding thoughts (1/2)

- A lot of biological information can be extracted from MRI
 - Incorporating information across biological scales and modalities can lead to improved predictions of prognosis and treatment response
- Different modalities carry different kinds of information
- Optimal techniques for normalization, registration, and fusion are open challenges
 - Driven by the increasing availability of multimodal datasets
 - Need high quality annotations and data collection workflows
- Need better model validation tools
 - Further investigation into how multi-modal features relate, model interpretability

Concluding thoughts (2/2)

- Desiderata of a good multimodal learning model (Srivastava and Salakhutdinov)
 - Similarity in the representation space implies similarity of the corresponding concepts
 - Robust to missing information / fill-in missing modalities given observed ones
- Need better model validation tools
 - Further investigation into how multi-modal features relate, model interpretability
- Additional resources
 - Survey and taxonomy of multimodal learning (Baltrusaitis et al, <https://doi.org/10.1109/TPAMI.2018.2798607>)
 - Recent special issue on multimodal data fusion in IEEE Journal of Biomedical and Health Informatics
<https://ieeexplore.ieee.org/xpl/tocresult.jsp?isnumber=8949677>

Thank you



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